

Chemically modified plastic tube for high volume removal and collection of circulating tumor cells

In this preliminary effort, we use a commercially available and chemically modified tube to selectively capture circulating tumor cells (CTCs) from the blood stream by immobilizing human anti-EpCAM antibodies on the tube's interior surface. We describe the steps required to modify a tube into a cancer cell capturing device. Using these simple modifications, at this proof-of-concept stage of development, we were able to capture about 85% of cancer cells from suspension and 44% of cancer cells from spiked whole blood, the capture percentage being dependent on the tube's length and the number of cancer cells present. Previous work by other researchers has focused on extracting small blood volumes and capturing CTCs with complicated micro-fluidic devices for diagnostic purposes. In addition, prior results of other researchers point to a possible reduction in metastasis achieved by removing CTCs from the bloodstream. We believe that with the utilization of appropriate tube lengths and procedures, we can ensure capture and removal of nearly the entire CTC population in whole blood. Following whole blood flow through the tube, the tube can be trypsinized to release the captured live CTCs for further analysis and testing.

Chemically modified plastic tube for high volume removal and collection of circulating tumor cells.

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Abstract

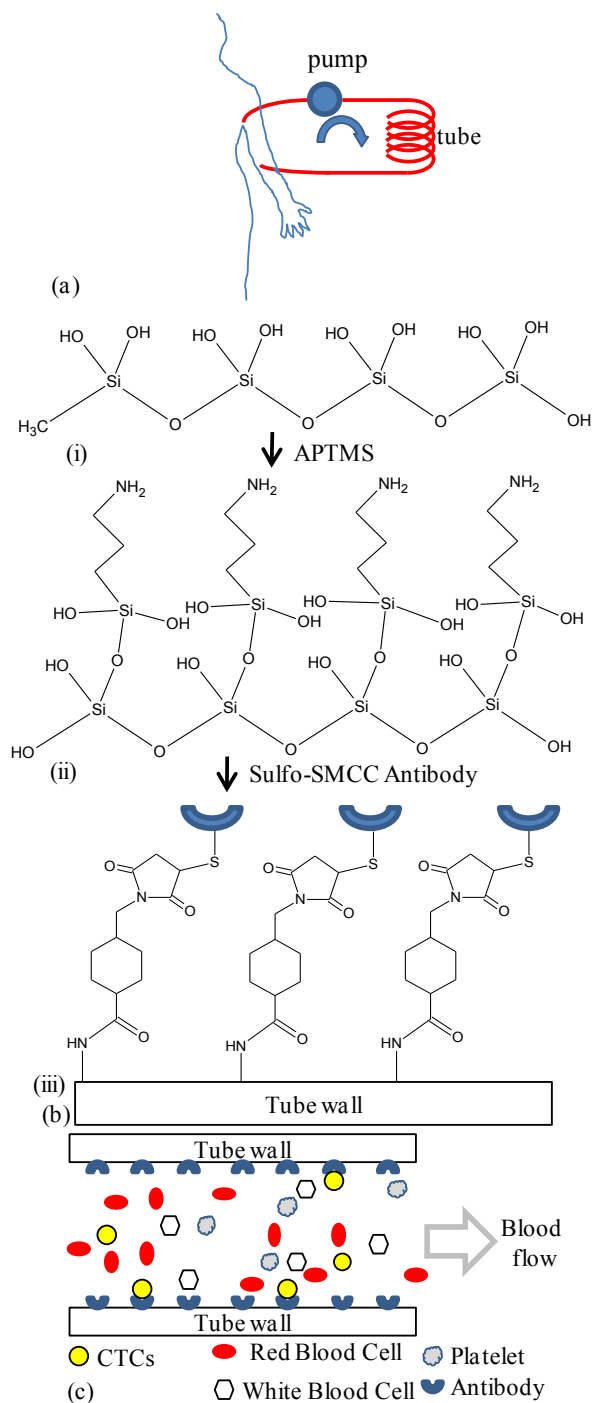
In this preliminary effort, we use a commercially available and chemically modified tube to selectively capture circulating tumor cells (CTCs) from the blood stream by immobilizing human anti-EpCAM antibodies on the tube's interior surface. We describe the steps required to modify a tube into a cancer cell capturing device. Using these simple modifications, at this proof-of-concept stage of development, we were able to capture about 85% of cancer cells from suspension and 44% of cancer cells from spiked whole blood, the capture percentage being dependent on the tube's length and the number of cancer cells present. Previous work by other researchers has focused on extracting small blood volumes and capturing CTCs with complicated micro-fluidic devices for diagnostic purposes. In addition, prior results of other researchers point to a possible reduction in metastasis achieved by removing CTCs from the bloodstream. We believe that with the utilization of appropriate tube lengths and procedures, we can ensure capture and removal of nearly the entire CTC population in whole blood. Following whole blood flow through the tube, the tube can be trypsinized to release the captured live CTCs for further analysis and testing.

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Introduction

In cancer metastasis via the cardiovascular system, cells from a primary tumor detach, circulate in the bloodstream and ultimately adhere to other organs. Current treatments have been largely ineffective in treating metastasis, as has been made evident by the fact that more than 90% of cancer deaths are due to metastasis [1]. Treatments such as chemotherapy and radiation therapy are severe and have, in many cases, toxic side effects. Further, recent evidence supports the "tumor self-seeding" concept, in which circulating tumor cells colonize an existing tumor, thus increasing its aggressiveness [2].

CTCs are generally believed to play a significant role in the metastatic process. In the past decade, research has concentrated on developing methodologies for the detection, enrichment, and enumeration of CTCs for diagnosis. These efforts include micro-fluidic separation devices [3,4,5], devices that rely on size exclusion by centrifugation [6,7] or filtration [8,9], immuno-magnetic separation [10,11] and fluorescence-activated cell sorting (FACS) technologies [3,12] and several other techniques or combinations thereof. These techniques are generally referred as "liquid biopsy" [4,13]. In liquid biopsy, a small blood sample is drawn from a patient and analyzed ex-vivo for CTCs. CTCs are typically separated and purified by antibodies, such as the epithelial cell adhesion molecule (EpCAM) [14], cytokeratins [15], etc., and enumerated. Their numbers are indicative of the progression of the disease. These techniques are constrained by the low volume extracted for analysis and thus by the low number of CTCs that can be detected. Other efforts have targeted larger blood volumes; for example, one effort incorporated the use of a structured and functionalized medical wire coated with anti-EpCAM to enrich CTC from larger volumes [16].



2

3 Fig. 1. (a) Conceptual diagram of extracorporeal device. (b) Schematic of the tube preparation: (i)

4 activation of PDMS tube surface; (ii) amine functionalized tube surface; (iii) antibody

5 conjugation. (c) CTC capturing by antibody immobilized on tube.

Researchers have suggested that techniques that remove CTCs from blood circulation in vivo could reduce metastatic events, as well as perhaps reducing the aggressiveness of existing tumors. There is indirect evidence that blood filtering, such as hemodialysis, might reduce cancer metastasis by removing circulating tumor cells (CTCs) from the bloodstream [17,18,19]. Extracorporeal filtration devices using leukocyte depletion filters have been used during tumor surgical procedures to remove tumor cells in order to reduce the risk of their dissemination [20,21,22]; however, these devices were not used to reduce metastasis post-surgery. There have been efforts to remove or kill cancer cells using microtubes functionalized with antibodies, selectin and TRAIL with a capture and a kill rate between 30-41% [23,24]. Recently, a technique to kill cancer cells in the bloodstream was demonstrated by functionalizing circulating leukocytes with cancer-specific TNF-related apoptosis inducing ligand (TRAIL) and E-selectin adhesion receptor [25].

In this preliminary work, we put forward a simple method that employs an extracorporeal tube to remove and collect CTCs from the bloodstream with possible applications in reducing metastasis and in diagnostics such as CTC enumeration and genetic analysis. Our device consists of a modified commercially available plastic tube that is functionalized with EpCAM antibodies. EpCAM is a widely used CTC marker [14]. At this proof-of-concept stage, the device already exhibits improved capturing efficiency with a design that is simple, inexpensive, and able to handle large volumes of whole blood without separation and processing (Fig. 1 (a)). Our method does not introduce any foreign agents into the bloodstream; instead, blood flows through a tube in which CTCs bind to appropriate antibodies (such as EpCAM) coated on the inner surface of the tube.

Materials and Methods

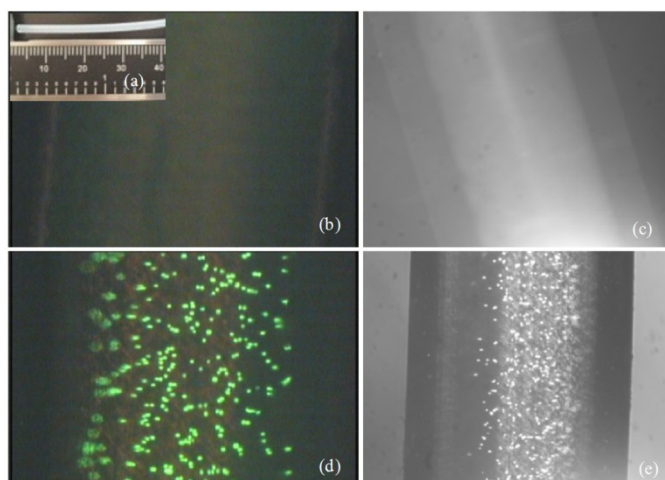


Fig. 2 (a) Tube, like the one shown in the picture, were functionalized with human anti-EpCAM (ruler scale in mm). (b & c) PC-3 cells were placed in an unmodified tube (without EpCAM coating), for control measurements, no capture was observed. (d & e) Fluorescent microscopic images of captured PC-3 cells on anti-EpCAM immobilized tube.

Tube surface modification

A polydimethylsiloxane (PDMS) tubing (Dow Corning Silastic laboratory tubing with 1.02 mm in inner diameter) was chosen for this study (Fig. 2(a)). The tube length was about 120 cm for cancer only suspension and 15 cm for blood tests. The tube's internal surface was activated by treatment with an acidic hydrogenperoxide solution ($\text{H}_2\text{O}:\text{HCl}:\text{H}_2\text{O}_2$ in 5:1:1 volume ratio) for five minutes at room temperature [27]. The tube was rinsed with excess deionized (DI) water five times and dried in air. This treatment formed the hydrophilic surface with hydroxyl groups available for further functionalization (Fig. 1 (b) (i)). The tube was then filled with aminopropyltrimethoxysilane (APTMS) for 10 minutes (Fig. 1 (b) (ii))). The tube was rinsed with excess amount of DI water at least five times and dried in air. This step adds the

1 primary amine group on the surface based on the sol-gel reaction principle [28,29]. To verify the
2 presence of the primary amine group on the tube surface, a short section of the treated tube was
3 filled with an amine reactive fluorescence dye, fluorescein isothiocyanate (FITC, 0.1 mg/mL in
4 PBS pH 7.4) for one hour (Fig. 1 (b) (ii)). The tube was then rinsed and the fluorescence from its
5 inner surface was monitored using a fluorescence microscope.

7 **Immobilization of anti-EpCAM on the surface of the tube**

8 Phycoerythrin (PE) - labeled human EpCAM (eBiosciences) antibody was treated for one
9 hour with Traut's reagent (2-iminothiolane HCl, 2-IT) to generate an available sulfhydryl group
10 (-SH) (anti-EpCAM:2-IT=1:10 in mole ratio) in PBS (pH 7.4). Then, unbound 2-IT was removed
11 from the antibodies using centrifugal filter (MWCO 30 kDa, Amicon filter or Corning Spin-X
12 protein concentrator) at 4000 RCF for 30 minutes. The concentrated anti-EpCAM was re-
13 suspended in PBS, adjusting the volume of 1 mL. During the antibody-2-IT reaction, the amine
14 functionalized tube was filled with a hetero-bifunctional (amine reactive at one terminal and thiol
15 reactive at the other terminal) cross-linker, sulfo-SMCC (sulfosuccinimidyl 4-[N-
16 maleimidomethyl]cyclohexane-1-carboxylate) in 2 mg/mL concentration in PBS (pH 7.4). After
17 the EpCAM was spun down, the sulfo-SMCC solution was removed and the tube was rinsed in
18 PBS and re-filled with 1 mL EpCAM solution. The reaction was run on a shaker for two hours at
19 room temperature and continued overnight at 4 °C. The next day, after the unbound EpCAM
20 solution was collected, the tube was gently rinsed with PBS and then refilled with 1 mg/mL L-
21 cystein for another two hours (Fig. 1 (b) (iii)). The conjugation of anti-EpCAM on the tube
22 surface was confirmed by PE's fluorescence on a fluorescence microscope.

23 **Cell culture**

1 A human prostate cancer cell line, PC-3, was purchased from American Type Culture
2 Collection (ATCC) and propagated in RPMI 1640 media supplemented with 10 % fetal bovine
3 serum and 1 % Penicillin-Streptomycin. The expression of EpCAM on the cell surface was
4 positively confirmed by performing the reaction with PE-labeled EpCAM and monitoring the
5 fluorescence label on the cell surface.

6 7 8 **Cell capturing in cell suspension**

9 PC-3 cells were detached from the culture flask by treatment with 0.25% trypsin-EDTA.
10 The cell density was determined using a hemocytometer. 250,000 cells in 1 mL RPMI were
11 selected for the capturing experiments. The anti-EpCAM immobilized tube was filled with 1 mL
12 PC-3 cell solution. The tube was incubated at room temperature for one hour; the cell solution
13 was then collected from the tube and the number of cells remaining in the collected solution were
14 measured by hemocytometry. The capturing efficiency was calculated using the following
15 equation $(\text{Initial cell density} - \text{final cell density}) / \text{initial cell density} \times 100 (\%)$. After removing
16 the cell solution, the tube was refilled with cell media containing a live cell fluorescence marker,
17 Calcein AM. The captured cells inside tube were imaged by fluorescence microscopy based on
18 Calcein AM's fluorescence at 4 x objective magnification. A control experiment was performed
19 in parallel using another silicone tube without surface modification and antibody immobilization.
20 All the sample solutions were processed for flow cytometry.

21 22 **Processing samples for flow cytometry**

23 All the samples collected through capturing experiments were pelleted by centrifugation

at 1000 RPM for 5 min. The supernatant was removed and the cell pellet was re-suspended in 4% glutaraldehyde in PBS for fixation (PC-3 cells only in equal volume (1 mL) and PC-3 cells in blood in 10x excess volume (10 mL)). Samples were then gently agitated for 15 minutes at room temperature. The samples were centrifuged again to remove excess fixative. The supernatant was removed and fixed cells were re-suspended in PBS. Once again, a centrifugation and re-suspension cycle was run for washing. PC-3 only samples were adjusted to 1 mL final volume while PC-3 in blood samples were diluted in 10 mL (10x dilution) with PBS; fixed specimens were kept refrigerated until flow cytometry.

Flow cytometry

Further evaluation of cell capture was investigated using flow cytometry to determine the cell capture before and after exposure to the anti-EpCAM immobilized tube. PC-3 in media samples were measured using a Milteny MACSQuant device based on scattering (SSC vs FSC) because the cells were not labeled by any fluorescence tag and this device could provide data based on actual cell count / volume. 50 μ L were injected for the measurements.

Cell capturing in blood

Human whole blood was purchased from Innovative Research (www.innov-research.com). PC-3 cells were trypsinized for suspension and the initial cell density was measured using hemocytometry. After cell counting, cells were stained with Calcein AM for 15 min at 37 °C, after which PC-3 cells were centrifuged at 1000 RPM for five minutes to exclude free Calcein AM from suspension. After removing the supernatant, the cell pellet was re-suspended in RPMI media to make 50,000 cells/20 μ L cell density. 20 μ L of Calcein AM labeled

PC-3 cells were added to 100 μ L whole blood containing various anti-coagulants (Li-heparin, K2-EDTA, Na-citrate), and in blood with no coagulants. Prepared EpCAM immobilized tubes (with 15 cm long) were filled with PC-3 spiked whole blood and incubated for two hours on a shaker at room temperature ((Fig. 1 (c)). The solutions were collected and processed for cell counting. Six replicated sets of PC-3 spiked whole blood samples were prepared, including three for cell count determination before tube (initial count) and three for cell count determination after capturing in tube (final count). The cell counts before and after were determined by hemocytometry based on green fluorescence from Calcein AM staining to discriminate PC-3 cells in the presence of other blood cells.

Table 1. Cell count estimation by hemocytometry. The values are of mean \pm standard error of the mean (n=3).

Samples	Initial (# cell/mL)	Final (# cell/mL)	Capture %
PC-3 in EpCAM immobilized tube	253,333 \pm 2,083	38,750 \pm 9,922	84.8 \pm 3.8 %
PC-3 in unmodified tube (Control)	257,917 \pm 2,887	255,833 \pm 5,774	0.8 \pm 1.1 %

Table 2. Cell count estimation by flow cytometry. The values are of mean \pm standard error of the mean (n=3).

Samples	Initial (# cell/mL)	Final (# cell/mL)	Capture %
PC-3 in EpCAM immobilized tube	93,467 \pm 13,360	12,907 \pm 5,153	85.2 \pm 6.6 %
PC-3 in unmodified tube (Control)	58,980 \pm 17,907	54,527 \pm 14,138	5.48 \pm 6.45 %

Table 3. Quantitative analysis of cell capture from hemocytometry. Three independent experiments exhibited an average of 44.7% capture efficiency in PC-3 cell spiked whole blood system.

Count/ 100 μ L	Initial 1	Initial 2	average Initial	final 1	final 2	average final	capture efficiency
trial 1	29000	31500	30250	14750	15750	15250	49.6 %
trial 2	27500	22750	25125	16500	17250	16875	32.8 %
trial 3	27000	21750	24375	10250	13250	11750	51.8 %
average	26583 \pm 1846			14625 \pm 1512			44.7 \pm 6.0 %

Results and discussion

The images in Fig. 2(d & e) are of PC-3 cells captured by anti-EpCAM conjugated silicone (PDMS) tube after 1 hour of incubation. After collecting the solution from the tube, captured cells were stained with Calcein AM containing cell media and imaged using GFP filter cube (Ex: 485 nm / Em: 525 nm) with an Olympus IMT-2 fluorescence microscope. The result showed that PC-3 cells were effectively captured by the anti-EpCAM immobilized tube. Because Calcein AM is a cell viability indicating fluorescent probe, these images also confirmed that the captured cells are alive. In contrast, the unmodified control tubes, shown in Fig. 2 (b & c), exhibited negligible capture of PC-3 cells.

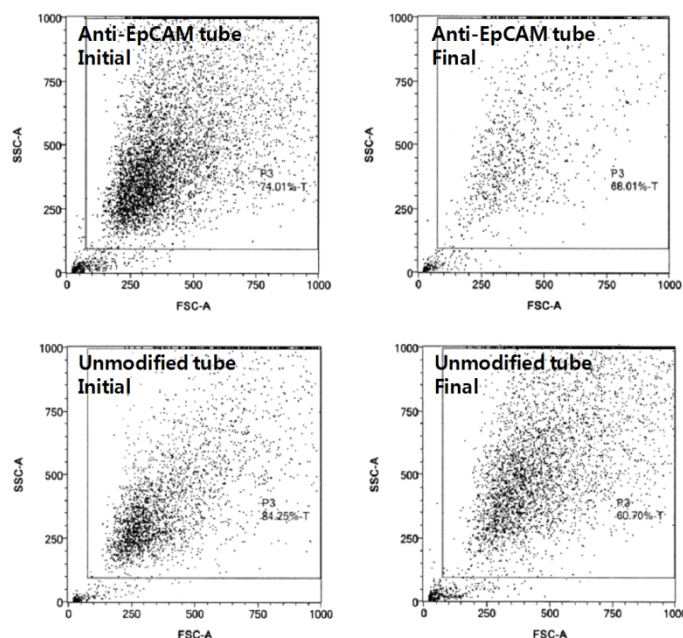


Fig. 3. Representing flow cytometry results. Upper figures clearly demonstrated the reduction in cell count by anti-EpCAM immobilized tubes, while lower figures showed minor difference between initial and final count by unmodified tube control.

The cell capture was quantitatively determined by using hemocytometry (Table 1) and flow cytometry (Table 2 and Fig. 3). These results clearly demonstrated that target cells (PC-3) can be captured in a highly effective manner, resulting in a significantly reduced number of cancer cells in the media (about 85%, confirmed by both hemocytometry and flow cytometry). The unmodified tube captured a significantly lower number of cells (about 0.8% in hemocytometry and 5.5% in flow cytometry). This indicates that slight non-specific binding occurred during the 1 hour of exposure to the unmodified tube surface. Non-specific binding can be further reduced by surface modification using, for example, a PEGylation (polyethyleneglycol) coating.

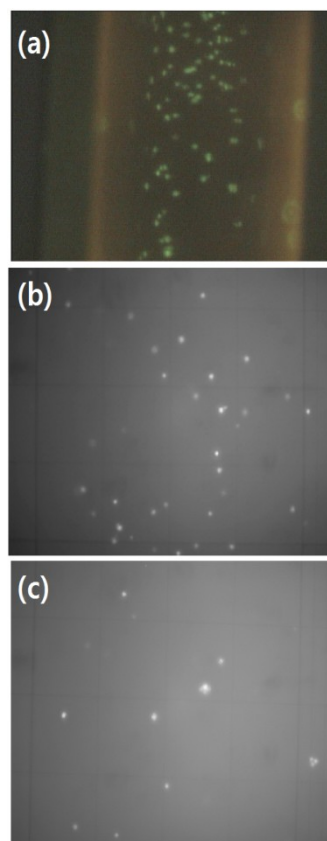


Fig. 4. (a) a fluorescence microscopy image for captured PC-3 cells on anti-EpCAM immobilized tubes in the presence of whole blood. The PC-3 cells were pre-stained by Calcein AM and Na-citrate was used as an anticoagulant for the blood sample. (b) and (c) are representing images PC-3 cells from the hemocytometry counting using Calcein AM fluorescence. Initial (b) showed significantly more cells than final (c), indicating reduction of cell density by capture.

The EpCAM immobilized tubes showed about 44% capture efficiency of PC-3 cells in whole blood (Table 3 and Fig. 4). The reduction in capture efficiency confirms the existing complications in CTC capturing in blood. Blood is a suspension that is heavily populated with various cells and particulates, including red blood cells, white blood cells, platelets, and other vesicles. The presence of these blood components could limit the movement of PC-3 cells in the solution and reduce the chances of PC-3 cells having contact with anti-EpCAM on the tube's

1 inner surface.

2 Secondly, we found that anti-coagulants can significantly interfere with the binding of
3 EpCAM antibody to the targeted PC-3 cells. In order to avoid blood clotting during the capture
4 experiments, which could inhibit the movement of cells by gelation and also clog the tube, anti-
5 coagulants are necessary. It is also known that platelets aggravate CTC metastasis; therefore, the
6 use of anticoagulants may aid in the reduction of metastatic events [30]. We originally used Li-
7 heparin as an anti-coagulant and consistently obtained negligible capture of PC-3 cells. We
8 confirmed the lack of captured cells by fluorescence imaging and by hemocytometry. While
9 exploring solutions for this problem, we found that the capturing experiment using whole blood
10 without any anti-coagulant showed positive cell capture despite interference by clotting. The
11 presence of anti-coagulants was suspected of being responsible for the inhibition of affinity to
12 anti-EpCAM. Two additional anti-coagulants, Na-citrate and K₂-EDTA, were studied (shown in
13 Supplementary Fig. 1). The results revealed that K₂-EDTA also inhibited cell capturing, while
14 Na-citrate allowed cell binding. It is still not certain whether Na-citrate does not interfere with
15 binding or does so partially. We were unable to find any interfering effects anti-coagulants may
16 have in CTC detection/diagnosis studies in literature.

17 Third, we discovered that other antibodies can impede the anti-EpCAM to PC-3 binding.
18 In order to estimate the cell density change in the presence of blood, we initially used dye
19 conjugated CD-44 antibody to visualize the PC-3 cells. CD-44 expression in PC-3 cells has been
20 previously reported [31]. The capturing efficiency of anti-EpCAM immobilized tubes between
21 CD-44 labeled PC-3 cells and PC-3 with no label was compared; this revealed that the number of
22 captured cells was reduced by half when the PC-3 cells were labeled by CD-44 as compared to
23 PC-3 cells with no label (Supplementary Fig. 2 and Table 1). These results indicated that CD-44

1 interferes with the EpCAM antibody-antigen binding. EpCAM is known to often associate with
2 other proteins, including claudin-7, tetraspanin or CD44, etc., and a possible explanation could
3 be that EpCAM affinity can be inhibited by co-existence of a high affinity antibody [32]. It is not
4 known whether CD-44 antibody and EpCAM have a common epitope to compete with each
5 other in PC-3 cells. This result also allows the inference that other isolation technologies that rely
6 on multiple antibodies may be influenced by this effect.

7 We believe that capture efficiency can be further improved. While we discovered the
8 aforementioned complications in whole blood, we reduced the tube length for the experiment
9 from 120 cm tube for PC-3 suspension study to 15 cm tube for capturing in blood. However, the
10 number of cells could not be reduced sufficiently to maintain reliable numbers in hemocytometer
11 counting (250,000 cells for suspension study to 50,000 cells for blood study). Considering the
12 ratio of the number of captured cell over the tube length, the capturing efficiency in the blood
13 study was only 17% less than that in suspension (1,770 cells/cm vs 1,467 cells/cm). The
14 capturing efficiency can be improved by using a longer tube, thus making it necessary to
15 optimize the tube length, dependent on the blood volume required to cleanse. Unlike other CTC
16 detection/diagnostics technologies which concentrate on small volumes and enrich CTCs, the
17 tube format is not necessarily limited by sample volume. Eventually, an unlimited volume of
18 samples can be circulated through the tube, thus removing the majority of CTCs from blood. We
19 believe that this procedure can be done safely and successfully in a clinical setting by processing
20 the entire blood in continuous or intermittent flow. Alternatively, consecutive drawings of as
21 much as 0.5 liter of blood (a quantity in line with typical blood donations) can undergo the
22 cleaning process for CTC removal. The blood can then be re-injected in the patient. The process

1 can be repeated until all of the blood is cleared of CTCs (a typical adult has a blood volume of
2 between 4.7 and 5 liters).

3 We also confirmed that, by removing captured cells by trypsinization (data not included),
4 the tubes can be reused with only a minor reduction in capturing ability. This method can be
5 easily adapted to current medical practices using existing medical tubing without the need for
6 complicated microfluidics and micro-fabrication.

7 While, in these experiments, we used EpCAM, we do recognize that other types of cancer
8 cells that have undergone epithelial-to-mesenchymal transition (EMT) do not express epithelial
9 markers on their surfaces. Thus, additional markers would have to be added in the future.

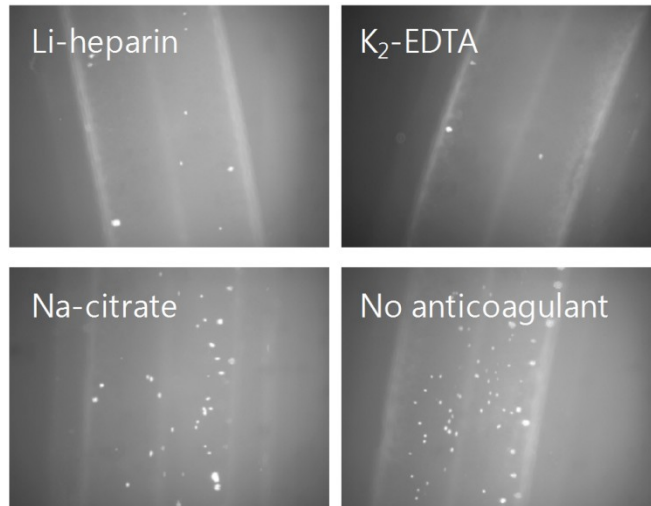
10 The device can be used for diagnostics as well as therapy, given that the captured cells on
11 the tube can be counted and further re-suspended and genetically analyzed. An interesting
12 application of this technique is in collecting live cancer cells for patient-derived tumor
13 xenografts (PDX) models to be used in cancer drug research. Additional filters and apoptosis-
14 causing agents may also be added to enhance the capture/kill rate. This device can be used
15 during tumor surgery to remove CTCs to reduce the risk of their spreading through the blood.
16 Finally, we want to note that this principle can also be applied to other conditions such as
17 bacterial or viral blood borne infections.

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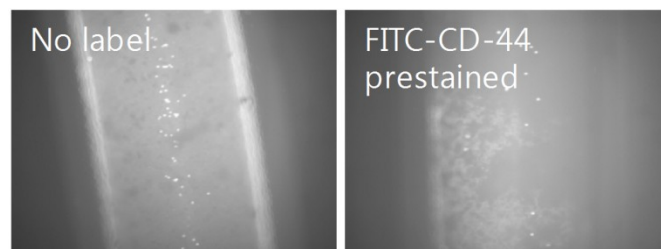
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Supporting Information Captions



Supplementary Fig. 1. The effect of anticoagulants on cell capture. Cell capture was significantly reduced in the blood when Li-heparin and K₂-EDTA were used. Successful cell capture was observed in blood with Na-citrate. The cell capturing in the blood without any anti-coagulant was examined by removing early blood clots from blood specimen. The anti-EpCAM immobilized tube could effectively capture the cells in this blood sample.



Supplementary Fig. 2. The effect of additional antibodies on cell capturing. PC-3 cells were labeled by FITC conjugated CD-44 antibodies prior to the cell capturing experiment in the blood. Captured cells were re-stained after capture by filling the tube with Calcein AM contained RPMI media. Compared to PC-3 cell without prior labeling (left), cell capture in CD-44 pre-stained PC-3 was considerably reduced (right).

# cell / 100 μ L	Initial	Final	Capture efficiency
CD-44 stained PC-3	27,750	22,625	18.5%
PC-3 with no label	29,125	16,625	42.9%

Supplementary Table 1. The reduction in capture efficiency by CD-44 pre-staining was quantified using hemocytometry.