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# A customizable microscopy system for the automated quantification and characterization of multiple adherent cell types: an alternative to flow cytometry

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Cell quantification assays are essential components of most biological and clinical labs. However, many currently available quantification assays, including flow cytometry and commercial cell counting systems, suffer from unique drawbacks that limit their overall efficacy. In order to address the shortcomings of traditional quantification assays, we have designed a robust, low-cost, automated optical cell cytometer that quantifies individual cells in a multiwell plate using tools readily available in most labs. Plating and subsequent quantification of various dilution series using the automated optical cytometer demonstrates the single-cell sensitivity, near-perfect  $R^2$  accuracy, and greater than 5-log dynamic range of our system. Further, the optical cytometer is capable of obtaining absolute counts of multiple cell types in one well as part of a co-culture setup. To demonstrate this ability, we recreated an experiment that assesses the tumoricidal properties of primed macrophages on co-cultured tumor cells as a proof-of-principle test. The results of the experiment reveal that primed macrophages display enhanced cytotoxicity towards tumor cells while simultaneously losing the ability to proliferate, an example of a dynamic interplay between two cell populations that our optical cytometer is successfully able to elucidate.

1           **A Customizable Microscopy System for the Automated Quantification and**  
2           **Characterization of Multiple Adherent Cell Types: an Alternative to Flow Cytometry**

3

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34 principle test. The results of the experiment reveal that primed macrophages display enhanced  
35 cytotoxicity towards tumor cells while simultaneously losing the ability to proliferate, an  
36 example of a dynamic interplay between two cell populations that our optical cytometer is  
37 successfully able to elucidate.

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## 46 **Introduction**

47           Cell quantification assays are essential components of most biological labs, and are used  
48 for a variety of applications, including cytotoxicity, viability, and proliferative studies. Though  
49 these assays have improved significantly since the advent of hemocytometers, they still suffer  
50 from a number of unique limitations. Current cell quantification assays can be divided into two  
51 major classes: metabolic and cell counting. Metabolic assays, though originally designed to  
52 assess cell viability, are often used to indirectly assess cell number. These assays, like MTT or  
53 alamarBlue, are relatively easy to perform, and can provide additional information on cell health  
54 that a counting assay may not. However, they are not ideal for certain experimental setups, as  
55 they have a limited dynamic range and are prone to confounding interference in the presence of  
56 certain chemicals (Chakrabarti et al. 2000; Doak et al. 2009; Hamid et al. 2004; Ulukaya et al.  
57 2004; Vistica et al. 1991). These assays also do not always align well with the DNA content of  
58 the cell—a parameter that correlates strongly with cell number—limiting the cell quantification  
59 potential of these assays (Quent et al. 2010). Cell counting assays on the other hand, though  
60 generally more manually intensive, are more representative of actual cell counts than metabolic-  
61 based proxy assays (Chan et al. 2013). Flow cytometry, often considered the gold standard for  
62 cell counting and analysis, is an especially powerful technique for quantifying individual cells,  
63 and is one of the few modalities capable of identifying cell population counts in both a mono-  
64 culture and co-culture setup (Gedye et al. 2014; Gerashchenko 2008; Gerashchenko & Howell  
65 2013).

66           Co-culture systems are fundamental to studying any kind of cell-to-cell interaction. Many  
67 areas of research could benefit immensely from co-culture setups—including biomaterials,  
68 immunology, and cancer biology—if better characterization and quantification methods were

69 available for these studies (Bidarra et al. 2011; Miki et al. 2012). Most approaches to co-culture  
70 are restrictive, and often require that plated cells be physically separated via a transwell insert or  
71 microfluidic chamber that only permits the exchange of media (Arrigoni et al. 2016; Goers et al.  
72 2014; Katt et al. 2016). Yet physical contact has been shown to be important for studying the  
73 interactions of many cell types in a variety of physiological contexts (Cruickshank et al. 2004; de  
74 Goer de Herve et al. 2010; Holt et al. 2010; Suzuki et al. 2004). Most cell populations do not  
75 behave independently and a better understanding of the interaction between multiple cell types in  
76 a system will help improve our understanding of many physiological phenomena.

77         Most studies that utilize a true co-culture setup with physical contact rely on flow  
78 cytometry to quantify individual cell types. Unfortunately, flow cytometry has several drawbacks  
79 that apply not only to co-culture setups but mono-culture setups as well. As a starting point, flow  
80 cytometers are fairly sophisticated; as a result, these instruments are generally expensive and  
81 often require skilled upkeep (Nasi et al. 2015). Flow cytometry also requires cells to be in  
82 suspension—thus the majority of experiments that are conducted on adherent cells in multiwell  
83 plates require trypsin treatment for cell detachment. Trypsin, however, can damage cells and  
84 cleave extracellular markers that may be used for cellular identification or other forms of  
85 analysis (Gedye et al. 2014). Additionally, certain cell types are not amenable to trypsin  
86 treatment and as a result require manual cell scraping, a process that is prone to human error.  
87 Cell scraping can also mechanically damage some cell types, leading to erroneous results with  
88 certain assays that are used in combination with flow cytometry: for example, false positives  
89 with membrane permeable cell viability assays such as propidium iodide (Batista et al. 2010;  
90 Bundscherer et al. 2013). All together, the need to bring adherent cells into suspension makes  
91 flow cytometry less than ideal for many types of studies.

92 An additional limitation unique to co-culture setups is that typical flow cytometry obtains  
93 relative counts rather than absolute counts, i.e. each cell type is expressed as a percent of the total  
94 sample assayed. This may generate misleading results when comparing counts for multiple cell  
95 types between conditions.

96 To address the shortcomings of the various cell quantification assays, we have put  
97 together a relatively simple optical counting setup with tools readily available in most labs (Fig  
98 1). The proposed system uses a standard fluorescent microscope to quantify individual cells on a  
99 multiwell plate with superior sensitivity, resolution, and dynamic range. The system utilizes  
100 established staining techniques to label cells, and subsequently quantifies every cell in the entire  
101 experimental space via whole-well imaging, thus precluding the need for trypsinization or cell  
102 scraping. The image data is then run through ImageJ for preprocessing and then analyzed in  
103 CellProfiler, a free-to-use cell segmentation software, to generate absolute cell counts for every  
104 well. In addition, by utilizing a combination of staining techniques, multiple cell types (even  
105 those with complex morphologies) can be uniquely identified and absolutely counted, permitting  
106 the setup of more complicated co-culture experiments that were not previously feasible, one of  
107 the strongest aspects of the proposed system.

108 It should be noted that other optical counting systems have been developed to address the  
109 aforementioned limitations of flow cytometry. However, the optical system we present here still  
110 bears a number of advantages over these pre-sold cytometric platforms. First, for labs that  
111 already possess a fluorescent microscope, the optical cytometer is a relatively small investment  
112 to the overhead cost of buying a prebuilt optical counting system or flow cytometer. Further,  
113 unlike most commercial counting systems, the optical cytometer discussed here is flexible in the  
114 assays and cell types that can potentially be analyzed, and highly customizable in both setup and

115 analysis, permitting the extraction of more relevant and robust information per experiment. In  
116 this way, biological workflow is not limited by the vendor-specific restrictions of pre-built  
117 systems, but rather expanded to include all functionalities of standard fluorescent microscopes.

118 Many image cytometers currently on the market also exhibit a smaller dynamic range and  
119 reduced sensitivity compared to the system we present here. Lastly, most commercial cytometric  
120 platforms are not able to discriminate multiple unique cell populations, with potentially complex  
121 morphologies, within a single well. This is largely due to the inability of most commercial  
122 cytometers to accurately segment non-spherical morphologies, thus restricting their applicability  
123 for most co-culture setups. A more in depth comparison of our optical cytometer to  
124 commercially available systems, including in cost, can be found in the discussion as well as  
125 supplementary section (Text S1).

## 126 **Materials and Methods**

### 127 **Cell Culture and Plating**

128 JC CRL 2116 mouse adenocarcinoma cells were obtained from ATCC (American Type  
129 Culture Collection; Manassas, Virginia) and maintained in Dulbecco's Modified Eagle Medium  
130 (DMEM) supplemented with 10% Fetal Bovine Serum (FBS) and 1% penicillin/streptomycin.  
131 J774.A1 mouse macrophages were obtained from ATCC and maintained in Roswell Park  
132 Memorial Institute Medium (RPMI), supplemented with 10% Fetal Bovine Serum (FBS) and 1%  
133 penicillin/streptomycin. Both cells were grown at 37°C in 5% CO<sub>2</sub>.

134 For plating, cells were trypsinized (JC CRL 2216 cells) or scraped (J774.A1 cells) from  
135 their flasks and quantified manually using a bright-line hemocytometer (Sigma-Aldrich; St.  
136 Louis, Missouri). Due to the variability present in counts obtained using a hemocytometer,  
137 established values were primarily used to determine the approximate concentration of the



138 primary stock from which precise subsequent dilutions were performed. Dilution series were  
139 generated by pulling cells from the previous stock and diluting in fresh media. Triplicates of each  
140 dilution were then plated on either a 48- or 12-well Corning Costar flat bottom cell culture plate  
141 (Thermo Fisher Scientific; Waltham, Massachusetts) and left overnight to attach to the plate  
142 surface.

### 143 **Co-Culture Experiments**

144 J774.A1 cells were seeded at  $2.5 \times 10^4$  cells/well in RPMI media in a 48-well plate.  
145 Immediately following seeding, cells were exposed either to 1  $\mu\text{g}/\text{mL}$  of lipopolysaccharide  
146 (LPS) (Sigma-Aldrich; St. Louis, Missouri), 0.1  $\mu\text{g}/\text{mL}$  of mouse interferon gamma ( $\text{IFN}\gamma$ )  
147 (BioLegend; San Diego, California), both 1  $\mu\text{g}/\text{mL}$  of LPS and 0.1  $\mu\text{g}/\text{mL}$  of  $\text{IFN}\gamma$ , or neither.  
148 After a 24-hour incubation, the wells were washed twice with Phosphate Buffered Saline (PBS).  
149 JC CRL 2116 cells were then added at  $1 \times 10^4$  cells/well in RPMI media to every well. Cells were  
150 processed and imaged after 24 hours.

### 151 **Cell Staining**

152 For assays requiring only a nuclear stain, cell processing was performed immediately  
153 prior to imaging. After firm cell adhesion, media was removed from the wells by inverting the  
154 plate and cells were fixed for 15 minutes in BD Cytifix (BD Biosciences; San Jose, California).  
155 Fixative was removed by washing the plate twice with Hank's Balanced Salt Solution (HBSS).  
156 Cells were then stained for 5 minutes in a 2.5  $\mu\text{g}/\text{mL}$  DAPI stain solution (Thermo Fisher  
157 Scientific; Waltham, Massachusetts). The plate was again washed twice with HBSS and finally  
158 resuspended in HBSS for imaging.

159 Experiments involving multiple stains, including nuclear, cytoplasmic, and  
160 surface/antibody stains, required a slightly different protocol. Using the immune co-culture

161 experiment as an example, JC CRL 2116 cells were stained in their cell culture flask with 20  $\mu$ M  
162 of Vybrant CFDA SE (Invitrogen; Carlsbad, California) the day prior to plating using the  
163 recommended protocol. After completion of the experiment and immediately prior to imaging,  
164 media was removed from the wells by inverting the plate, and the plate was subsequently  
165 blocked with a 1% bovine serum albumin (BSA) (Sigma-Aldrich; St. Louis, Missouri) solution  
166 in HBSS for 15 minutes. HBSS supplemented with calcium was found to help prevent cell  
167 detachment prior to cell fixation. Cells were then incubated with a 5  $\mu$ g/mL PE anti-mouse  
168 CD11b antibody (BioLegend; San Diego, California) diluted in 1% BSA HBSS for 1 hour to  
169 stain the J774.A1 cells. After incubation, the antibody solution was removed by inverting the  
170 plate after which the wells were washed twice with 1% BSA HBSS. The cells were then fixed for  
171 20 minutes in BD Cytofix. Fixative was removed by washing the plate twice with HBSS. Cells  
172 were then stained for 5 minutes in a 2.5  $\mu$ g/mL DAPI stain solution. The plate was again washed  
173 twice with HBSS and finally resuspended in HBSS for imaging.

#### 174 **Acquiring Whole-Well Images**

175 All imaging was performed on a Nikon Eclipse Ti-E inverted fluorescent microscope  
176 with motorized x, y, and z stage (Nikon Instruments Inc.; Melville, New York). Images were  
177 captured using a NAMC 10x objective and Andor Zyla 4.2 sCMOS camera (Andor Technology;  
178 Belfast, Northern Ireland). DAPI/Hoechst (excitation: 360/40, emission: 460/50, dichroic mirror:  
179 400), GFP (Ex: 470/40, Em: 525/50, DM: 495), and Texas Red (Ex: 560/55, Em: 645/75, DM:  
180 595) filter cubes (Nikon Instruments Inc.; Melville, New York) were used to image cells stained  
181 with DAPI, Vybrant CFDA SE, and PE anti-mouse CD11b antibody respectively. Using the  
182 associated Nikon software, NIS-Elements, an automated macro was set up for whole-well  
183 acquisition. First, an x-y coordinate list demarcating the center of every well was generated by

184 manually determining the center of the first and last well of the plate and dividing these values  
185 by the number of rows and columns. The coordinate list will vary based on the type of multiwell  
186 plate but only needs to be generated once. Using a 10× objective and 1,600×1,600 pixel region of  
187 interest (ROI), 10×10 images for a 48-well plate and 19×19 images for a 12-well plate were tiled  
188 together to create a whole-well image. The center of each well serves as the origin point of the  
189 tiled images as well as the autofocus point.

### 190 **Processing Whole-Well Images**

191 Images were preprocessed using ImageJ (National Institute of Health; Bethesda,  
192 Maryland). The ring of autofluorescence around the well edges was removed using the *Subtract*  
193 *Background* function with a rolling ball radius of 50 pixels. Fluorescent channels that were too  
194 faint for analysis were occasionally made brighter using the *Enhance Contrast* function. If  
195 images were stitched during image acquisition they were subsequently cropped into 100 smaller  
196 images using the *Montage to Stack* function at which point they were transferred to CellProfiler  
197 (Broad Institute; Cambridge, Massachusetts) for segmentation. ImageJ macros (Macro S1) and  
198 CellProfiler codes (CellProfiler Code S1, and CellProfiler Code S2) are provided as  
199 supplementary files. A more detailed explanation of relevant ImageJ and CellProfiler functions  
200 can be found in the supplementary section (Text S1).

## 201 **Results**

### 202 **Accuracy of Nuclear Quantification in Conjunction with Whole-Well Imaging**

203 Many studies take representative or random images that represent only a small portion of  
204 the entire well to make a claim about differences in cell count/viability between conditions.  
205 Instead of manually acquiring a series of random or representative images, which is both tedious  
206 and potentially inaccurate, it is possible—using a fluorescent microscope with a motorized x, y,

207 and z stage—to automate capture of the whole well using movement in the x- and y-plane to  
208 image the well and movement in the z-plane to autofocus (Fig 2).

209 To count individual cells, wells were stained with a DAPI nuclear stain. Nuclei are often  
210 roundly shaped and spaced from adjacent nuclei by the cell cytoplasm and membrane, making  
211 segmentation relatively straightforward. In addition, there is usually one nucleus per cell, making  
212 nuclear segmentation ideal for cell counting. To demonstrate the power of nuclear counting and  
213 whole-well imaging, a linear dilution series of JC CRL 2116 mouse adenocarcinoma cells going  
214 from 10,000 cells/well all the way down to 1,000 cells/well was plated; an experiment spanning  
215 one order of magnitude. Three linear curves were then generated from five random images, a box  
216 crop of the whole-well image, or the whole-well image itself, and used to determine cell count  
217 (Fig 3). Accuracy improves significantly as the percentage of the experimental space being  
218 assayed increases, with whole-well imaging displaying a near-perfect  $R^2$  and minimal error  
219 between replicates.

### 220 **Establishing Dynamic Range and Sensitivity**

221 The optical cell cytometer obtains accurate counts by counting individual cells. In theory  
222 it should be able to count anywhere from one cell to the confluency limit of the well plate the  
223 experiment is conducted in with single-cell precision. To demonstrate the dynamic range of the  
224 system, half-log dilutions of JC CRL 2116 cells going from 100,000 cells/well all the way down  
225 to 100 cells/well were plated in a 12-well plate; an experiment spanning three orders of  
226 magnitude (Fig 4). The system performs strongly up to the confluency limit of the plate with a  
227 dynamic range limited only by the surface area of the multiwell. Even at confluency, nuclei  
228 remain sufficiently spaced apart permitting accurate segmentation (Fig S1).

229 To validate the sensitivity of the system, a linear dilution series starting at 100 cells/well  
230 and going down to 1 cell/well was also plated. However it was found that at such low  
231 concentrations, it was not feasible to reliably plate the desired number of cells. Accordingly, the  
232 cells that were plated were manually counted in the brightfield channel and compared with  
233 CellProfiler counts obtained from segmenting nuclei in the DAPI channel (Fig 5). The system  
234 demonstrates an extraordinary level of sensitivity and resolution, as it performs robustly even at  
235 the single-cell level, with most deviations attributable to human error when manually counting.

### 236 **Counting Using Surface and Cytoplasmic Stains**

237 In order to count multiple cell types in a co-culture experiment, additional cell stains are  
238 required. Cell stains can be grouped into one of three categories: nuclear, surface, and  
239 cytoplasmic. Because most nuclear stains non-specifically stain DNA and compromise cell  
240 viability, they cannot be used to differentiate cell types. Instead, vital cytoplasmic dyes like  
241 Vybrant CFDA SE (Vybrant carboxyfluorescein diacetate succinimidyl ester), or antigen-  
242 specific surface stains, such as fluorophore-conjugated antibodies, need to be used.

243 Surface and cytoplasmic staining alone can be used to differentiate cells, but primary  
244 segmentation of these stains is fairly difficult. Factors including inhomogeneous staining, cell  
245 contact with neighboring objects, and complex cell morphologies make segmentation less than  
246 ideal. One way to overcome this limitation is to use easily identifiable and spatially resolvable  
247 nuclei delineated in one fluorescent channel as a seed/primary object to guide detection of the  
248 cell border/secondary object outlined in a separate fluorescent channel (Jones et al. 2005;  
249 Vincent & Soille 1991). However, when plating more than one cell type, for example in a co-  
250 culture setup, this approach alone is insufficient because every nuclei will generate a secondary  
251 object regardless of whether there is an associated cell in CellProfiler (Carpenter et al. 2006). To

252 overcome this limitation, several additional layers of image processing, including mask  
253 generation, need to be performed; these are elaborated upon in the discussion section.

254 To validate the power of this approach as well as the efficacy of cytoplasmic and surface  
255 staining, a linear dilution series of J774.A1 cells, a mouse macrophage cell line, was plated going  
256 from 10,000 cells/well down to 1,000 cells/well. These cells were stained with Vybrant CFDA  
257 SE (cytoplasmic stain) prior to plating, and phycoerythrin (PE)-conjugated anti-CD11b  
258 antibodies (surface stain) as well as DAPI (nuclear stain) immediately prior to imaging. The  
259 system performs less than ideally when segmenting the cytoplasmic or surface stains alone (Fig  
260 S2). When nuclei are used as seeds however, the optical cytometer performs robustly both for  
261 cytoplasmic and surface staining (Fig 6).

## 262 **Quantification of Multiple Adherent Cell Types**

263 To demonstrate the ability of the optical cell cytometer to determine absolute counts of  
264 multiple cell types in a single well, we recreated an immunology experiment that was conducted  
265 in 1991 as a proof-of-principle test. Novotney, et al. set out to determine the tumoricidal  
266 properties of J774.A1 mouse macrophages when primed with lipopolysaccharide (LPS). To do  
267 this, the target tumor cell line needed to be radiolabeled with  $^{51}\text{Cr}$  then co-cultured with primed  
268 J774.A1 macrophages. The extent of tumor killing was determined by measuring the increase in  
269 radioactivity of the supernatant due to tumor cell death and detachment (Novotney et al. 1991).

270 To recreate this experiment, JC CRL 2116 tumor cells were labeled with Vybrant CFDA  
271 SE in their cell culture flask 24 hours prior to plating. J774.A1 macrophages were plated first and  
272 were either left unprimed or primed with either LPS, interferon gamma ( $\text{IFN}\gamma$ )—a known  
273 macrophage activator, or both (Schoenborn & Wilson 2007). After a 24-hour incubation, LPS  
274 and  $\text{IFN}\gamma$  were removed from the wells and the previously stained JC CRL 2216 cells were

275 added. After another 24-hour incubation, the wells were stained with a PE-conjugated anti-  
276 CD11b targeting antibody to uniquely label the J774.A1 macrophages, as well as DAPI to stain  
277 all nuclei.

278         The results of the test reveal an interesting relationship between macrophage activation  
279 and tumoricidal activity. The more strongly primed the macrophages, the more pronounced the  
280 tumoricidal response; however, strongly primed macrophages also lose the ability to proliferate,  
281 indicated by a sharp drop in macrophage count (Fig 7a). Absolute counts of both cell populations  
282 show that erroneous results would have been obtained by any setup that looks at relative counts  
283 (Fig 7b). Cytometric analysis reveals that primed J774.A1 macrophages are also larger in size  
284 (Fig 7c) and appear to have either increased uptake or phagocytic activity, as demonstrated by  
285 the retention of Vybrant dye that was initially present in the cytoplasm of the JC CRL 2116  
286 tumor cells (Fig 7d). CD11b expression levels, which are known to be upregulated under certain  
287 activation conditions, do not appear to increase under these experimental conditions (Biswas &  
288 Sodhi 2002).

## 289 **Discussion**

290         We present here a relatively simple optical counting setup that brings together several  
291 established techniques—including automated microscopy, cellular staining, and cell  
292 segmentation—to quantify every cell in an experimental space, without the need for  
293 trypsinization or cell scraping. Using whole-well imaging, we demonstrate that taking  
294 representative or random images of a well to make a claim about cell viability/counts may be  
295 misleading given the non-uniform distribution of cells in a well. In addition, by counting each  
296 individual cell using nuclear segmentation, we demonstrate the impressive accuracy and  
297 resolution of our optical quantification system. In general, counting single events/cells provides a

298 resolution that cannot be obtained with bulk ensemble measurements, and can significantly  
299 improve sensitivity (Chang et al. 2012; Rissin et al. 2010). This approach, in conjunction with  
300 whole-well imaging, also offers increased statistical power as the experimentally relevant region  
301 is sampled in its entirety.

302         Next, we show that the system can accurately quantify cells up to the confluency limit of  
303 the plate. By increasing the surface area of each well however, it is possible to expand the  
304 working range of the optical cytometer. Though 12-well plates were used here to accurately  
305 quantify up to 100,000 cells/well, it is possible to use 6-well plates or less, with a larger  
306 corresponding surface area per well, to push the upper limits of detection.

307         On the lower end of the optical cytometer's operating range, illumination correction,  
308 sufficient post-stain washing, and binary quantification make counting of just a single-cell  
309 theoretically possible with minimal interference from background or noise. Data from tests that  
310 were conducted with only a few cells per well demonstrate the incredible sensitivity of the  
311 system, but slight deviations in segmented nuclei-derived counts versus manual counts are  
312 evident as demonstrated by the imperfect  $R^2$ . While manual counts were performed solely on  
313 brightfield images, merging of nuclei in the DAPI channel with cell outlines in the brightfield  
314 channel reveal that deviations in the lower range data were actually due to human error.  
315 Ultimately, counts obtained via CellProfiler proved more reliable than manual counting  
316 validating the ability of the optical cytometer to quantify down to the single-cell level. Systems  
317 with improved sensitivity are not only advantageous when conducting screening assays on  
318 smaller sized plates (such as 96-, 384-, and 1536-well plates), but also when detecting a very low  
319 concentration of cells on large well plates. A sensitive system may also prove useful for  
320 detecting rare cell subpopulations in a heterogeneous group (Lin et al. 2011).



321           Testing of the upper and lower extremes of the optical cytometer reveal the greater than  
322 5-log detection range that can be achieved with the instrument. Systems with a large dynamic  
323 range are particularly advantageous for screening cytotoxic compounds such as antineoplastic  
324 agents. It has been shown that compounds that reduce cell viability by at least two orders of  
325 magnitude *in vitro* are more likely to demonstrate a response in clinical trials, making an assay  
326 with an even larger dynamic range more appealing (Frgala et al. 2007). All together, the  
327 combination of improved sensitivity, resolution, and dynamic range afforded by the automated  
328 optical cytometer opens up the possibility of a new set of cell culture experiments that were not  
329 previously feasible.

330           We next show that certain cytoplasmic and surface stains, in conjunction with a nuclear  
331 stain, can be used to effectively differentiate cell populations in a co-culture setup. Vybrant  
332 CFDA SE dyes, for example, are designed to form intracellular fluorescent conjugates that  
333 homogenously stain the cell cytoplasm, are well-retained, and are not transferred to adjacent  
334 cells or passed onto daughter cells during division (Bronner-Fraser 1985; Hodgkin et al. 1996;  
335 Lyons & Parish 1994; Nose & Takeichi 1986; Weston & Parish 1990). Alternatively, cells can  
336 be stained post-experiment and just prior to imaging using target-specific dyes, such as  
337 fluorescently-conjugated antibodies.

338           For counting of more than one cell type in a co-culture setup, using a mask generated  
339 from the fluorescent outlines of either a surface or cytoplasmic stain to delineate which nuclei  
340 belong to which cell type proved to be the most robust. To do this, whole-cell fluorescence—  
341 generated from either a surface or cytoplasmic stain—is used to create an inclusive mask that  
342 retains nuclei contained within. This method can be repeated iteratively for each cell specific  
343 stain, eventually grouping every nucleus with its associated cell population. These filtered nuclei

344 images can then be segmented and quantified using standard nuclear segmentation to generate  
345 respective counts for each cell type. This approach is made possible using the unique fluorescent  
346 staining and algorithmic combination proposed herein, and overcomes many of the limitations of  
347 traditional segmenting systems. A sample workflow of this process with associated images can  
348 be found in the supplementary section (Fig S3).

349         It should be mentioned that many commercial image cytometers largely rely on primary  
350 segmentation for the quantification of multiple adherent cell types in a single well. This often  
351 requires the utilization of an array of algorithmic functions such as thresholding, contouring,  
352 water shedding, cleaning, eroding, dilating, opening, closing, and smoothing to uniquely identify  
353 individual cells. Classifiers (both object and pixel) are also occasionally utilized to train systems  
354 to recognize user-delineated objects. However, these algorithmic approaches are largely  
355 inadequate for quantifying cells with complex morphologies ultimately limiting the accuracy and  
356 performance of commercial systems in these settings. For our study in particular, primary  
357 segmentation of the cytoplasmic and surface stains alone performed reasonably well when cell  
358 morphology was round and staining was homogenous (as was the case with the J774.A1 triple  
359 stain). When cell morphology became more spindly (as seen with JC CRL 2116 cells), or  
360 staining became more inhomogeneous (as seen with activated J774.A1 cells) however, a marked  
361 decrease in primary segmentation performance was observed (data not shown) indicating that the  
362 aforementioned algorithmic functions are limited in their generalizability. Using the fluorescent  
363 outline of the cell to generate a mask removes the need for primary segmentation of these stains,  
364 and instead harnesses the accuracy/power of nuclear segmentation, allowing for highly accurate  
365 quantification of multiple cell types with varying morphologies in a co-culture setup. If a user

366 was already in possession of a commercial optical counting system, the proposed algorithmic  
367 approach could be adapted to achieve the same results.

368         The ability of the optical cytometer to accurately count individual cells of a specific  
369 population is best demonstrated by the macrophage-tumor co-culture experiment we recreated.  
370 Unfortunately, the use of  $^{51}\text{Cr}$  to radiolabel target tumor cells is expensive and manually  
371 intensive by today's standards. While cell-permeable fluorogenic protease substrates have been  
372 developed as a replacement for  $^{51}\text{Cr}$ , neither is capable of dynamically quantifying changes in  
373 effector cell (macrophage) count and the tumor cells they target (Packard & Komoriya 2008). A  
374 suitable alternative assay to count both tumor cell and macrophage populations does not exist for  
375 this particular experiment. Flow cytometry, for example, would not be preferable here because  
376 J774.A1 macrophages are not amenable to trypsin treatment, and thus require manual scraping.  
377 In addition, standard flow cytometry would struggle to tease out individual counts of each cell  
378 type because the data is collected as a relative count to total number of cells gated. As shown in  
379 Figure 7b, the quantification of relative counts rather than absolute counts would have led the  
380 user to believe that macrophage priming actually promotes tumor cell growth as opposed to  
381 inhibiting it (tumor cells represent 18.0% of the total sample in the unprimed control versus  
382 36.1% of the total sample in the LPS + IFN $\gamma$  primed condition). The optical cell cytometer  
383 system we have developed, however, can determine absolute counts of both cell types with  
384 remarkable accuracy. With the priming of the J774.A1 macrophages, we were able to not only  
385 elucidate the tumoricidal activity of the macrophages, but also the inverse nature of macrophage  
386 proliferation and cytotoxic potential.

387         In addition to cell count, the optical cytometer was able to extract morphological data,  
388 such as cell size and mean fluorescence intensity, for every cell. The system is also capable of

389 extracting additional parametric data, such as cell eccentricity, orientation, number of neighbors,  
390 first closest object distance, and granularity, extending its capacity beyond simply counting, and  
391 into cytometry. The cytometer is also compatible with other fluorescent-based assay stains  
392 including annexin V and/or propidium iodide for assessing cell death, CFSE or BrdU for  
393 measuring cell proliferation, and alamarBlue or calcein AM for determining cell viability. For  
394 many fields of biology where the interaction between multiple cell types is important, the ability  
395 to conduct this type of co-culture experiment may prove invaluable.

396         Suggestions for improving and expanding the capacities of the optical cell cytometer for  
397 co-culture as well as mono-culture studies can be found in the supplementary section. They  
398 include recommendations for optimizing workflow, handling of an increasing number of  
399 cells/parameters in a single experimental setup (multiplexing), management of multinucleated  
400 cells, processing of tissue samples, and analysis of poorly adherent cells. An overview of the  
401 technical specifications of the optical cell cytometer can also be found in the supplementary  
402 (Additional File 4: Text S1).

### 403 **Conclusions**

404         All together, the optical cell cytometer is a viable alternative to flow cytometry, and other  
405 currently available imaging cytometers, and is available at only a fraction of the cost for labs that  
406 already possess a fluorescent microscope. The system is automated and high throughput using  
407 tools already available in most labs. Optical cell counting offers unprecedented sensitivity, going  
408 down to the single-cell level, while still boasting an impressive dynamic range limited only by  
409 the size of the well plate used. Because counts are binary, the system offers remarkable  
410 resolution. Further, the use of whole-well images allows for quantification across the entire  
411 experimental space conferring remarkable accuracy. In addition to cell counts, other features can

412 be gathered from each experiment, including the spatial distribution of cells as well as various  
413 morphological analyses. The system is also compatible with other fluorescent-based assay stains.  
414 Since the system is put together by the user, it is highly customizable, and allows for direct  
415 assessment of assay performance.

416         The optical cytometer has the added benefit of assessing adherent cells directly on the  
417 plate without needing to bring them into solution. As a result, the system does not require caustic  
418 trypsin treatment to resuspend cells in solution, as is the case with flow cytometry. One of the  
419 most promising aspects of the system is that multiple cell types can be plated together and  
420 absolute counts of each population can be elucidated. For many fields of biology, absolute counts  
421 can help tease out interesting relationships between cell populations that might not be discernible  
422 using relative counts. After imaging and analysis, population statistics—including cell counts  
423 and fluorescence intensity—can be extracted, thresholded, and displayed in histogram or dot-plot  
424 form much like the output of a flow cytometer. Overall, we believe the optical cell cytometer  
425 will improve the quality of cell cytometric studies and open up the possibility of a new class of  
426 experiments centered around the ability to assess multiple cell types in a co-culture setup. The  
427 impressive sensitivity and dynamic range of the instrument are also strongly compelling.

428

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432

#### 433 **Author's Contributions**

434 Conceived and designed the experiments: VA, RAD. Performed the experiments: YT, AF, AA,  
435 BSS, VA. Analyzed the data: VA, YT, AF. Contributed reagents/materials/analysis tools: ALC,  
436 RAD. Wrote the paper: VA, PB, ERE, RAD. All authors read and approved the final manuscript.

437

#### 438 **Conflict of Interest**

439 The authors declare that they have no competing interests

440

#### 441 **Data Availability**

442 Raw data files can be found at

443 <https://www.dropbox.com/sh/it4e56my94xmlba/AADRuhXlkkX1xnziAu4bYJLLa?dl=0>

444

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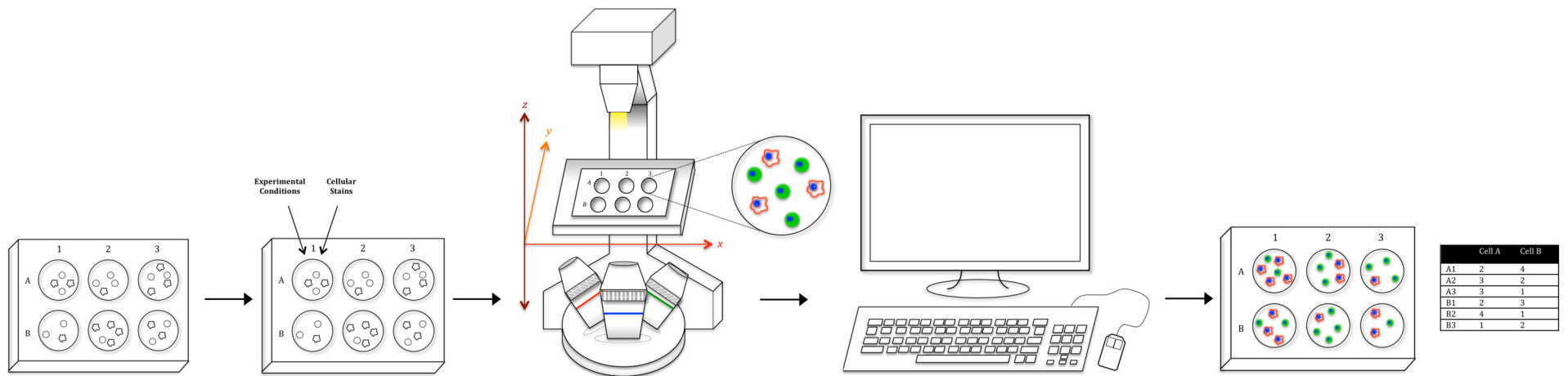
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**Figure 1**(on next page)

Workflow schematic.

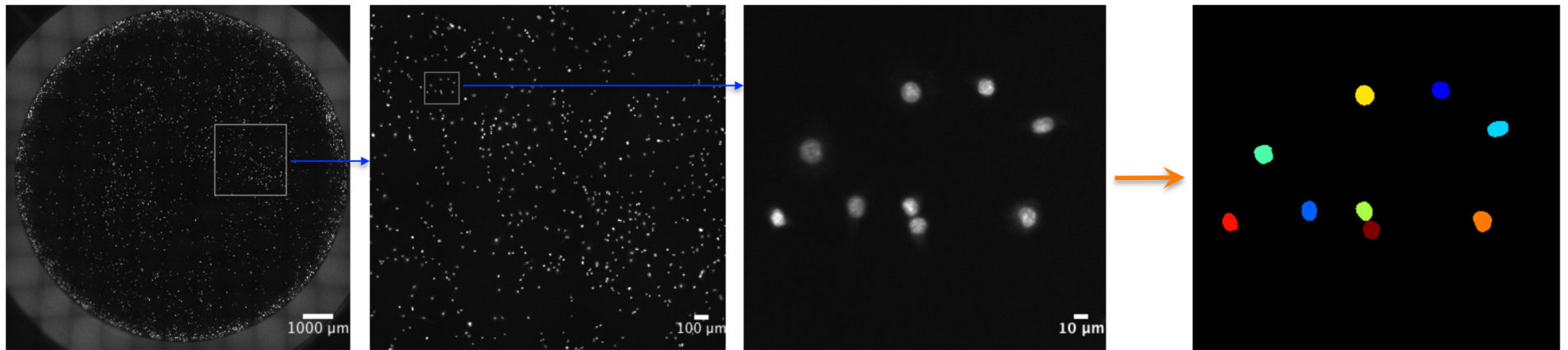
Using tools available in most labs, we have created a relatively simple optical counting setup for the quantification of multiple adherent cell types in a multiwell plate. After plating cells, adding condition, and fluorescent staining, the proposed system uses a standard fluorescent microscope to capture whole-well images. Image data is then run through ImageJ for preprocessing and CellProfiler for analysis to generate both absolute cell counts for every well as well as morphological values. Furthermore, utilizing a combination of staining techniques, multiple cell types in a co-culture setup (Cell A & B as an example) can be uniquely identified and absolutely counted.



**Figure 2**(on next page)

Automated, whole-well imaging.

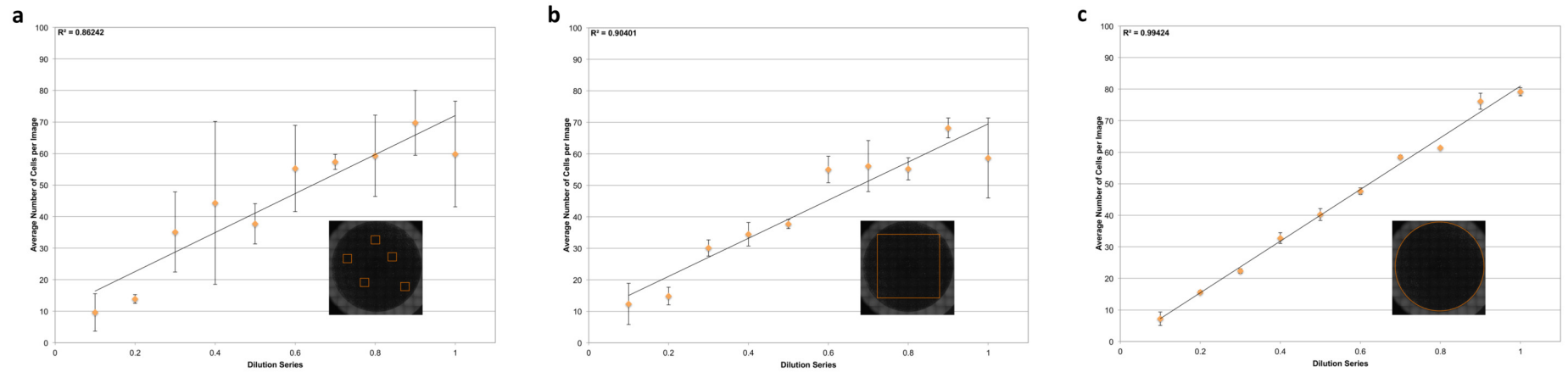
Using a fluorescent microscope with motorized x, y, and z stage, images spanning the entire well can be sequentially captured and stitched together to produce a high resolution, whole-well image. In the image series above, cell nuclei stained with DAPI were imaged on a 48-well plate with a 10x objective and stitched together. Sequential zooms of the whole-well image demonstrate the incredibly high resolution of the photo, which enables single-cell counting and analysis using a cell segmentation software like CellProfiler (used to generate the final mask).



**Figure 3**(on next page)

Power of whole-well imaging and nuclear quantification.

A linear dilution series of JC CRL 2116 cells going from 10,000 cells/well down to 1,000 cells/well was plated on a 48-well plate. Whole-well images of cell nuclei stained with DAPI were then captured and processed to produce either (a) five random images, (b) box crop, or (c) whole-well images, which were then used to determine cell count and generate a linear curve. Accuracy improves significantly as the percent of the experimental space being assayed increases. Error bars represent the standard deviation between triplicate conditions.

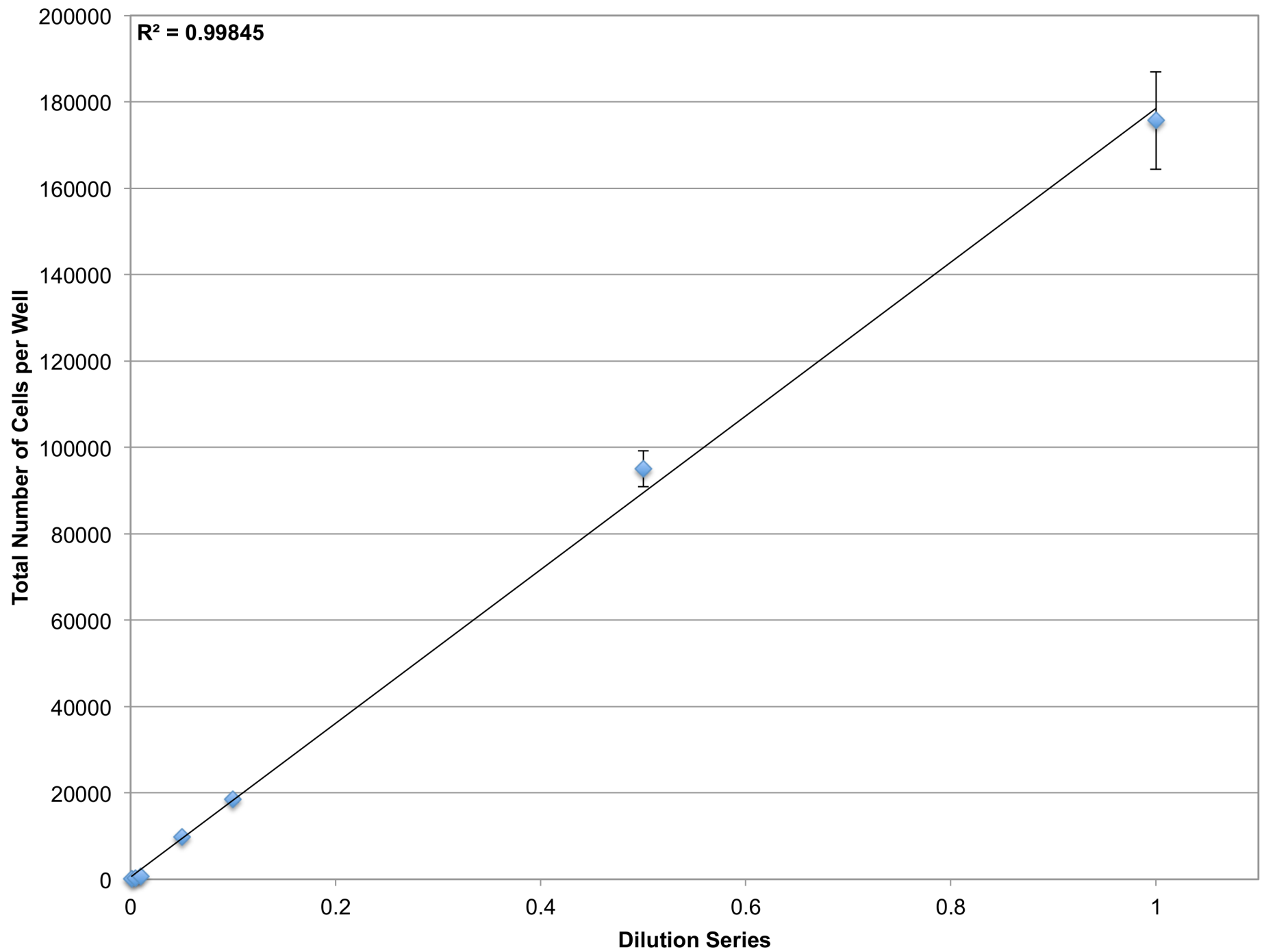




**Figure 4**(on next page)

Determining dynamic range.

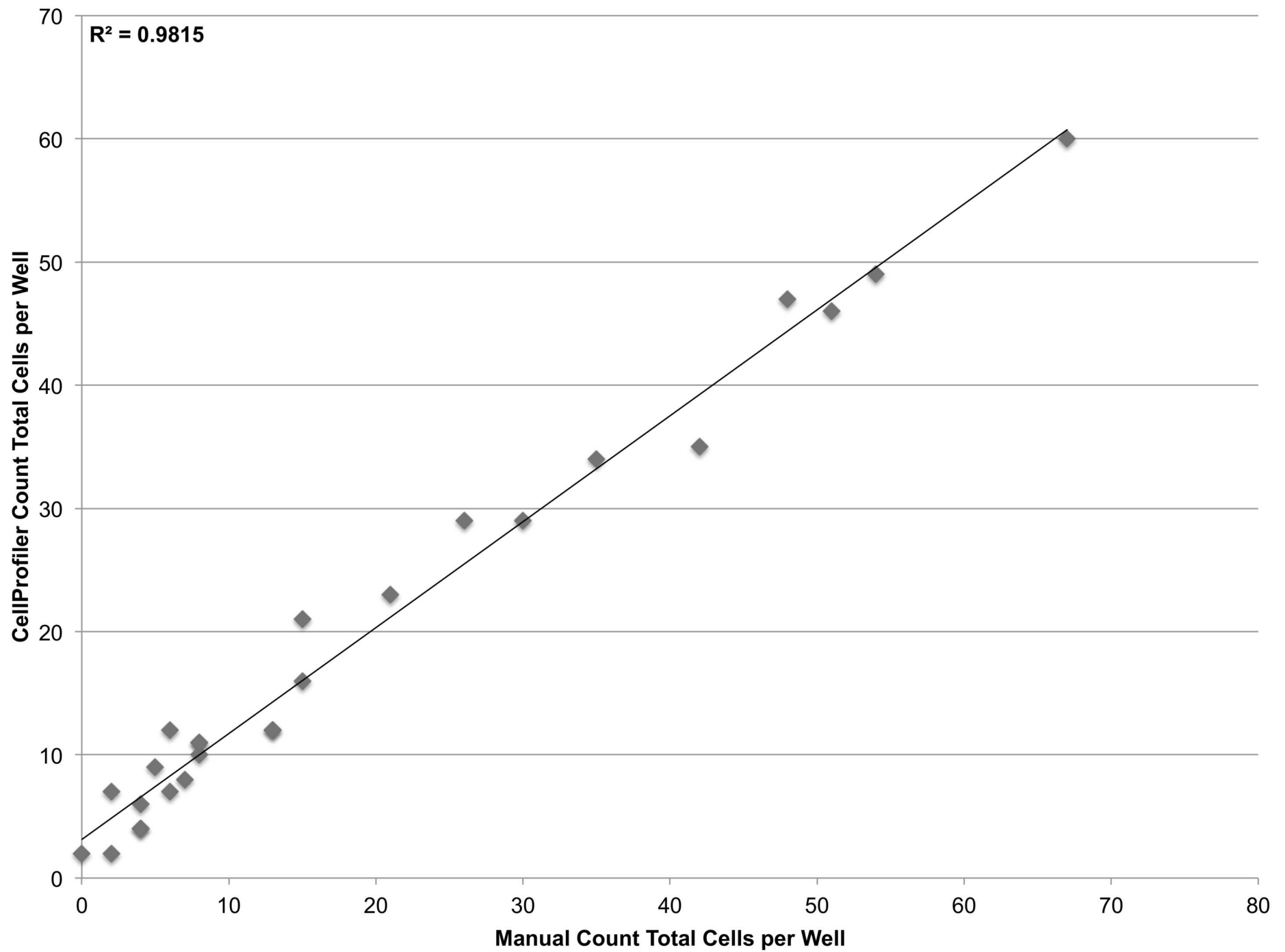
Half-log dilutions of JC CRL 2116 cells going from 100,000 cells/well down to 100 cells/well were plated on a 12-well plate (an experiment spanning three orders of magnitude). Cell nuclei stained with DAPI were then quantified and used to generate a linear curve. The system performs robustly over a wide dynamic range and is limited only by the surface area of the multiwell. Error bars represent the standard deviation between triplicate conditions.



**Figure 5**(on next page)

Establishing sensitivity.

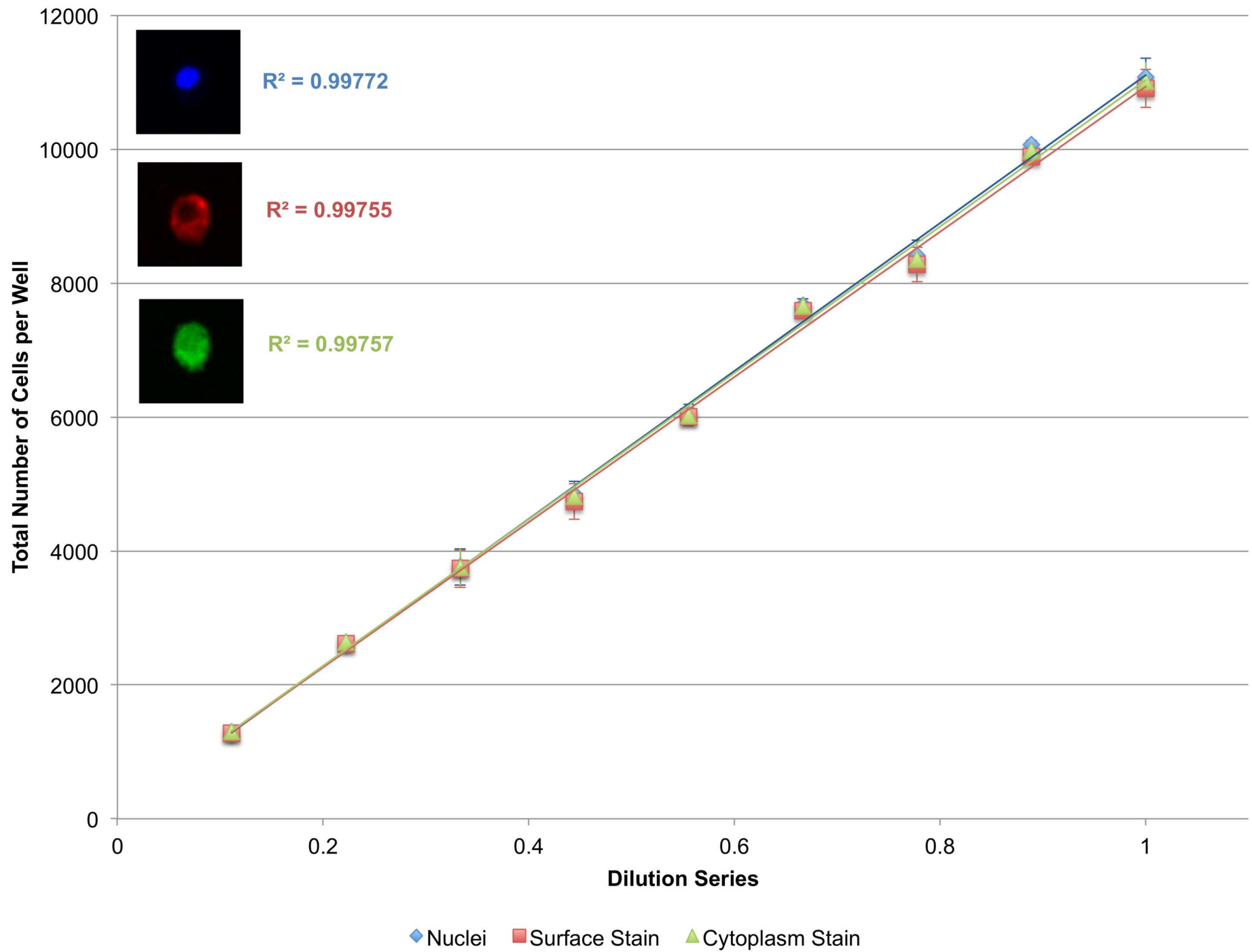
Various concentrations of JC CRL 2116 cells going from 100 cells/well down to 1 cell/well were plated on a 48-well plate. CellProfiler-derived counts of DAPI stained nuclei were compared with cell counts obtained by human assessment of associated brightfield images for each well. The system performs robustly even at the single-cell level with most deviations attributable to human error when manually counting.



**Figure 6**(on next page)

Secondary quantification of surface and cytoplasmic stains using nuclei as seeds.

A linear dilution series of J774.A1 cells going from 10,000 cells/well down to 1,000 cells/well was plated on a 48-well plate. Cells were stained with Vybrant CFDA SE (cytoplasmic stain), phycoerythrin (PE)-conjugated anti-CD11b antibodies (surface stain), and DAPI (nuclear stain). Using nuclei as seeds, cells delineated by a surface or cytoplasmic stain could be accurately quantified as demonstrated by the near-perfect  $R^2$ . Error bars represent the standard deviation between triplicate conditions.



**Figure 7** (on next page)

Tumoricidal properties of primed macrophages in the presence of co-cultured tumor cells.

J774.A1 macrophages were primed with either IFN $\gamma$ , LPS, or both and subsequently co-cultured with JC CRL 2116 tumor cells. J774.A1 cells were labeled with PE-conjugated anti-CD11b antibodies (red surface stain) while JC CRL 2116 cells were labeled with Vybrant (green cytoplasmic stain). Both cells were also stained with DAPI. (a) Normalized and (b) absolute cell counts as well as (c) cell area were determined for each condition. (d) CD11b expression levels as well as macrophage uptake/phagocytic activity were calculated by extracting the mean fluorescent intensity of macrophage PE and Vybrant staining respectively. The experiment reveals an interesting, dynamic relationship between activated macrophages and target tumor cells that would have been missed by any setup that looks at relative counts. Data for (a), (c), and (d) are normalized to the unprimed control. Error bars represent the standard deviation between triplicate conditions.

