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Computational Testing for Automated Preprocessing: a Matlab toolbox for better electroencephalography data processing

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EEG is a rich source of information regarding brain functioning, and is the most lightweight and affordable method of brain imaging. However, the pre-processing of EEG data is quite complicated and most existing tools present the experimenter with a large choice of methods for analysis, but no framework for method comparison to choose an optimal approach. Additionally, many tools still require a high degree of manual decision making for, e.g. the classification of artefacts in channels, epochs or segments. This introduces excessive subjectivity, is slow, and is not reproducible. Batching and well-designed automation can help to regularise EEG preprocessing, and thus minimise human effort, subjectivity, and consequent error. The Computational Testing for Automated Preprocessing (CTAP) toolbox facilitates: i) batch processing that is easy for experts and novices alike; ii) testing and comparison of automated methods. CTAP uses the existing data structure and functions from the well-known EEGLAB tool, based on Matlab, and produces extensive quality control outputs.

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ABSTRACT

EEG is a rich source of information regarding brain functioning, and is the most lightweight and affordable method of brain imaging. However, the pre-processing of EEG data is quite complicated and most existing tools present the experimenter with a large choice of methods for analysis, but no framework for method comparison to choose an optimal approach. Additionally, many tools still require a high degree of manual decision making for, e.g. the classification of artefacts in channels, epochs or segments. This introduces excessive subjectivity, is slow, and is not reproducible. Batching and well-designed automation can help to regularise EEG preprocessing, and thus minimise human effort, subjectivity, and consequent error. The Computational Testing for Automated Preprocessing (CTAP) toolbox facilitates: i) batch processing that is easy for experts and novices alike; ii) testing and comparison of automated methods. CTAP uses the existing data structure and functions from the well-known EEGLAB tool, based on Matlab, and produces extensive quality control outputs.

Keywords: electroencephalography, computation, testing, automation, preprocessing, EEGLAB, signal processing

1 INTRODUCTION

2 Measurement of human electroencephalography (EEG) is a rich source of information regarding
3 certain aspects of brain functioning, and is the most lightweight and affordable method of brain
4 imaging. However, among those types of human electrophysiology data recorded from surface
5 electrodes (to which EEG is most similar in terms of recording methods, see e.g. Cowley et al.
6 (2016) for a review), EEG data is comparatively difficult to pre-process. The qualities which cause
7 difficulty for EEG analysis come in two classes: A) number and complexity of operations, and B)
8 size and indeterminacy of the data.

9 Specifically in class A, normally many operations are required, which is time-consuming
10 and therefore costly. Many of these operations require repeated human judgements, leading to
11 subjectivity, non-reproducibility of outcomes, and non-uniformity of decisions. Compared to, e.g.,
12 counting peaks in an electrocardiogram signal, most variables of interest are relatively complicated
13 derivations from the raw signal, implying more room for error in analysis. Related to that, the
14 relatively complex 'standard' EEG processing operations are harder to debug.

15 In class B, for most research applications we can see that EEG data is high-bandwidth, systems
16 which consist of 256+ channels are available. Due to the *inverse problem* it is not possible to
17 precisely determine a 'ground truth' for the signal, i.e. a unique relationship to neural sources. The
18 signal is also highly variable between individuals, and even between intra-individual recording
19 sessions Dandekar et al. (2007).

20 Bigdely-Shamlo et al. (2015) emphasise the need for tools to process EEG data in an efficient
21 manner, and have pointed out that "artifact removal and validation of processing approaches remain
22 a long-standing open problem for EEG". While some standards have been suggested Keil et al.
23 (2014), there remains a deficit of tools and methods to support standardisation. These issues illustrate
24 the need for a software tool that helps to minimise human effort, subjectivity, and consequent error.
25 Batching and careful automation can help to regularise and streamline EEG pre-processing, for
26 which we present a solution in this paper.

27 Approach

28 We present the Computational Testing Automated Preprocessing (CTAP) toolbox, available from
29 GitHub ¹. CTAP is built on Matlab (r2015a and higher) and EEGLAB v13.4.4b (Delorme and
30 Makeig, 2004). The main aim of CTAP is to regularise and streamline EEG preprocessing. We
31 regularise with a scripted data-processing pipeline that ensures the treatment of each file is the
32 same. We streamline by separating the process of building functions from that of exploring and
33 tuning the data. These features improve reproducibility, and separate the menial and important tasks,
34 respectively.

35 In practice, the CTAP toolbox provides functionality for i) batch processing using scripted
36 EEGLAB-compatible functions; ii) testing and comparison of automated methods based on extensive
37 quality control outputs. In more detail, the core code supports scripted specification of a pipeline
38 of diagnostic and artefact correction steps, with robust looping execution of steps and automated
39 output of 'quality control' (QC) logs and imagery (more details provided below in Results). This
40 helps to maintain transparency and traceability of all operations performed for every EEG file. After
41 specification the pipeline can be adjusted to respond to QC issues.

42 Although CTAP works as a batch processing pipeline, it supports seamless integration of manual
43 operations. This works such that the user can define a pipeline of operations, insert save points at
44 appropriate steps, and work manually on that data before passing it back to the pipe.

45 CTAP is focused on leveraging existing methods that are compatible with EEGLAB-structured
46 data, and on providing a simple interface to plug in different styles of EEG signal processing. The
47 contribution we present is to extend EEGLAB for automated batch processing. This facilitates
48 reproducible brain imaging research with the following features:

- 49 • script based automated batch processing (no GUI)
- 50 • time consuming bookkeeping of intermediate analysis files and script execution is automated
- 51 • existing EEGLAB based analysis methods can be easily integrated
- 52 • automated QC output help to spot problems (see section Peeks)
- 53 • includes ready made tools for feature storage and export (see section CTAP outcomes)

54 In summary, CTAP lets the user focus on content, instead of time-consuming implementation of
55 foundation functionality. In the rest of the paper, we will describe how CTAP toolbox does this, and
56 provide a motivating example of its application.

57 After we address related work, section Materials & Methods details the architecture and usage of
58 CTAP. Section Results then describes the technical details and outcomes of a motivating example
59 application. In section Discussion we set out the philosophy and possible uses of CTAP toolbox,
60 including development as well as preprocessing; and describe issues and potential directions for
61 future work.

62 RELATED WORK

63 Many methods are available from the literature to facilitate automated preprocessing (for a review
64 see, e.g. Barua and Begum (2014)), and the rate of new contributions is also high. For example,
65 we conducted a search of the SCOPUS database for articles published after 1999, with "EEG"

¹<https://github.com/bwrc/ctap>

66 and "electroencephalography" in the title, abstract, or keywords, plus "Signal Processing" or
67 "Signal Processing, Computer-Assisted" in keywords, and restricted to subject areas "Neuroscience",
68 "Engineering" or "Computer Science". The search returned over 300 hits, growing year-by-year
69 from 5 in 2000 up to a mean value of 36 between 2010 and 2015. Non-systematic reviews of the
70 software tools available have been made by Agapov et al. (2016); Baillet et al. (2010), and in a
71 milestone special issue, Baillet et al. (2011) gathered a large number of the academic contributions
72 available at that time. This special issue is quite skewed toward tools for feature extraction, which
73 illustrates again the need for better/more up-to-date solutions for the fundamental stages of EEG
74 processing.

75 Among tools dedicated to EEG processing, EEGLAB (Delorme and Makeig, 2004) stands out
76 for popularity and high number of third-party contributors, to the degree that it is considered by
77 some to be a *de facto* standard. However EEGLAB is a graphical user interface (GUI)-based tool,
78 which limits the scale at which it can be used.

79 Other popular tools focus on a more diverse set of signals, especially including magnetoen-
80 cephalography (MEG). Brainstorm Tadel et al. (2011), Fieldtrip (Oostenveld et al., 2011), and
81 EMEGS (ElectroMagnetic EncaphaloGraphy Software) Peyk et al. (2011) are all open source tools
82 for EEG and MEG data analysis. Like EEGLAB, these tools are all *free* and *open source*, but
83 based on the commercial platform Matlab (Natick, MA), which can be a limitation in some contexts
84 due to high licence cost. Brainstorm in particular, but also the others, have originated with an
85 emphasis on cortical source estimation techniques and their integration with anatomical data. More
86 recently, Bigdely-Shamlo et al. (2015) released the PREP pipeline for Matlab, which also uses the
87 EEGLAB data structure but is aimed only at experiment-induced artefacts and not those deriving
88 from subject-activity such as, e.g. blinks.

89 The most notable commercial tool is Brainalyzer (Brain Products GmbH, Munich, Germany),
90 a graphical programming interface with a large number of features. NeuroPype is a commercial
91 Python-based graphical programming environment for biosignal processing. It is only available as a
92 closed beta and, to the authors' knowledge, has not been documented in a peer reviewed publication.

93 Tools which are completely *free* and *open source* are fewer in number and have received much
94 less supplemental input from third parties. Python tools include MNE-Python for processing MEG
95 and EEG data (Gramfort et al., 2013), and PyEEG (Bao et al., 2011), a module for EEG feature
96 extraction. MNE, like Brainstorm and Fieldtrip, is primarily aimed at integrating EEG and MEG
97 data. Several packages exist for the R computing environment, e.g. Tremblay and Newman (2015),
98 however these do not seem to be intended as general-purpose tools.

99 We have chosen to extend EEGLAB because it has received many contributions to the core
100 functionality, and is thus compatible with a good portion of the methods of EEG processing from
101 the literature. Some compatible tools from the creators of EEGLAB at the Swartz Centre for
102 Computational Neuroscience (SCCN) are detailed in Delorme et al. (2011), including tools for
103 forward head modelling, estimating source connectivity, and online signal processing. Other key
104 third-party preprocessing contributions to EEGLAB include SASICA (Chaumon et al., 2015),
105 FASTER (Nolan et al., 2010), and ADJUST (Mognon et al., 2011), all semi-automated solutions for
106 selection of artefactual data. The latter two are featured in CTAP as options for detecting bad data.

107 This integration of existing solutions illustrates the key difference of CTAP: it aims to extend an
108 existing rich ecosystem of EEG-specific methods, by meeting a clear need within that ecosystem.

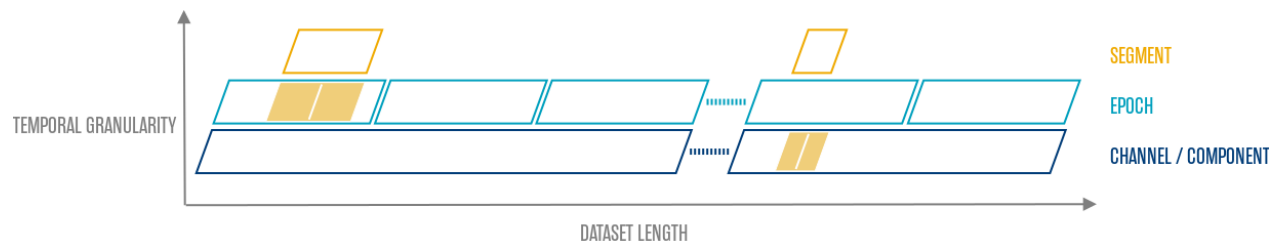


Figure 1. Relationship of the time domain data constructs dealt with in CTAP.

MATERIALS & METHODS

The core activity of CTAP is preprocessing EEG data by cleaning artefacts, i.e. detection and either correction or removal of 'bad' data, that is not likely to be attributable to neural sources. CTAP is able to operate on three different temporal granularities: channel, epoch and segment. Channel operations affect the entire time series at one spatial location. Epoch operations are performed on one or several epochs produced by EEGLAB epoching function. Finally, segments are fixed time-windows around specific events which can be extracted from both channel and epoch levels, see Figure 1. An example of a typical segment could be a blink artefact with a window wide enough to include the entire blink waveform. Further functionality is provided for independent component analysis (ICA)-based methods. Artefact-detection methods based on some flavour of ICA algorithm have been shown to outperform temporal approaches Delorme et al. (2007). It was also shown that independent components (ICs) are valid representations of neural sources (Delorme et al., 2012). CTAP can thus help to combine the existing methods for EEG signal processing.

Outline of usage

Figure 2 shows the core components of CTAP. The colored boxes represent entities that the user has to specify in order to use CTAP. These are:

- what analysis functions to apply and in which order (analysis-pipe)
- parameters for the analysis functions (parameters)
- which EEG measurements/files to process (what-to-analyze)

Typically the analysis is run by calling a single script that defines all of the above and passes these on to a function that performs all requested analysis steps on all specified measurements. In the following, we describe in more detail how the configurations are made, how the pipe is executed, what outputs it provides and what options the user has to control the pipe. The complete details of all these aspects of CTAP are provided in the wiki pages of the GitHub repository, which will be referenced below as 'the wiki'².

Configuration

Let us assume that the main analysis script is stored in a file called `runcatap_projectX.m`. First of all, this file specifies which *analysis steps* are performed in which order. An example of an analysis step is e.g. filtering or bad channel detection. Analysis steps can further be grouped into sets of steps referred to as *step sets*. An intermediate save is done after each step set, providing

²<https://github.com/bwrc/ctap/wiki>

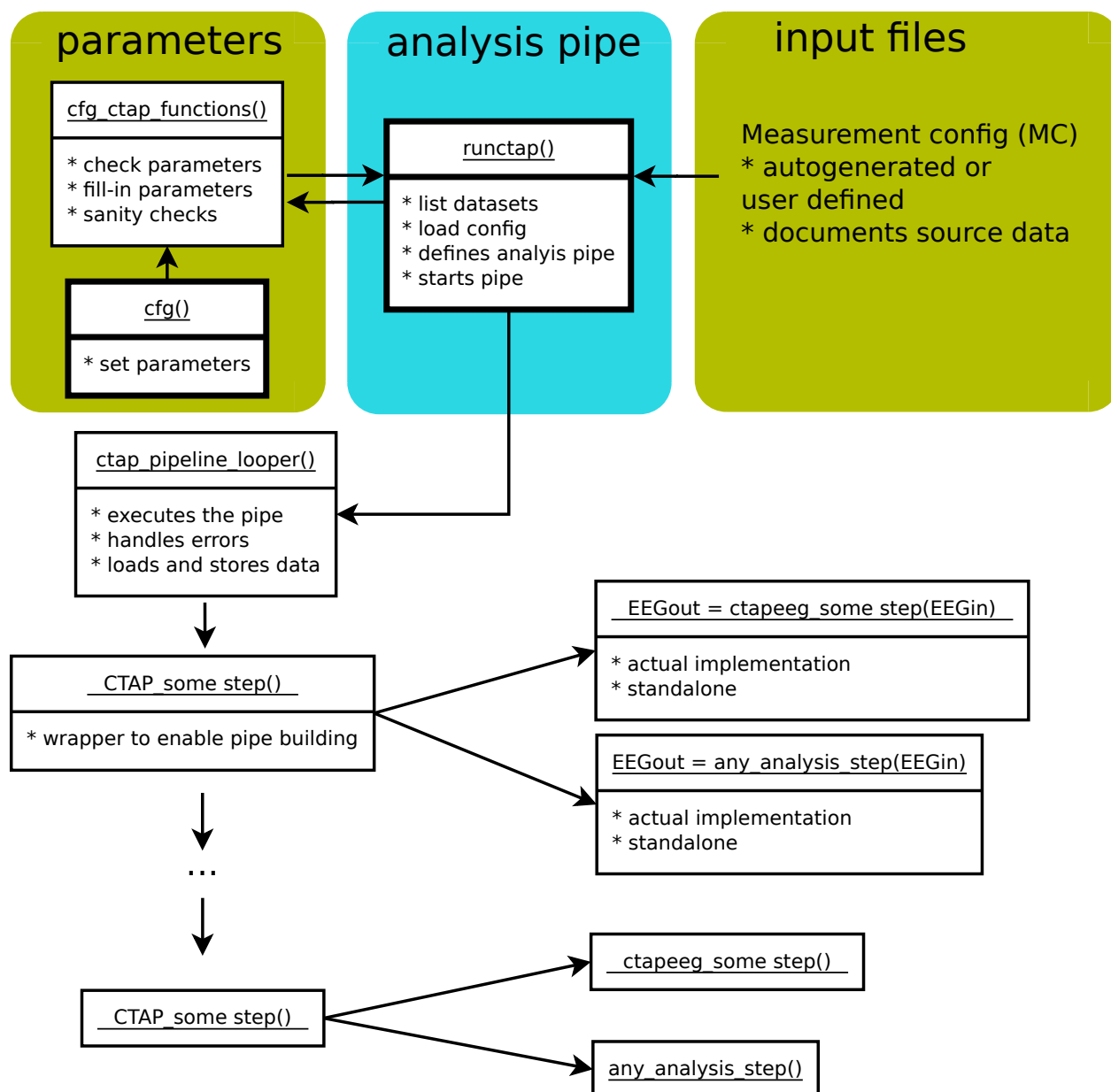


Figure 2. An overview of the core logic of CTAP. 'parameters', 'analysis pipe' and 'input files' illustrate the parts user must specify. White boxes represent Matlab functions, with the function-name on top and bulleted notes below. The functions which require user attention, `cfg()` and `runctap()`, have bold borders and can be freely named by the user. For good practice, these two functions take the name of the analysis pipe they implement, e.g. `runctap_mypipe()`.

139 a possibility run the whole pipe in smaller chunks. Below is a sample definition of a very small
140 analysis pipe with two step sets:

```
141 i = 1; %stepSet 1
142 stepSet(i).funH = { @CTAP_load_data, ...
143                   @CTAP_load_chanlocs, ...
144                   @CTAP_tidy_chanlocs, ...
```



```

145         @CTAP_reref_data, ...
146         @CTAP_blink2event};
147 stepSet(i).id = [num2str(i) '_load_WCST'];
148 stepSet(i).srcID = '';
149
150 i = i+1; %stepSet 2
151 stepSet(i).funH = { @CTAP_filter_data};
152 stepSet(i).id = [num2str(i) '_filter'];
153 stepSet(i).srcID = '';

```

154 The core function for pipe processing is designed to use functions named `CTAP_*()`, as these
155 are defined to have a fixed interface. They take two arguments: data (EEG) and configuration struct
156 (`Cfg`); and they return the same after any operations. Some `CTAP_*()` perform all operations
157 (e.g. call EEGLAB functions) directly, while others call a corresponding `ctapeeg_()` function
158 that actually implements the task. Hence `CTAP_*()` functions can be regarded as wrappers that
159 facilitate batch processing (uniform interface) and also implement e.g. the plotting of quality control
160 figures. Since they are quite simple, new `CTAP_*()` functions can easily be added by the user to
161 include new analysis steps, according to the provided `CTAP_template_function()`. Users can
162 also call the `ctapeeg_()` functions directly as part of their own custom scripts, since these are
163 meant to be used like e.g. any EEGLAB analysis function.

164 Once the analysis functions have been defined the next step is to define parameters for the whole
165 pipe, and for each analysis function. Default parameters are provided for most cases, but it is optimal
166 to fine tune the behaviour. Like before, parameter information is passed to CTAP using a struct.
167 It is usually practical to store the struct in a separate m-file, lets say `ctapcfg_projectX.m`. A
168 typical minimal contents of this file might be:

```

169 function [Cfg, FP] = cfg_minimal(dataRoot, branchID)
170
171 %% Analysis output (data, quality control) storage location
172 Cfg.env.paths.analysisRoot = fullfile(dataRoot,'ctap',branchID);
173
174 %% Channel specifications
175 Cfg.eeg.chanlocs = fullfile(dataRoot,'channel_locations_acticap_32.ced');
176 Cfg.eeg.reference = {'TP10' 'TP9'}; % EEG reference channels to use
177
178 %% Configure analysis functions
179
180 % Load data
181 FP.load_data = struct('type', 'neurone');
182
183 % Amplitude thresholding from continuous data (bad segments)
184 FP.detect_bad_segments = struct('amplitudeTh', [-100, 100]); %in muV

```

185 The third requirement to run the pipe is input data. In CTAP the input data are specified
186 using a table-like structure called *measurement config* that lists all available measurements, the
187 corresponding raw EEG files etc. The reason for using a dedicated data structure is that it allows
188 for an easy selection of what should be analysed and it also helps to document the project. The

189 measurement config structure can be either created manually, or it can be auto-generated based
 190 on a list of files or a directory (for details see the wiki). The former allows for full control and
 191 enforces project documentation whereas the latter is intended for effortless one-off analyses. Both
 192 spreadsheet and SQLite formats are supported.

193 In the last required step before pipeline execution, the configuration struct and the parameter
 194 struct are checked, finalised and integrated by `cfg_ctap_functions()`.

195 Pipe execution

196 Once all the prerequisites listed above have been specified, the pipe is run using `CTAP_pipeline_looper()`.
 197 This function takes care of loading the correct (initial or intermediate) data set, applying the specified
 198 functions from each step set, and intermediate saving of the data. The looper manages error handling
 199 such that it is robust to crashing (unless in Debug mode), and will simply skip the remaining steps
 200 for a crashed file. Other settings determine how to handle crashed files at later runs of the pipe (see
 201 Documentation).

202 Analysis results are saved into the `Cfg.env.paths.analysisRoot` directory. A typical
 203 structure of this directory is shown in Figure 3.

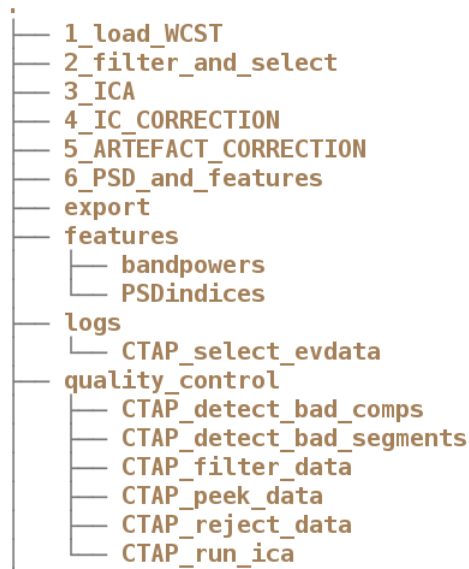


Figure 3. Typical directory tree.

204 First five directories contain intermediate results; their names are taken from the step set IDs
 205 as defined by the user. Directory `export` contains exported feature data (txt, csv or SQLite
 206 format), `features` computed EEG features in Matlab format, `logs` log files from each run, and
 207 `quality_control` contains quality control plots. The quality control plots reflect the analysis
 208 steps chosen by the user.

209 Apart from running the complete pipe at once the user has many options to run just a subset
 210 of the pipe, analyse only certain measurements, or otherwise adjust usage. Table 1 gives some
 211 examples.

212 CTAP outcomes

213 **Visual evaluation** CTAP automatically produces plots that help the user to answer questions such
 214 as: what has been done, what the data looks like, and was an analysis step successful or not. A full

Table 1. Some advanced ways to use the pipe.

| Usage | Options | Possible Reasons | How |
|-----------------------------------|---------------|---|---|
| Subset sets | step | investigate a bug; recompute only intermediate results | set run sets to subset index, e.g. <code>Cfg.pipe.runSets = 3:5</code> |
| Run <i>test</i> set | step | test new feature before including in pipe | add step set with id 'test', then set <code>Cfg.pipe.runSets = 'test'</code> |
| 'Rewire' pipe | the | test an alternative ordering of existing steps or temporarily change the input of some step | set the <code>.srcID</code> of a given step set equal to the <code>id</code> of another |
| Measurement configuration filter | run pipe for: | subset of test subjects, or: measurements classes with separate configurations, e.g. pilots | use function <code>struct_filter()</code> |
| Run in debug mode | debug | develop new method in CTAP | set <code>CTAP_pipeline_looper</code> parameter 'debug', true |
| Overwrite obsolete results | ob- | update part of pipe: write new step set output over existing files | set <code>CTAP_pipeline_looper</code> parameter 'overwrite', true |
| Write files from failed step sets | files | check partial outcome of step set | set <code>CTAP_pipeline_looper</code> parameter 'trackfail', true |
| Turn off intermediate saves | inter- | extract numerical/visual analytics without producing updated files | set <code>stepSet(x).save = false;</code> set <code>stepSet(x+1).srcID = stepSet(x-1).id</code> |

215 list of features can be found in the wiki documentation. Selected visualizations are described in
 216 more detail in Section Results. Examples include:

- 217 • blinks: detection quality, blink ERP
- 218 • bad segments: snippets of raw EEG showing detections
- 219 • EEG amplitudes: amplitude histograms, peeks
- 220 • filtering: PSD comparison
- 221 • ICA: IC scalpmap contact sheets, zoom-ins of bad components

222 **Quantitative evaluation** Every major pipe operation writes a record to the main log file. Data
 223 rejections, including channels, epochs, ICs or segments, are summarised here and also tabulated

224 in a separate 'rejections' log. Values are given for how much data was marked as bad, and what
225 percentage of the total was bad. If more than 10% of data is marked bad by a single detection, a
226 warning is given in the main log.

227 In addition, useful statistics of each channel are logged at every call to `CTAP_peek_data()`,
228 based on the output of the EEGLAB function `signalstat()`. Datapoints include trimmed and
229 untrimmed versions of mean, median, standard deviation as well as skewness, kurtosis and normality
230 testing.

231 **Feature export** Extracted EEG features are stored internally as Matlab structs that fully document
232 all aspects of the data. These can be used to do statistical analysis inside Matlab. However, often
233 users like to do feature processing in some other environment such as R or similar. For this, CTAP
234 provides export functionality that transforms the EEG feature mat files into txt/csv text files, and/or
235 an SQLite database. For small projects (for example, up to 10 subjects and 16 channels) txt/csv
236 export is feasible but for larger datasets SQLite is more practical.

237 **Data formats** CTAP uses a number of custom data formats for configuration and data export
238 purposes. Examples include the *measurement config* file for storing information related to available
239 raw EEG files, measurement structure specifications and internal feature storage format used for
240 storing features prior to export. All these are documented in detail in the wiki pages. However, as
241 demonstrated by the motivating example (section Results), a basic analysis using CTAP does not
242 require any knowledge of these.

243 RESULTS

244 We describe a motivating example that can also be used as a starting point for one's own analysis
245 pipe.

246 **Data.** We use synthetically generated data with blink, myogenic (EMG), and channel variance
247 artefacts to demonstrate the usage and output of CTAP. The example is part the repository (see
248 function `runctap_manuscript.m`) and the details of the synthetic data generation process are
249 documented in the wiki³.

250 **Pipeline.** In the following sections, we show some example output of CTAP applied to the
251 synthetic dataset, based on the analysis-pipe step sets shown below. The analysis steps marked
252 red are next discussed in more detail. For each step, we will first step through the data processing
253 outcomes, then illustrate the QC output generated.

```
stepSet(1).funH = { @CTAP_load_data, ...  
                  @CTAP_load_chanlocs, ...  
                  @CTAP_tidy_chanlocs, ...  
                  @CTAP_reref_data, ...  
                  @CTAP_blink2event, ...  
                  @CTAP_peek_data};  
  
stepSet(2).funH = { @CTAP_filter_data, ...  
                  @CTAP_select_evdata, ...  
                  @CTAP_run_ica};
```

³<https://github.com/bwrc/ctap/wiki/syndata-generation>

```
stepSet(3).funH = { @CTAP_detect_bad_comps, ...
                   @CTAP_reject_data, ...
                   @CTAP_peek_data};

stepSet(4).funH = { @CTAP_detect_bad_channels, ...
                   @CTAP_reject_data, ...
                   @CTAP_detect_bad_segments, ...
                   @CTAP_reject_data, ...
                   @CTAP_interp_chan, ...
                   @CTAP_peek_data};

stepSet(5).funH = { @CTAP_compute_psd, ...
                   @CTAP_extract_bandpowers, ...
                   @CTAP_extract_PSDindices};
```

254 Blinks

255 **Detection** The function `CTAP_blink2event()` creates a set of new events with latencies and
256 durations matched to detected blinks.

257 The current blink detection implementation is based on the EOGERT algorithm by Toivanen
258 et al. (2015)⁴. The algorithm finds all local peaks in the data, constructs a criterion measure and
259 classifies peaks into blinks and non-blinks based on this measure.

260 Blinks can either be rejected or corrected using a method combining blink template matching
261 and Empirical Mode Decomposition (EMD) based on high-pass filtering of ICs by Lindsen and
262 Bhattacharya (2010). Thus, in this pipe the blink events are used by `CTAP_detect_bad_comps()`
263 and `CTAP_reject_data()` to detect and correct the blinks.

264 **Visualization** The EOGERT detection process visualizes the classification result for QC purposes,
265 as shown in Figure 4. Such figures make it easy to spot possible misclassifications.

266 The success of the blink correction is evaluated using blink Evoked Response Potentials (ERPs)
267 (see e.g. Frank and Frishkoff (2007)) as shown in Figure 5. The correction method clearly removes
268 the blink but leaves the underlying EEG largely intact. Some baseline shifts are visible but distortions
269 to oscillatory activity are minor.

270 Peeks

271 **Peek logic** The `CTAP_peek_data()` function helps to regularize data inspection. Visual in-
272 spection of raw data is a fundamental step in EEG evaluation. A logical approach is to compare
273 the raw data from before and after any correction operations. If ICA-based corrections are made,
274 the same approach can also be used on the raw plot of IC data. CTAP aims to expedite this step.
275 `CTAP_peek_data()` will generate raw data plots of randomly-chosen time-points⁵. These 'peek-
276 points' are embedded as events which can then be plotted at a later stage in the pipe, generating true
277 before-after comparisons even if the data time course changes (due to, e.g., removal of segments). If
278 no peek-point data remains at the 'after' stage, no comparison can be made; however if peek-points
279 are randomly chosen, then such an outcome is itself a strong indication that the data is very bad, or
280 the detection methods are too strict.

⁴See code repository at <https://github.com/bwrc/eogert>

⁵Points can also be set by the user, e.g. chosen from existing events.

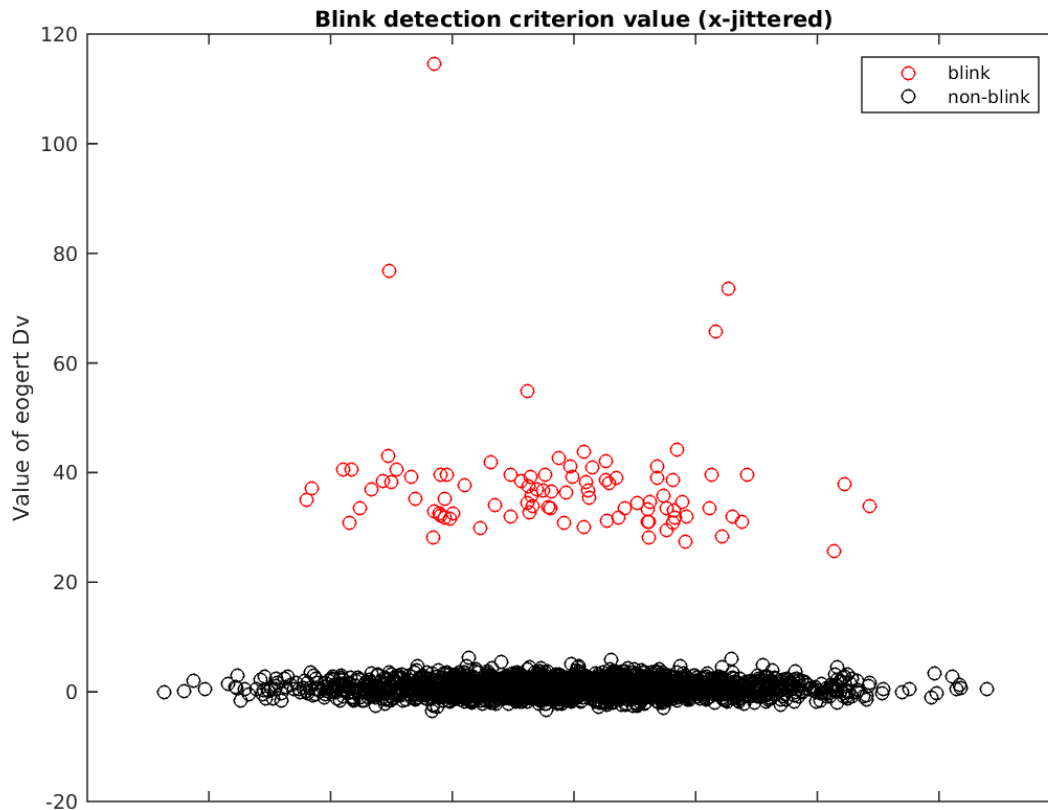


Figure 4. An example of the criterion used to detect blinks. Vertical axis shows the criterion value while horizontal axis is random data to avoid overplotting. The classification is done by fitting two Gaussians using the EM algorithm and assigning labels based on likelihoods.

281 `CTAP_peek_data()` will also estimate a set of statistics for every data channel, saved in
 282 Matlab table format and also aggregated to a log file.

283 **EEG amplitudes** Many EEG artefacts cause large changes in signal amplitudes and consequently
 284 several basic yet effective EEG artefact detection methods are based on amplitude thresholding. On
 285 the other hand measurement conditions and test subject can affect the amplitude of the recorded
 286 signal. Hence accurate knowledge of the average signal amplitude is often important. CTAP
 287 includes plotting routines for signal amplitude histograms as well as for raw EEG data.

288 A sample signal amplitude histogram produced using CTAP is show in Figure 6. It can be used
 289 e.g. to detect loose electrodes or in finding a suitable threshold for bad segment detection.

290 **Bad IC detection & rejection**

291 CTAP usage logic suggests that one or more detect operations for a given data type, e.g. chan-
 292 nels, *or* epochs, *or* components, should be followed by a reject operation. It is bad practice to
 293 detect bad data across modalities, e.g. channels and epochs, before rejecting any of it, because
 294 artefacts of one type may affect the other. Thus we describe `CTAP_detect_bad_comps()` and
 295 `CTAP_reject_data()` together.

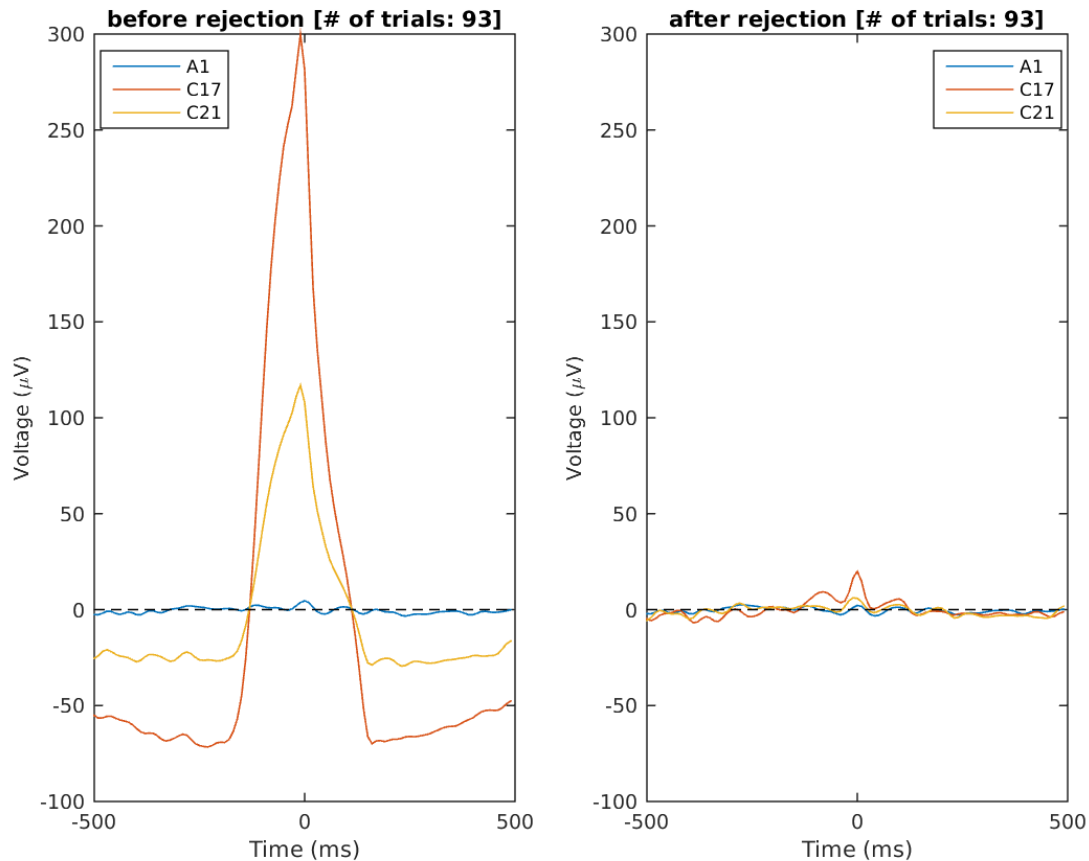


Figure 5. An example of the blink ERP. The left panel shows the blink centered ERP before correction with a clearly visible blink signal. The right panel shows the same plot after correction. The blink is clearly removed but the underlying EEG remains largely unaffected because the correction was done in IC base.

296 **Detection** CTAP contains several options to detect artifactual ICs (for details, see function
 297 documentation), similarly to other `CTAP_detect_bad_*` () functions. Whichever option is used,
 298 a field is created in the EEG struct to store the results. Another field collects all detections, pointing
 299 to the results. The logic that is then available to the user is to call one or many detection functions,
 300 possibly pooling the results of several approaches to bad data detection, and then pass the aggregate
 301 results to the `CTAP_reject_data` () function.

302 **Rejection** `CTAP_reject_data` () checks the detect field to determine which data type is due
 303 for rejection, unless explicitly instructed otherwise. Based on the data labelled by prior calls to
 304 detection functions, `CTAP_reject_data` () will call some internal EEGLAB function such as
 305 `pop_select` (), to remove the bad data.

306 **Visualization** Upon rejection EEGLAB plotting tools are used to produce plots that characterize
 307 the rejected components. An example of such plot is given in Figure 7.

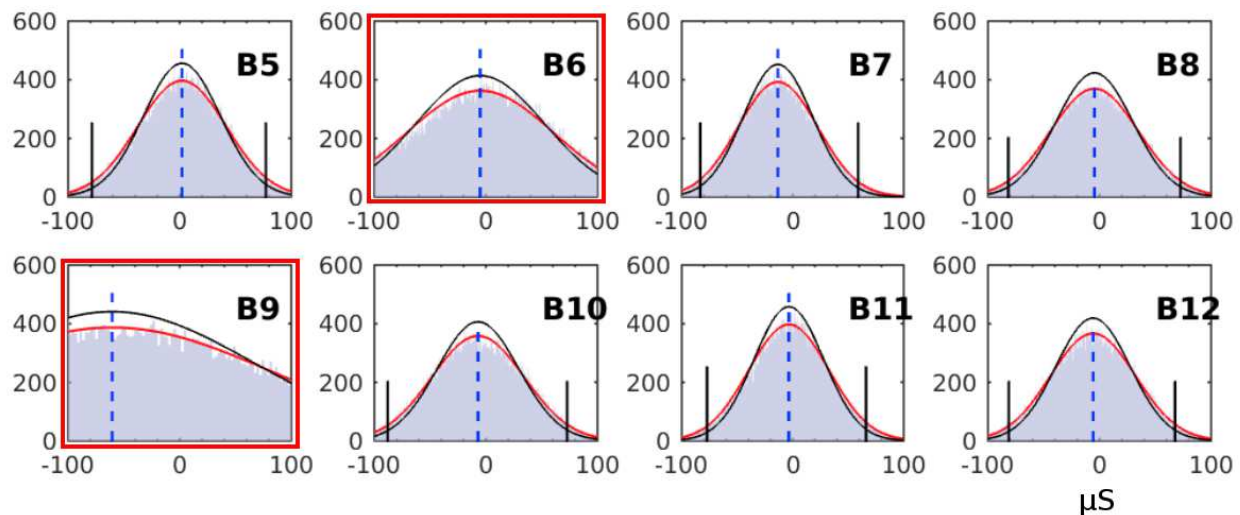


Figure 6. EEG amplitude histograms for eight channels. Fitted normal pdf is shown in red solid line, fitted normal pdf using trimmed sd in black solid line, upper and lower 2.5 % quantiles are vertical black solid lines, and distribution mean is vertical dashed blue line. Bad channels B6, B9 are highlighted red.

DISCUSSION

Philosophy, Benefits and Issues

The overall goal of CTAP is to improve on typical ways of preprocessing high-dimensional EEG data through a structured framework for automation. Automation both reduces the work load of the user and also removes subjectivity from the analysis. CTAP output can also be more easily reproduced because manual processing steps have been minimized. This enables the user to perform multiple comparative analyses for testing the robustness of the results against different preprocessing methods.

CTAP provides many default parameters, and streamlines many features into a handful of wrapper functions. This is in order to facilitate rapid build and testing of analysis pipes. The philosophy is to prevent users becoming 'stuck' in a single approach to the data because they have invested much in building the preprocessing code for it from scratch; or worse, because they have completed a laborious manual processing task and cannot afford to repeat it. However, the user should not usually rely on defaults, because the optimal choice often depends on the data. This is also one reason to have separate files for pipeline and parameters. Separating these by files is convenient for e.g. testing multiple parameter configurations.

As different analysis strategies and methods can vary greatly the best approach was to implement CTAP as a modular system. Each analysis can be constructed from discrete steps which can be implemented as standalone functions. The only requirement is to suppress all types of pop-ups or GUI-elements which would prevent the automatic execution of the analysis pipe. It is also up to the user to call the functions in the right order (e.g., not calling averaging before epoching). As CTAP is meant to be extended with custom analysis functions the interface between core CTAP features and external scripts is also well defined in the documentation.

CTAP never overrides the user's configuration options, even when these might break the pipe. For example, `CTAP_reject_data()` contains code to autodetect the data to reject. However the user can set this option explicitly, and can do so without having first called any corresponding

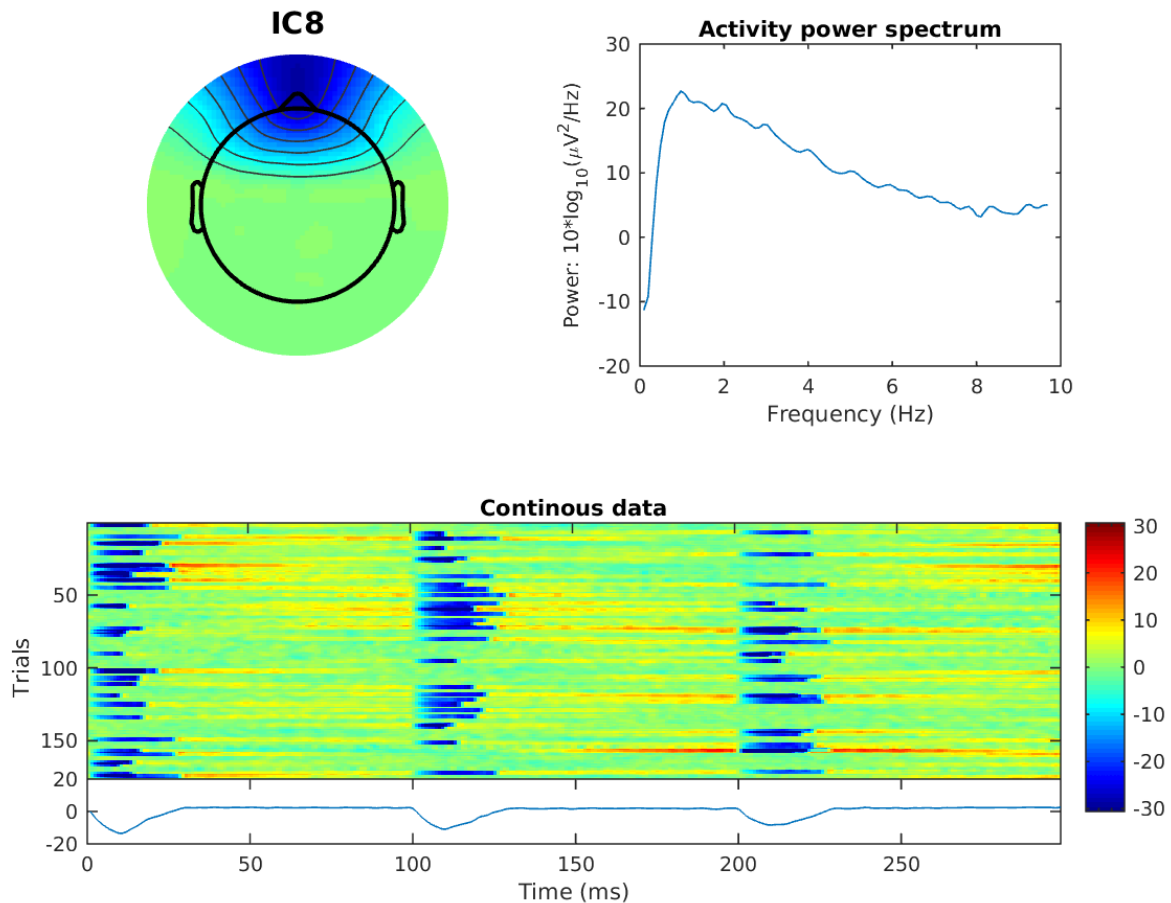


Figure 7. An example of a plot describing a bad ICA component - in this case the algorithm used to find the bad data was the blink detection procedure described above. Shown are component scalp map (top left), component power spectrum (top right), event-related spectral potential (ERSP) plot (bottom).

334 detection function, which will cause preprocessing on that file to fail. Allowing this failure to happen
 335 is the most straightforward approach. Combined with an informative error message the user gets
 336 immediate feedback on what is wrong with the pipe.

337 On the other hand, CTAP does provide several features to handle failure gracefully. As noted, the
 338 pipe will not crash if a single file has an unrecoverable error, although that file will not be processed
 339 further. This allows a batch to run unsupervised. Then, because no existing outputs are overwritten
 340 automatically, you can easily 'mop up' the files that failed without redoing all those that succeeded,
 341 if the fault is identified. Because pipes can be divided to step sets, the 'tricky' processes that are
 342 prone to failure can be isolated and reduce the overall time spent on crash recovery. CTAP also
 343 allows crashed files to be saved at the point of failure, permitting closer analysis of the problematic
 344 data.

345 In contrast to most analysis plugins built on top of EEGLAB, no graphical user interface (GUI)
 346 was included in CTAP. While GUIs have their advantages (more intuitive data exploration, easier
 347 for novice users, etc) it would have been very difficult and time consuming to add one to a complex a
 348 system like CTAP. The GUI also sets limits to configurability and can cause problems for automation

349 if analysis pipes is executed on a hardware with no graphical capabilities. The absence of GUI also
350 makes the development of extensions easier as there are fewer dependencies to worry about.

351 In contrast to many other physiological data analysis tools, CTAP is designed to meet a very
352 focused goal with a specific approach. This does however create some drawbacks. Compared to
353 scripting ones own pipeline from scratch, there are usage constraints imposed by the heavy use of
354 struct passing interfaces. There is a learning curve for using some non-obvious features and it can
355 be difficult to understand some the more complex underlying processes.

356 CTAP is also built to enable easy further development by third parties, by using standardised
357 interfaces and structures. This was a feature of original EEGLAB code, but contrasts with many
358 of the EEGLAB-compatible tools released since, where functionality was often built in an *ad hoc*
359 manner. The main requirement for development is to understand the content and purpose of the
360 EEG .CTAP field (which is extensively documented in the wiki), and the general logic of CTAP.

361 Developers can easily extend the toolbox by using (or emulating) the existing `ctapeeg_*()`
362 functions, especially the `ctapeeg_detect_*()` functions, which are simply interfaces to external
363 tools for detecting artefacts. Existing `CTAP_*()` functions can be relatively more complex to
364 understand, but the existing template provides a guideline for development with the correct interface.

365 Future work

366 CTAP is far from finalized, and development will continue after the initial release of the software.

367 Many publications have described methods for processing EEG for different purposes, such as
368 removing artefacts, estimating signal sources, analysing event-related potentials (ERPs), and so
369 on. However despite the wealth of methodological work done, there is a lack of benchmarking, or
370 tools for comparison of such methods. The outcome is that the most reliable way to assess each
371 method is to learn how to it works, apply it, and test the outcome on one's own data: this is a highly
372 time-consuming process which is not competitive with simply performing the bulk of preprocessing
373 in a manual way, as seems to remain the 'gold standard'. The effect of each method on the data is
374 also not commonly characterised, such that methods to correct artefacts can often introduce noise to
375 the data, especially where there was no artefact (false positives).

376 In section Approach we described the aim to test and compare automated methods for prepro-
377 cessing. This is still work in progress, as we are building an extension for CTAP that improves
378 testing and comparison of preprocessing methods by repeated analyses on synthetic data. This
379 extension, tentatively titled Handler for sYnthetic Data and Repeated Analyses (HYDRA), will
380 use synthetic data to generate ground truth controlled tests of preprocessing methods. It will have
381 capability to generate new synthetic data matching the parameters of the lab's own data. This
382 allows experimenters to select the best methods for their purpose, or developers to flexibly test and
383 benchmark their novel methods.

384 Another desirable but not vital future task is to expand the QC output, to include functionality
385 such as statistical testing of detected bad data, for the experimenter to make a more informed
386 decision. Although statistical testing is already implied in many methods of bad data detection, it is
387 not visible to users.

388 We will also provide an automated tool to compare output from two (or more) peeks, to help
389 visualize both changes in baseline level as well as changes in local waveforms.

390 CONCLUSIONS

391 The ultimate aims of CTAP are: a) to facilitate processing of large quantities of EEG data; b)
392 to improve reliability and objectivity of such processing; c) to support development of 'smart'
393 algorithms to tune the thresholds of statistical selection methods (for bad channels, epochs, segments
394 or components) to provide results which are robust enough to minimise manual intervention. With
395 this contribution, we have addressed aim a), partly also b), and laid the groundwork to continue
396 developing solutions for c). CTAP will thereby help to minimise human effort, subjectivity and
397 error; and facilitate easy, reliable batch processing for experts and novices alike.

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