

A peer-reviewed version of this preprint was published in PeerJ on 5 April 2016.

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Panagiotopoulou O, Spyridis P, Mehari Abraha H, Carrier DR, Pataky TC. 2016. Architecture of the sperm whale forehead facilitates ramming combat. PeerJ 4:e1895 <https://doi.org/10.7717/peerj.1895>

Architecture of the sperm whale forehead facilitates ramming combat

Olga Panagiotopoulou, Panagiotis Spyridis, Hyab Mehari Abraha, David R Carrier, Todd Pataky

Herman Melville's novel *Moby Dick* was inspired by historical instances in which large sperm whales (*Physeter macrocephalus* L.) sank 19th century whaling ships by ramming them with their foreheads. The immense forehead of sperm whales is possibly the largest, and one of the strangest, anatomical structures in the animal kingdom. It contains two large oil-filled compartments, known as the "spermaceti organ" and "junk", that constitute up to one-quarter of body mass and extend one-third of the total length of the whale. Recognized as playing an important role in echolocation, previous studies have also attributed the complex structural configuration of the spermaceti organ and junk to acoustic sexual selection, acoustic prey debilitation, buoyancy control, and aggressive ramming. Of these additional suggested functions, ramming remains the most controversial, and the potential mechanical roles of the structural components of the spermaceti organ and junk in ramming remain untested. Here we explore the aggressive ramming hypothesis using a novel combination of structural engineering principles and probabilistic simulation to determine if the unique structure of the junk significantly reduces stress in the skull during quasi-static impact. Our analyses indicate that the connective tissue partitions within the junk reduce stress across the skull during impact; stress reduction is greatest in the anterior aspect of the skull; and removal of the connective tissue partitions increases stress concentrations on the tip of the skull, possibly making it prone to fracture. Although the unique structure of the junk certainly serves multiple functions, our results are consistent with the hypothesis that the structure also evolved to function as a massive battering ram during male-male competition.

1 **Title: Architecture of the sperm whale forehead facilitates ramming combat**

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3 **Authors:** Olga Panagiotopoulou^{1 *}, Panagiotis Spyridis², Hyab Mehari Abraha¹, David R.
4 Carrier³, Todd Pataky⁴

5 **Affiliations:**

6 ¹ Moving Morphology and Functional Mechanics Laboratory, School of Biomedical Sciences,
7 The University of Queensland, Brisbane 4072, Australia.

8 ² Polytropos Ltd, London N1 7JL, United Kingdom.

9 ³ Department of Biology, University of Utah, Salt Lake City, UT 84112, USA.

10 ⁴ Department of Bioengineering, Shinshu University, Ueda, Nagano 386-8567, Japan.

11

12 *Correspondence to:

13 Dr. Olga Panagiotopoulou

14 Moving Morphology and Functional Mechanics Laboratory, School of Biomedical Sciences, The
15 University of Queensland, Room 433-Otto Hirschfeld Building (81), Brisbane, QLD 4072,
16 Australia.

17 o.panagiotopoulou@uq.edu.au

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Abstract

32 Herman Melville's novel *Moby Dick* was inspired by historical instances in which large
33 sperm whales (*Physeter macrocephalus L.*) sank 19th century whaling ships by ramming them
34 with their foreheads. The immense forehead of sperm whales is possibly the largest, and one of
35 the strangest, anatomical structures in the animal kingdom. It contains two large oil-filled
36 compartments, known as the "spermaceti organ" and "junk", that constitute up to one-quarter of
37 body mass and extend one-third of the total length of the whale. Recognized as playing an
38 important role in echolocation, previous studies have also attributed the complex structural
39 configuration of the spermaceti organ and junk to acoustic sexual selection, acoustic prey
40 debilitation, buoyancy control, and aggressive ramming. Of these additional suggested functions,
41 ramming remains the most controversial, and the potential mechanical roles of the structural
42 components of the spermaceti organ and junk in ramming remain untested. Here we explore the
43 aggressive ramming hypothesis using a novel combination of structural engineering principles
44 and probabilistic simulation to determine if the unique structure of the junk significantly reduces
45 stress in the skull during quasi-static impact. Our analyses indicate that the connective tissue
46 partitions within the junk reduce stress across the skull during impact; stress reduction is greatest
47 in the anterior aspect of the skull; and removal of the connective tissue partitions increases stress
48 concentrations on the tip of the skull, possibly making it prone to fracture. Although the unique
49 structure of the junk certainly serves multiple functions, our results are consistent with the
50 hypothesis that the structure also evolved to function as a massive battering ram during male-
51 male competition.

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64 **Introduction**

65 The sperm whale (*Physeter macrocephalus L.*) is unique in having a massively expanded
66 forehead that is highly sexually dimorphic, being much larger and extending up to a meter and a
67 half beyond the anterior tip of the jaws in mature males (Benzin, 1972; Cranford, 1999).

68 Internally the forehead is composed of two large oil-filled sacs, stacked one on top of the other,
69 known as the spermaceti organ and junk (Fig. 1). These sacs extend for one-third of the total
70 length of the whale and can constitute more than one-quarter of the whale's mass (Benzin, 1972;
71 Clarke, 1978). The oil contained in the upper sac (spermaceti organ) was a primary target of the
72 whaling industry of the early 19th century. At the same time, the forehead of sperm whales was
73 considered by whalers to be a battering ram that the whales sometimes used to attack and sink
74 oak whaling ships of up to 238 tons (Chase, 1821; Starbuck, 1878; Philbrick, 2000).

75 The lower sac (junk) is derived from the ondocete melon (Heyning & Mead, 1990) and is
76 organized into sections by transverse partitions of connective tissue that contain waxy oil
77 (Clarke, 1978) (Fig. 1). The connective tissue partitions are widest about 10-25% of the length
78 from the anterior end and the sections are narrow ventrally and broad dorsally (Clarke, 1978).
79 The partitions become thinner progressively towards the posterior aspect of the junk until they
80 are totally replaced by a mixture of oil and wax. The oil and connective tissue partitions of the
81 junk are enclosed in a fibrous connective tissue case which sits in a trough formed by the upper
82 jaw (Clarke, 1978).

83 The function of the spermaceti organ and junk in adding directionality and amplitude to
84 sonar clicks is relatively well studied and accepted (Møhl et al., 2000; Møhl, 2001; Møhl et al.,
85 2003a; Møhl et al., 2003b; Huggenberger, André & Oelschläger, 2014). Previous studies have
86 also suggested that the unique structural configuration of the sperm whale forehead is
87 functionally related to, acoustic sexual selection (Cranford, 1999), acoustic prey debilitation
88 (Norris & Møhl, 1972), communication (Madsen, Wahlberg & Møhl, 2002) and buoyancy
89 control (Clarke, 1970). Although all of these functional hypotheses are plausible, they cannot
90 explain how the forehead of sperm whales can function as a battering ram capable of sinking
91 ships that are four to five times the mass of the whale.

92 The ramming hypothesis was originally proposed by whalers following the sinking of at
93 least 2 whaling ships, *the Essex* in 1821 and *the Ann Alexander* in 1851 (Chase, 1821; Starbuck,

94 1878; Philbrick, 2000; Sawtell, 1962). Based on these incidents, researchers have recently
95 suggested that the forehead of a swimming sperm whale possess sufficient momentum to injure
96 an opponent when used as a battering ram, and may at the same time absorb energy to protect the
97 brain and skull of the attacking whale allowing mature males to use their foreheads as battering
98 rams in male-male contests over harems of females (Carrier, Deban & Otterstrom, 2002).

99 The ramming hypothesis remains highly controversial because (1) the structures that
100 generate sound, the distal sac and monkey lips of the right nasal passage, are located at the
101 rostral end of spermaceti organ (Fig. 1) and are therefore assumed to be in harm's way in a
102 ramming event (Huggenberger, André & Oelschläger, 2014), and (2) ramming episodes have not
103 been observed by scientists who study the behavior of sperm whales. Although the monkey lips
104 do reside at the front end of the spermaceti organ, these structures are located well above and to
105 the right of the rostral end of the junk (Huggenberger, André & Oelschläger, 2014), and it is the
106 junk, not the spermaceti organ, that has been suggested to function as a battering ram during
107 aggressive encounters (Chase, 1821; Carrier, Deban & Otterstrom, 2002). As far as we know, the
108 scientific literature does not include observations of sperm whale ramming behavior, yet there is
109 one documented observation of male-male ramming that we report here (Supplementary
110 Material). On January 30, 1997, a reputable marine biologist, while flying over the Gulf of
111 California, watched two mature males swim directly toward each other, from an initial observed
112 distance of approximately 6.4 kilometers, at an estimated average swimming speed of 17 km/h
113 and collide forehead-to-forehead. Shortly before impact both whales, which had been swimming
114 at the surface, "shallow dove" so that the impact occurred below the surface of the water. This
115 ramming event occurred a few miles north of a group of approximately of 50 females. This
116 observation plus reports of ramming attacks on 19th century whaling ships suggest that sperm
117 whales do sometimes engage in ramming contests. If these ramming contests generally occur at a
118 shallow depth, they may be much more common than whale biologists realize because a human
119 observer would have to be located well above the surface of the water to watch it happen.

120 Another reason to consider the ramming hypothesis is the extreme body size sexual
121 dimorphism of sperm whales. This species is the most sexually dimorphic of all cetaceans, with
122 mature males being 3-times bigger than mature females (Whitehead, 2003). Among mammals,
123 body size sexual dimorphism is generally greatest in polygynous species in which males compete
124 through fighting and the threat of fighting (Clutton-Brock & Harvey, 1977; Parker, 1983;

125 Andersson, 1994). Additionally, because sexual dimorphism is often greatest in those characters
126 that enhance a male's capacity to dominate other males (Clutton-Brock & Harvey, 1977;
127 Hamilton, 1979; Clutton-Brock, Albon & Harvey, 1980; Parker, 1983; Jarman, 1983; Andersson,
128 1994), the observation that the part of the body that is most dimorphic in sperm whales is the
129 length of the head (Nishiwaki, Ohsumi & Maeda 1963) is consistent with the head being a
130 weapon important to male-male competition.

131 This paper addresses the battering-ram hypothesis using finite element analysis and
132 probabilistic simulation. Our main objective was to determine if the connective tissue partitions
133 of the spermaceti junk have potential to reduce stress in the bones of the skull during ramming
134 impact. We predict that the vertically oriented connective tissue partitions within the junk can
135 dissipate load through tension during posteriorly directed compressive loading of the forehead.
136 Bone stress reduction would be particular important on the anterior aspect of the skull (i.e., upper
137 jaw) that would otherwise be most vulnerable to potential tissue damage.

138

139 **Materials and Methods**

140 Finite element analysis (FEA) is a numerical technique well entrenched in comparative
141 biomechanics as a tool to assess the mechanical architecture of anatomical tissues and to better
142 comprehend the complex interaction of their form–function relationships. Nevertheless, FEA
143 accuracy is dependent on a variety of factors and its reproducibility is often obscured in scientific
144 publications due to both public unavailability of the underlying models and the lack of standard
145 reporting guidelines (Erdemir et al., 2012). To mitigate these problems we here describe our
146 methods in accordance with biomechanical FEA reporting guidelines (Erdemir et al., 2012) and
147 we also make all raw data and FE models available for public use (Panagiotopoulou et al. 2015).

148 **Model Identification.** Our study utilized three FE models to study the effect of the connective
149 tissue partitions on the reduction of bone stresses in quasi-static loading of the sperm whale head
150 (Fig. 2).

151 **Model name.** Sperm Whale Head Model A (Generic Base) consisted of twelve connective tissue
152 partitions embedded in the spermaceti tissue of junk.

153 Sperm Whale Head Model B (Half Partitions) had reduced number (six) of connective tissue
154 partitions.

155 Sperm Whale Head Model C (No Partitions) had no connective tissue partitions.

156 **Model keywords.** Sperm whale skull, quasi-static impact.
157 **Version.** 0.1 (unpublished).
158 **Physiological domain.** No segmental motion, evenly distributed anterior surface loading, small
159 deformations of hard and soft tissue.
160 **Mechanical domain.** All models were static and linear elastic.
161 **Structure of interest.** The biological structure under investigation was the sperm whale upper
162 jaw (skull).
163 **Demographics.** Adult male sperm whale (*Physeter macrocephalus L.*).
164 **State of represented organism.** *in vitro*.
165 **Disease state.** Healthy.
166 **Spatial scale.** Within a volume of (length 5.3 m x height 1.6 m x width 0.1 m).
167 **Time scale.** Not applicable (quasi-static analysis).
168 **Primary utility.** To provide mechanical insight into a physiologic process.
169 **Secondary utility.** First model of sperm whale skull mechanics.
170 **Primary highlight.** To elucidate the likely mechanically protective role of the vertical
171 connective tissue partitions within the sperm whale skull.
172 **Secondary highlight.** Not applicable.
173 **Primary limitation.** Linear isotropic and homogeneous materials.
174 Due to lack of experimental data on the elasticity of the sperm whale head tissues,
175 anisotropy and heterogeneity, as well as environmental and time dependencies could not be
176 modeled in this study. Thus, isotropy, homogeneity and linear elasticity were assumed and the
177 material properties assigned to each tissue were the closest estimations based on published
178 values of tissues similar to those of interest (Rho, Ashman & Turner 1993; Shahar et al., 2007).
179 A biologically unrealistic consequence of this assumption was that the dorsal horizontal
180 components of connective tissue partitions provided resistance to compression in the model. To
181 this end we assigned a Young's modulus (E) value of 14.8 GPa and Poisson (ν) value of 0.1 for
182 the skull; E = 2 GPa and $\nu = 0.2$ for the connective tissue partitions; and E = 1 GPa and $\nu = 0.49$
183 for the oil/wax mixture enclosed within the spermaceti organ and junk (Fig.2) (Rho, Ashman &
184 Turner 1993; Shahar et al., 2007). Nevertheless, our study was comparative and such an
185 assumption likely created a constant error across all models. Additionally, uncertainties due to
186 material variations had been handled through numerical statistic elaboration of the models.

187 Lastly, the basic mechanism of skull-stress reduction we described was independent of model
188 realism.

189 **Secondary limitation.** Simplifications in the model geometry (see below), static simulation.

190 **Reference to publications.** Clarke (1970, 1978); no explicit mechanical model described.

191 *Model Structure*

192 **Loading and boundary conditions.** We used a static force of 764 kN (Fig. 3) distributed evenly
193 over the most anterior aspect of the head as a simplified model of ramming force. We calculated
194 the applied force by assuming that each of the two colliding whales were traveling at an
195 intermediate speed of 6.26 ms^{-1} (Aoki et al., 2007) had masses of 39,000 kg, and decelerated over
196 a distance of 1 meter upon impact. The deceleration distance was based on the length of the
197 spermaceti junk that extended beyond the tip of the skull. Boundary conditions included no-
198 displacement constraints on all external nodes on the posterior surface of the skull.

199 **Primary output variables.** von Mises Stress.

200 **Source of anatomy.** To test our hypothesis, we developed FE models based partially on
201 previously published structural properties and schematic configurations of male sperm whale
202 adult cadavers. Due to the inaccessibility of sperm whale cadaveric species the report by Clarke
203 1978 was the most detailed hitherto available and encompassed skeletal and soft tissues such as
204 the connective tissue partitions, and the oil cases of the spermaceti case and junk. To calculate
205 the dimensions of the various structural components of the model, we scaled the anatomical
206 elements shown in Figure 1 of Clark (1978) to a total spermaceti organ length of 5m (Clarke
207 1970). For modelling purposes and due to the unclear description of the individual connective
208 tissue partitions thickness, we assumed a universal thickness of 0.05m and 0.150m for all
209 connective tissue partitions and the spermaceti junk compartments between the connective tissue
210 partitions respectively (Fig. 2).

211 Model A, representative of the sperm whale head, consisted of the upper sack or
212 spermaceti organ; the lower sack or spermaceti junk; the connective tissue partitions and their
213 subsequent connective tissue case enclosed in the spermaceti junk and the upper jaw (Fig. 2).

214 We compared Model A against two modified models (Models B and C) to assess the
215 mechanical function of the spermaceti organ (Fig. 2). Model B had fewer connective tissue
216 partitions than Model A. Model C lacked the connective tissue partitions altogether (Fig. 2).

217 The skin and the blubber were discarded from the modeling process due to their
218 negligible thickness and stiffness.

219 The FE mesh assembly of all models consisted of solid continuum linear tetrahedral
220 elements (type “C3D4” in the Abaqus Library, Simulia-Dassault Systemes, Waltham, USA).
221 Each model contained approximately 42,000 to 48,000 nodes and 220,000 to 260,000 elements.
222 Model A had 257,542 elements in total (28,009 for the upper jaw; 65,588 for the spermaceti
223 case; 91,272 for the spermaceti junk; and 72,673 for the connective tissue partitions). Model B
224 had 242,509 elements in total (278,96 for the upper jaw; 654,67 for the spermaceti case; 93,482
225 for the spermaceti junk; and 55,664 for the connective tissue partitions). Model C had 227,925
226 elements in total (281,37 for the upper jaw; 65,519 for the spermaceti case; 134,269 for the
227 spermaceti junk. The nominal element size was 50 mm (0.05 m), and the actual elements sizes
228 across the model varied from 15 to 85 mm approximately.

229 **Reference configuration.** The Abaqus default x (cranial-caudal), y (medial-lateral), z (vertical)
230 coordinate system was used.

231

232 *Simulation structure*

233 **Name of simulation software.** Abaqus/CAE (Simulia-Dassault Systemes).

234 **Version of simulation software.** 6.12

235 **Solution strategy.** Abaqus/Standard implicit direct static solver. Minimum and maximum
236 increments set to 1.000E-05 and 1 respectively.

237 **Numerical algorithms.** Full Newton default iterations.

238 **Convergence criteria.** Default convergence tolerances of the simulation software were used. We
239 interpreted stress differences amongst our models using a Monte Carlo simulation. A total of
240 1000 Monte Carlo iterations were run for each of the three models, varying the three materials’
241 stiffness values randomly with a standard deviation of 10%, and von Mises stress distributions
242 were stored for each iteration (Supplementary Materials Code). This resulted in a population of
243 1000 random individuals which represented the population of interest, under an assumption of
244 10% error in each of the material parameters. The latter is an essential approach in cases when
245 the assigned material properties are based on generalized published values and not on
246 experimental analysis of the tissues of interest.

247 For each population pair (i.e. Model B vs. Model A, Model C vs. Model B and Model C vs.
248 Model A), the following statistic was calculated for each element:

249
250

$$z_i = \frac{(\bar{\sigma}_i)_B - (\bar{\sigma}_i)_A}{\frac{1}{2}[(\sigma_i)_A + (\sigma_i)_B]}$$

251
252

253 where i indexes the elements, A and B represent models, $\bar{\sigma}_i$ represents mean elemental von Mises
254 stress and σ_i represents elemental standard deviation. Since the input variance nonlinearly maps
255 to elemental variance, the z distribution is a non-trivial function of mean group differences.

256 Next, the “significance” of the z distribution was assessed using paired non-parametric
257 permutation tests (one for each model pair). A total of 10,000 label permutations were applied to
258 each model pair, yielding a non-parametric distribution of the z statistic at each element. The
259 99th percentile of that distribution was taken as the “significance” threshold. In other words, if
260 an element’s z value survived that threshold, it would suggest that 99% of all randomly labelled
261 individuals would yield a z value less than that observed in the original labellings, and thus that
262 threshold-surviving elements represented true population differences at $\alpha=0.01$ under the
263 assumption of 10% true population material parameter variance.

264 **Validation.** Validation of the FE models against experimental *ex vivo* data was not feasible due
265 to size and accessibility constraints. Nevertheless our study is comparative and conclusions are
266 fundamentally mechanical rather than empirical.

267 **Availability.** Not yet public.

268

269 Results

270 In all our FE models the highest concentration of von Mises stresses occurred in the most
271 anterior aspect of the skull (Figs. 4, 5 and Table 1). The anterior connective tissue partitions
272 within the junk were subjected to higher tensile loading than the posterior portions (Fig. 6).
273 Tension in the connective tissue partitions redistributed compressive stresses across the skull
274 (Models A and B) and the absence of the partitions (Model C) raised anterior skull stresses (Fig.
275 4, 5 and Table 1).

276 A reduced number of partitions (Model B) did reduce stresses in the anterior skull, but stress

277 reduction was not as effective as Model A (Fig. 4, 5 and Table 1). The skull stress difference
278 distributions resulting from Monte Carlo simulations suggest that our main finding regarding the
279 load-redistribution functionality of the connective tissue is insensitive to relatively large changes
280 in both material parameters (Fig. 7) and, indirectly, load magnitudes.

281

282 **Discussion**

283 Our findings suggest that the connective tissue partitions of the junk may be able to
284 reduce impact stresses and thus potentially function as a protective mechanism during ramming.
285 The mechanism of skull stress reduction appears to be connective partition tension; as the
286 spermaceti junk is compressed upon impact, the oil between the partitions is displayed vertically
287 and laterally, placing the connective tissue partitions into tension (Fig. 6). This connective tissue
288 tension allows the total compressive bone load to be shared over a greater volume (Figs. 4-7).
289 While our static simulations do not quantify dynamic effects of the connective partitions
290 including energy dissipation, our results suggest that connective partition tension would in fact
291 dissipate energy in dynamic impacts because dynamic loading, like the current quasi-static
292 loading, would be distributed over a broader region of the skull. Additionally, during a dynamic
293 impact soft tissues within the skull would displace, and the connective tissue partitions would
294 limit this displacement. The connective tissue might therefore protect both bone and soft tissue
295 from injury. Absence of the partitions increased stresses by 45%, concentrated on the most
296 anterior aspect of the skull, making the skull more prone to tissue failure (Table 1, Figs.4-7).

297 Our findings appear to provide an explanation for previous observations that, in real
298 whales, the partitions become progressively thinner posteriorly until they are replaced by a
299 mixture of oil and wax (Clark, 1978). The anterior thicker partitions are subjected to the greatest
300 tensile loading (Fig. 6) and, if the battering ram hypothesis is correct, they likely play the biggest
301 role in skull stress reduction in the face of posteriorly-directed impact forces.

302 The connective tissue partitions of the junk are acquired traits that likely facilitate a
303 variety of functions. In addition to acoustic signals between groups (Madsen, Wahlberg & Møhl
304 2002), the partitions may play an important role in the dissipation of stresses during ramming
305 combat to protect the skull and brain. This “mechanical advantage” is a trait that is likely related
306 to selection on male-male aggressive behavior. Such developmental non-independent
307 morphological features of the junk are an example of how a derived structure, such as the

308 connective tissue partitions, facilitates evolutionary modifications while maintaining functional
309 integrity (Wagner & Altenberg 1996).

310 Our results are not directly relevant to the behavioral strategies behind ramming impacts;
311 however, our findings are consistent with the hypothesis proposed in 1821 by Owen Chase
312 (Chase, 1821). Following the sinking of *the Essex* whaling ship, Owen Chase hypothesized that
313 sperm whales not only use their immense and elaborately complex foreheads as battering rams
314 when fighting, but also that "*the whale's head is admirably designed for this mode of attack*".
315 The prevalence of head-butting in sperm whales is not well documented. However, ramming is a
316 basal behavior for bovidae (Farke, 2008; Alvaraez, 1990) and cetacean (Carrier, Deban &
317 Otterstrom, 2002), including humpback whales (Baker & Herman 1984), bottle-nosed whales
318 (Gowans& Rendell 1999), narwhales (Silverman & Dunbar 1980), long-finned pilot whales
319 (Reilly & Shane, 1986) and killer whales (Goley & Straley, 1994). Based on these reports, it has
320 previously been hypothesized that the spermaceti organ of male sperm whales may function as a
321 weapon and is more developed in males due to sexual selection (Carrier, Deban & Otterstrom,
322 2002). If this is true then males may be exposed to increased stresses during head-butting
323 ramming and as such necessitate additional support via a dramatically increased and more
324 structurally robust melon.

325 Our study illustrates how structural engineering principles and probabilistic simulation
326 can be used to address hypotheses of mechanical function in biological systems that are too big
327 or inaccessible to be studied directly. We anticipate our study will stimulate future research
328 aimed at unraveling the mechanical function of the head during aggressive head-butting and
329 ramming in other species such as the *Hippopotamus* (Kingdon, 1979) which head-butting
330 aggressive behavior is common but remains unsimulated.

331

332 **Acknowledgments:**

333 We thank Sandra Lanham for sharing with us her report on the sperm whale ramming incident
334 that occurred near Mildriff Island at the Gulf of California, on the 30th of January 1997. We are
335 also grateful to Dr. Ali Nabavizadeh (University of Chicago) for creating Figure 1. The authors
336 declare no conflicts of interest.

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464 **Figure legends**

465 **Fig. 1.** Schematic representation of sperm whale head structure.

466 **Fig. 2.** Finite element models. Young's moduli for the connective tissue partitions (blue),
467 spermaceti organ (yellow) and skull (red) were 14.8 GPa, 1 GPa and 2 GPa, respectively. Models
468 A, B and C have twelve, six and zero connective tissue partitions, respectively.

469 **Fig. 3.** Loads and constraints assigned to all FE models. A force of 764 kN was applied to the
470 anterior surface of the head (1). Motion was constrained at the posterior surface (2) in all
471 directions.

472 **Fig. 4.** Von Mises stress distribution results.

473 **Fig. 5.** Region definitions (blue vertical bars).

474 **Fig. 6.** Maximum principal stress distributions across the connective tissue partitions. Positive
475 and negative stresses indicate areas of tension and compression respectively.

476 **Fig. 7.** Z statistic distributions depicting mean elemental von Mises stress differences divided by
477 elemental standard deviation under an assumed population material stiffness variance of 10%.
478 Data are thresholded at $\alpha=0.01$.

479

Table 1 (on next page)

Maximum (Max.), mean and minimum (Min.) percentage increase of the regional (Fig. 5) von Mises stress values (Pa) between Models A and C and Models B and C.

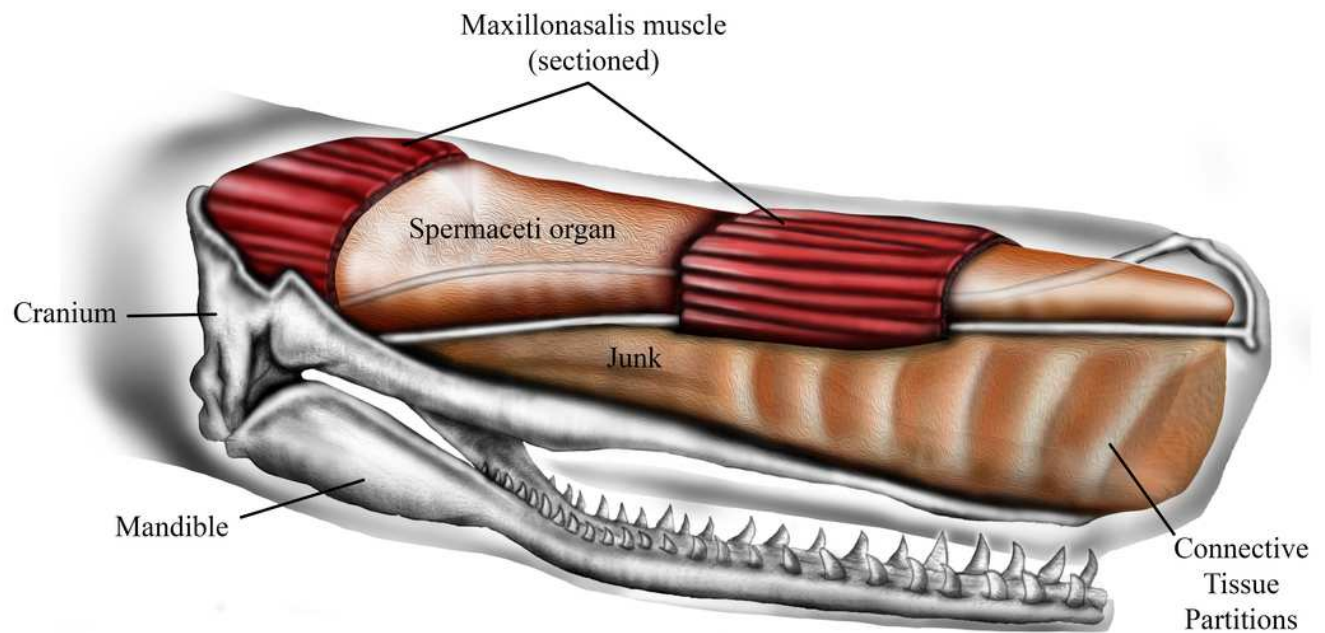
Table 1.

Maximum (Max.), mean and minimum (Min.) percentage increase of the regional (Fig. 5) von Mises stress values (Pa) between Models A and C and Models B and C.

	% increase														
	1			2			3			4			5		
	Max.	Mean	Min.	Max.	Mean	Min.	Max.	Mean	Min.	Max.	Mean	Min.	Max.	Mean	Min.
Model A - Model C	42.9	45.7	3.6	25	24.1	9.4	-8.8	6.1	60.8	-6.5	-0.9	-27.3	1.4	-0.3	-62.8
Model B - Model C	10.1	15.5	12.8	-7.3	4.1	35.7	0.6	0.8	-6.9	-6.7	-1.4	-27.4	1.4	-0.2	-59.6

1

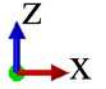
Schematic representation of sperm whale head structure.



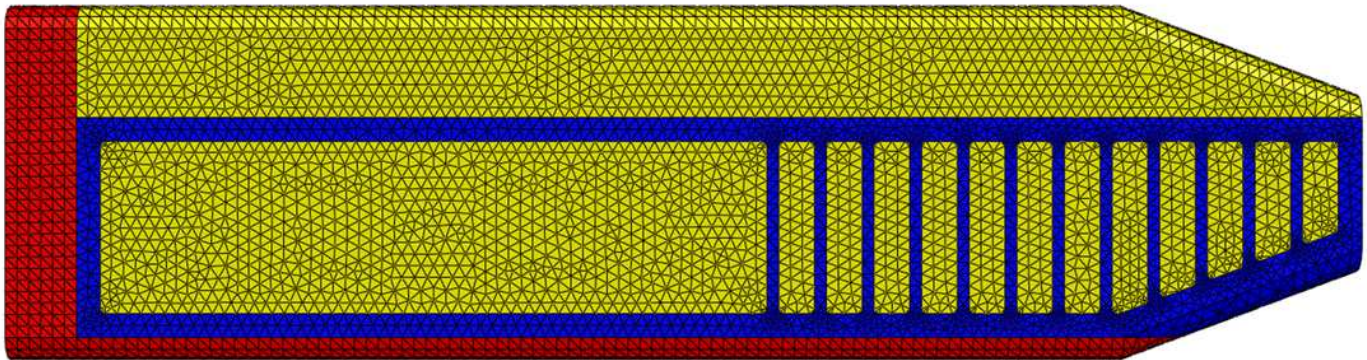
2

Finite element models.

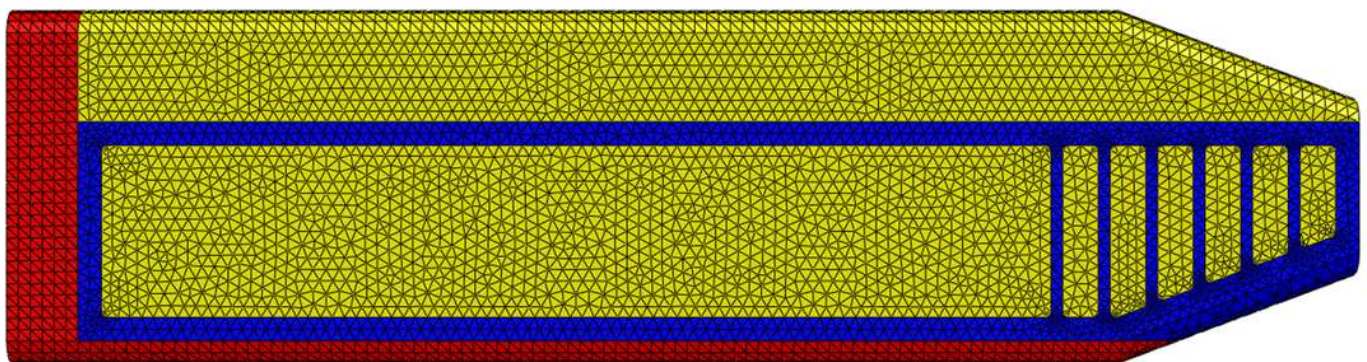
Young's moduli for the connective tissue partitions (blue), spermaceti organ (yellow) and skull (red) were 14.8 GPa, 1 GPa and 2 GPa, respectively. Models A, B and C have twelve, six and zero connective tissue partitions, respectively.



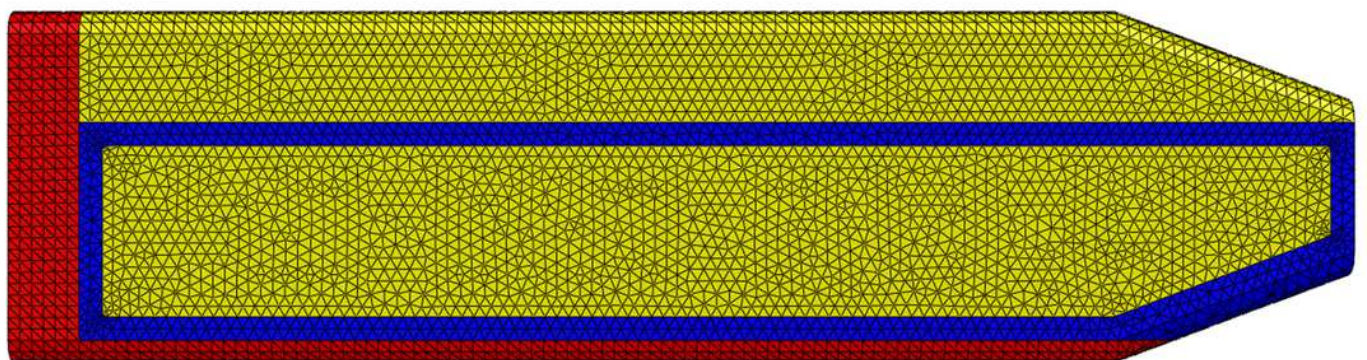
Model A



Model B



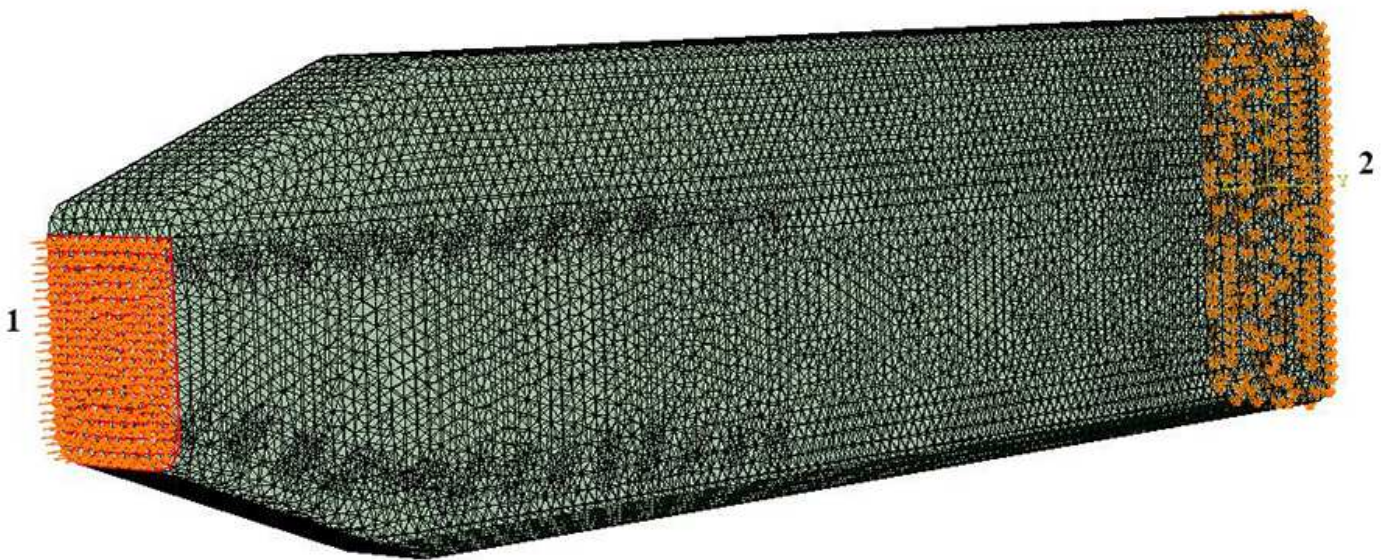
Model C



3

Loads and constraints assigned to all FE models.

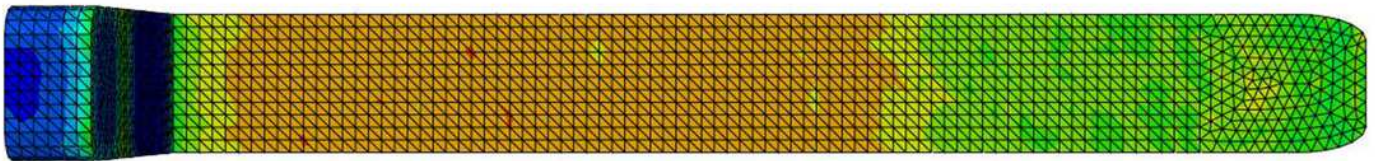
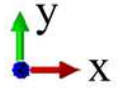
A force of 764 kN was applied to the anterior surface of the head (1). Motion was constrained at the posterior surface (2) in all directions.



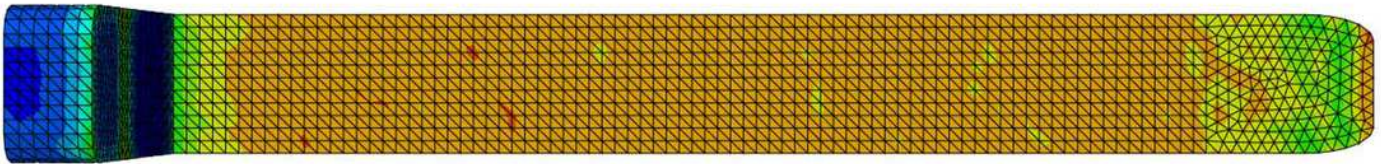
4

Von Mises stress distribution results.

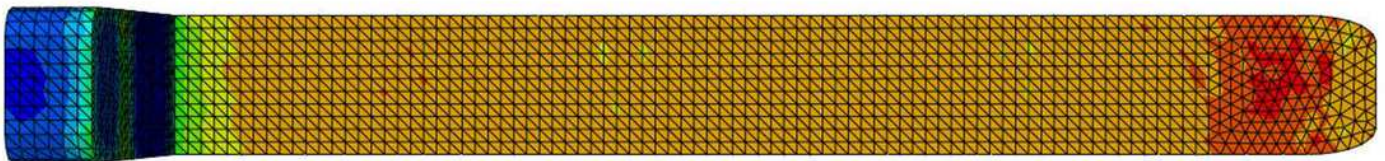
Model A



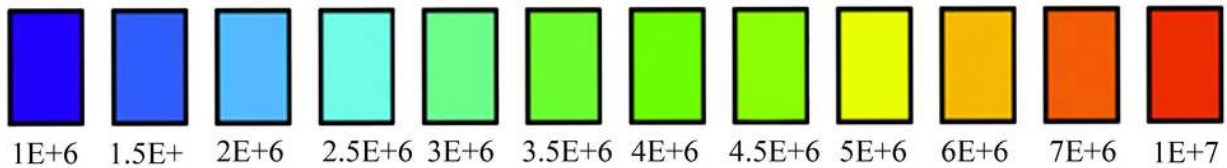
Model B



Model C

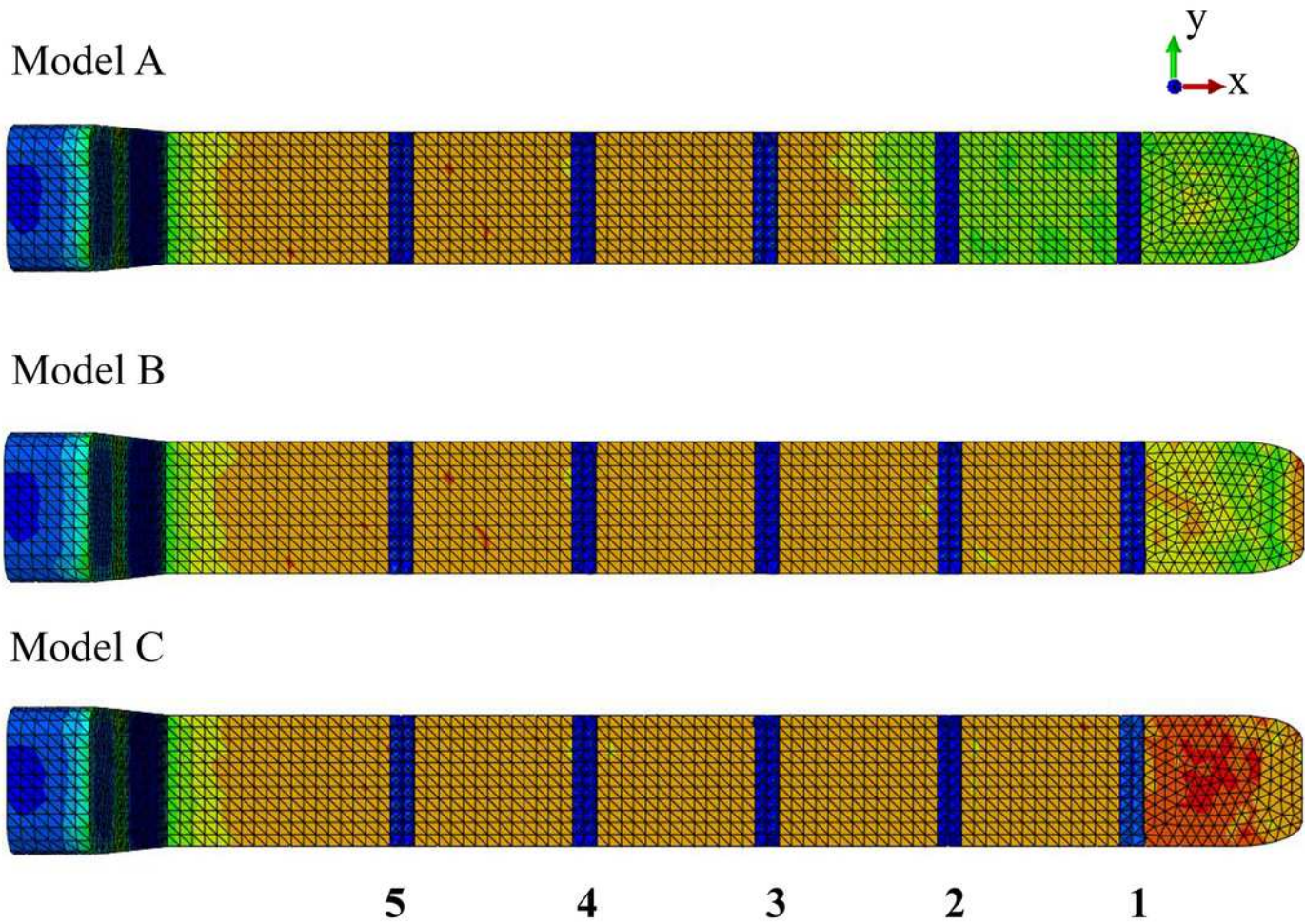


von Mises stress (Pa)



5

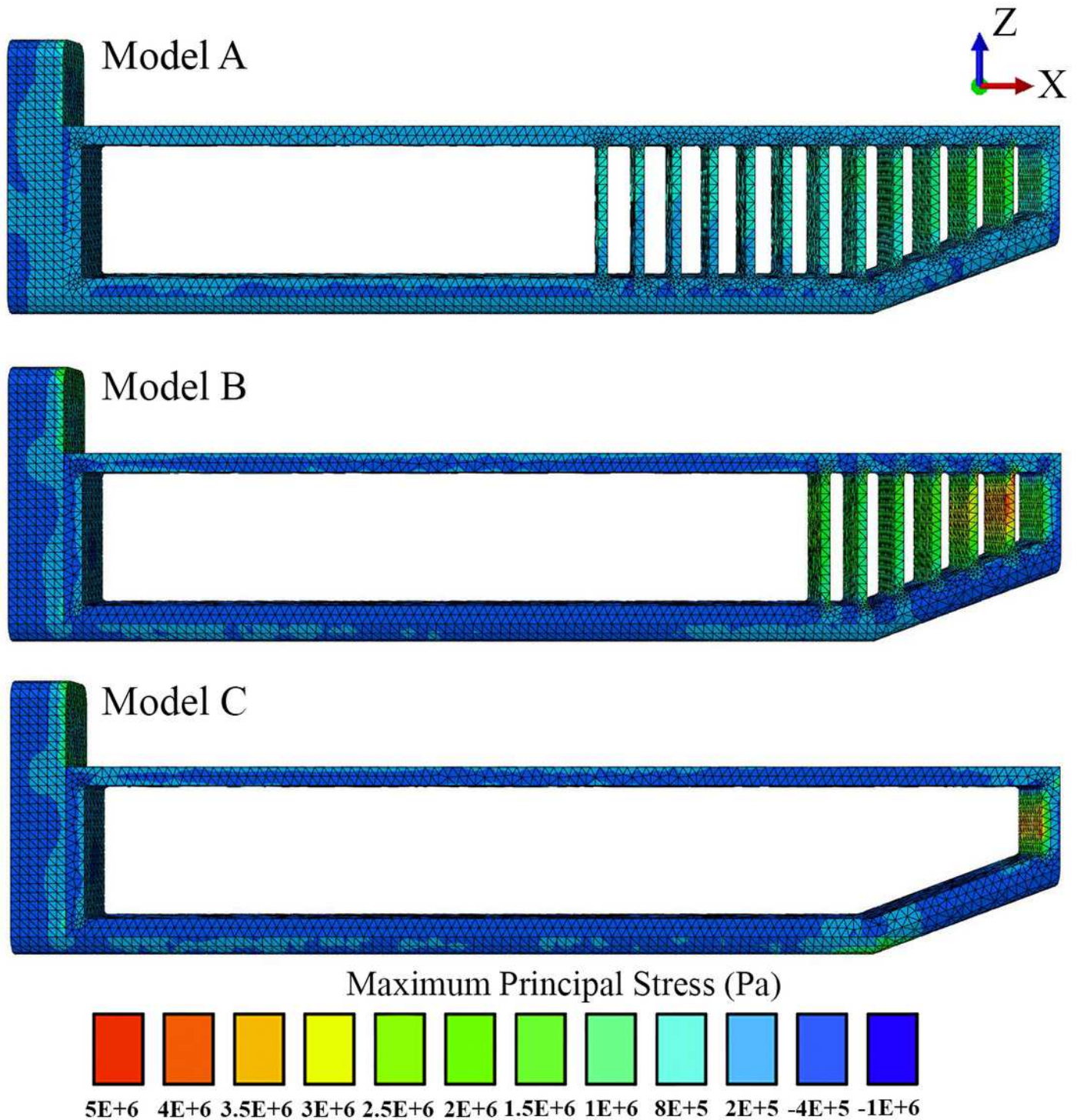
Region definitions (blue vertical bars).



6

Maximum principal stress distributions across the connective tissue partitions.

Positive and negative stresses indicate areas of tension and compression respectively.



7

Probabilistic FEA simulation.

Z statistic distributions depicting mean elemental von Mises stress differences divided by elemental standard deviation under an assumed population material stiffness variance of 10%. Data are thresholded at $\alpha=0.01$.

