

# Survival and grade of the glioma prediction using transfer learning

**Santiago Valbuena Rubio**<sup>1</sup>, **María Teresa García-Ordás**<sup>2</sup>, **Oscar García-Olalla Olivera**<sup>1</sup>, **Héctor Alaiz Moretón**<sup>2</sup>, **Maria-Inmaculada González-Alonso**<sup>3</sup>, **José Alberto Benítez-Andrades**<sup>Corresp. 4</sup>

<sup>1</sup> IA Department, Xeridia S.L., León, León, Spain

<sup>2</sup> SECOMUCI Research Group, Escuela de Ingenierías Industrial e Informática, Universidad de León, León, Spain

<sup>3</sup> Department of Electric, Systems and Automatics Engineering, Universidad de León, León, Spain

<sup>4</sup> SALBIS Research Group, Department of Electric, Systems and Automatics Engineering, Universidad de León, León, Spain

Corresponding Author: José Alberto Benítez-Andrades  
Email address: jbena@unileon.es

Glioblastoma is a highly malignant brain tumor with a life expectancy of only 3-6 months without treatment. Detecting and predicting its survival and grade accurately are crucial. This study introduces a novel approach using transfer learning techniques. Various pre-trained networks, including EfficientNet, ResNet, VGG16, and Inception, were tested through exhaustive optimization to identify the most suitable architecture. Transfer learning was applied to fine-tune these models on a Glioblastoma image dataset, aiming to achieve two objectives: survival and tumor grade prediction. The experimental results show 65% accuracy in survival prediction, classifying patients into short, medium, or long survival categories. Additionally, the prediction of tumor grade achieved an accuracy of 97%, accurately differentiating low-grade gliomas (LGG) and high-grade gliomas (HGG). The success of the approach is attributed to the effectiveness of transfer learning, surpassing the current state-of-the-art methods. In conclusion, this study presents a promising method for predicting the survival and grade of Glioblastoma. Transfer learning demonstrates its potential in enhancing prediction models, particularly in scenarios with limited large datasets. These findings hold promise for improving diagnostic and treatment approaches for Glioblastoma patients.

# Survival and grade of the glioma prediction using transfer learning

Santiago Valbuena Rubio<sup>1</sup>, María Teresa García-Ordás<sup>2</sup>, Oscar García-Olalla<sup>1</sup>, Héctor Alaiz-Moretón<sup>2</sup>, Inmaculada González-Alonso<sup>3</sup>, and José Alberto Benítez-Andrades<sup>4</sup>

<sup>1</sup>IA department, Xeridia S.L., Avda. Padre Isla 16, León, 24002, León, Spain

<sup>2</sup>SECOMUCI Research Group, Escuela de Ingenierías Industrial e Informática, Universidad de León, Campus of Vegazana s/n, León, 24071, León, Spain

<sup>3</sup>Department of Electric, Systems and Automatics Engineering, Universidad de León, Campus of Vegazana s/n, León, 24071, León, Spain

<sup>4</sup>SALBIS Research Group, Department of Electric, Systems and Automatics Engineering, Universidad de León, Campus of Vegazana s/n, León, 24071, León, Spain

Corresponding author:

José Alberto Benítez-Andrades<sup>4</sup>

Email address: jbena@unileon.es

## ABSTRACT

Glioblastoma is a highly malignant brain tumor with a life expectancy of only 3-6 months without treatment. Detecting and predicting its survival and grade accurately are crucial. This study introduces a novel approach using transfer learning techniques. Various pre-trained networks, including EfficientNet, ResNet, VGG16, and Inception, were tested through exhaustive optimization to identify the most suitable architecture. Transfer learning was applied to fine-tune these models on a Glioblastoma image dataset, aiming to achieve two objectives: survival and tumor grade prediction. The experimental results show 65% accuracy in survival prediction, classifying patients into short, medium, or long survival categories. Additionally, the prediction of tumor grade achieved an accuracy of 97%, accurately differentiating low-grade gliomas (LGG) and high-grade gliomas (HGG). The success of the approach is attributed to the effectiveness of transfer learning, surpassing the current state-of-the-art methods. In conclusion, this study presents a promising method for predicting the survival and grade of Glioblastoma. Transfer learning demonstrates its potential in enhancing prediction models, particularly in scenarios with limited large datasets. These findings hold promise for improving diagnostic and treatment approaches for Glioblastoma patients.

## 1 INTRODUCTION AND RELATED WORK

Cancer is one of the leading causes of death in the world with more than 18 million cases and 9.5 million deaths in 2018, but these figures are estimated to get even worse to 29.5 million cases and 16, 4 million deaths in the year 2040 (est, 2022). Malignant gliomas are the most common brain tumors, with different degrees of aggressiveness and different regions where they can appear (Pei et al., 2020). The classification established by the World Health Organization (WHO) (Louis et al., 2007) divides gliomas into four types: Astrocytomas, Oligodendrogliomas, Ependymomas and Oligo-astrocytomas.

Each of these types is divided into phases, which take into account characteristics such as the spread of the tumor to the rest of the organs or lymph nodes, the size of the tumor or the level of penetration.

The most common tumor staging system is the TNM (Society, 2022). T refers to the original tumor; N indicates that the cancer has spread to the lymph nodes, and M indicates that the cancer has spread and metastasized. Depending on the malignancy, Astrocytomas-type tumors are subdivided into four subtypes (JOVČEVSKA et al., 2013):

- Pilocytic - grado I
- Diffuse - grado II

- 46 • Anaplastic - grado III
- 47 • Glioblastoma multiforme - grado IV

48 The latter, Glioblastoma multiforme, is the most common type of glioma, affecting 60-70% of cases.  
49 Furthermore, its 5-year survival rate is 22% in people ages 20-44, 9% in people ages 45-54, and only 6% in  
50 people ages 55-64 (Brown et al., 2016). Glioblastoma multiforme is followed by Anaplastic Astrocytoma  
51 with 10-15% of cases (JOVČEVSKA et al., 2013). The term multiforme refers to the heterogeneity of this  
52 tumor, which can take different forms and be found in different regions of the brain.

53 Without treatment, survival for glioblastoma multiforme is about 3 to 6 months, so, like all tumors,  
54 but especially this malignant one, early diagnosis can increase the chances of survival. Treatments include  
55 chemotherapy and radiotherapy, but the one that has shown a greater increase in survival expectancy is  
56 tumor resection, which can be classified into two (Brown et al., 2016):

- 57 • GTR: Eliminate the tumor completely, although depending on the location and state of the glioma  
58 it is not always possible.
- 59 • STR: Partial removal of the tumor.

60 Both techniques are important in our study since the dataset used to train the different learning models  
61 contains this data, in which it is reported whether the patient underwent partial surgery, total surgery or  
62 no surgery. Glioblastoma multiforme (GBM) is classified as High Grade Glioma (HGG), while the rest  
63 of the lower grade gliomas are classified as Low Grade Glioma (LGG) (Menze et al., 2015). This is the  
64 classification used to train the models described in section 2.

65 Over the years, studies have been carried out to predict glioblastoma survival based on different  
66 parameters: In (Wankhede and Selvarani, 2022), the authors find the significant features from the  
67 extracted images using Gray Wolf Optimizer and proposed an architecture of Multilevel Layer modelling  
68 in Faster R-CNN approach based on feature weight factor and relative description model to build the  
69 selected features. With the same purpose, Fu et al. (Fu et al., 2021), proposed an architecture composed by  
70 27 convolutional layers, forming an encoder (based on VGG16 model) and decoder model and JajRoudi  
71 et al (Jajroudi et al., 2022) try to determine the qualitative and quantitative features affecting the survival  
72 of glioblastoma multiforme.

73 Also in recent years there has been an increasing trend in the use of pre-trained networks for multiple  
74 purposes. For example, in the field of medicine, which is the case at hand, transfer learning is being  
75 widely used for heart diseases problems detection (Deniz et al., 2018; Lopes et al., 2021; Kwon and  
76 Dong, 2022; Liao et al., 2020; Fang et al., 2022), for breast cancer detection and classification (Aljuaid  
77 et al., 2022; Byra, 2021; Assari et al., 2022; Kavithaa et al., 2021; Kavitha et al., 2022), for Glaucoma  
78 classificarion (Claro et al., 2019; Wang et al., 2022), respiratory pathologies (Roy and Kumar, 2022;  
79 Bargshady et al., 2022; Minaee et al., 2020), COVID-19 detection (Rahman et al., 2022) and so on. All  
80 this literature suggests that it is a useful technique for this type of problem.

81 In order to make a comparison under equal conditions, below are shown the studies carried out using  
82 the same data set that will be used in this work:

83 Previous studies attempting to predict the survival of patients with glioblastoma have used combina-  
84 tions of deep learning techniques with classical learning techniques, as in the case of the work by Lina  
85 and Shahram (Chato and Latifi, 2017). In their work, different methods were used to extract the image  
86 features and, once extracted, they were classified into two or three classes, differentiating between short-  
87 medium-, and long-term survivors, using different machine learning techniques. In the case of three  
88 classes, the best results were obtained using "Complex and median tree" with an accuracy of 62.5% and  
89 in the case of the two-class classification between short-term and long-term survivors, the best results  
90 were obtained with logistic regression, obtaining an accuracy of 68.8%. In (Suter et al., 2018), Suter et  
91 al. obtained an accuracy of 51.5% in predicting patient survival using convolutional networks, but once  
92 again, as in the previous case, the best results were obtained with classical techniques, specifically using a  
93 SVC (Support Vector Classifier) obtaining a 72.2% of accuracy in the training set, 57.1% in the validation  
94 set and 42.9% in the test set.

95 On the other hand, studies aimed at classifying the grade of glioblastoma have obtained promising  
96 results as it is a simpler task than determining the survival of the patient, which is affected by many more  
97 factors.

98 In (Cho and Park, 2017), the extraction of 180 characteristics was carried out and an accuracy of  
99 89.81% was obtained using logistic regression techniques. In the work developed by Pei et al. (Pei et al.,  
100 2020), both predictions were made along with tumor segmentation. In the first place, a segmentation  
101 of the tumor was performed and a 3D convolutional network was used to classify the tumor between  
102 the different classes. Finally, they carry out a hybrid technique like the previous studies using deep  
103 learning and traditional learning to be able to predict patient survival. In this study, an accuracy of 48.40%  
104 was obtained in the test set and a 58.6% in the validation set in predicting survival using convolutional  
105 networks to extract features from the images, and together with age using linear regression to obtain  
106 the predictions. The best state of art test accuracy (Banerjee et al., 2019) was obtained by the use of  
107 convolutional networks which achieved a 95% accuracy in the classification of LGG and HGG in MRI.

108 Analyzing the state of the art it can be observed that the approach that has obtained the most promising  
109 results is the use of hybrid techniques (deep learning and classical techniques) and that there is great  
110 potential for improving the models up to date since the precisions obtained are less than 69% when trying  
111 to make a classification of the survival time in two classes, less than 62.5% in the case of three classes,  
112 and less than 59% when trying to give a prediction of the estimated time of survival. Better results have  
113 been obtained in tumor classification, although they are still below 95%.

114 In this article, transfer learning techniques with two objectives are used and optimized according to  
115 the problem. On the one hand, to determine the survival time of people suffering from a glioma and on  
116 the other hand, to determine the grade of the tumor in order to carry out the most effective treatment.

117 Our approach involves using transfer learning techniques with multiple pre-trained convolutional  
118 neural networks (CNNs) to extract features from medical images of glioblastoma patients. These features  
119 are then fine-tuned using the same CNNs to improve their accuracy in predicting the survival and grade  
120 of the tumor. This approach represents a significant improvement over previous methods and has the  
121 potential to significantly improve the accuracy of predicting the survival and grade of glioblastoma.

122 The prediction of the survival and grade of glioblastoma is a highly complex and challenging task that  
123 has important implications for patient care and treatment. By improving the accuracy of these predictions,  
124 our approach has the potential to improve patient outcomes and reduce healthcare costs. Our paper  
125 demonstrates the effectiveness of our approach and shows that it represents a significant improvement  
126 over previous methods. This has important implications for the field of medical imaging and for the  
127 prediction of the survival and grade of glioblastoma.

128 Our approach of using transfer learning to predict the survival and grade of glioblastoma is based  
129 on computer vision and deep learning. Specifically, we use pre-trained models and transfer learning  
130 techniques to improve the accuracy of predictions on a new task, which has been shown to be highly  
131 effective in a variety of applications, including medical image analysis. Furthermore, our paper includes  
132 a detailed description of the dataset and preprocessing of the data, as well as an explanation of the  
133 experiments carried out and the optimization process of the model. These aspects of our paper demonstrate  
134 the thoroughness and logic of our approach.

135 The rest of the paper is organized as follows. The dataset and the preprocessing of the data is explained  
136 in section 2, together with all the pretrained models that have been used. In section 3, the experiments  
137 carried out and the optimization process of the model are explained and finally, we conclude in section 4.

## 138 2 METHODOLOGY

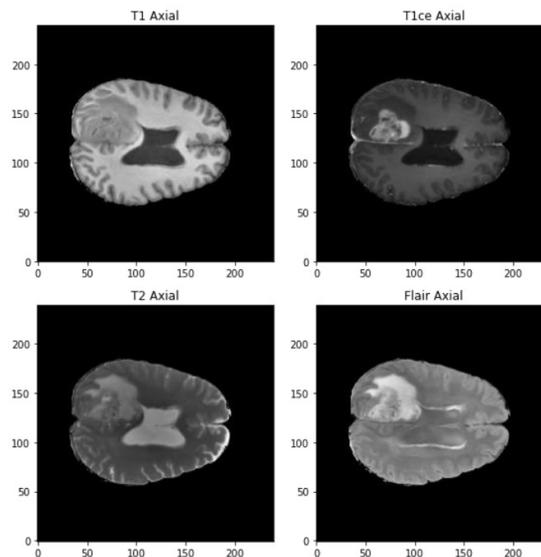
### 139 2.1 Dataset

140 The data set used in this paper is obtained from the BraTS 2020 (Menze et al., 2015; Bakas et al., 2017,  
141 2018), which is a competition for glioma segmentation, grade classification and survival classification.  
142 The dataset consists of 31GB with images and data from 369 patients. For each of these patients their  
143 age, survival in days and whether they have undergone a GTR, STR or no resection is stored. Regarding  
144 medical images, the data set contains 5 types of images for each of the 369 patients. These images are  
145 different 3D scans taken using different techniques. The techniques used were T1, T2, T1ce and T2-Flair  
146 scanners.

147 The images in three dimensions have a size of 240x240x155 and four different types of images can be  
148 found in the data set (See figure 1):

- 149 • T1: They show the normal anatomy of soft tissue and fat. They serve, for example, to confirm that  
150 a dough contains fat.

- 151 • T1ce: These are contrast-enhanced images that allow blood vessels or other soft tissues to be seen  
152 more clearly.
- 153 • T2: They show liquids and alterations such as tumors, inflammation or trauma.
- 154 • T2-Flair: Uses contrast to detect a wide range of lesions.



**Figure 1.** Visualization of the different types of scanner at 90mm

155 Along with these 4 images, there is also the segmented tumor scanner, but this is not used in this study.  
156 Not all patients have all the data such as age or survival, so a preprocessing step is necessary.

157 The images are in NifTI format. This is a format for medical images in which we can find the image  
158 along with more information about it. Each NifTI image is made up of three components.

- 159 • An N-D array containing the image data. In our case it is a 3-Dimensional matrix that contains a  
160 mapping of the patients' brains. Thanks to this any region or section of the patient's brain can be  
161 obtained.
- 162 • A 4x4 affine matrix with information about the position and orientation of the image in a given  
163 space.
- 164 • A header with metadata and information about the image.

## 165 2.2 Data preprocessing

166 The dataset used contains data from 369 patients. The number of data of each class is not balanced: 293  
167 patients belong to the HGG class, while only 76 belong to the LGG class. To balance both classes we have  
168 used subsampling. In this case, the ratio of HGG to LGG is approximately 4:1 (293:76), which means  
169 that the HGG class is significantly larger than the LGG class. This can cause the model to be biased  
170 towards the majority class and result in lower accuracy for the minority class. By subsampling the data,  
171 we ensured that both classes had an equal number of patients, which allowed us to train the model more  
172 effectively and obtain more accurate results. This is a common technique used in machine learning to  
173 address class imbalance and improve the performance of the model. In this way, the number of elements  
174 of both classes has been set at 76 patients and to increase the data to train and validate the models, each  
175 of the four images of each patient has been treated as if they were images of different patients. So the  
176 number of images for training, validation and test is 608. In this way, two things are obtained, on the one  
177 hand, the network is able to classify the degree and survival of the tumor in different images and, on the  
178 other hand, it is possible to increase the number of images for training, validation and testing. Even with  
179 this number of images, the models trained from scratch, both 3D and 2D, would not give good results

180 since they need a larger volume of data to be able to carry out precise classifications, so transfer learning  
181 techniques with different pre-trained models will be used to perform the classification.

182 Analyzing the data, it can be observed that all patients with a LGG-type tumor grade do not have  
183 information about their age, survival or type of resection. This is largely because these patients have a  
184 fairly favorable prognosis (Pardal Souto et al., 2015) and most do not undergo surgery. Their age will  
185 be set taking into account the mean of the rest of the ages and the standard deviation, so that the ages  
186 generated will be at most the mean plus the standard deviation and at least the mean minus the standard  
187 deviation.

188 To determine the survival time, we have relied on the study (Bush and Chang, 2016), so we will  
189 assume that 76% have survived more than 5 years and 24% less. So survival time was filled, taking into  
190 account that a 24% chance of surviving between 4 and 5 years and a 76% chance of surviving between 5  
191 and 7 years. Once they have randomly chosen which period of time the person will survive, based on  
192 the aforementioned probabilities, the number of days they have survived within that period is randomly  
193 generated and all the information is completed.

194 Once verified that there is no missing data, the age of the patients was normalized between the  
195 maximum and minimum ages and the data was transformed from text to numerical format so that the  
196 model can be trained. Tumor grades were codified as 0 for LGG and 1 for HGG and patient survival was  
197 codified as: 0 less than 1 year; 1 between 1-5 years; and 2 for survivors of more than 5 years.

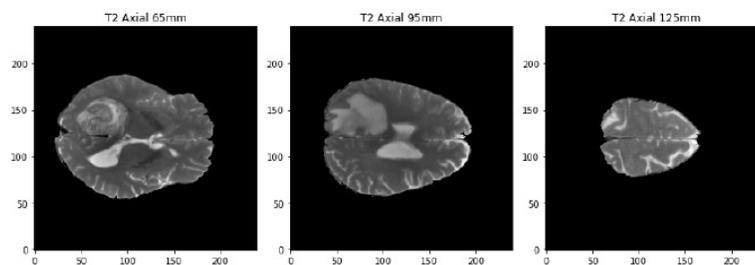
198 Three-dimensional images have different orientations depending on the orientation of the subject at  
199 the time of scanning. So the images are reoriented to a common space so that all images passed to the  
200 model will have the same orientation. The images are oriented using the nibabel library (@li, 2022) to the  
201 RAS axis.

202 After that, an image normalization step is carried out: Images are three-dimensional arrays. The  
203 content of these arrays are not integers from 0 to 255 like most images, but are decimal numbers  
204 which represent Hounsfield units (HU) (Bell and Greenway, 2015). These units are universally used in  
205 tomography and scanners in a standardized way. They are obtained by the linear transformation of the  
206 measured attenuation coefficients. It is based on the densities of pure water which corresponds to 0 HU  
207 and of air which corresponds to -1000 HU. Scanner values are generally in the range from -1000 (air) to  
208 +2000 HU for denser bones. To avoid bones appearing in the images and confusing the network, in this  
209 paper, values are limited between [-1000, 800], in such a way that bones with a measurement of about  
210 1000 HU are avoided (Han and Kamdar, 2018). Once the values have been delimited, a normalization is  
211 this range was performed.

212 The last preprocessing step is the image segmentation. The pre-trained models used have been trained  
213 with images of size 224x224x3, although the first two dimensions can vary by a certain margin. That is  
214 why we need to adjust the images to fit them into these models. Our images are sized at 240x240x155 so  
215 our target size will be 240x240x3. It is not necessary to modify the first two dimensions, but the third  
216 one does. The images are three-dimensional models of the brain, so to reduce the dimensionality, three  
217 segments of the brain are taken. These cuts have been made through three different areas of the brain  
218 separated by 30mm. In figure 2, how these cuts have been made is shown and in figure 3 an example of  
219 how these three segments would look in a T2 image are represented. We can clearly differentiate different  
220 sizes of the tumor in them as they are different regions within the complete 3D model. After all these  
221 steps, the segmented, normalized image with a fixed orientation is ready to be used in the model.



**Figure 2.** Visualization of the location of the three cuts made



**Figure 3.** Example of the three cuts made to each image, corresponding to a T2-type scanner

222 Table 1 in the study provides a comparison of the clinical characteristics of LGG and HGG patients,  
223 including age, survival time, and tumor grade. The table shows that LGG patients are generally younger  
224 than HGG patients, with a mean age of 38.5 years compared to 56.5 years for HGG patients. Additionally,  
225 LGG patients have a longer survival time than HGG patients, with a mean survival time of 5.5 years  
226 compared to 1.1 years for HGG patients.

**Table 1.** Clinical Characteristics of LGG and HGG Patients

Clinical Characteristics	LGG Patients	HGG Patients
Mean Age (years)	38.5	56.5
Mean Survival Time (years)	5.5	1.1
Tumor Grade Distribution	Grade II: 50%. Grade III: 50%	Grade IV: 100%

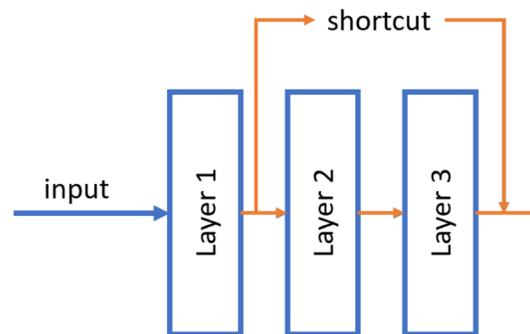
## 2.3 Pre-trained Models

The training process has been carried out using pre-trained models that facilitate the image feature extraction stage, only having to train the layers that are responsible for classifying the images according to the classes defined in the experiment. In the last years, many models have been trained with large image sets and have been made publicly available to researchers to benefit from the weights learned during this process. In the next sections, the pre trained networks evaluated are briefly described.

### 2.3.1 ResNet

ResNet was published by He et al in 2015 (He et al., 2015). These neural networks differ from traditional ones in that they have a shortcut connection between non-contiguous layers of the network. With this, it is possible to propagate the information better and avoid the fading of the gradient in the backpropagation phase. Numerous recent studies have been conducted in the field of tumor detection utilizing ResNet, showcasing the remarkable performance and efficacy of this architectural approach (El-Feshawy et al., 2023; Shehab et al., 2021; Aggarwal et al., 2023).

An example of this shortcut can be shown in figure 4.



**Figure 4.** Example of the shortcut connection used in residual network (resnet). In this case, the output of layer 1 is merged directly into the output of layer 3.

Two models with different number of hidden layers have been evaluated: ResNet50 and ResNet101.

### 2.3.2 EfficientNet

EfficientNet was proposed by Tan and Le in (Tan and Le, 2019). This neural networks uniformly scales all dimensions of the images (depth, width and resolution) at the same time using a coefficient called "compound coefficient". With this approach, EfficientNet achieved great accuracies on classical datasets such as ImageNet while being 8.4x smaller and 6.1x faster on inference than the previous convolutional neural networks. This EfficientNet architecture has shown great performance in some recent studies about brain tumor (Tripathy et al., 2023; Nayak et al., 2022). Some EfficientNet models were evaluated but only results of the best one, EfficientNetB4, were shown in this paper.

### 2.3.3 VGG16

VGG16 (Simonyan and Zisserman, 2014) is a deep architecture consisting of convolutional layers with filters of dimension  $3 \times 3$  using the ReLU activation function. Interspersed between the convolutional layers, some Maxpooling layers are used to avoid network overfitting with size  $2 \times 2$  and make the network generalize as much as possible. VGG16 has shown good performance in some recent brain tumor researches (Gayathri et al., 2023; Younis et al., 2022). Fig 5 shows the architecture of the network.

### 2.3.4 InceptionV3

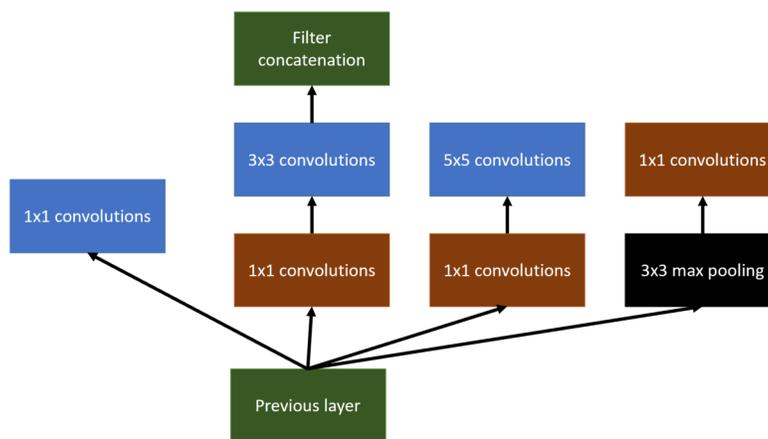
Inception architecture (Szegedy et al., 2016b) tries to get wider networks instead of deeper ones. The main objective of this change is the tendency of very deep networks to overfitting in addition to the difficulty of propagating the gradient to update the network. Inception has been also used for tumor detection and localization in the last few years (Rastogi et al., 2023; Taher et al., 2022).

Inception tries to use different variable-size convolutional filters at the same level, concatenating the result of all of them to define the input of the next layer of the network.



**Figure 5.** VGG16 architecture

263 An example of this can be shown in figure 6. In this paper, Inception v3 has been used..



**Figure 6.** Inception main idea using multiples convolutional layers at the same level

### 264 **2.3.5 InceptionResNetV2**

265 As a combination of two of the architectures we have seen, InceptionResNet was created. This neural  
 266 network combines the ability to create wider networks with the ability of residual blocks to better  
 267 propagate information across layers (Szegedy et al., 2016a).

### 268 **2.3.6 DenseNet**

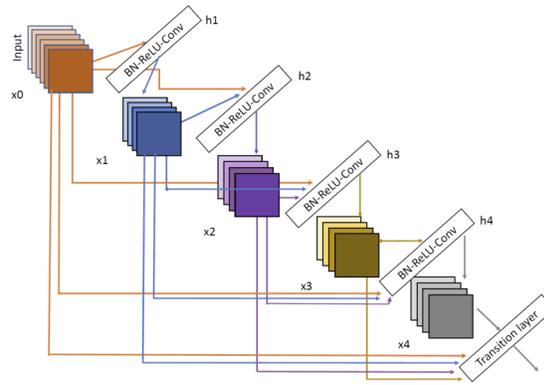
269 The last architecture evaluated is DenseNet (Huang et al., 2016). We have selected two variants  
 270 DenseNet121 and DenseNet201. DenseNet architecture can be shown in figure 7. As we can see,  
 271 the input of each layer is created as a combination of the outputs of all the previous layers so, as with  
 272 Inception network, the propagation is done in a much more direct way, avoiding gradient fading when the  
 273 depth of the network is very large. Using DenseNet, several paper have demonstrated good performance  
 274 in brain tumor tasks (Özkaraca et al., 2023; Alshammari, 2023; Zhu et al., 2022).

## 275 **3 EXPERIMENTS AND RESULTS**

### 276 **3.1 Experimental setup**

277 The model is designed to harness the synergy between pre-processed images and textual data during  
 278 the training process. This fusion of multimedia inputs aims to enhance the accuracy and effectiveness  
 279 of our classification task. The process commences with the pre-processed images, which are subjected  
 280 to an initial phase within the pre-trained model. This phase is characterized by the utilization of a  
 281 GlobalAveragePooling2D layer, a pivotal component in feature extraction from the images.

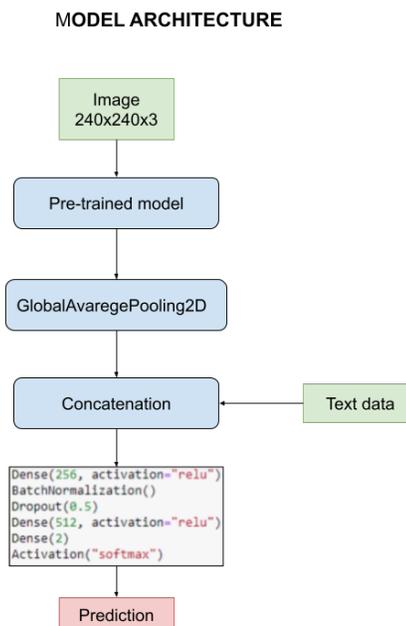
282 However, what sets our model apart is the subsequent stage, where the outcomes of the image  
 283 convolution process are intelligently combined with textual data. This textual data includes crucial  
 284 information such as the patient's age and the specific state of tumor resection. This amalgamation of



**Figure 7.** DenseNet architecture extracted from (Huang et al., 2016)

285 image-based and text-based information forms the core foundation upon which our classification task is  
 286 executed.

287 For a holistic understanding of the model's architecture, please refer to figure 8. In this visual  
 288 representation, you will find a detailed overview of the model's structure, complete with its parameters  
 289 and the distinct layers that collectively facilitate the classification process. Notably, these layers remain  
 290 consistent throughout our quest for the optimal pre-trained model. However, it's essential to highlight that  
 291 the manual optimization of these layers is a critical step in fine-tuning the model's performance, a process  
 292 we meticulously undertake to ensure the best results.



**Figure 8.** Architecture of the model used to carry out the experiments

293 Survival and glioma grade have been predicted using two different networks. This decision was  
 294 made to optimize both networks since otherwise there would be a certain dependency between them,  
 295 for example when we try to avoid overfitting. The most important parameters initially chosen common  
 296 to every train are: A learning rate of 0.0002, optimizer Adam, 16 as batch size and 10 epochs. For the  
 297 classification, the architecture discussed above has been used, with 256-512 neurons for the first and

298 second dense layers respectively, BatchNormalization and a dropout layer with a rate of 0.5.

### 299 3.2 Results

300 All networks have been tested with the same set of test, which is a different set from the training and  
301 validation set and does not has never been seen by the trained neural network. In table 2 results obtained  
302 by the different networks can be observed.

**Table 2.** Accuracy results obtained with different networks.

	Grade F1-Macro	Survival F1-Macro
ResNet50	0.58	0.16
ResNet101	0.31	0.42
EfficientNetB4	0.62	0.39
VGG16	0.89	0.46
InceptionV3	0.96	0.43
InceptionResNetV2	0.74	0.50
Densenet121	0.95	0.52
Densenet201	0.91	0.51

303 Although the best results in predicting the grade were obtained by the InceptionV3 architecture, the  
304 results for survival were not very satisfactory. For that reason, the network to be optimized for obtaining  
305 the best possible results will be DenseNet121 since it has obtained the most balanced results in both  
306 experiments.

307 Using the same data from the previous trainings, different tests to find the best hyperparameters and  
308 classification layer architecture with the DenseNet121 pretrained network were performed. As there  
309 are two independent experiments, the hyperparameter optimization has been done twice, once for each  
310 purpose.

311 The following table 3 shows the results obtained in each of the experiments varying one parameter  
312 each time, leaving all the other parameters at they default value. The best results and therefore the option  
313 chosen for each parameter and experiment are highlighted.

**Table 3.** Hyperparameter optimization results for grade and survival experiments. Best results for each network are highlighted.

Experiments	Grade F1-Macro	Survival F1-Macro	
BatchNormalization	2 layers	0.88	0.48
	1 layer	0.96	0.44
	0 layers	0.94	0.51
Number of neurons	1° 32 - 2° 64	0.96	0.51
	1° 64- 2° 128	0.90	0.47
	1° 128- 2° 256	0.89	0.29
	1° 256- 2° 256	0.97	0.16
Dropout rate	0.2	0.93	0.60
	0.3	0.97	0.51
	0.4	0.93	0.52
	0.5	0.96	0.58
Activation function	relu	0.97	0.60
	tanh	0.95	0.50
Learning rate	0.0005	0.97	0.60
	0.001	0.93	0.48
	0.002	0.92	0.34

314 After determining the best network configuration parameters, we proceeded to evaluate which was  
 315 the best division of the dataset. To do this, we carry out a Monte Carlo cross validation process with ten  
 316 iterations and we are left with the average value of the evaluated metrics. We performed tests with the  
 317 following train percentage settings: 90-10, 80-20, 70-30,60-40 and 50-50. In table 4 you can see the  
 318 results obtained for each of the two trained models.

**Table 4.** Dataset division evaluation to determine the best configuration of train-test split

Training proportion	Model	Precision	Recall	F1-Score
90%	Grade	0.89	0.90	0.89
90%	Survival	0.63	0.48	0.40
80%	Grade	<b>0.97</b>	<b>0.97</b>	<b>0.97</b>
80%	Survival	0.61	<b>0.61</b>	<b>0.60</b>
70%	Grade	0.87	0.86	0.86
70%	Survival	0.47	0.40	0.38
60%	Grade	0.83	0.83	0.83
60%	Survival	0.24	0.32	0.27
50%	Grade	0.86	0.86	0.86
50%	Survival	0.52	0.48	0.48

319 As you can see, the best results are obtained with the 80-20 configuration, so that is determined as the  
 320 optimal one.

321 The final model has been meticulously trained utilizing the pre-trained DenseNet121 model, ensuring  
 322 that each parameter was optimized for peak performance. Specifically, for the grade classification task,  
 323 we found that a single layer of BatchNormalization, 256 neurons in each dense layer, a dropout rate of  
 324 0.3, relu as the activation function, and a learning rate of 0.0005 produced exceptional results. Conversely,  
 325 when focusing on survival prediction, we observed that a configuration featuring two BatchNormalization  
 326 layers, 32 neurons in the initial dense layer, and 64 in the subsequent one, along with a dropout rate of 0.2,

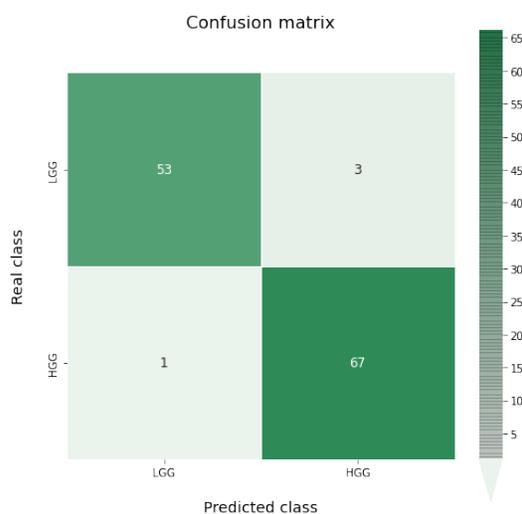
327 relu as the activation function, and a learning rate of 0.0005s, yielded outstanding predictive capabilities.

328 In the context of tumor grade classification, which encompasses both HGG and LGG, our model  
 329 achieved a remarkable accuracy of 97% on the test dataset, as demonstrated in Table 5. These results  
 330 underscore the robustness and reliability of our approach, positioning it as a valuable tool in the field of  
 331 medical image analysis for brain tumor diagnosis and prognosis.

**Table 5.** Scores obtained for the prediction of the grade in the test data by the optimal grade model.

	precision	recall	f1-score	accuracy
LGG	0.98	0.95	0.96	
HGG	0.96	0.99	0.97	
Macro avg	0.97	0.97	0.97	0.97

332 A confusion matrix for this classification can be seen in figure 9. As we can see, the results obtained  
 333 are almost perfect, failing only in 4 images (3 LGG images classified as HGG and 1 HGG image classified  
 334 as LGG).



**Figure 9.** Confusion matrix obtained for the prediction of the grade in the test data by the optimal grade model

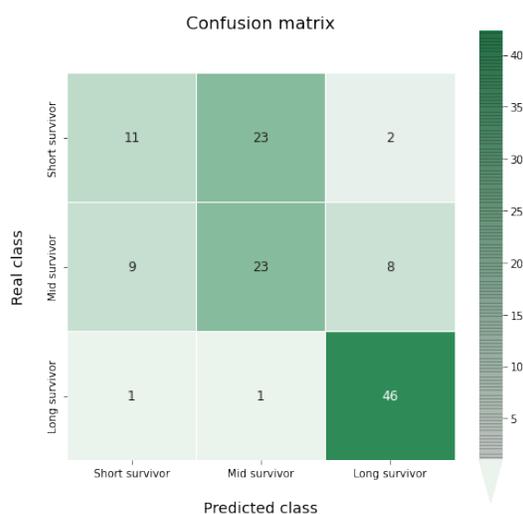
335 In the case of the classification of survival in short, medium or long, a 65% accuracy has been obtained.  
 336 Results by classes with precision recall and f-score, and the global accuracy can be shown in table 6.

**Table 6.** Scores obtained for the prediction of the survival in the test data by the optimal survival model.

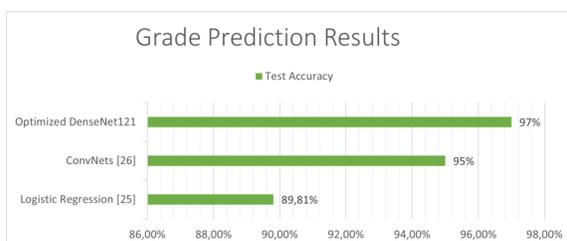
	precision	recall	f1-score	accuracy
short survivor	0.52	0.31	0.39	
mid survivor	0.49	0.57	0.53	
long survivor	0.82	0.96	0.88	
macro avg	0.61	0.61	0.60	0.65

337 The confusion matrix of this multiclass classification can be seen in the figure 10. This problem is  
 338 much more complex than in the previous case, so we can see several more failures in the classification.  
 339 The worst results occur in the short survivor class where 25 cases are incorrectly classified (23 as mid  
 340 survivor). However, the long survivor cases are correctly classified in almost 96% of the data evaluated.

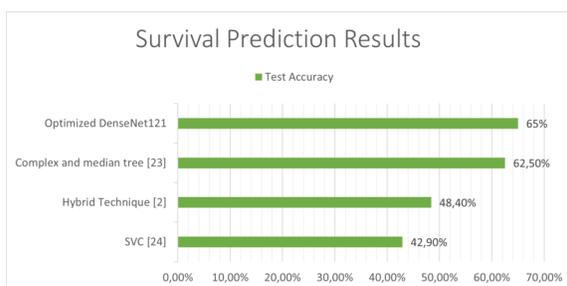
341 The next figures 11 and 12, show a comparison between the state of art results and our results. Our  
 342 models have obtained the best test accuracy in each task outperforming the previous state of art results.



**Figure 10.** Confusion matrix obtained for the prediction of the survival in the test data by the optimal survival model



**Figure 11.** Comparison between our results and the state of art results for the grade classification.



**Figure 12.** Comparison between our results and the state of art results for the survival prediction.

#### 343 4 CONCLUSIONS

344 In this study, we pursued the development of two neural networks with a dual objective: to assess the  
345 degree of progression and predict the probability of survival in patients with gliomas. Leveraging transfer  
346 learning techniques, we harnessed the power of pre-trained neural networks, fine-tuning them for our  
347 specific task. Our dataset comprised a comprehensive set of images drawn from the BraTS 2020 dataset,  
348 encompassing 369 unique patient cases.

349 Our chosen neural architectures not only performed image description but also seamlessly conducted  
350 classification tasks concurrently. This dual functionality allowed us to harness classification information  
351 for the precise extraction of salient features tailored to each case. To ensure the optimal performance of  
352 these neural networks, we conducted an exhaustive investigation, exploring multiple pre-trained models  
353 and refining their hyperparameters through an extensive gridsearch analysis.

354 The outcomes of our study have yielded compelling results that outperform existing state-of-the-art  
355 techniques evaluated on the same dataset. Specifically, we observed a notable improvement in the degree of  
356 disease classification accuracy, surpassing the existing benchmarks by more than 2.1%. Furthermore, our  
357 survival prediction model demonstrated a remarkable 4.0% enhancement compared to current approaches.

358 These findings not only underscore the efficacy of our proposed methodologies but also hold significant  
359 implications for the clinical field. Our research has the potential to refine the diagnosis and prognosis  
360 of glioma patients, ultimately contributing to improved patient care and outcomes. In conclusion, this  
361 study represents a significant advancement in the realm of medical image analysis and underscores the  
362 promising prospects of leveraging transfer learning and dual-purpose neural networks in the domain of  
363 glioma research.

364 In future work we intend to carry out a more detailed study of the problem incorporating more images  
365 of different patients and analyzing this technological solution with different fields of application in the  
366 field of medicine.

#### 367 REFERENCES

- 368 (2022). Estadísticas del cáncer - NCI.
- 369 (2022). Neuroimaging in Python — NiBabel 4.0.0 documentation.
- 370 Aggarwal, M., Tiwari, A. K., Sarathi, M. P., and Bijalwan, A. (2023). An early detection and segmentation  
371 of brain tumor using deep neural network. *BMC Medical Informatics and Decision Making*, 23(1):78.
- 372 Aljuaid, H., Alturki, N., Alsubaie, N., Cavallaro, L., and Liotta, A. (2022). Computer-aided diagnosis for  
373 breast cancer classification using deep neural networks and transfer learning. *Computer Methods and  
374 Programs in Biomedicine*, 223:106951.
- 375 Alshammari, A. (2023). Densenet hybwwoa: A densenet-based brain metastasis classification with a  
376 hybrid metaheuristic feature selection strategy. *Biomedicine*, 11(5).
- 377 Assari, Z., Mahloojifar, A., and Ahmadinejad, N. (2022). A bimodal BI-RADS-guided GoogLeNet-based  
378 CAD system for solid breast masses discrimination using transfer learning. *Computers in Biology and  
379 Medicine*, 142:105160.
- 380 Bakas, S., Akbari, H., Sotiras, A., Bilello, M., Rozycki, M., Kirby, J. S., Freymann, J. B., Farahani, K.,  
381 and Davatzikos, C. (2017). Advancing The Cancer Genome Atlas glioma MRI collections with expert  
382 segmentation labels and radiomic features. *Scientific Data 2017 4:1*, 4(1):1–13.
- 383 Bakas, S., Reyes, M., Jakab, A., Bauer, S., Rempfler, M., Crimi, A., Shinohara, R. T., Berger, C.,  
384 Ha, S. M., Rozycki, M., Prastawa, M., Alberts, E., Lipkova, J., Freymann, J., Kirby, J., Bilello, M.,  
385 Fathallah-Shaykh, H., Wiest, R., Kirschke, J., Wiestler, B., Colen, R., Kotrotsou, A., Lamontagne, P.,  
386 Marcus, D., Milchenko, M., Nazeri, A., Weber, M.-A., Mahajan, A., Baid, U., Gerstner, E., Kwon,  
387 D., Acharya, G., Agarwal, M., Alam, M., Albiol, A., Albiol, A., Albiol, F. J., Alex, V., Allinson, N.,  
388 Amorim, P. H. A., Amrutkar, A., Anand, G., Andermatt, S., Arbel, T., Arbelaez, P., Avery, A., Azmat,  
389 M., B., P., Bai, W., Banerjee, S., Barth, B., Batchelder, T., Batmanghelich, K., Battistella, E., Beers, A.,  
390 Belyaev, M., Bendszus, M., Benson, E., Bernal, J., Bharath, H. N., Biros, G., Bisdas, S., Brown, J.,  
391 Cabezas, M., Cao, S., Cardoso, J. M., Carver, E. N., Casamitjana, A., Castillo, L. S., Catà, M., Cattin,  
392 P., Cerigues, A., Chagas, V. S., Chandra, S., Chang, Y.-J., Chang, S., Chang, K., Chazalon, J., Chen, S.,  
393 Chen, W., Chen, J. W., Chen, Z., Cheng, K., Choudhury, A. R., Chylla, R., Clérigues, A., Colleman, S.,  
394 Colmeiro, R. G. R., Combalia, M., Costa, A., Cui, X., Dai, Z., Dai, L., Daza, L. A., Deutsch, E., Ding,  
395 C., Dong, C., Dong, S., Dudzik, W., Eaton-Rosen, Z., Egan, G., Escudero, G., Estienne, T., Everson,

- 396 R., Fabrizio, J., Fan, Y., Fang, L., Feng, X., Ferrante, E., Fidon, L., Fischer, M., French, A. P., Fridman,  
397 N., Fu, H., Fuentes, D., Gao, Y., Gates, E., Gering, D., Gholami, A., Gierke, W., Glocker, B., Gong, M.,  
398 González-Villá, S., Groszes, T., Guan, Y., Guo, S., Gupta, S., Han, W.-S., Han, I. S., Harmuth, K., He,  
399 H., Hernández-Sabaté, A., Herrmann, E., Himthani, N., Hsu, W., Hsu, C., Hu, X., Hu, X., Hu, Y., Hu,  
400 Y., Hua, R., Huang, T.-Y., Huang, W., Van Huffel, S., Huo, Q., HV, V., Iftekharuddin, K. M., Isensee,  
401 F., Islam, M., Jackson, A. S., Jambawalikar, S. R., Jesson, A., Jian, W., Jin, P., Jose, V. J. M., Jungo, A.,  
402 Kainz, B., Kamnitsas, K., Kao, P.-Y., Karnawat, A., Kellermeier, T., Kerimi, A., Keutzer, K., Khadir,  
403 M. T., Khened, M., Kickingereeder, P., Kim, G., King, N., Knapp, H., Knecht, U., Kohli, L., Kong, D.,  
404 Kong, X., Koppers, S., Kori, A., Krishnamurthi, G., Krivov, E., Kumar, P., Kushibar, K., Lachinov, D.,  
405 Lambrou, T., Lee, J., Lee, C., Lee, Y., Lee, M., Lefkovičs, S., Lefkovičs, L., Levitt, J., Li, T., Li, H., Li,  
406 W., Li, H., Li, X., Li, Y., Li, H., Li, Z., Li, X., Li, Z., Li, X., Li, W., Lin, Z.-S., Lin, F., Lio, P., Liu, C.,  
407 Liu, B., Liu, X., Liu, M., Liu, J., Liu, L., Llado, X., Lopez, M. M., Lorenzo, P. R., Lu, Z., Luo, L., Luo,  
408 Z., Ma, J., Ma, K., Mackie, T., Madabushi, A., Mahmoudi, I., Maier-Hein, K. H., Maji, P., Mammen,  
409 C., Mang, A., Manjunath, B. S., Marcinkiewicz, M., McDonagh, S., McKenna, S., McKinley, R., Mehl,  
410 M., Mehta, S., Mehta, R., Meier, R., Meinel, C., Merhof, D., Meyer, C., Miller, R., Mitra, S., Moiyadi,  
411 A., Molina-Garcia, D., Monteiro, M. A. B., Mrukwa, G., Myronenko, A., Nalepa, J., Ngo, T., Nie, D.,  
412 Ning, H., Niu, C., Nuechterlein, N. K., Oermann, E., Oliveira, A., Oliveira, D. D. C., Oliver, A., Osman,  
413 A. F. I., Ou, Y.-N., Ourselin, S., Paragios, N., Park, M. S., Paschke, B., Pauloski, J. G., Pawar, K.,  
414 Pawlowski, N., Pei, L., Peng, S., Pereira, S. M., Perez-Beteta, J., Perez-Garcia, V. M., Pezold, S., Pham,  
415 B., Phophalia, A., Piella, G., Pillai, G. N., Piraud, M., Pisov, M., Popli, A., Pound, M. P., Pourreza, R.,  
416 Prasanna, P., Prkowska, V., Pridmore, T. P., Puch, S., Puybureau, É., Qian, B., Qiao, X., Rajchl, M.,  
417 Rane, S., Rebsamen, M., Ren, H., Ren, X., Revanuru, K., Rezaei, M., Rippel, O., Rivera, L. C., Robert,  
418 C., Rosen, B., Rueckert, D., Safwan, M., Salem, M., Salvi, J., Sanchez, I., Sánchez, I., Santos, H. M.,  
419 Sartor, E., Schellingerhout, D., Scheufeke, K., Scott, M. R., Scussel, A. A., Sedlar, S., Serrano-Rubio,  
420 J. P., Shah, N. J., Shah, N., Shaikh, M., Shankar, B. U., Shboul, Z., Shen, H., Shen, D., Shen, L.,  
421 Shen, H., Shenoy, V., Shi, F., Shin, H. E., Shu, H., Sima, D., Sinclair, M., Smedby, O., Snyder, J. M.,  
422 Soltaninejad, M., Song, G., Soni, M., Stawiaski, J., Subramanian, S., Sun, L., Sun, R., Sun, J., Sun, K.,  
423 Sun, Y., Sun, G., Sun, S., Suter, Y. R., Szilagy, L., Talbar, S., Tao, D., Tao, D., Teng, Z., Thakur, S.,  
424 Thakur, M. H., Tharakan, S., Tiwari, P., Tochon, G., Tran, T., Tsai, Y. M., Tseng, K.-L., Tuan, T. A.,  
425 Turlapov, V., Tustison, N., Vakalopoulou, M., Valverde, S., Vanguri, R., Vasiliev, E., Ventura, J., Vera,  
426 L., Vercauteren, T., Verrastro, C. A., Vidyaratne, L., Vilaplana, V., Vivekanandan, A., Wang, G., Wang,  
427 Q., Wang, C. J., Wang, W., Wang, D., Wang, R., Wang, Y., Wang, C., Wang, G., Wen, N., Wen, X.,  
428 Weninger, L., Wick, W., Wu, S., Wu, Q., Wu, Y., Xia, Y., Xu, Y., Xu, X., Xu, P., Yang, T.-L., Yang, X.,  
429 Yang, H.-Y., Yang, J., Yang, H., Yang, G., Yao, H., Ye, X., Yin, C., Young-Moxon, B., Yu, J., Yue, X.,  
430 Zhang, S., Zhang, A., Zhang, K., Zhang, X., Zhang, L., Zhang, X., Zhang, Y., Zhang, L., Zhang, J.,  
431 Zhang, X., Zhang, T., Zhao, S., Zhao, Y., Zhao, X., Zhao, L., Zheng, Y., Zhong, L., Zhou, C., Zhou,  
432 X., Zhou, F., Zhu, H., Zhu, J., Zhuge, Y., Zong, W., Kalpathy-Cramer, J., Farahani, K., Davatzikos,  
433 C., van Leemput, K., and Menze, B. (2018). Identifying the Best Machine Learning Algorithms for  
434 Brain Tumor Segmentation, Progression Assessment, and Overall Survival Prediction in the BRATS  
435 Challenge.
- 436 Banerjee, S., Mitra, S., Masulli, F., and Rovetta, S. (2019). Deep radiomics for brain tumor detection and  
437 classification from multi-sequence mri. *ArXiv*, abs/1903.09240.
- 438 Bargshady, G., Zhou, X., Barua, P. D., Gururajan, R., Li, Y., and Acharya, U. R. (2022). Application of  
439 CycleGAN and transfer learning techniques for automated detection of COVID-19 using X-ray images.  
440 *Pattern Recognition Letters*, 153:67–74.
- 441 Bell, D. and Greenway, K. (2015). Hounsfield unit. *Radiopaedia.org*.
- 442 Brown, T. J., Brennan, M. C., Li, M., Church, E. W., Brandmeir, N. J., Rakszawski, K. L., Patel, A. S.,  
443 Rizk, E. B., Suki, D., Sawaya, R., and Glantz, M. (2016). Association of the Extent of Resection With  
444 Survival in Glioblastoma: A Systematic Review and Meta-analysis. *JAMA oncology*, 2(11):1460–1469.
- 445 Bush, N. A. O. and Chang, S. (2016). Treatment strategies for low-grade glioma in adults. *Journal of*  
446 *Oncology Practice*, 12(12):1235–1241.
- 447 Byra, M. (2021). Breast mass classification with transfer learning based on scaling of deep representations.  
448 *Biomedical Signal Processing and Control*, 69:102828.
- 449 Chato, L. and Latifi, S. (2017). Machine Learning and Deep Learning Techniques to Predict Overall  
450 Survival of Brain Tumor Patients using MRI Images. *Proceedings - 2017 IEEE 17th International*

- 451 *Conference on Bioinformatics and Bioengineering, BIBE 2017, 2018-January:9–14.*
- 452 Cho, H. H. and Park, H. (2017). Classification of low-grade and high-grade glioma using multi-modal  
453 image radiomics features. *Proceedings of the Annual International Conference of the IEEE Engineering  
454 in Medicine and Biology Society, EMBS*, pages 3081–3084.
- 455 Claro, M., Veras, R., Santana, A., Araújo, F., Silva, R., Almeida, J., and Leite, D. (2019). An hybrid  
456 feature space from texture information and transfer learning for glaucoma classification. *Journal of  
457 Visual Communication and Image Representation*, 64:102597.
- 458 Deniz, E., Sengur, A., Kadiroglu, Z., Guo, Y., Bajaj, V., and Budak, U. (2018). Transfer learning based  
459 histopathologic image classification for breast cancer detection. *Health Information Science And  
460 Systems*.
- 461 El-Feshawy, S. A., Saad, W., Shokair, M., and Dessouky, M. (2023). IoT framework for brain tumor  
462 detection based on optimized modified ResNet 18 (OMRES). *The Journal of Supercomputing*,  
463 79(1):1081–1110.
- 464 Fang, R., Lu, C. C., Chuang, C. T., and Chang, W. H. (2022). A visually interpretable detection  
465 method combines 3-D ECG with a multi-VGG neural network for myocardial infarction identification.  
466 *Computer Methods and Programs in Biomedicine*, 219:106762.
- 467 Fu, J., Singhrao, K., Zhong, X., Gao, Y., Qi, S. X., Yang, Y., Ruan, D., and Lewis, J. H. (2021). An  
468 Automatic Deep Learning–Based Workflow for Glioblastoma Survival Prediction Using Preoperative  
469 Multimodal MR Images: A Feasibility Study. *Advances in Radiation Oncology*, 6(5):100746.
- 470 Gayathri, P., Dhavileswarapu, A., Ibrahim, S., Paul, R., and Gupta, R. (2023). Exploring the potential  
471 of vgg-16 architecture for accurate brain tumor detection using deep learning. *Journal of Computers,  
472 Mechanical and Management*, 2(2):13–22.
- 473 Han, L. and Kamdar, M. R. (2018). MRI to MGMT: Predicting methylation status in glioblastoma patients  
474 using convolutional recurrent neural networks. *Pacific Symposium on Biocomputing*, 0(212669):331–  
475 342.
- 476 He, K., Zhang, X., Ren, S., and Sun, J. (2015). Deep residual learning for image recognition. *CoRR*,  
477 abs/1512.03385.
- 478 Huang, G., Liu, Z., and Weinberger, K. Q. (2016). Densely connected convolutional networks. *CoRR*,  
479 abs/1608.06993.
- 480 Jajroudi, M., Enferadi, M., Homayoun, A. A., and Reiazi, R. (2022). MRI-based machine learning  
481 for determining quantitative and qualitative characteristics affecting the survival of glioblastoma  
482 multiforme. *Magnetic Resonance Imaging*, 85:222–227.
- 483 JOVČEVSKA, I., KOČEVAR, N., and KOMEL, R. (2013). Glioma and glioblastoma - how much do we  
484 (not) know? *Molecular and clinical oncology*, 1(6):935–941.
- 485 Kavitha, T., Mathai, P. P., Karthikeyan, C., Ashok, M., Kohar, R., Avanija, J., and Neelakandan, S. (2022).  
486 Deep Learning Based Capsule Neural Network Model for Breast Cancer Diagnosis Using Mammogram  
487 Images. *Interdisciplinary Sciences: Computational Life Sciences*, 14(1):113–129.
- 488 Kavithaa, G., Balakrishnan, P., and Yuvaraj, S. A. (2021). Lung Cancer Detection and Improving Accuracy  
489 Using Linear Subspace Image Classification Algorithm. *Interdisciplinary Sciences: Computational  
490 Life Sciences*, 13(4):779–786.
- 491 Kwon, S. H. and Dong, L. (2022). Flexible sensors and machine learning for heart monitoring. *Nano  
492 Energy*, 102:107632.
- 493 Liao, X., Qian, Y., Chen, Y., Xiong, X., Wang, Q., and Heng, P. A. (2020). MMTLNet: Multi-Modality  
494 Transfer Learning Network with adversarial training for 3D whole heart segmentation. *Computerized  
495 Medical Imaging and Graphics*, 85:101785.
- 496 Lopes, R. R., Bleijendaal, H., Ramos, L. A., Verstraelen, T. E., Amin, A. S., Wilde, A. A., Pinto, Y. M.,  
497 de Mol, B. A., and Marquering, H. A. (2021). Improving electrocardiogram-based detection of rare  
498 genetic heart disease using transfer learning: An application to phospholamban p.Arg14del mutation  
499 carriers. *Computers in Biology and Medicine*, 131:104262.
- 500 Louis, D. N., Ohgaki, H., Wiestler, O. D., Cavenee, W. K., Burger, P. C., Jouvett, A., Scheithauer, B. W.,  
501 and Kleihues, P. (2007). The 2007 WHO classification of tumours of the central nervous system. *Acta  
502 neuropathologica*, 114(2):97–109.
- 503 Menze, B. H., Jakab, A., Bauer, S., Kalpathy-Cramer, J., Farahani, K., Kirby, J., Burren, Y., Porz, N.,  
504 Slotboom, J., Wiest, R., Lanczi, L., Gerstner, E., Weber, M. A., Arbel, T., Avants, B. B., Ayache, N.,  
505 Buendia, P., Collins, D. L., Cordier, N., Corso, J. J., Criminisi, A., Das, T., Delingette, H., Demiralp,

- 506 Ç., Durst, C. R., Dojat, M., Doyle, S., Festa, J., Forbes, F., Geremia, E., Glocker, B., Golland, P., Guo,  
507 X., Hamamci, A., Iftekharuddin, K. M., Jena, R., John, N. M., Konukoglu, E., Lashkari, D., Mariz,  
508 J. A., Meier, R., Pereira, S., Precup, D., Price, S. J., Raviv, T. R., Reza, S. M., Ryan, M., Sarikaya, D.,  
509 Schwartz, L., Shin, H. C., Shotton, J., Silva, C. A., Sousa, N., Subbanna, N. K., Szekely, G., Taylor, T. J.,  
510 Thomas, O. M., Tustison, N. J., Unal, G., Vasseur, F., Wintermark, M., Ye, D. H., Zhao, L., Zhao, B.,  
511 Zikic, D., Prastawa, M., Reyes, M., and Van Leemput, K. (2015). The Multimodal Brain Tumor Image  
512 Segmentation Benchmark (BRATS). *IEEE Transactions on Medical Imaging*, 34(10):1993–2024.
- 513 Minaee, S., Kafieh, R., Sonka, M., Yazdani, S., and Jamalipour Soufi, G. (2020). Deep-COVID: Predicting  
514 COVID-19 from chest X-ray images using deep transfer learning. *Medical Image Analysis*, 65:101794.
- 515 Nayak, D. R., Padhy, N., Mallick, P. K., Zymbler, M., and Kumar, S. (2022). Brain tumor classification  
516 using dense efficient-net. *Axioms*, 11(1).
- 517 Pardal Souto, M. J., Hernández Marqués, C., Lassaletta Atienza, A., Ruano, D., Cormenzana, M., and  
518 Madero, L. (2015). Gliomas de bajo grado: revisión de 10 años. *Anales de Pediatría*, 82(2):68–74.
- 519 Pei, L., Vidyaratne, L., Rahman, M. M., and Iftekharuddin, K. M. (2020). Context aware deep learning  
520 for brain tumor segmentation, subtype classification, and survival prediction using radiology images.  
521 *Scientific Reports 2020 10:1*, 10(1):1–11.
- 522 Rahman, T., Akinbi, A., Chowdhury, M., Rashid, T., Şengür, A., Khandakar, A., Islam, K., and Ismael, A.  
523 (2022). COV-ECGNET: COVID-19 detection using ECG trace images with deep convolutional neural  
524 network. *Health Information Science And Systems*, 10(1).
- 525 Rastogi, D., Johri, P., and Tiwari, V. (2023). Brain tumor detection and localization: An inception v3  
526 - based classification followed by resnet-based segmentation approach. *International Journal of*  
527 *Mathematical, Engineering and Management Sciences*.
- 528 Roy, P. K. and Kumar, A. (2022). Early prediction of COVID-19 using ensemble of transfer learning.  
529 *Computers and Electrical Engineering*, 101:108018.
- 530 Shehab, L. H., Fahmy, O. M., Gasser, S. M., and El-Mahallawy, M. S. (2021). An efficient brain tumor  
531 image segmentation based on deep residual networks (resnets). *Journal of King Saud University -*  
532 *Engineering Sciences*, 33(6):404–412.
- 533 Simonyan, K. and Zisserman, A. (2014). Very deep convolutional networks for large-scale image  
534 recognition. *arXiv preprint arXiv:1409.1556*.
- 535 Society, A. C. (2022). Estadificación del cáncer.
- 536 Suter, Y., Jungo, A., Rebsamen, M., Knecht, U., Herrmann, E., Wiest, R., and Reyes, M. (2018). Deep  
537 Learning versus Classical Regression for Brain Tumor Patient Survival Prediction. *Lecture Notes in*  
538 *Computer Science (including subseries Lecture Notes in Artificial Intelligence and Lecture Notes in*  
539 *Bioinformatics)*, 11384 LNCS:429–440.
- 540 Szegedy, C., Ioffe, S., and Vanhoucke, V. (2016a). Inception-v4, inception-resnet and the impact of  
541 residual connections on learning. *CoRR*, abs/1602.07261.
- 542 Szegedy, C., Vanhoucke, V., Ioffe, S., Shlens, J., and Wojna, Z. (2016b). Rethinking the inception  
543 architecture for computer vision. In *Proceedings of the IEEE conference on computer vision and*  
544 *pattern recognition*, pages 2818–2826.
- 545 Taher, F., Shoaib, M. R., Emar, H. M., Abdelwahab, K. M., Abd El-Samie, F. E., and Haweel, M. T.  
546 (2022). Efficient framework for brain tumor detection using different deep learning techniques. *Frontiers*  
547 *in Public Health*, 10:959667.
- 548 Tan, M. and Le, Q. V. (2019). Efficientnet: Rethinking model scaling for convolutional neural networks.  
549 *CoRR*, abs/1905.11946.
- 550 Tripathy, S., Singh, R., and Ray, M. (2023). Automation of brain tumor identification using efficientnet  
551 on magnetic resonance images. *Procedia Computer Science*, 218:1551–1560. International Conference  
552 on Machine Learning and Data Engineering.
- 553 Wang, S. Y., Tseng, B., and Hernandez-Boussard, T. (2022). Deep Learning Approaches for Predicting  
554 Glaucoma Progression Using Electronic Health Records and Natural Language Processing. *Ophthalmology*  
555 *Science*, 2(2):100127.
- 556 Wankhede, D. S. and Selvarani, R. (2022). Dynamic architecture based deep learning approach for  
557 glioblastoma brain tumor survival prediction. *Neuroscience Informatics*, 2(4):100062.
- 558 Younis, A., Qiang, L., Nyatega, C. O., Adamu, M. J., and Kawuwa, H. B. (2022). Brain tumor analysis  
559 using deep learning and vgg-16 ensembling learning approaches. *Applied Sciences*, 12(14).
- 560 Zhu, Z., Lu, S., Wang, S.-H., Gorriz, J. M., and Zhang, Y.-D. (2022). Dsnn: A densenet-based snn for

- 561 explainable brain disease classification. *Frontiers in Systems Neuroscience*, 16.
- 562 Özkaraca, O., Bağrıaçık, O., Gürüler, H., Khan, F., Hussain, J., Khan, J., and Laila, U. (2023). Multiple
- 563 brain tumor classification with dense cnn architecture using brain mri images. *Life (Basel)*, 13(2):349.