Assessment of methods used for 3-dimensional superimposition of craniofacial skeletal structures: A systematic review

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Background. So far, several techniques have been recommended for the assessment of craniofacial changes through skeletal tissue superimposition, but the evidence that supports them remains unexplored. The purpose of the present study is to assess the available literature on skeletal-tissue superimpositions of serial craniofacial CT or CBCT images used to detect morphological changes. **Materials and methods.** Medline (via Pubmed), EMBASE, Google Scholar, Cochrane Library, Open Grey and Grey Literature Report were searched (last search: 17.11.2019) using specific terms that fulfilled the requirements of each database in the context of the study aim. Hand searches were also performed. The outcomes of interest were the accuracy, precision, or agreement between skeletal-tissue superimposition techniques to assess changes in the morphology of craniofacial structures. Studies of any design with sample size ≥ 3 were assessed by two authors independently. The study protocol was registered in PROSPERO (ID: CRD42019143356). **Results.** Out of 832 studies, fifteen met the eligibility criteria. From the 15 included studies, 12 have shown high total risk of bias, one low risk of bias, and 2 studies have shown unclear risk of bias. Thirteen out of the 15 studies showed high applicability concerns, 2 unclear and no study had low applicability concerns. There was high heterogeneity among studies regarding the type of participants, sample size, growth status, machines, acquisition parameters, superimposition techniques, assessment techniques and outcomes measured. Fourteen of them were performed on Cone Beam Computed Tomography (CBCT) and one on Computed Tomography (CT) derived 3D models. Most of the studies (eleven) used voxel-based registration, one landmark-based registration and three studies compared different registration techniques, which include the surface-based registration. Concerning the area of interest, nine studies focused on the anterior cranial base and certain facial structures, four on maxillary structures and four on mandibular structures. Non-growing participants were included in six studies, growing in eight, whereas one study had both. **Conclusion.** Most of the available studies had

methodological shortcomings and high applicability concerns. At the moment, certain voxel-based and surface-based superimpositions seem to work properly and to be superior to landmark-based superimposition. However, further research in the field is required to develop and properly validate these techniques on different samples, through high quality studies with low applicability concerns.

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2 **skeletal structures: a systematic review**

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14 **ABSTRACT**

15 **Background.** So far, several techniques have been recommended for the assessment of

16 craniofacial changes through skeletal tissue superimposition, but the evidence that supports them

17 remains unexplored. The purpose of the present study is to assess the available literature on

18 skeletal-tissue superimpositions of serial craniofacial CT or CBCT images used to detect

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23 searches were also performed. The outcomes of interest were the accuracy, precision, or

24 agreement between skeletal-tissue superimposition techniques to assess changes in the

25 morphology of craniofacial structures. Studies of any design with sample size ≥ 3 were assessed

26 by two authors independently. The study protocol was registered in PROSPERO (ID:

27 CRD42019143356).

28 **Results.** Out of 832 studies, fifteen met the eligibility criteria. From the 15 included studies, 12

29 have shown high total risk of bias, one low risk of bias, and 2 studies have shown unclear risk of

30 bias. Thirteen out of the 15 studies showed high applicability concerns, 2 unclear and no study

31 had low applicability concerns. There was high heterogeneity among studies regarding the type

32 of participants, sample size, growth status, machines, acquisition parameters, superimposition

33 techniques, assessment techniques and outcomes measured.

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42 applicability concerns. At the moment, certain voxel-based and surface-based superimpositions

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45   samples, through high quality studies with low applicability concerns.

INTRODUCTION

47 Superimpositions of serial craniofacial images have been widely applied in dental or other fields

48 as a mean to depict changes over time. It is a valuable tool facilitating the better understanding of

49 the effects of treatment or growth on dental and craniofacial morphology. The "structural

50 method" developed by Björk (Björk, 1969; Björk & Skieller, 1977) is still considered today as

51 the standard 2D superimposition technique for craniofacial radiographs. This is based on

52 reference structures that are considered stable, allowing the visual inspection of craniofacial

53 changes relative to these stable structures. Such 2D methods were adopted and modified to be

54 applicable in 3D data, since the same principles for reference area selection apply to both 2D and

55 3D approaches.

56 There are several advantages of the 3D over the 2D imaging techniques including the more

57 accurate, real size information in all dimensions of space. Furthermore, the 3D information is not

58 highly dependent on head positioning, which might be a critical source of error in 2D imaging.

59 However, the higher amount and quality of 3D information does not come without a cost. This

60 has to do mainly with the increased radiation dose needed to obtain the 3D images. Moreover,

61 the data acquisition, handling, and processing of 3D data is usually more complex, time

62 consuming, and expensive.

63 In growing individuals, the identification of stable superimposition reference areas might be

64 more difficult, since the morphology of most craniofacial structures changes considerably over

65 time. Thus, changes in the reference areas might affect the superimposition outcomes on the

66 areas of interest, due to the icomplete matching of the first. For this reason, similar to the

67 registration in 2D, the anterior cranial base still holds its position as the gold standard reference

68 area, since its growth is more or less completed around the age of seven (Buschang et al., 1986;

69 Afrand et al., 2014). To include this part of the head in the 3D images requires a larger field of

70 view, and thus, larger dose of radiation. Furthermore, structures that are more vulnerable to

71 radiation exposure, such as the eyes or certain brain structures, are included. Due to this fact,

72 researchers have explored other possibilities, to substitute the anterior cranial base as a

73 superimposition reference, which can be applied in smaller field of view scans and still perform

74 properly (Nada et al., 2011; Gkantidis et al., 2015).

75 Following the development of such methods and due to the technological advancements, that can

76 lead to 3D image acquisition with small radiation exposure, in the foreseeable future, large

77   amount of reliable 3D data could be generated. This could facilitate the valid prediction of

78   morphological changes that will occur in a specific patient after a certain treatment or growth

79   occurrence, leading to individualised, less invasive and more efficient treatment strategies in the

80   future.

81   Since the first application of 3D superimposition, three main techniques have been used for serial

82   image registration: namely landmark-based, surface-based, and voxel-based techniques (Grauer,

83   Cevidanes & Proffit, 2009; Cevidanes et al., 2010; Almeida et al., 2011; AlHadidi et al., 2011).

84   Each technique has been widely used for clinical and research purposes and has inherent

85   limitations, advantages, and disadvantages. Furthermore, all techniques have been suggested in

86   the literature to work properly.

87   Various relevant studies have been published so far, but the heterogeneity of the protocols,

88   machines, acquisition parameters, and superimposition references did not allow for the

89   development of solid conclusions (Ponce-Garcia et al., 2018). The only existing systematic

90   evaluation of the literature included studies that were published prior to 2017 and regarded only

91   the anterior cranial base (Ponce-Garcia et al., 2018). Thus, neither the accuracy, the precision,

92   and the reproducibility of hard-tissue superimposition techniques nor the choice of reference

93   structures have been thoroughly investigated recently. Hence, the purpose of this review is to

94   provide a synopsis and a thorough assessment of the current evidence, aiming to provide

95   guidelines for the proper use of the techniques and interpretation of the outcomes and identify

96   areas where further research is needed.

97   **MATERIALS AND METHODS**

98   **Protocol and registration**

99   The protocol was registered in PROSPERO prior to the study implementation (ID:

100   CRD42019143356). This protocol consists a modification of a previously published protocol by

101   Stucki & Gkantidis (2019) for an analogous, but completely different topic.

102   **Search strategy**

103   The following databases were searched for eligible studies: Medline (via Pubmed), EMBASE,

104   Google Scholar, Cochrane Library, OpenGrey and GreyLiteratureReport. The last search was

105   performed on 17.11.2019, without time restriction. Unpublished literature was searched through

106   the National Research Register, Pro-Quest Dissertation Abstracts and Thesis database, additional

107   hand searches of all relevant studies were also performed. The specific search strategies applied

108   for each database are provided as supplementary information (Appendix 1).

109   Selection criteria applied for the review

110   • Study design: Any study design, including prospective, and retrospective studies of any type.

111   • Study sample: Studies with sample size ≥ 3.

112   • Index test: 3D skeletal-tissue superimposition techniques to assess any change in the

113   morphology of the craniofacial complex.

114   • Types of participants: Serial craniofacial CT or CBCT images of individuals or skulls who have

115   received any kind of actual or simulated treatment, or whose craniofacial morphology is

116   expected to be altered due to growth or pathology.

117   • Type of intervention: 3D skeletal-tissue superimposition to assess any morphological change in

118   the craniofacial complex.

119   • Primary outcome: Superimposition accuracy or precision of a technique, or agreement between

120   techniques measured in terms of angles or distances between specific skeletal or facial landmarks

121   or area distances between corresponding models. Volume differences measured following 3D

122   superimposition were also considered. Studies that evaluated any of the above parameters as a

123   secondary outcome were also included.

124   • Comparator/control group: Studies that compared different superimposition techniques, direct

125   measurements, or repeated measurements were selected.

126   • Unit of analysis: The measured distance, angle, or volume.

127   • Follow-up: Any observation period between subsequent models.

128   • Exclusion criteria: None.

129   Study selection

130   Following the search strategy, the selected databases were screened by two authors of the review

131   (Daniel Dinh-Phuc Mai and Sven Stucki). There was no blinding concerning the authors' names

132   and affiliations, or the outcomes of the included studies. Titles and abstracts were evaluated first,

133   if necessary the full text was read to evaluate the eligibility. The same authors read all eligible

134   studies again in full text, independently, whereas non-eligible studies were excluded. Thereafter

135   the eligibility was discussed between all team members until a consensus was reached, under the

136   guidance of the last author (Nikolaos Gkantidis). A record of all decisions made during this

137   process was retained.

138   **Data extraction**

139   The first and the last author performed data extraction independently and in duplicate, aiming to

140   extract from the eligible studies the following information:

141   • Methods: Author, title, year, objectives, and design of study.

142   • Participants: Patient number, age, and gender.

143   • Materials: 3D model acquisition method and time between serial models.

144   • Superimposition method: Type of superimposition reference areas or points and software with

145   specific settings used.

146   • Comparison/control group: Type and characteristics.

147   • Outcome: Type of outcome(s) and method of outcome assessment.

148   If necessary, the authors were contacted by email to request missing data. If the relevant

149   information was not provided, only the available information was used.

150   **Assessment of heterogeneity**

151   Study characteristics, similarity between types of participants, compared methods and assessed

152   outcomes were considered to define heterogeneity among studies.

153   **Assessment of reporting bias**

154   We conducted an accurate, but also broad enough search of multiple sources, including on-going

155   studies, to minimize potential reporting biases, such as publication bias and duplicate reports.

156   **Data synthesis**

157   A meta-analysis will be performed if there are at least two studies graded with an unclear or a

158   low risk of bias and additionally use similar methods or report the same outcomes measured on

159   similar data.

160   **Subgroup analysis**

161   Results will also be tested for the following factors, if possible:

162   • CBCT vs. CT data.

163   • Growing vs. non-growing patients.

164 • Short-term (within 1 year) vs. medium/long-term (> 1 year) interval between serial models.

165 • Superimposition on the anterior cranial base vs. superimposition on maxillary structures vs.

166 superimposition on mandibular structures

Quality assessment

168 The quality of the selected studies was evaluated using the QUADAS-2 tool (Whiting, 2011).

169 This is a widely used tool to evaluate the diagnostic accuracy of methods in systematic reviews.

170 Using the QUADAS-2 tool the patient selection, the index test, the reference standard and the

171 flow and timing are evaluated regarding their risk of bias and applicability concerns. Usually,

172 gradings are shown in a table using happy (low risk) or sad smiles (high risk). In case an

173 evaluation is not possible, e.g. because of missing data, an interrogation mark is shown (unclear

174 risk). The total risk of bias or applicability concerns of each study correspond to the worst rating

175 given in the individual items assessed each time.

176 The quality assessment of all studies was performed by two authors (Daniel Dinh-Phuc Mai and

177 Nikolaos Gkantidis) independently. If there was a disagreement, a consensus was reached

178 through discussion among all authors. Studies graded with a high risk of bias were not to be

179 included in a meta-analysis.

180 **RESULTS**

181 **Description of studies**

182 The search results are shown in Figure 1. After searching various databases, 2'540 studies were

183 found. Seven additional studies were identified through hand searches. After removing the

184 duplicates, 832 studies remained. These studies were screened by reading the titles and abstracts.

185 Full-text reading of 24 studies was performed to evaluate the eligibility. Nine studies did not

186 match the review question and thus, they were excluded as irrelevant to the study topic.

187 Following the selection process 15 studies were included in this review.

188 All included studies used 3D skeletal-tissue superimposition techniques to assess morphological

189 changes in the craniofacial complex, the accuracy or precision of the applied processes, or the

190 agreement between different techniques as a primary outcome.

191 **Quality assessment**

192   The quality assessment of the included studies is provided in Table 1.

193   From the 15 included studies, 12 of these have shown a high total risk of bias, one a low risk of

194   bias, and 2 studies have shown an unclear risk of bias. Regarding the individual items 4 studies

195   have high, 7 low, and 4 unclear risk of bias in the patient selection. Regarding the index test, 8

196   studies have high, 6 low, and one unclear risk of bias. The reference standard of 9 studies shows

197   a high risk of bias, of 2 low, and of 4 unclear. The flow and timing of 2 studies has high, of 11

198   low, and of 2 unclear risk of bias.

199   Thirteen out of the 15 studies showed high total applicability concerns, 2 unclear and no study

200   had low applicability concerns. Concerning the individual items, 6 studies had high, 6 unclear

201   and 3 low applicability concerns in the patient selection. Regarding the index test, 9 studies had

202   high, one unclear and 5 low applicability concerns. The reference standard of 9 studies showed

203   high, of 3 unclear and of 3 low applicability concerns.

204   **Characteristics of the included studies**

205   One of the included studies utilized prospective radiographic image acquisition and 14 a

206   retrospective one. Regarding the superimposition data generation and method comparison all

207   studies were prospective. Eight studies included only growing patients, 6 only non-growing and

208   1 study both. None of the eligible studies was performed in patients with severe craniofacial

209   malformations, such as those related to systemic conditions, congenital anomalies, or syndromes.

210   Fourteen studies were performed on Cone Beam Computed Tomography (CBCT) and 1 on

211   Computed Tomography (CT) images. Eleven studies used voxel-based registration, 1 landmark-

212   based registration, and 3 compared different registration techniques. Concerning the area of

213   interest, 9 studies focused on the anterior cranial base and certain facial structures, 4 on

214   maxillary structures and 4 on mandibular structures.

215   The characteristics of the included studies are provided in detail in tables 2, 3, and 4.

216   **Results and Qualitative synthesis of the included studies**

217   The results of the included studies are shown in Table 4 and the conclusions and limitations in

218   Table 5.

219 There was high heterogeneity among studies regarding the type of participants, sample size,

220 growth status, machines, acquisition parameters, superimposition techniques, assessment

221 techniques and outcomes measured. Therefore, no quantitative synthesis was performed.

222 For the qualitative synthesis, the included studies are categorized in four groups based on the

223 registration technique assessed: 1. voxel-based registration, 2. landmark-registration and 3.

224 comparison of different registration techniques, which include the surface-based registration.

225 **Voxel-based registration**

226 Eleven studies tested the voxel-based registration. Six of those studies included only growing

227 patients, 4 only non-growing and one study included both. Nine studies of this subgroup had

228 high, and 2 unclear risk of bias. Similarly, 9 studies had high and 2 unclear applicability

229 concerns. Six studies used cranial base structures as superimposition reference, whereas 2 studies

230 used maxillary and 4 mandibular sites.

231 Bazina et al. (Bazina et al., 2018) superimposed CBCTs of 31 non-growing patients on the

232 anterior cranial base to evaluate the reproducibility of Dolphin voxel-based superimposition and

233 its agreement with ITK-Snap+3D Slicer superimposition. The Dolphin 3D software seemed to

234 work properly, but the study showed important limitations, high risk of bias, and high

235 applicability concerns.

236 Cevidanes et al. (Cevidanes et al., 2005) tested the reproducibility of 3D cranial base

237 superimpositions for the evaluation of mandibular ramus changes in maxillary orthognathic

238 surgery patients. To verify reproducibility, changes from pre- to post-treatment were measured

239 on mandibular areas of 10 non-growing patients. The surgery was performed exclusively on the

240 maxilla and the assessments on the mandible. Hence, no or minimal changes are expected in the

241 mandible. Under these circumstances, the technique showed acceptable reproducibility, though

242 in certain cases the inter-observer variation was relatively high, compared to the limited original

243 changes. The study had unclear risk of bias and applicability concerns.

244 In another study, Cevidanes et al. (Cevidanes et al., 2009) performed 3D superimpositions on the

245 anterior cranial base to investigate the reproducibility of the technique for the evaluation of

246 overall facial changes in three growing patients. Nine regions distributed on the whole face were

247 assessed by three operators. Detailed results acquired by each operator were not reported and

248 only the ranges were provided. Within this limitation, this method seemed reproducible in

249 growing patients. However, as the sample size was quite small and did not allow statistical

250 comparisons, no rigid conclusion can be made. This study showed high risk of bias and

251 applicability concerns.

252 Häner et al. (Häner et al., 2020) evaluated the trueness, reproducibility, and segmentation effect

253 on hard tissue outcomes using the Dolphin voxel-based superimposition. Fifteen growing

254 patients were included, and the superimposition was performed on the anterior cranial base. The

255 trueness of the voxel-based superimposition was assessed through visual inspection of

256 corresponding reference structures, and the intra and inter-operator reproducibility was assessed

257 through repeatedly superimposed 3D models. The superimposition technique exhibited adequate

258 performance in growing patients, in terms of efficiency, cranial base matching, and

259 reproducibility. The segmentation error was also acceptable in most cases. However, due to

260 certain limitations the study showed unclear risk of bias and applicability concerns.

261 Koerich et al. (Koerich et al., 2016) investigated the precision and the reproducibility of one

262 superimposition method in the maxilla and one in the mandible. As superimposition references

263 for the maxilla, they used two areas (zygomatic process; palate) and for the mandible three areas

264 (symphysis; corpus; part ramus). The sample for this study included two dry skulls and 15 non-

265 growing patients. Different machines and acquisition parameters were used in the dry skulls and

266 the actual patients. This technique has shown excellent precision and reproducibility, although

267 the evaluated regions are considered relatively unaltered. Surprisingly, the distances obtained

268 from the superimposition of the two dry skulls were higher than expected and than those

269 acquired from the superimposition of actual serial scans. This study had high risk of bias and

270 high applicability concerns.

271 Koerich et al. (Koerich et al., 2017) also assessed the precision and reproducibility of a 3D

272 mandibular voxel-based superimposition in 24 growing patients. To test the performance of this

273 technique, distances between serial models at five mandibular regions located at the outer surface

274 of the mandible were measured. Although the assessed structures were originally relatively

275 unaltered the inter-observer variation was larger than expected. Thus, this mandibular technique

276 showed moderate precision and reproducibility in the assessment of relatively unaltered

277 structures. The study had high risk of bias and high applicability concerns.

278 Nada et al. (Nada et al., 2011) evaluated the accuracy and reproducibility of a voxel-based

279 registration of CBCT models on two different regions: the anterior cranial base and the

280   zygomatic arches. Data were collected from 16 non-growing patients. Changes were measured

281   afterwards on four anatomical regions, which were deemed stable: the anterior cranial base, the

282   forehead, the left zygomatic arch, and the right zygomatic arch. The accuracy and reproducibility

283   of this technique seems to be high, although the original changes measured were small. The

284   superimposition on the left zygomatic arch appears to be a valid alternative to that on the anterior

285   cranial base in non-growing patients. The added advantage is that it can be used in images with

286   smaller field of view, and thus, lower radiation. However, individual changes were not reported

287   and only mean values were assessed. The study had high risk of bias and applicability concerns.

288   Nguyen et al. (Nguyen et al., 2018) searched for stable anatomical regions in the mandible by

289   superimposing CBCTs of growing patients on bony plates and miniscrews. They concluded that

290   the chin and symphysis region might be anatomically stable, whereas the third molar region

291   displayed a higher instability. However, among other limitations, the bone plates and screws

292   were confirmed to be immobile clinically, but their stability in space was not tested. The study

293   had high risk of bias and high applicability concerns.

294   Ruellas et al. (Ruellas et al., 2016a) aimed to identify stable maxillary superimposition

295   references for growing patients. The precision and reproducibility of two different maxillary

296   regions were tested on a sample of 16 patients. To quantify changes distances between

297   corresponding landmarks at pre- and post-treatment models after registration were assessed.

298   However, the absence of comparative statistics and the evaluation of average effects of different

299   variables did not allow for a clear conclusion. The study had high risk of bias and high

300   applicability concerns.

301   Ruellas et al. (Ruellas et al., 2016b) evaluated three reference regions for mandibular

302   superimposition using a sample of 16 growing patients. Following superimposition of the serial

303   scans and analysis of the distances between corresponding landmarks, the body of the mandible

304   seemed to show better agreement with direct measurements from a point considered stable, when

305   compared to the modified Björk technique. The performance of the Björk technique was not

306   reported in the study, due to software performance issues. The reporting of the results was poor,

307   since the presented mean values were outside of the provided limits of agreement. The study had

308   high risk of bias and high applicability concerns.

309   Weissheimer et al. (Weissheimer et al., 2015) also performed voxel-based superimposition on

310   the anterior cranial base in serial 3D CBCT models of growing and non-growing patients. The

311   assessment of the accuracy was done through visual inspection of the congruence of the anterior

312   cranial base between serial models using colour coded distance maps. Through this, it was

313   established that the highest distance was less than 0.5 mm. Thus, it seemed that the software

314   works properly and the anterior cranial base is a stable superimposition reference in both

315   growing and non-growing patients. However, the study has no descriptive or comparative

316   statistics. Merely data from two patients were shown. Thus, the study has shown high risk of bias

317   and applicability concerns.

318   **Landmark-based registration**

319   Lemieux et al. (Lemieux et al., 2014) evaluated the trueness of a maxillary superimposition plane

320   using the nasomaxillary complex as reference. CBCTs of 30 growing patients were

321   superimposed on a maxillary superimposition plane formed by the nasion, the bilateral

322   infraorbital foramina and the incisive foramen. However, the performance of this landmark-

323   derived maxillary plane cannot be assessed through the present methodology. The study is

324   graded with high risk of bias and high applicability concerns.

325   **Comparison of different registration techniques**

326   Since now, a single study compared the accuracy of voxel-based registration and surface-based

327   registration for the 3D assessment of surgical change following orthognathic surgery (Almukhtar

328   et al., 2014). The sample included only non-growing patients. The surface-based registration on

329   hard tissues was performed on the anterior cranial base; as for the registration on soft tissues, the

330   forehead and the eyes were selected. Regarding the voxel-based registration, the structures

331   described above were chosen, but in this case hard and soft tissues were used simultaneously as

332   superimposition references. The assessment of accuracy in this study was tested via

333   measurements on the anterior cranial base for the hard tissues and on the forehead for the soft

334   tissues. The mean absolute distances of surface models in hard tissues did not differed much

335   between the voxel and the surface-based registrations, but this was not the case for the soft

336   tissues. This can be attributed to the differences in the superimposition references used each

337   time. The study showed high risk of bias and applicability concerns.

338   Gkantidis et al. (Gkantidis et al., 2015) investigated the accuracy, precision, and reproducibility

339   of four surface-based and one landmark-based 3D superimposition technique. Pre-existing CT

340   data from eight non-growing patients were analysed by three operators. To confirm the accuracy

341   of each technique, the congruence of serial models was measured in three areas that were

342   considered stable. For precision testing, the distances between four corresponding landmarks

343   were quantified. The whole procedure was repeated to test reproducibility. The superimposition

344   on the anterior cranial base showed acceptable outcomes that were comparable with the

345   superimposition on both zygomatic arches. The study concluded that the superimposition of 3D

346   surface models created from voxel data can provide accurate, precise, and reproducible results

347   when appropriate references are used. Since this study used CT data, a similar study on CBCT

348   data of non-growing patients would be required to confirm these findings. Therefore, this study

349   had low risk of bias, but high applicability concerns.

350   Ghoneima et al. (Ghoneima et al., 2017) evaluated the reproducibility of landmark-based,

351   surface-based, and voxel-based superimpositions, as well as their performance in matching

352   duplicated scans. They superimposed CBCTs of 20 growing patients. The superimposition area

353   for the landmark-based method was defined on seven homologous points on the frontal and

354   zygomatic bones, for the surface-based method on the anterior cranial base, as well as for the

355   voxel-based method. Regarding the results, the surface-based and voxel-based superimpositions

356   seemed to be reproducible, whereas the landmark-based superimposition was less reproducible.

357   Based on certain limitations the study was graded to have high risk of bias and applicability

358   concerns.

359   **DISCUSSION**

360   Due to the inherent limitations of 2D superimposition methods various scientific fields have

361   turned their focus to the more thorough and accurate 3D imaging techniques, and worked to

362   create more reliable, faster, and easy to handle software facilitating this purpose. This allowed

363   researchers and clinicians to work with real size and shape 3D representations of anatomical

364   structures. However, till today there is no single method that has been proved to be accurate,

365   easy to use, and is widely accepted for superimposing 3D craniofacial radiographic images. This

366   review performed a thorough, critical assessment of the recent literature and analysed 15

367   identified studies that tested one or more of the three available superimposition techniques for

368   this; namely, the voxel-based, the landmark-based, and the surface-based technique. Overall, the

369   study detected high heterogeneity and moderate study quality, emphasizing the urgent need for

370   further relevant research in this rapidly expanding field.

371 The single previous systematic evaluation of the literature included six studies that were all

372 published prior to 2017 and regarded only the anterior cranial base (Ponce-Garcia et al., 2018).

373 In our review, we performed a more thorough selection process including all relevant studies for

374 the whole craniofacial area and we managed to include 15 studies, though still the vast majority

375 of these focuses on the anterior cranial base area.

376 For clarity reasons we divided the included studies in the following three major categories, based

377 on the type of superimposition tested: landmark-based registration, voxel-based registration, and

378 comparison of different registration techniques, which includes the surface-based registration.

379 Landmark-based superimposition is relatively simple to use and understand, but small errors in

380 the identification of landmarks may have a large negative impact on the results. This is especially

381 true if a limited number of landmarks is used, but only then the method is simple and easy

382 (Gkantidis et al., 2015; Becker et al., 2018). Only one study investigated exclusively a landmark-

383 based superimposition technique (Lemieux et al., 2014). This was graded as high risk of bias and

384 applicability concerns. Two further studies (Gkantidis et al., 2015; Ghoneima et al., 2017) that

385 compared the landmark-based superimposition to other superimposition techniques (voxel- or

386 surface-based) concluded that the landmark-based superimposition was inferior to the others.

387 Overall, there is a lack of well-designed studies to support the use of landmark-based

388 superimposition. The existing weak evidence indicates that this technique might be unreliable,

389 especially when few landmarks are used as superimposition reference. Thus, the use of

390 landmark-based superimposition remains questionable.

391 Most of the included studies (11/15) investigated a voxel-based superimposition technique

392 (Cevidanes et al., 2005, 2009; Nada et al., 2011; Weissheimer et al., 2015; Ruellas et al.,

393 2016a,b; Koerich et al., 2016, 2017; Bazina et al., 2018; Nguyen et al., 2018; Häner et al., 2020).

394 This type of superimposition utilizes the original volume generated from a 3D radiographic scan

395 and no further data processing is required prior to the superimposition. That might also be a

396 reason why most studies focused on this type of superimposition. Most of the studies that

397 investigated a voxel-based superimposition technique (6) used cranial base structures as

398 superimposition reference, whereas two studies used maxillary and four mandibular sites. Thus,

399 the cranial base is the most widely tested and supported reference for voxel-based

400 superimposition, but until now the quality of evidence for this ranges from low to moderate.

401 More work needs also to be performed to find alternative reference areas that might be

402   applicable is smaller field of view scans, reducing the required radiation amount. So far, two

403   studies have investigated this issue (Nada et al., 2011; Gkantidis et al., 2015), but they both had

404   high applicability concerns. Regarding the maxillary and the mandibular areas the amount of

405   existing evidence is lower and of low quality. Overall, nine of the included studies in this

406   category had high risk of bias and high applicability concerns and two unclear. There is no study

407   graded with low risk of bias or low applicability concerns. Hence, there is an urgent need for

408   well-designed studies with low risk of bias and low applicability concerns to support the voxel-

409   based superimposition techniques.

410   There was no study that focused only on surface-based superimposition. Surface-based

411   registration compares the triangular representations of corresponding 3D surface geometries on

412   the models. This technique might show adequate accuracy, it is less sensitive and time-

413   consuming, and has increased post-processing capabilities (Gkantidis et al., 2015). Three studies

414   that compared different registration techniques (Almukhtar et al., 2014; Gkantidis et al., 2015;

415   Ghoneima et al., 2017) included a surface-based technique. Two of them had high risk of bias

416   and all of them had high applicability concerns. The study of Gkantidis et al. (Gkantidis et al.,

417   2015) showed low risk of bias, but high applicability concerns, and did not support the use of

418   landmark-based superimposition but showed acceptable results for surface-based

419   superimposition. Ghoneima et al. (Ghoneima et al., 2017) did not recommend the use of

420   landmark-based superimposition as well, but they showed promising results for voxel-based and

421   surface-based superimposition. Almukhtar et al. (Almukhtar et al., 2014) provided similar and

422   promising results for voxel-based and surface-based superimposition of hard-tissues. Thus, the

423   three above studies support the surface-based superimposition on the anterior cranial base

424   structures. Two of them also support the voxel-based superimposition (Almukhtar et al., 2014;

425   Ghoneima et al., 2017), whereas other two do not support the landmark-based superimposition

426   (Gkantidis et al., 2015; Ghoneima et al., 2017). However, the quality of evidence for the above

427   outcomes ranges from moderate to low.

428   Overall the literature supports the use of voxel-based and surface-based superimposition

429   techniques, though the existing evidence is not yet strong. Because of the limited amount of

430   well-designed studies, further research is needed to confirm the present findings. It seems that

431   these techniques show better accuracy and are less operator-sensitive compared to the landmark-

432   based superimposition. A limitation of the surface-based registration is the lack of information

433 concerning inner structures as only the surface information is available after processing.

434 Furthermore, an additional step is required to segment the surface model of interest from the

435 original 3D volume and this might induce error (Häner et al., 2020). The voxel-based registration

436 is applied to the original volumetric data derived from a 3D radiographic scan, and thus, this

437 might be advantageous in terms of less error prone steps required to achieve model registration.

438 However, after the registration of serial volumes, surface models are usually required for

439 thorough assessment and visualization of the results. Thus, this possible source of error is not

440 fully eliminated also through this method. Furthermore, the surface models are widely used in

441 various other scientific disciplines and in the industry, leading to well-developed methods and

442 software applications for data processing and evaluation. Thus, the acquisition of accurate

443 surface models from the original volume is quite important to take advantage of these

444 possibilities for data processing and visualisation and will also facilitate accurate surface model

445 superimposition techniques (Henninger et al., 2019).

446 Though a significant amount of studies was identified, a limitation of the present study is that the

447 heterogeneity of the included studies is high, and the quality of the available evidence is limited.

448 This can be attributed to the fact that the field has been developed in the last few years and

449 gained much attention only recently.

450 **CONCLUSION**

451 The fast evolution of 3D superimposition techniques has provided a key element in the toolkit of

452 relevant fields to evaluate craniofacial changes following growth or treatment. Due the high

453 heterogeneity and the moderate to low quality of the included studies, few valid conclusions can

454 be drawn. Most of the available studies had methodological shortcomings and high applicability

455 concerns. Therefore, no clear recommendation could be given at present for proper methods used

456 for 3D-superimposition of craniofacial skeletal structures. At the moment, certain voxel-based

457 and surface-based superimpositions seem to work properly and to be superior compared to

458 landmark-based superimposition. However, further research is necessary to develop and properly

459 validate these techniques on different samples, through studies with high quality and low

460 applicability concerns.

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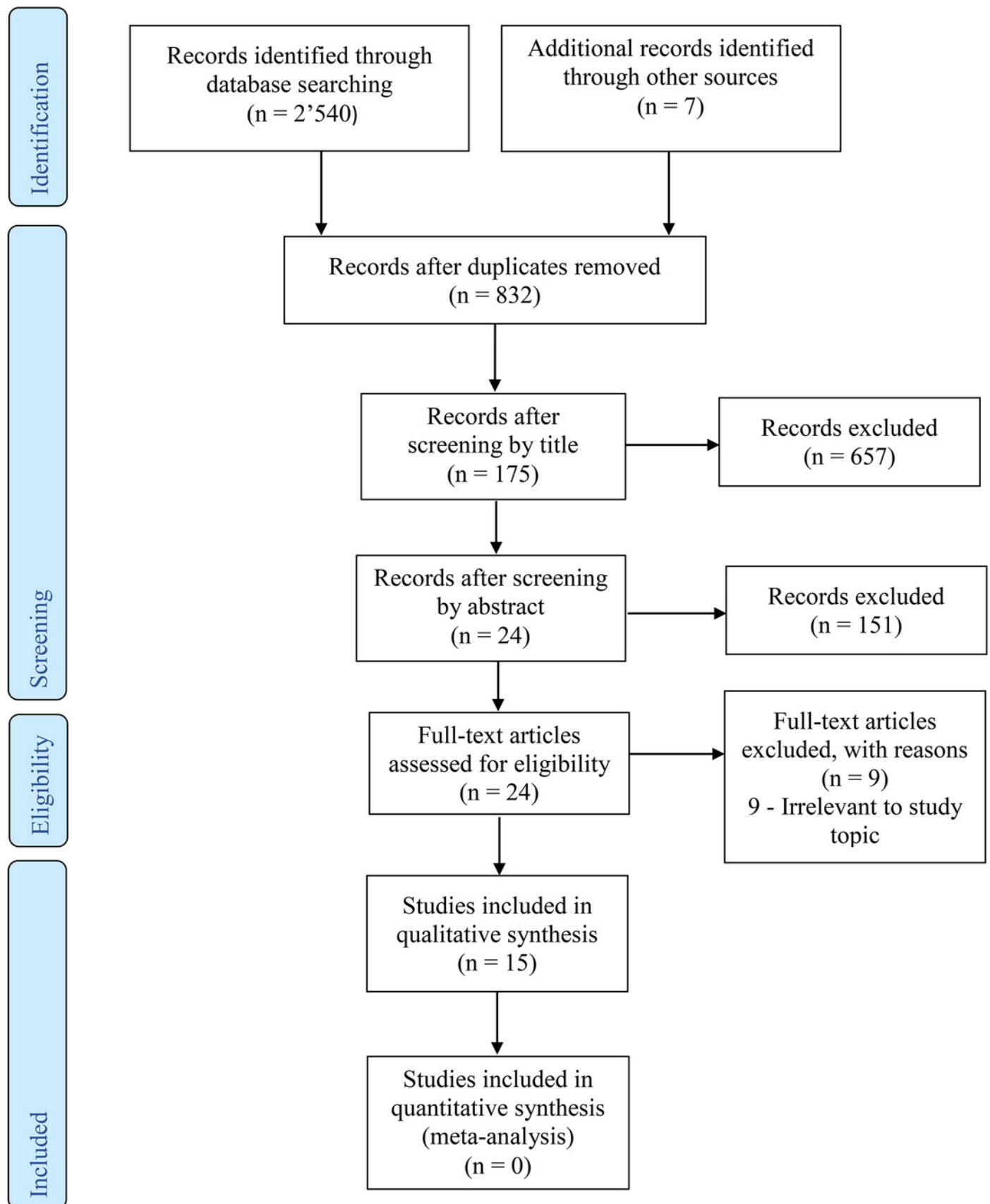
Figure 1

Happy face = low risk of bias/low applicability concerns; Sad face = high risk of bias/high applicability concerns; ? = unclear risk of bias/unclear applicability concerns

1 **Table 1** Quality assessment of the included studies through the QUADAS-2 tool.

Study	Risk of Bias					Applicability Concerns			
	Patient Selection	Index Test	Reference Standards	Flow & Timing	Total Risk of Bias	Patient Selection	Index Test	Reference Standards	Total Applicability Concerns
Almukhtar et al., PLoS One (2014)	☺	☺	☹	☺	☹	☺	☹	☹	☹
Bazina et al., Am J Orthod Dentofacial Orthop (2018)	☺	☹	☹	☺	☹	☺	☹	☹	☹
Cevidanes et al., Dentomaxillofac Radiol (2005)	?	☺	☺	☺	?	?	☺	☺	?
Cevidanes et al., Am J Orthod Dentofacial Orthop (2009)	☹	☺	?	☺	☹	☹	☺	?	☹
Gkantidis et al., PLoS One (2015	☺	☺	☺	☺	☺	☹	☺	☺	☹
Ghoneima et al., Orthod Craniofac Res (2017)	☹	☹	☹	☹	☹	?	☹	☹	☹
Häner et al., Orthod Craniofac Res (2019)	?	?	?	☺	?	?	?	?	?
Koerich et al., Int J Oral Maxillofac Surg (2016)	☺	☺	☹	☺	☹	☹	☺	☹	☹
Koerich et al., Angle Orthod (2017)	?	☺	☹	?	☹	☹	☺	☹	☹
Lemieux et al., Am J Orthod Dentofacial Orthop (2014)	?	☹	☹	?	☹	?	☹	☹	☹
Nada et al., PLoS One (2011)	☺	☹	?	☺	☹	?	☹	☺	☹
Nguyen et al., Am J Orthod Dentofacial Orthop (2017)	☹	☹	☹	☺	☹	☹	☹	☹	☹
Ruellas et al., Am J Orthod Dentofacial Orthop (2016a)	☺	☹	☹	☹	☹	☺	☹	☹	☹
Ruellas et al., PLoS One (2016b)	☺	☹	☹	☹	☹	?	☹	☹	☹
Weissheimer et al., Int J Oral Maxillofac Surg (2015)	☹	☹	?	☺	☹	☹	☹	?	☹

2 ☺ = low risk of bias/low applicability concerns; ☹ = high risk of bias/high applicability concerns; ? = unclear risk of bias/unclear applicability concerns

1   **Table 2** Main general characteristics of the included studies.

Study	Study objectives	Study design	Type of participants	Sample size	Growth status	Time span
Almukhtar et al., PLoS One (2014)	To compare the trueness of voxel-based registration and surface-based registration for 3D assessment of surgical change following orthognathic surgery.	Retrospective (radiographs) // prospective methodological study	pre- & post-orthognatic surgery CBCTs	31 Patients	Non-growing	min. 6 months
Bazina et al., Am J Orthod Dentofacial Orthop (2018)	To evaluate the reproducibility of Dolphin voxel-based superimposition and its agreement with ITK-Snap+3D Slicer superimposition.	Retrospective (Scans) // prospective methodological study	Pre- and post-1-jaw or 2-jaw orthognatic surgery including LeFort I osteotomy, bilateral sagittal split osteotomy, or genioplasty CBCTs	31 Patients	Non-growing (21 ± 8 years, range: 15-47 years)	13 months (within 1 month prior surgery and 12 months after surgery)
Cevidanes et al., Dentomaxillofac Radiol (2005)	To determine the reproducibility of voxel-based superimposition to evaluate mandibular ramus changes in maxillary orthognatic surgery patients.	Prospective methodological study	Pre- and post-orthognatic surgery CBCTs	10 Patients	Non-growing	1 week
Cevidanes et al., Am J Orthod Dentofacial Orthop (2009)	To determine the reproducibility of voxel-based superimpositions to evaluate overall facial changes in growing patients.	Retrospective (radiographs) // prospective methodological study	Pre- and post-orthopedic treatment of Class III malocclusion with miniplates CBCTs	3 Patients	Growing (mean age: 11.4 years)	1 year
Gkantidis et al., PLoS One (2015)	To test the applicability, trueness, precision, and reproducibility of various 3D superimposition techniques for radiographic data, transformed to triangulated surface data.	Retrospective (radiographs) // prospective methodological study	Pre- and post-rapid maxillary expansion CTs	8 Patients	Non-growing (median age: 16.2 years)	10-23 days
Ghoneima et al., Orthod Craniofac Res (2017)	To evaluate the reproducibility of landmark-based, surface-based and voxel-based superimpositions, as well as their performance in matching duplicated scans.	Retrospective (CBCT images) // prospective methodological study	Pre- and post-correction of Class II malocclusion with Herbst appliance CBCTs	20 Patients (9 males, 11 females)	Growing (range: 8-15 years)	NA
Häner et al., Orthod Craniofac Res (2019)	To evaluate the trueness, reproducibility and segmentation effect on hard tissue outcomes using voxel-based superimposition.	Retrospective (CBCT images) // prospective methodological study	Orthodontic patients without accounting for performed treatment or skeletal growth pattern CBCTs	15 Patients (8 males, 7 females)	Growing (11.75 ± 0.59 years)	1.69 ± 0.37 years
Koerich et al., Int J Oral Maxillofac Surg (2016)	To evaluate the reproducibility of a superimposition method for the maxilla and mandible in non-growing patients.	Retrospective (radiographs) // prospective methodological study	1. Two serial CBCT images of dry skulls after changing their position 2. Two serial CBCT images of orthodontic or wisdom tooth surgery patients	1. 2 Dry skulls 2. 15 Patients	Non-growing	12.3 months (range: 4-24 months)

3   **Table 2** Continued

Study	Study objectives	Study designs	Type of participants	Sample size	Growth	Time span
Koerich et al., Angle Orthod (2017)	To evaluate the reproducibility of a voxel-based superimposition of the mandible in growing patients.	Retrospective (scans) // prospective methodological study	Pre- and post-rapid palatal expansion CBCTs	24 Patients	Growing (mean age: 10.8 ± 1.7 years)	16 ± 2.9 months
Lemieux et al., Am J Orthod Dentofacial Orthop (2014)	To evaluate the trueness of a maxillary superimposition plane using the nasomaxillary complex as reference.	Retrospective (CBCT images) // prospective methodological study	Pre- and post-rapid palatal expansion CBCTs	30 Patients	Growing (dental age of 12)	within 12 months
Nada et al., PLoS One (2011)	To evaluate the trueness and reproducibility of a semi-automated voxel-based registration on two regions: 1. anterior cranial base and 2. zygomatic arches	Retrospective (radiographs) // prospective methodological study	Pre- and-post-orthognatic surgery CBCTs	16 Patients	Non-growing (mean age: 26 ± 9 years)	18 ± 4.6 months
Nguyen et al., Am J Orthod Dentofacial Orthop (2017)	1. To identify stable anatomical regions in the mandible. 2. To evaluate the reproducibility of the chin+symphysis registration.	Retrospective (CBCT images) // prospective methodological study	1. CBCTs of 20 Class III patients with bone plates and screws in the mandibular anterior area 2. Pre- and post-correction of Class II with Herbst appliances CBCTs (n = 10); Pre- and post-correction of Class II with elastics CBCTs (n = 10); Pre- and post-correction of Class III with bone anchors CBCTs (n = 5)	25 Patients	Growing (mean age: 12.7 ± 1.4 years)	1. 1.2 years 2.12.6 ± 0.9 months
Ruellas et al., Am J Orthod Dentofacial Orthop (2016a)	To evaluate the differences between voxel-based registration on 2 regions of the maxilla (1. Maxillary region and 2. Palate and Infrazygomatic region) and the reproducibility of each technique	Retrospective (radiographs) // prospective methodological study	Pre- and post-rapid maxillary expansion for crossbite correction (n = 8) and Pre- and post-correction of Class II malocclusion with Herbst appliance (n = 8)	16 Patients	Growing (9 - 13 years)	6 months
Ruellas et al., PLoS One (2016b)	To evaluate superimposition of serial mandibular models on 3 reference regions (Björk, modified Björk and mandibular body) as compared to directly measured changes in interlandmark distances.	Retrospective (radiographs) // prospective methodological study	NA	16 Patients	growing (9 - 13 years)	min. 18 months
Weissheimer et al., Int J Oral Maxillofac Surg (2015)	To evaluate the trueness of a voxel-based superimposition technique using the anterior cranial base as reference for growing and non-growing patients	Retrospective (radiographs) // prospective methodological study	1. Pre-treated images reoriented and superimposed on the original (n = 10) 2. Pre- and post-orthognatic surgery (n = 4) 3. Pre- and post-rapid palatal expansion (n = 4) Time span: 1 year	18 Patients	1. Growing (11.4 ± 1 year) 2. Non-growing (26.3 ± 5.7 years) 3. Growing (9.5 ± 1.8 years)	1 year

1   **Table 3** Main superimposition-related characteristics of the included studies.

Study	Superimposition methods	References	No of Operators	Machines	Acquisition parameters	Software
Almukhtar et al., PLoS One (2014)	Voxel-based registration (iterative best match of grey scale intensities) Surface-based registration (iterative closest point)	VBR: Anterior cranial base (extended to involve the frontal bone) and forehead region (including the forehead and the eyes) SBR: Anterior cranial base (for the hard tissue) and forehead region (for the soft tissue)	NA	CBCT: i-CAT Classic (Imaging Sciences, Hatfield, UK)	NA	Maxilim software (Medicim-Medical Image Computing, Belgium) for voxel-based registration (VBR). VRMesh software (VirtualGrid, Bellevue City, WA) for surface-based registration (SBR).
Bazina et al., Am J Orthod Dentofacial Orthop (2018)	Voxel-based Registration (approximation using 3 landmarks located at the right and left frontozygomatic sutures and the left mental foramen)	Voxel-based Registration (iterative best match of grey scale intensities)	1	CBCT: CB MercuRay scanner (Hitachi Medical Systems America Inc, Twinsburg, OH)	Tube voltage: 120 kVp; Tube current: 15 mA; FOV: 12-in; Grey scale 4096; Voxel size: 0.38 mm3; Exposure: 9.5 s	1. Dolphin 3D software (version 11.8.06.15 premium; Dolphin Imaging, Chatsworth, Calif) for the registration of T2 CBCT image to T1. 2. ITK-SNAP software program (version 3.0.0; http://www.itksnap.org) and 3D Slicer (version 4.4.0; http://www.slicer.org) for DICOM files conversion, segmentation of the area of cranial base and image registration.
Cevidanes et al., Dentomaxillofac Radiol (2005)	Voxel-based Registration (iterative best match of grey scale intensities)	Cranial base	3	CBCT: NewTom 9000 (Aperio Services LLC, Sarasota, FL, 34236)	FOV: 23x23 cm; Exposure: 70 s	MIRIT Software for the fully automated rigid registration. VALMET Software for the 3D models comparison.
Cevidanes et al., Am J Orthod Dentofacial Orthop (2009)	Voxel-based Registration (iterative best match of grey scale intensities)	Anterior cranial base	3	CBCT: iCat (Imaging Sciences International, Hatfield, PA)	FOV: 16x22 cm; Voxel size: 0.5 mm3; Exposure: 40 s	Imagine software (http://ia.unc.edu/dev/download/imagine/index.htm) for the rigid registration.
Gkantidis et al., PLoS One (2015	Surface-based registration (iterative closest point)	1. Three point registration (3P); 2. One zygomatic arch (1Z); 3. Both zygomatic arches (BZ); 4. Anterior cranial base (AC: body and small wing of the sphenoid bone and part of the bottom of the anterior cranial fossa); 5. Anterior cranial base + Foramen magnum (middle posterior part of the edge of the foramen magnum) (AC+F)	3	CT: Philipps Brillance 16 CT Scanner	Tube voltage: 120 kV; Tube current: 293 mA; FOV: 21x21x12 cm; Voxel size: 0.3mm3; Exposure: 2.5 s; Slice thickness: 0.8 mm; Spacing between slices: 0.4 mm; Spatial resolution: 16 lp/cm	Geomagic Qualify 2012 software for Windows (Geomagic GmbH, Stuttgart, Germany) for data conversion, model processing, registration, and 3D analysis.
Ghoneima et al., Orthod Craniofac Res (2017)	1. Landmark-based Registration 2. Surface-based Registration (iterative closest point) 3. Voxel-based Registration (iterative best match of grey scale intensities)	1. Seven homologous points on the frontal and zygomatic bones 2. Anterior cranial base surface 3. Anterior cranial base (anterior wall of frontal sinus anteriorly, the anterior clinoid process posteriorly, the superior wall of ethmoid sinus superiorly and the inferior floor of sphenoid sinus inferiorly)	NA	CBCT: iCAT 3D imaging System (Imaging Sciences International, Hatfield, PA, USA)	Tube voltage: 120 kV; Tube current: 20 mA; FOV: 17x23cm; Voxel size: 0.3 mm3; Exposure: 8.9 s	1 and 3: Dolphin software version 11.8 Premium (Dolphin Imaging and Management Solutions, Chatsworth, CA, USA) for the registration. 2: 3dMD Vultus software (3dMD, Atlanta, GA, USA) for the registration.

3   **Table 3** Continued

Study	Superimposition methods	References	No of Operators	Machines	Acquisition parameters	Software
Häner et al., Orthod Craniofac Res (2019)	Voxel-based Registration (iterative best match of grey scale intensities)	Anterior cranial base (from the middle of the sella turcica to the posterior wall of the sinus frontalis. The vertical height of the area is about 3.5 cm. The lower vertical limit was set 2-4 mm below the lowest point of the sella turcica. The lateral limits extend till the lateral walls of the cranium)	2	CBCT: KaVo3D eXam (Hatfield, PA 19440, USA)	Tube voltage: 120 kV; Tube current: 5 mA; FOV: 170 height mm x 232 mm; Voxel size: 0.4 mm3; Scan time: 8.9 s; Exposure: 3.7 s	Dolphin 3D software (version 2.1.6079.17633) for surface model creation and the voxel-based registration. Viewbox 4 software (version 4.1.0.1 BETA 64) for surface model processing and analysis.
Koerich et al., Int J Oral Maxillofac Surg (2016)	Voxel-based Registration (iterative best match of grey scale intensities)	Maxilla (zygomatic process and palate) and Mandible (Symphysis, corpus and part of ramus)	2	1. CBCT: Kodak Carestream 9300 (Carestream Health Inc., Rochester, NY, USA) 2. CBCT: i-CAT scanner (Imaging Sciences International LLC, Hatfield, PA, USA)	1. Tube voltage: 85 kVp; Tube current: 4 mA; FOV: 13.5x17 cm; Voxel size: 0.3mm3; Exposure: 11.3 s 2. Tube voltage: 120 kVp; Tube current: 8 mA; FOV: 16x13 cm; Voxel size: 0.25 mm3; Exposure: 27 s	OnDemand 3D software v1.0.10.5261 (Cybermed, Seoul, Korea) for image processing, segmentation and registration. VAM software (Canfield Scientific, Fairfield, NJ, USA) for analysis.
Koerich et al., Angle Orthod (2017)	Voxel-based Registration (iterative best match of grey scale intensities)	Lower mandibular border below to tooth apices, extending from the middle of the symphysis to the distal of the first molars	2	CBCT: i-CAT scanner (Imaging Sciences International, Hatfield, PA)	Tube voltage: 120 kVp; Tube current: 8 mA; Voxel size: 0.3 mm3; Exposure: 40 s	OnDemand 3D software v1.0.10.5261 (Cybermed, Seoul, Korea) for image processing, segmentation and registration. VAM software (Canfield Scientific, Fairfield, NJ, USA) for analysis.
Lemieux et al., Am J Orthod Dentofacial Orthop (2014)	Landmark-derived plane Registration	Maxillary superimposition plane formed by nasion, bilateral infraorbital foramina and incisive foramen	1	CBCT: NewTom 3G volumetric scanner (Aperio, Verona, Italy)	Tube voltage: 110 kV; Tube current: 6.19 mAs; Voxel size: 0.25 mm3; Thickness Aluminium filtre: 8 mm	MATLAB software (R2008a; MathWorks, Natick, Mass) for landmarks-based registration. Avizo software (version 6.0; Visualization Sciences Group, Burlington, Mass) for landmark location and analysis.
Nada et al., PLoS One (2011)	Voxel-based Registration (iterative best match of the grey scale intensities)	1. Anterior cranial base (AC) 2. Left zygomatic arch (ZL)	2	CBCT: i-CAT 3D Imaging System (Imaging Sciences International INC, Hatfield, PA, USA)	FOV: 22x16 cm; Voxel size: 0.4 mm3	Maxilim software (Medicim, Mechelen, Belgium) for 3D model construction, superimposition and analysis
Nguyen et al., Am J Orthod Dentofacial Orthop (2017)	Voxel-based Registration (iterative best match of grey scale intensities)	1. Bony plates and mini-screws in the mandibular anterior area 2. Chin (anterior surface of the chin bounded vertically from pogonion to B-point and laterally at the distal-incisal point of the right and left lateral incisors) + Symphysis (internal cortical bone of the mandibular symphysis at the lateral limit of its lingual surface and from its inferior border to the level of the center of both mental foramina)	2	CBCT: i-CAT machine (Imaging Sciences International, Hatfield, PA) CBCT: NewTom 3G (AFP Imaging, Elmsford, NY)	Tube voltage: 12 kV(p); Tube current: 5 mA; Voxel size: 0.3 mm3; Exposure: 20-25 s	ITK-SNAP software (version 3.6; open-source software, http://www.itksnap.org) for 3D mandibular models creation. Slicer CMF software (version 3.1; http://www.slicer.org) to create surface models and registration.

5   **Table 3** Continued

Study	Superimposition methods	References	No of Operators	Machines	Acquisition parameters	Software
Ruellas et al., Am J Orthod Dentofacial Orthop (2016a)	Voxel-based Registration (iterative best match of the grey scale intensities)	1. Maxillary region (maxillary bone clipped inferiorly at the dentoalveolar processes, superiorly at the plane passing through the right and left orbitale points, laterally at the zygomatic processes through the orbitale point, and posteriorly till the distal surface of the second molars) 2. Palate and Infrazygomatic region (same as above cropped posteriorly distal aspects to the first molars and anteriorly at the canines)	2	CBCT: i-Cat machine (Imaging Sciences International, Hatfield, PA)	FOV: 16x22 cm; Voxel size: 0.4 mm3	Slicer software (version 4.3.1; http://www.slicer.org) for the registration ITK-SNAP software (http://www.itksnap.org) for data conversion and 3D models construction. VECTRA Anaylsis Module software (version 3.7.6; Canfield Scientific, Fairfield, NJ) for landmark generation and analysis.
Ruellas et al., PLoS One (2016b)	Voxel-based Registration (iterative best match of grey scale intensities)	1. Maxillary region (maxillary bone clipped inferiorly at the dentoalveolar processes, superiorly at the plane passing through the right and left orbitale points, laterally at the zygomatic processes through the orbitale point, and posteriorly at a plane passing through the distal surface of the second molars) 2. Palate & infrazygomatic region (same as above cropped posteriorly at the plane passing through the distal aspects of the first molars and anteriorly at the canines)	NA	CBCT: NA	FOV: 16x22 cm; Voxel size: 0.4 mm3	Slicer software (v4.4; http://www.slicer.org) for data analysis and registration. ITK-SNAP software (http://www.itkspnap.org) for the segmentation.
Weissheimer et al., Int J Oral Maxillofac Surg (2015)	Voxel-based Registration (iterative best match of grey scale intensities)	Anterior cranial base	NA	CBCT: iCat (Imaging Sciences International, Hatfield, PA)	Tube voltage: 120 kVp; 8 mA; FOV: large; Voxel size: 0.25 mm3; Exposure: 40 s	OnDemand 3D software v1.0.10.5261 (Cybermed, Seoul, Korea) for the registration.

1   **Table 4** Results of the included studies.

Study	Main Outcomes	Secondary Outcomes	Main Results	Secondary Results
Almukhtar et al., PLoS One (2014)	Mean absolute distance of surface models in unchanged areas (anterior cranial base for hard tissue and forehead for soft tissue models): 1. VBR hard; 2. VBR soft; 3. SBR hard; 4. SBR soft	Correlation between VBR and SBR results on hard and soft tissues	Mean absolute distances (mm): 1. 0.050 ± 0.206; 2. 0.294 ± 0.334; 3. 0.047 ± 0.259; 4. 0.230 ± 0.561 VBR hard - SBR hard ($p = 0.392$) VBR soft - SBR soft ($p = 0.243$)	VBR hard - SBR hard: $r = 0.886$ VBR soft - SBR soft: $r = 0.126$
Bazina et al., Am J Orthod Dentofacial Orthop (2018)	1. Reproducibility of the Dolphin technique 2. Agreement with the ITK-Snap+3D Slicer assessed through the mean differences at 7 areas: a. Nasion area; b. A-point area; c. Right zygomatic area; d. Left zygomatic area; e. Right gonial angle; f. B-point area; g. Left gonial angle	NA	1. ICC = 0.964 (0.941 - 0.978) 2. Mean differences (mm) = a. 0.099 ± 0.072; b. 0.188 ± 0.110; c. 0.113 ± 0.086; d. 0.092 ± 0.057; e. 0.210 ± 0.136; f. 0.189 ± 0.101; g. 0.169 ± 0.082	NA
Cevidanes et al., Dentomaxillofaci Radiol (2005)	Inter-operator agreement on surface distance measurements of 3D models at 3 mandibular regions: 1. Anterior mandibular ramus, 2. Posterior mandibular ramus, 3. Condyles	NA	Surface distances (mm): 1. 0.25 ± 0.11; 2. 0.13 ± 0.05; 3. 0.09 ± 0.05	NA
Cevidanes et al., Am J Orthod Dentofacial Orthop (2009)	Inter-operator agreement on surface distance measurements of 3D models at 9 regions: 1. Zygomatic process, 2. Anterior maxilla, 3. Chin, 4. Right anterior condyle, 5. Right posterior condyle, 6. Left anterior condyle, 7. Left posterior condyle, 8. Mandibular inferior border, 9 Soft-tissue upper lip	NA	Surface distances (mm): 1. 0.1 - 0.4; 2. 0.2 - 0.5; 3. 0.1 - 0.4; 4. 0.0 - 0.3; 5. 0.1 - 0.4; 6. 0.0 - 0.3; 7. 0.0 - 0.4; 8. 0.2 - 0.4; 9. 0.3 - 0.5	NA
Gkantidis et al., PLoS One (2015)	A. Trueness (overall deviation of surface models at unchanged areas: AC + F) B. Intra-operator agreement (on measured structural changes at four corresponding landmarks) of different superimposition techniques: 1. 3P; 2. 1Z; 3. BZ; 4. AC; 5. AC+F C. Inter-operator agreement assessed as described above	NA	A. Trueness (median values of the 3 operators in mm): 1. 0.79 - 1.01; 2. 1.42 - 1.76; 3. 0.31 - 0.57; 4. 0.35 - 0.52; 5. 0.07 - 0.11 ($p = 0.0002$) B. $p = 0.854$ C. $p = 0.661$; $r > 0.91$ for all except 3P	NA
Ghoneima et al., Orthod Craniofac Res (2017)	A. Reproducibility of each superimposition technique B. Mean absolute distance between manually located landmarks on superimposed duplicated scans (ACP, Ba-x, Ba-y, PNS-y, B point-x, Me-x, U1-x, L1-x)	NA	Surface-based and Voxel-based superimposition methods using the anterior cranial base as reference seem to be reproducible whereas Landmarks-based superimposition is less reproducible.	NA
Häner et al., Orthod Craniofac Res (2019)	1. Trueness of the voxel-based superimposition assessed through visual inspection of corresponding reference structures 2. Intra-operator reproducibility assessed through the mean absolute distance (MAD) of the repeatedly superimposed T0 surface models measured in the following areas: N-point, A-point, Pogonion, Right and Left zygomatic arch, Right and left gonial angle 3. Inter-operator reproducibility assessed as described above	Segmentation effect (manual and automatic) assessed as the intra- and interoperator reproducibility	1. In all cases, visual inspection of the superimposed T0-T1 volumes presented adequate overlap 2. MAD (0.06 - 0.16 mm). In very few cases, it exceeded 0.5 mm and never 1 mm 3. MAD (0.15 - 0.24 mm). In few cases, it exceeded 0.5 mm and never 1.5 mm	The median segmentation error ranged from 0.05 - 0.12 mm. The biggest segmentation error was found at A-point (0.3 mm)
Koerich et al., Int J Oral Maxillofac Surg (2016)	A. Intra-operator agreement on surface distance measurements (RMSD) of serial 3D models at 2 regions of the maxilla and 3 regions of the mandible (average difference) B. Inter-operator agreement assessed as described above	NA	A.1 Intra-operator agreement (mm): NA A.2 Intra-operator agreement (mm). Maxilla: 0.183 - 0.184, Mandible: -0.005 - 0.001 B.1 Inter-operator agreement (mm). Maxilla: 0.087 - 0.098, Mandible: 0.183 - 0.184 B.2 Inter-operator agreement (mm). Maxilla: 0.072 - 0.092, Mandible: 0.087 - 0.105	NA

3   **Table 4** Continued

Study	Main Outcomes	Secondary Outcomes	Main Results	Secondary Results
Koerich et al., Angle Orthod (2017)	Inter-operator agreement on surface distance measurements (RMSD) at 5 mandibular regions: 1. Right mandible, 2. Chin, 3. Left mandible, 4. Right ramus, and 5. Left ramus, located at the outer surface of the mandible	NA	Surface distances (mm): 1. 0.11 ± 0.12; 2. 0.14 ± 0.1; 3. 0.11 ± 0.16; 4. 0.33 ± 0.29; 5. 0.36 ± 0.33	
Lemieux et al., Am J Orthod Dentofacial Orthop (2014)	Amount of expansion at the levels of the first premolars (from tip to tip of each buccal cusp) and the first molars (from tip to tip of each mesiobuccal cusp) on 1. plaster models and 2. 3D plane superimposition	Landmark identification reproducibility through ICC	Mean distances measured between premolars (mm): 1. 2.97 ± 2.12; 2. 3.06 ± 1.97 Mean distances measured between molars (mm): 1. 4.18 ± 1.62; 2. 4.28 ± 1.61	ICC > 0.924, 0.992, 0.973 in the x, y, and z axes respectively
Nada et al., PLoS One (2011)	Mean absolute distance of surface models on the following stable areas: a. anterior cranial base (CB); b. forehead (FH); c. left zygomatic arch (ZL); d. right zygomatic arch (ZR)	A. Mean differences between the two superimposition techniques B. Mean differences between repeated AC superimposition measurements C. Mean differences between repeated LZ superimposition measurements	Mean distances measured between the models (mm): 1. 0.20 - 0.37 (SD: 0.08 - 0.16); 2. 0.20 - 0.45 (SD: 0.09 - 0.27)	A. Mean differences (mm): a. 0.12 ± 0.19; b. 0.19 ± 0.12; c. 0.15 ± 0.18; d. -0.17 ± 0.13 B. Mean differences (mm): a. 0.02 ± 0.09; b. 0.01 ± 0.07; c. -0.07 ± 0.12; d. 0.04 ± 0.09 C. Mean differences (mm): a. -0.07 ± 0.25; b. 0.04 ± 0.24; c. 0.14 ± 0.10; d. 0.04 ± 0.09
Nguyen et al., Am J Orthod Dentofacial Orthop (2017)	1. Absolute mean surface distance of the registered models on plates and screws, calculated at 3 regions: a. Chin, b. Symphysis, c. Lower contour of the third molar crypt 2. Reproducibility of the combined chin+symphysis regions measured through ICC and mean absolute distances of the entire surface of T2 registered mandibular models by two operators	NA	1. Absolute mean surface distance (mm): a. 0.37 ± 0.16; b. 0.40 ± 0.14; c. 1.94 ± 0.06 2. ICC = 0.998 (95% CI: 0.995-1.000)	NA
Ruellas et al., Am J Orthod Dentofacial Orthop (2016a)	Differences between corresponding landmark distances from T0-T1 measured through the two superimpositions	A. Precision and B. reproducibility of each technique measured as differences in Euclidean distances of corresponding landmarks	Mean differences (mm): 0.35 - 0.39 (SD: 0.23 - 0.24)	A. Mean differences (mm): 0.36 - 0.42 (SD: 0.21 - 0.24) B. Mean differences (mm): 0.31 - 0.44 (SD: 0.16 - 0.28)
Ruellas et al., PLoS One (2016b)	Difference of corresponding landmark distances between T0-T1 calculated through superimposition on 3 different reference regions, compared to direct measurements of landmark movements from a point considered stable	NA	NA (Mean values provided were outside of the Limits of Agreement range)	NA
Weissheimer et al., Int J Oral Maxillofac Surg (2015)	Visual inspection of the superimposition technique and trueness assessment through visualisation of 3D colour maps	Visual inspection of the effectiveness of the technique through superimposition of reoriented identical models	Highest distance between corresponding anterior cranial base references is less than 0.5 mm for growing and non-growing patients	Highest distance between identical, reoriented anterior cranial bases was less than 0.25 mm

1 **Table 5** Conclusions and limitations of the included studies.

Study	Conclusions	Limitations
Almukhtar et al., PLoS One (2014)	No differences between Voxel-based registration and Surface-based registration. High inconsistency between VBR and SBR regarding soft tissues.	I. No method error II. In SBR, hard and soft tissues were superimposed separately whereas in VBR, hard and soft tissues were all superimposed at once
Bazina et al., Am J Orthod Dentofacial Orthop (2018)	The Dolphin 3D software seems to work properly for voxel-based registration in the anterior cranial base.	I. The original change that occurred over time is not reported. II. ICC values were calculated from only 10 patients and for the average of all measurements. III. There was no assessment of the reproducibility of each individual measurement/case. IV. The type of ICC used is not reported.
Cevidanes et al., Dentomaxillofac Radiol (2005)	The technique shows acceptable reproducibility in the assessment of relatively unaltered structures.	I. There were relatively large interobserver errors compared to the detected changes. II. The actual measured changes were originally small (< 0.8 mm).
Cevidanes et al., Am J Orthod Dentofacial Orthop (2009)	The technique provides reproducible 3D assessment of growing patients.	I. Small sample size that did not allow statistical comparisons
Gkantidis et al., PLoS One (2015	Superimposition of 3D surface models created from voxel data can provide accurate, precise and reproducible results when appropriate references are used. Superimposition on BZ could be an alternative to AC.	I. CT data were used II. No assessment of individual measurements regarding reproducibility
Ghoneima et al., Orthod Craniofac Res (2017)	Surface-based and Voxel-based superimposition methods using the anterior cranial base as reference seem to be reproducible whereas Landmarks-based superimposition is less reproducible.	I. The original change that occurred over time is not reported. II. ICC values were calculated from only 10 patients and for the average of all measurements. There was no assessment of the reproducibility of each individual measurement/case. III. The type of ICC used is not reported. IV. The time span between serial images is not reported.
Häner et al., Orthod Craniofac Res (2019)	The Dolphin voxel-based superimposition technique exhibited adequate performance in growing patients, in terms of efficiency, cranial base matching, and reproducibility. The segmentation error was also acceptable in most cases.	I. The trueness of the voxel-based superimposition was assessed through visual inspection of corresponding reference structures in 2D. II. The original changes between T0 and T1 were relatively limited, though no relation was evident between the amount of change and the error of the process.
Koerich et al., Int J Oral Maxillofac Surg (2016)	The technique shows high precision and reproducibility tough these were assessed in relatively unaltered structures. Furthermore, differences between reoriented dry skulls were larger than expected.	I. The changes of the structures that were evaluated were quite small (< 0.3 mm). II. Differences between the serial images of reoriented dry skulls were higher than those of actual serial scans. III. Samples from different machines were tested
Koerich et al., Angle Orthod (2017)	The technique shows moderate reproducibility in the assessment of relatively unaltered structures.	I. Relatively large interobserver errors compared to the detected changes. II. The changes measured were small (<0.9 mm)
Lemieux et al., Am J Orthod Dentofacial Orthop (2014)	The landmark-derived maxillary plane cannot be assessed through the present methodology.	I. The main outcome is not suitable for the assessment of the superimposition result because it remains unaffected by the superimposition itself. II. The landmark identification error is not thoroughly assessed for individual cases.
Nada et al., PLoS One (2011)	This technique might show good trueness and reproducibility. Registration on the left zygomatic arch seems to be less accurate, but it might still be clinically acceptable and reproducible.	I. Only structures considered stable were evaluated and thus the measured changes were small. II. Only mean values are provided and analysed and thus possible larger individual differences are ignored.

3   **Table 5** Continued

Study	Conclusions	Limitations
Nguyen et al., Am J Orthod Dentofacial Orthop (2017)	The chin and the symphysis region might be an anatomically stable reference area for mandibular superimpositions, whereas the third molar region displayed a higher instability. The chin+symphysis area seems to provide reproducible results.	I. The bone plates and screws were confirmed to be immobile clinically, but their stability in space was not tested (e.g. through best fit registration). II. The areas identified as stable were located at the same place where the superimposition reference area was. III. Only average measures were used to assess all outcomes. There was no assessment of individual cases. IV. Reproducibility outcomes were tested assessing the whole mandibular surface. V. The performance of the chin+symphysis area was shown only for 1 subject.
Ruellas et al., Am J Orthod Dentofacial Orthop (2016a)	No clear evidence is provided that the 2 regions of maxillary registration show similar results and adequate intraobserver and interobserver reproducibility values for growing patients.	I. The changes measured were originally small, except from landmarks 2 and 6 where the error was greater. II. In individual cases the amount of differences was not small compared to the original changes. III. No detailed information is provided (e.g. Bland Altman plot for every variable and results for any landmarks and every coordinates). Only means of different variables were assessed. IV. No comparative statistics.
Ruellas et al., PLoS One (2016b)	The body of the mandible might show better agreement with direct measurements from a point considered stable, compared to the modified Björk superimposition.	I. Results from one superimposition technique (Björk) are not reported. II. The gold standard reference values were not reliable since one geometrical point that was speculated to be stable was used to generate them. However, landmark point identification error is expected to be high in this case and this was not evaluated. III. Two cases were not included in the analysis. IV. Reported mean values were outside of the Limits of Agreements.
Weissheimer et al., Int J Oral Maxillofac Surg (2015)	The software seems to be user-friendly and might work properly for voxel-based registration in the anterior cranail base, both for growing and non-growing patients.	I. No results quantification. II. No method error. III. No descriptive and comparative statistics. IV. Only data from 2 patients shown.