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2 EEG based assessment of stress in horses: A Pilot Study

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20 Abstract

21 As has been hypothesized more than 20 years ago, data derived from EEG (Electroencephalography)
22 measurements can be used to distinguish between behavioral states associated with animal welfare. In our
23 current study we found a high degree of correlation between the modulation index of phase related
24 amplitude changes in the EEG of horses (n=6 measurements with three different horses, mare and
25 gelding) and their facial expression, measured by the use of the horse grimace scale. Furthermore, the
26 pattern of phase amplitude coupling was significantly different between a rest condition and a stress
27 condition in horses. This pilot study paves the way for a possible use of EEG derived phase amplitude
28 coupling as an objective tool for the assessment of animal welfare. Beyond that, the method might be
29 useful to assess welfare aspects in the clinical setting for human patients, as for example in the neonatal
30 intensive care unit.

31 Introduction

32 Is EEG a useful tool to assess welfare in horses? Animal welfare and animal well-being is part of
33 controversial discussions. This happens in different contexts, be it socio-political or ethical discourses,
34 factory farming and food production, animals in private husbandry, animal-assisted therapy, zoos, wildlife
35 or animal experiments. They all have in common that both forming and exchange of opinions are often
36 based on emotions rather than on scientific findings. The assessment of welfare and well-being of animals
37 is sometimes made by how humans feel when they find animals in certain situations. Besides the lack of

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39 ethological knowledge, in many areas related to animal husbandry or the use of animals, there are none or
40 only imprecise legal regulations. In the field of laboratory animal science, legal matters are more closely
41 regulated, both in the context of authorization and in connection with surveillance. The commencement of
42 Directive 63/2010/EU enforced efforts concerning animal welfare on a national and European level and
43 specified personal and institutional prerequisites. People working in this field have to prove their expertise
44 and have to be continuously educated. Housing facilities and experiments have to be approved and
45 procedures have to be ethically justified. Serious and extensive efforts have to be made in order to replace,
46 reduce and refine (3Rs) experimental procedures performed on the animals or their housing conditions.
47 There must be a close documentation of all interventions and a scientifically reasoned assessment and
48 classification in degrees of severity according to the impairment of the animals' well-being.

49 For the assessment of welfare and well-being of animals in factory farming and food production, animals
50 in private husbandry, animal-assisted therapy, zoos, wildlife or animal experiments, we need adequate
51 techniques for an objective measurement of animal welfare (Barnett & Hemsworth, 1990) and associated
52 physiological states as for example EEG, because, judging about animal welfare is most often based on or
53 at least influenced by human assumptions and humanization
54 (http://www.oie.int/index.php?id=169&L=0&htmfile=chapitre_1.7.1.htm). It has been shown that
55 observers who are "used" to expressions of horses that are associated with pain or stereotypic behaviors
56 tend to underestimate these signs regarding horses' welfare (Lesimple & Hausberger, 2014). In a very recent
57 review article, the authors explicitly mention EEG as potential tool to assess cognition and welfare, which
58 are strongly associated (Hausberger et al., 2019). Especially in horses, which are most often kept as working
59 animals, husbandry systems as well as education and training of the animals impact the welfare state even
60 though behavioral data do not always represent the internal state of the animal, as has been shown in a
61 comparative behavioral study with Chilean working horses and Rodeo horses (Rosselot et al., 2019). The
62 need for an objective assessment of animal welfare is clearly apparent. Several authors proposed EEG as
63 promising tool, but it is necessary to show that EEG is significantly correlated with behavioral data and to
64 determine how to best analyze relatively complex skin derived EEG data to assess subtle changes.

65 We addressed these questions by combining a well-established technique for pain and stress assessment,
66 the horse grimace scale (Dalla Costa et al., 2014, 2018), with telemetric EEG recordings as a promising
67 novel tool for the measurement of objective data related to animal welfare and signs of stress (Senko et al.,
68 2017, Hohlbaum et al., 2017, Häger et al., 2017). Facial expression scores are well-established to measure
69 pain in human infants (Grunau & Craig, 1987) and for some nonhuman species with clear facial expression,
70 such as horses HGS (Dalla Costa et al., 2014), mice MGS (Langford et al., 2010) and rats (Sotocinal et al.,
71 2011). Dalla Costa et al. validated the facial expression score by promising a statistical approach to identify
72 a classifier that can estimate the pain status of the animal based on Facial Action Units (FAUs). There exists

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75 no doubt that animals are able to experience pain, fear, stress and other moods and show these through
76 facial expressions. The electroencephalogram (EEG), first described by Berger, is a method to measure tiny
77 summed electrical potentials on the scalp surface that arise from pyramidal cells of the cortex (Berger,
78 1929). Therefore, non-invasive EEG measurements always represent network activity of cortical neurons
79 rather than single cell activity. Cortical networks are highly dynamic and they are broadly orchestrated,
80 which leads to electrical oscillations that can be measured on the surface of the scalp (Kida et al., 2016).
81 These oscillations are in the range of very slow waves below 0.1 Hz, as they occur for example in preterm
82 babies (Vanhatalo et al., 2002). Faster oscillations are categorized as theta, alpha, beta and gamma bands.
83 Some authors additionally define waves above 90 Hz as a “high gamma EEG-band” (Cavelli et al., 2017).
84 A shift from low frequency EEG activity towards high frequency, low amplitude activity has been described
85 during the castration procedure of calves (Coetzee, 2013). A shift of EEG band activity and lateralization
86 have also been observed during attention-related processes in horses (Rochais et al., 2018).
87 More than 20 years ago, it was hypothesized that new tools of EEG analysis will lead to objective
88 measurements for the assessment of animal welfare (Klemm, 1992). One method to find qualitative
89 changes of network activity is phase amplitude coupling (PAC), also known as cross frequency coupling
90 (Tort et al., 2010). PAC is based on amplitude modulations between EEG bands if they occur in a certain
91 phase relation to each other (Tort et al., 2010). This phenomenon does, for example, occur during certain
92 vigilance states (Scheffzück et al., 2011) or it can be modified by the application of drugs (Scheffzück et
93 al., 2013). Therefore, we used, in a proof of concept experiment, the HGS as well as the PAC as a
94 qualitative network change index and compared the intensity of amplitude modulation under resting
95 condition and during stress condition (i.e., anticipating a medical treatment of horses in the veterinary
96 clinic). We hypothesized that the HGS as well as the PAC are significantly different in the horses in
97 accordance to the different conditions and that there is an association between HGS and PAC, which
98 means the EEG could be an objective tool for the assessment of animal welfare.

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102 **Methods**

103 **Ethical Approval**

104 All procedures were approved by the local ethics committee (L0294113, Berlin, LAGeSo), and followed
105 the European and the German national regulations (Animal Welfare act, 2010/63/EU). All animal
106 procedures were performed in accordance with the animal care committee’s regulations [Freie Universität
107 Berlin].

108

109 Subjects

110 The three adult horses belonged to the demonstration stock for veterinary students at the Freie Universität
 111 Berlin. The horses were adults, of different sex and diverse breedings (one trotter, two warmblood
 112 horses). The mare had been used in three veterinary demonstration treatments, the trotter (gelding) in two
 113 and the warmblood gelding in one treatment. The horses were not used as working or sports horses at the
 114 university but they had unknown origin. All horses are healthy, used to handling and kept in boxes during
 115 the night and a paddock or pasture during the day. The experiments took place in their familiar
 116 environment at the horse clinic.

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117 Procedure

118 During six different days, three adult horses were recorded (n=6 different veterinary interventions). All of
 119 our measurements took place during routine teaching lessons for the students, which does mean that no
 120 further experimental animals have been used solely for our study. We measured two vigilance states of
 121 each horse for each experimental day (some horses have been recorded at two different veterinary
 122 treatments) with the horse grimace scale and with EEG. Both measurements took place simultaneously
 123 for about 30 minutes duration. The recordings were always performed by the same persons. One person
 124 did the video recordings, another person did the EEG recordings and a third person remained near to the
 125 horse to relocate the antenna, if necessary. The two experimenters, responsible for data acquisition (video
 126 and EEG), always started their new video and EEG files at the same time (each file approximately 10
 127 minutes). First, the animals were recorded in a familiar situation in the stable to assess the relaxed state
 128 as a reference, called "resting condition". The second measurement took place in the examination stand in
 129 anticipation of stressful situation i.e. a veterinary treatment, called "stress condition" (Fig. 1).

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130 Materials

131 Panasonic Digital camera Lumix FMC-FZ200, Disposable adhesive surface silver/silverchloride
 132 electrodes (Spes Medica S.r.l., 111 Genova, Italy), abrasive cream (Abralyt HiCl, Easycap GmbH,
 133 Herrsching, Germany), EEG telemetry unit (with an AC coupled amplifier, sampling rate 500Hz) (Lapray
 134 et al., 2009)

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135 Horse Grimace Scale

136 A Panasonic Digital camera Lumix FMC-FZ200 was used to record the facial expression of the horses
 137 during the different conditions. The records were used for analyzing the HGS in accordance to Dalla
 138 Costa et al. (2014). One HGS value was calculated for each video file. Regarding the correlation with
 139 EEG coupling coefficients, corresponding files were selected, but the video files were of longer duration

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143 than the EEG files. To calculate the total pain score with the HGS, six facial coding units are used (Ears
144 stiffly backwards, orbital tightening, tension above eye area, prominent strained chewing muscles, mouth
145 strained and pronounced chin, strained nostrils and flattening of the profile). For each coding unit a score
146 of 0, 1 or 2 can be given. This results in a maximal total pain score of 12 points. The HGS has a relatively
147 high inter observer reliability. The Interclass Correlation Coefficient (ICC) has a value of 0.92 (Dalla
148 Costa et al., 2014).

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150 EEG recordings

151 Disposable adhesive surface silver/silverchloride electrodes (Spes Medica S.r.l., 111 Genova, Italy) were
152 placed on the nose (between the ears) as ground and reference (Fig 2 (2, 3) and between the eye and ear
153 to record from the right somatosensory cortex region (parietal position, Fig 2 (1)). Before fixating the
154 electrode, the location was shaved and the skin was cleaned with an abrasive cream (Abralyt HiCl,
155 Easycap GmbH, Herrsching, Germany) in order to remove dead skin cells and to achieve a lower
156 impedance. The data was recorded and sent by a telemetry unit (with an AC coupled amplifier, sampling
157 rate 500Hz) (Lapray et al., 2009). Only phases without artefacts were taken into account for analysis.
158 Selected sequences lasted on an average 90s in case of the resting condition and 50 s in case of the stress
159 condition. **For each veterinary intervention and each condition (rest or stress), only one sequence was**
160 **used for analysis. Some horses have been treated two times, at different days (at least one week between**
161 **the first and the second measurement).**

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163 EEG analysis

164 EEG segments without artefacts (muscle, extended line noise) were selected.
165 We analyzed the data with Matlab (2016, MathWorks) and with Brainstorm (Tadel et al., 2011). EEG raw
166 data were filtered with digital butterworth filters with a custom written Matlab script. The filter was
167 designed with the function butter (n=3rd order). We calculated the normalized cutoff frequency (Wn) for
168 EEG bands delta [0-4Hz], theta [4-8Hz], alpha [8-13Hz], beta [13-30Hz], low gamma [30-80Hz] and high
169 gamma [80-120Hz]. Wn is a number between 0 and 1, where 1 corresponds to the Nyquist frequency which
170 is half the sampling rate (here: 500Hz).
171 The numerator and denominator values (IIR filter), achieved with the function butter, were used with the
172 Matlab function filtfilt to filter the EEG data. For the delta EEG band, a lowpass filter was used. We
173 extracted all other EEG frequency bands with a bandpass filter design.

174 Phase amplitude coupling and Phase Locking Value (PLV) were analyzed with brainstorm software (Tadel
175 et al., 2011).

176 To obtain Canolty maps (Canolty et al., 2006), the following procedure was computed
177 (neuroimage.usc.edu/brainstorm/Tutorials/Resting): The EEG was filtered at the low frequency of interest,
178 using a narrow band pass filter. The amplitude troughs of the desired low frequency were detected in the
179 signal. A time window was defined around the detected troughs in order to compute a time frequency
180 decomposition using a set of narrow band-pass filters.

181

182 Analysis

183 To extract statistically significant changes of amplitude modulation, we compared the modulation indices
184 calculated with the open source software brainstorm (Tadel et al., 2011) between the resting condition and
185 the stress condition of the horses. With the brainstorm function “Canolty”, the data are screened for
186 amplitude modulations at higher frequency bands in relation to a certain slower phase frequency (here, we
187 show the results for 8 Hz, figure 3). First, we pooled all cycles of the phase frequency (8Hz) for each animal
188 during a time window of 1s, corresponding to 8 phase cycles, and used the sum for each animal. The 1s
189 time window is independent of the duration of raw data; it means that 8 phase frequency waves are
190 represented in the resulting Canolty-map computation by the program brainstorm. Furthermore, we were
191 interested in the information, at which point in the phase frequency cycle a possible amplitude modulation
192 takes place (for example, at the trough or the up-stroke of the 8 Hz phase frequency wave). We had a
193 resolution of 125 modulation index values (given by the program brainstorm with the function “Canolty”)
194 within a single cycle of the phase frequency, which corresponds to 360° of the 8Hz phase frequency wave.
195 10ms in the Canolty-maps correspond to $2,9^\circ$ of the phase frequency. We calculated the differences of
196 modulation indices for every 2.9° of the phase frequency between the resting and the stress condition. The
197 statistically significant results are shown as polar plot (number of statistically significant differences in
198 relation to 360° of the phase frequency, Figure 4). Furthermore, we calculated the coefficient of correlation
199 between the modulation index of the EEG and the results of the horse grimace scale for both behavioral
200 states (function "corr", type “Spearman”, Matlab, 2016b). For each kind of analysis, we used timely
201 corresponding files of EEG and video. The sequences taken into account are longer for the video files than
202 for the EEG, because, in the case of the EEG, we chose sequences without artefacts (most often artefacts
203 from mobile phones in near vicinity).

204 We tested data for distribution with the Lilliefors test (Matlab 2016b). Tests were performed with the non-
205 parametric Kruskal Wallis test and a subsequent multiple comparison test in order to achieve exact

206 statistical relations between groups. All tests are implemented in the Matlab statistics toolbox (Matlab
207 2016b, MathWorks) .

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211 Results

212 We graded the horses' comfort behavior according to the horse grimace scale (Dalla Costa et al., 2014).
213 EEG data and behavioral data were analyzed independently by two different persons to avoid a statistical
214 bias. Both methods reflect changes of behavioral state.

215

216 Horse Grimace Scale

217 We were able to identify statistically significant changes of the facial expressions between the resting
218 condition and the stressful condition in horses ($p=0,006$). The mean facial expression score for the resting
219 condition is 4.12 (with a standard deviation of 0.57 and an upper and lower confidence interval of 5.42 and
220 2.83). The mean facial expression score for the condition stress is 6 (with a standard deviation of 0.61 and
221 an upper and lower confidence interval of 7.34 and 4.66).

222

223 EEG

224 We were not able to detect statistically significant changes of horses' EEG band power between the rest
225 condition and the stress condition in anticipation of a veterinary treatment. Nevertheless, there is a tendency
226 towards slightly elevated EEG band power during the stress condition in comparison to the rest condition.
227 In contrast, we were able to identify major changes of phase amplitude coupling between the rest, and the
228 stress condition (Fig 3). A progressive decay of phase amplitude coupling between 8Hz low frequency and
229 the gamma and high gamma band takes place from rest towards stress. Besides the mere decay of coupling
230 density, a qualitative change regarding phase relation between the high and low frequency is clearly visible.
231 For the rest condition, the coupling patterns extend from gamma to high gamma (up to 250 Hz) with
232 maximal coupling coefficients during the up stroke and the down stroke of the 8 Hz low frequency
233 (indicated as white sine wave in Fig 3a). For the condition stress (Fig 3b), the phase amplitude coupling
234 pattern is still visible in the gamma range but overall coupling strength is lower in comparison to the resting
235 state. Statistically significant differences of phase related amplitude modulation between the rest and the
236 stress condition can be found during the upstroke (around 90° of the phase frequency) and during the down
237 stroke (around 260°) (Fig 4), confirming the optical impression from the Canolty maps (supplementary

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238 table 1). Furthermore, only the down stroke of the 8Hz phase frequency reveals strong coupling coefficients
239 with gamma and high gamma EEG bands. The coefficient of correlation (Rho) between the EEG derived
240 data (Coupling coefficients of the Canolty map) and the horse grimace scale is -0.86 (p=0.00031) for the
241 down stroke of the phase frequency (here at 290°) and 0.71 (p=0.01) for the up stroke of the phase
242 frequency. The quality of raw data is good, the presence of nested activity (faster frequencies on top of slow
243 frequencies) was confirmed with a wavelet analysis (Fig 5 A,B).

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244 Discussion

245 Why assess welfare in horses? The horse is both companion as well as working animal (Hausberger et al.,
246 2019). Facial expressions associated with pain and stress are well described (for example Dalla Costa et al.,
247 2014) and relatively easy to assess for a trained observer. On the one hand, horses raise several issues of
248 animal welfare status, as, for example, regarding training methods, sports, as working animals and even as
249 companions (boredom) (Hausberger et al., 2019). On the other hand, they represent both companion as well
250 as working animal in husbandry and sports. To judge about the validity and utility of EEG measurements
251 in the context of animal welfare, horses are perfectly suited because they are used to handling procedures
252 (which reduces the impact of the EEG application procedure itself on the subjects' behavior) and other
253 indications of wellbeing, which we used as comparative value.

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254 As has been proposed earlier (Klemm, 1992), we were able to extract differences in EEG network
255 activity during stress and rest in horses, mental states that are obviously characterized by significant
256 changes in HGS. In order to validate the behavioral states "stress" and "rest" in horses, we used the horse
257 grimace scale (Dalla Costa et al., 2014, 2018). Phase amplitude coupling seems to be an extremely robust
258 tool to extract activity patterns in the brain, associated with distinct behavioral states to access animal
259 welfare. One reason for the robustness might be that phase amplitude coupling is extracting information
260 that is inherently linked to intrinsic neural network phenomena. The measurement does not rely on
261 absolute values, which may be influenced by technical or intra-individual issues, but on a relational
262 modulation index. Furthermore, phase related amplitude modulations seem to be an ubiquitous
263 phenomenon for neural networks, as they are also involved in the generation of peristaltic movements of
264 the intestinal tract (Huizinga et al., 2015). In fact, phase amplitude coupling in the intestinal tract is also
265 associated with the regulation of peristaltic movements according to incoming stimuli (for example food
266 intake). Further studies with a higher number of animals and more electrode positions may be beneficial
267 to confirm our results and to gain further insights regarding anatomical correlations of certain behavioral
268 representations in the EEG. Here, we used one electrode in a parietal position. This position is near to the
269 somatosensory cortex, a well characterized cortical region which is responsible for the representation of
270 one's own body. Other electrode positions may give different results, as, for example, frontal electrode
271 locations and should be addressed in subsequent studies.

272 Our results indicate a change of network activity during stress in the region of the somatosensory cortex.
273 The progressive decay of coupling strength between the rest and the stress condition, with a maximum at
274 half way of the down stroke (260°, figure 4), rather than an abrupt change, may be due to the general
275 wave characteristics of envelope-signals, which are recorded from bigger neural networks. We can only
276 speculate that the underlying entrainment of smaller sub-networks may work cascaded to form the
277 progressive decay. A combination with non-invasive imaging techniques, as, for example, MRI or fMRI
278 would be interesting to gain further insights regarding network entrainment and the anatomical
279 correlation. However, the technique is extremely challenging for behaving horses.
280 It can be excluded that physical pain is the main driver for the change of neural network activity because
281 we took all stress recordings in the anticipation state, before any kind of physical pain or sedation
282 appeared. The representation may look different in other brain regions. The mere touching or handling of
283 the horse or the presence of people can be excluded as influencing factors, because these factors appeared
284 in both conditions. Since the brain is more or less a black box in the case of non-invasive EEG
285 measurements, it is very difficult or maybe impossible to reason about the origin of the coupling pattern
286 on the cellular level with our method. The strong kind of stress reaction, which is probably associated
287 with a medical treatment, may be relatively conserved among individuals. This may be different for minor
288 forms of stress as, for example, during training, handling or social interaction. In these cases, we would
289 expect a high intra-individual difference. To understand the change of phase amplitude coupling in
290 relation to behavior in a better way, much more data are needed with different studies, different animals
291 and different behavioral contexts.

292
293 Facial expression can hardly be used to recognize welfare in species like birds, reptiles etc. with poor
294 facial expression. If it is possible to establish reliable EEG patterns associated with stress for different
295 species in future studies, a translational approach for species with poor facial expression might be
296 possible. It must be kept in mind that the activity of the brain is highly dynamic, also known as neural
297 plasticity. The context can change the activity of the brain. Every measurement of the EEG can also
298 potentially influence the content of the EEG – some kind of uncertainty relation. Telemetric EEG
299 recordings are extremely useful in this context, because they do not restrict the freedom of movement of
300 the animals. In this context, it must also be discussed whether the location (home box during the rest
301 condition versus treatment location during the stress condition) had an impact on the EEG. This
302 possibility cannot be fully excluded. But, the home box and the examination stand are located in the same
303 building; furthermore, both locations are familiar to the horses. Of course, the examination stand might
304 generally be associated with veterinary interventions for these horses because they are routinely used to
305 train veterinary students for several diagnostic techniques. Therefore, the change of PAC patterns cannot

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308 be triggered by novelty (here: a novel environment) but the stress factor may arise indirectly from the
309 location, which is associated with stress rather than directly due to the veterinary treatment itself.

310
311 Since we did not use “experimental” horses exclusively for our study but demonstration horses of the
312 university that were used for teaching purposes in a hands-on training for veterinary students, we were not
313 able to select the horses in an optimal way for the purpose of the study. The number of training sessions
314 was limited to six veterinary interventions at six different days with three different horses. It would be
315 important to repeat this study with more horses and more observations.

316
317 Another important factor is the miniaturization of EEG amplifiers as well as comfortable electrodes that
318 are as small as possible. For our future studies with a higher number of electrodes, we developed light
319 curing polymer electrodes (de Camp et al., 2018). Furthermore, in a current project, the amplifier with 8
320 Channels will be miniaturized to 9x12mm. This EEG system will be potentially useful to assess EEG
321 measurements in small species like birds or rodents. Another system is considered as bus system, to
322 include other bio-signals as for example ECG or breathing. Welfare monitoring may gain robustness by
323 integrating multi-modal data.

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324 325 **Conclusions**

326 We hypothesized that the HGS as well as the modulation index (phase amplitude coupling, PAC) derived
327 from EEG data are significantly different in the horses in accordance to different behavioral conditions and
328 second, that there is an association between HGS and PAC, which means the EEG could be an objective
329 tool for the assessment of animal welfare.

330 In conclusion, we were able to find an association between the scientifically validated horse grimace scale
331 and an EEG pattern, associated with two distinct behavioral states, namely stress and rest in horses. Phase
332 amplitude coupling might be a robust tool for the objective assessment of animal welfare and well-being of
333 animals. Furthermore, it may be useful to judge about brain states as well as comfort of neonates or disabled
334 persons, who are unable to communicate actively.

335 Our pilot study gives preliminary evidence that EEG measurements can be an objective tool for the
336 assessment of animal welfare and stress.

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338

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440
441 **Figure legends**

442 **Fig 1. Horse in examination stand.** The telemetry unit is fixed at the shoulder with a piece of tape. As an
443 example, typical facial expressions in this picture are: Ears oriented backwards (score 2), closed eyes
444 (here 0), tension above eyes (score 1), tension in the region around jaw muscles (score 1), tension around
445 muzzle and prominent chin (score 1), tension around nozzles, flattened profile (score 2). The sum of all
446 facial expression scores is 7 for this image.

447 **Fig 2. Electrode positions.** The ground and reference electrode were placed above the nose (2,3), the
448 recording electrode was placed in a parietal position between the right eye and ear (1).

449
450 **Fig 3. Canolty maps for rest EEG and stress EEG.** Phase related amplitude modulation is shown as
451 heat map. The low frequency for both behavioral conditions is 8 Hz (indicated as white sine wave in
452 subplot a). Maximal amplitude modulation is visible during the up- and down stroke of the low frequency
453 in the gamma and high gamma band with a peak at 130 Hz during rest (subplot a). In the stress condition
454 (subplot b) the coupling pattern is quantitatively weaker, additionally the phase relation is changed.

455 Amplitude modulation is maximal during the down stroke, the upstroke is only weakly associated with
456 amplitude modulation in contrast to the resting condition (subplot a). Maximal modulation index values
457 are again visible around 130 ° in the high gamma range.

458 **Fig 4. Number of statistically significant differences of phase related amplitude modulation between**
459 **rest and stress.** Most differences of the EEG derived modulation index between behavioral states can be
460 found for the upstroke of the phase frequency around 60°. A minor fraction of significant differences is
461 visible during the down stroke around 210°.

462 **Fig 5. EEG raw data trace with nested activity of multiple bands.** One second of original EEG
463 recording is shown as raw data trace (upper panel) and wavelet analysis (lower panel). High power is

464 coded as warm color (red). The wavelet analysis reveals nested activity in the alpha, beta and gamma
465 band of the EEG.
466

