

EEG based assessment of stress in horses: a pilot study

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As has been hypothesized more than 20 years ago, data derived from EEG (Electroencephalography) measurements can be used to distinguish between behavioral states associated with animal welfare. In our current study we found a high degree of correlation between the modulation index of phase related amplitude changes in the EEG of horses (n=6 measurements with three different horses, both sexes) and their facial expression, measured by the use of the horse grimace scale. Furthermore, the pattern of EEG derived phase amplitude coupling was significantly different between a rest condition and a stress condition in horses. This pilot study paves the way for a possible use of EEG derived phase amplitude coupling as an objective tool for the assessment of animal welfare. Beyond that, the method might be useful to assess welfare aspects in the clinical setting for human patients, as for example in the neonatal intensive care unit.

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20 Abstract

21 As has been hypothesized more than 20 years ago, data derived from EEG (Electroencephalography)
22 measurements can be used to distinguish between behavioral states associated with animal welfare. In our
23 current study we found a high degree of correlation between the modulation index of phase related
24 amplitude changes in the EEG of horses (n=6 measurements with three different horses, mare and
25 gelding) and their facial expression, measured by the use of the horse grimace scale. Furthermore, the
26 pattern of phase amplitude coupling was significantly different between a rest condition and a stress
27 condition in horses. This pilot study paves the way for a possible use of EEG derived phase amplitude
28 coupling as an objective tool for the assessment of animal welfare. Beyond that, the method might be
29 useful to assess welfare aspects in the clinical setting for human patients, as for example in the neonatal
30 intensive care unit.

31 Introduction

32 Is EEG a useful tool to assess welfare in horses? Animal welfare and animal well-being is part of
33 controversial discussions. This happens in different contexts, be it socio-political or ethical discourses,
34 factory farming and food production, animals in private husbandry, animal-assisted therapy, zoos, wildlife
35 or animal experiments. They all have in common that both forming and exchange of opinions are often
36 based on emotions rather than on scientific findings. The assessment of welfare and well-being of animals
37 is sometimes made by how humans feel when they find animals in certain situations. Besides the lack of

38 ethological knowledge, in many areas related to animal husbandry or the use of animals, there are none or
39 only imprecise legal regulations. In the field of laboratory animal science, legal matters are more closely
40 regulated, both in the context of authorization and in connection with surveillance. The commencement of
41 Directive 63/2010/EU enforced efforts concerning animal welfare on a national and European level and
42 specified personal and institutional prerequisites. People working in this field have to prove their expertise
43 and have to be continuously educated. Housing facilities and experiments have to be approved and
44 procedures have to be ethically justified. Serious and extensive efforts have to be made in order to replace,
45 reduce and refine (3Rs) experimental procedures performed on the animals or their housing conditions.
46 There must be a close documentation of all interventions and a scientifically reasoned assessment and
47 classification in degrees of severity according to the impairment of the animals' well-being.
48 For the assessment of welfare and well-being of animals in factory farming and food production, animals
49 in private husbandry, animal-assisted therapy, zoos, wildlife or animal experiments, we need adequate
50 techniques for an objective measurement of animal welfare (Barnett & Hemsworth, 1990) and associated
51 physiological states as for example EEG, because, judging about animal welfare is most often based on or
52 at least influenced by human assumptions and humanization
53 (http://www.oie.int/index.php?id=169&L=0&htmfile=chapitre_1.7.1.htm). It has been shown that
54 observers who are "used" to expressions of horses that are associated with pain or stereotypic behaviors
55 tend to underestimate these signs regarding horses' welfare (Lesimple & Hausberger, 2014). In a very recent
56 review article, the authors explicitly mention EEG as potential tool to assess cognition and welfare, which
57 are strongly associated (Hausberger et al., 2019). Especially in horses, which are most often kept as working
58 animals, husbandry systems as well as education and training of the animals impact the welfare state.
59 Nevertheless, behavioral data do not always represent the internal state of the animal, as has been shown in
60 a comparative behavioral study with Chilean working horses and Rodeo horses (Rosselot et al., 2019). The
61 need for an objective assessment of animal welfare is clearly apparent. Several authors proposed EEG as
62 promising tool, but it is necessary to show that EEG is significantly correlated with behavioral data and to
63 determine how to best analyze relatively complex skin derived EEG data to assess subtle changes.
64 We addressed these questions by combining a well- established technique for pain and stress assessment,
65 the horse grimace scale (Dalla Costa et al., 2014, 2018), with telemetric EEG recordings as a promising
66 novel tool for the measurement of objective data related to animal welfare and signs of stress (Senko et al.,
67 2017, Hohlbaum et al., 2017, Häger et al., 2017). Facial expression scores are well-established to measure
68 pain in human infants (Grunau & Craig, 1987) and for some nonhuman species with clear facial expression,
69 such as the horse grimace scale (HGS, Dalla Costa et al., 2014), the mouse grimace scale (MGS, Langford
70 et al., 2010) and the rat grimace scale (RGS, Sotocinal et al., 2011). Dalla Costa et al. validated the facial
71 expression score by using a statistical approach to identify a classifier that can estimate the pain status of

72 the animal based on Facial Action Units (FAUs). There exists no doubt that animals are able to experience
73 pain, fear, stress and other moods and show these through facial expressions. The electroencephalogram
74 (EEG), first described by Berger, is a method to measure tiny summed electrical potentials on the scalp
75 surface that arise from pyramidal cells of the cortex (Berger, 1929). Therefore, non-invasive EEG
76 measurements always represent network activity of cortical neurons rather than single cell activity. Cortical
77 networks are highly dynamic and they are broadly orchestrated, which leads to electrical oscillations that
78 can be measured on the surface of the scalp (Kida et al., 2016). These oscillations are in the range of very
79 slow waves below 0.1 Hz, as they occur for example in preterm babies (Vanhatalo et al., 2002). Faster
80 oscillations are categorized as theta, alpha, beta and gamma bands. Some authors additionally define waves
81 above 90 Hz as a “high gamma EEG-band” (Cavelli et al., 2017). A shift from low frequency EEG activity
82 towards high frequency, low amplitude activity has been described during the castration procedure of calves
83 (Coetzee, 2013). A shift of EEG band activity and lateralization have also been observed during attention-
84 related processes in horses (Rochais et al., 2018). In conclusion, EEG data can represent behavioral or
85 internal states of the animal.

86 More than 20 years ago, it was hypothesized that new tools of EEG analysis will lead to objective
87 measurements for the assessment of animal welfare (Klemm, 1992). One method to find qualitative
88 changes of network activity is phase amplitude coupling (PAC), also known as cross frequency coupling
89 (Tort et al., 2010). PAC is based on amplitude modulations between EEG bands if they occur in a certain
90 phase relation to each other (Tort et al., 2010). This phenomenon does, for example, occur during certain
91 vigilance states (Scheffzück et al., 2011) or it can be modified by the application of drugs (Scheffzück et
92 al., 2013). Therefore, we used, in a proof of concept experiment, the HGS as well as the PAC as a
93 qualitative network change index and compared the intensity of amplitude modulation under resting
94 condition and during stress condition (i.e., anticipating a medical treatment of horses in the veterinary
95 clinic). We hypothesized that the HGS as well as the PAC are significantly different in the horses in
96 accordance to the different conditions and that there is an association between HGS and PAC, which
97 means the EEG could be an objective tool for the assessment of animal welfare.

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101 **Methods**

102 **Ethical Approval**

103 All procedures were approved by the local ethics committee (L0294113, Berlin, LAGeSo), and followed
104 the European and the German national regulations (Animal Welfare act, 2010/63/EU). All animal

105 procedures were performed in accordance with the animal care committee's regulations [Freie Universität
106 Berlin].

107 **Materials**

108 We used a Panasonic Digital camera Lumix FMC-FZ200, disposable adhesive surface
109 silver/silverchloride electrodes (Spes Medica S.r.l., 111 Genova, Italy), abrasive cream (Abralyt HiCl,
110 Easycap GmbH, Herrsching, Germany) and an EEG telemetry unit (with an AC coupled amplifier,
111 sampling rate 500Hz) (Lapray et al., 2009)

112 **Subjects**

113 The three adult horses belonged to the demonstration stock for veterinary students at the Freie Universität
114 Berlin. The horses were adults, of different sex and diverse breedings (one trotter (a race horse), two
115 warmblood (most often used for show jumping or dressage) horses). The mare had been used in three
116 veterinary demonstration treatments, the trotter (gelding) in two and the warmblood gelding in one
117 treatment. The horses were not used as working or sports horses at the university but they had unknown
118 origin. All horses are healthy, used to handling and kept in stalls during the night and a paddock or
119 pasture during the day. The experiments took place in their familiar environment at the horse clinic.

120 **Procedure**

121 During six different days, three adult horses were recorded (n=6 different veterinary interventions). All of
122 our measurements took place during routine teaching lessons for the students. We measured two vigilance
123 states of each horse for each experimental day (some horses have been recorded at two different
124 veterinary treatments) with the horse grimace scale and with EEG. Both measurements took place
125 simultaneously for about 30 minutes duration. The recordings were always performed by the same
126 persons. One person did the video recordings, another person did the EEG recordings and a third person
127 remained near to the horse to relocate the antenna, if necessary. The two experimenters, responsible for
128 data acquisition (video and EEG), always started their new video and EEG files at the same time (each
129 file approximately 10 minutes). First, the animals were recorded in a familiar situation in the stable to
130 assess the relaxed state as a reference, called "resting condition". The second measurement took place in
131 the examination stand in anticipation of stressful situation i.e. a veterinary treatment, called "stress
132 condition" (Fig. 1).

133

134 **Horse Grimace Scale**

135 . The video recordings were used for analyzing the HGS in accordance to Dalla Costa et al. (2014). One
136 HGS value was calculated for each video file. Regarding the correlation with EEG coupling coefficients,

137 corresponding files were selected, but the video files were of longer duration than the EEG files. To
138 calculate the total pain score with the HGS, six facial coding units were used (Ears stiffly backwards,
139 orbital tightening, tension above eye area, prominent strained chewing muscles, mouth strained and
140 pronounced chin, strained nostrils and flattening of the profile). For each coding unit a score of 0, 1 or 2
141 was given. This results in a maximal total pain score of 12 points. The HGS has a relatively high inter
142 observer reliability. The Interclass Correlation Coefficient (ICC) has a value of 0.92 (Dalla Costa et al.,
143 2014).

144

145 **EEG recordings**

146 Disposable adhesive surface silver/silverchloride electrodes (Spes Medica S.r.l., 111 Genova, Italy) were
147 placed on the nose (between the ears) as ground and reference (Fig 2 (2, 3) and between the eye and ear
148 to record from the right somatosensory cortex region (parietal position, Fig 2 (1)). Before fixating the
149 electrode, the location was shaved and the skin was cleaned with an abrasive cream (Abralyt HiCl,
150 Easycap GmbH, Herrsching, Germany) in order to remove dead skin cells and to achieve a lower
151 impedance. The data was recorded and sent by a telemetry unit (with an AC coupled amplifier, sampling
152 rate 500Hz) (Lapray et al., 2009). Only phases without artefacts were taken into account for analysis.
153 Selected sequences lasted on an average 90s in case of the resting condition and 50 s in case of the stress
154 condition. For each veterinary intervention and each condition (rest or stress), only one sequence was
155 used for analysis. Two horses have been treated two and three times, at different days (at least one week
156 between the first and the second measurement).

157

158 **EEG analysis**

159 EEG segments without artefacts (muscle, extended line noise) were selected.

160 We analyzed the data with Matlab (2016, MathWorks) and with Brainstorm (Tadel et al., 2011). EEG raw
161 data were filtered with digital butterworth filters with a custom written Matlab script. The filter was
162 designed with the function butter ($n=3$ rd order). We calculated the normalized cutoff frequency (W_n) for
163 EEG bands delta [0-4Hz], theta [4-8Hz], alpha [8-13Hz], beta [13-30Hz], low gamma [30-80Hz] and high
164 gamma [80-120Hz]. W_n is a number between 0 and 1, where 1 corresponds to the Nyquist frequency which
165 is half the sampling rate (here: 500Hz).

166 The numerator and denominator values (IIR filter), achieved with the function butter, were used with the
167 Matlab function filtfilt to filter the EEG data. For the delta EEG band, a lowpass filter was used. We
168 extracted all other EEG frequency bands with a bandpass filter design.

169 Phase amplitude coupling and Phase Locking Value (PLV) were analyzed with brainstorm software (Tadel
170 et al., 2011).

171 To obtain Canolty maps (Canolty et al., 2006), the following procedure was computed
172 (neuroimage.usc.edu/brainstorm/Tutorials/Resting): The EEG was filtered at the low frequency of interest,
173 using a narrow band pass filter. The amplitude troughs of the desired low frequency were detected in the
174 signal. A time window was defined around the detected troughs in order to compute a time frequency
175 decomposition using a set of narrow band-pass filters.

176

177 **Analysis**

178 To extract statistically significant changes of amplitude modulation, we compared the modulation indices
179 calculated with the open source software brainstorm (Tadel et al., 2011) between the resting condition and
180 the stress condition of the horses. With the brainstorm function “Canolty”, the data are screened for
181 amplitude modulations at higher frequency bands in relation to a certain slower phase frequency (here, we
182 show the results for 8 Hz, figure 3). First, we pooled all cycles of the phase frequency (8Hz) for each animal
183 during a time window of 1s, corresponding to 8 phase cycles, and used the sum for each animal. The 1s
184 time window is independent of the duration of raw data; it means that 8 phase frequency waves are
185 represented in the resulting Canolty-map computation by the program brainstorm. Furthermore, we were
186 interested in the information, at which point in the phase frequency cycle a possible amplitude modulation
187 takes place (for example, at the trough or the up-stroke of the 8 Hz phase frequency wave). We had a
188 resolution of 125 modulation index values (given by the program brainstorm with the function “Canolty”)
189 within a single cycle of the phase frequency, which corresponds to 360° of the 8Hz phase frequency wave.
190 10ms in the Canolty-maps correspond to $2,9^\circ$ of the phase frequency. We calculated the differences of
191 modulation indices for every $2,9^\circ$ of the phase frequency between the resting and the stress condition. The
192 statistically significant results are shown as polar plot (number of statistically significant differences in
193 relation to 360° of the phase frequency, Figure 4). Furthermore, we calculated the coefficient of correlation
194 between the modulation index of the EEG and the results of the horse grimace scale for both behavioral
195 states (function "corr", type “Spearman”, Matlab, 2016b). For each kind of analysis, we used timely
196 corresponding files of EEG and video. The sequences taken into account are longer for the video files than
197 for the EEG, because, in the case of the EEG, we chose sequences without artefacts (most often artefacts
198 from mobile phones in near vicinity).

199 We tested data for distribution with the Lilliefors test (Matlab 2016b). Tests were performed with the non-
200 parametric Kruskal Wallis test and a subsequent multiple comparison test in order to achieve exact

201 statistical relations between groups. All tests are implemented in the Matlab statistics toolbox (Matlab
202 2016b, MathWorks) .

203

204

205

206 **Results**

207 We graded the horses' comfort behavior according to the horse grimace scale (Dalla Costa et al., 2014).
208 EEG data and behavioral data were analyzed independently by two different persons to avoid a statistical
209 bias. Both methods reflect changes of behavioral state. The HGS has a relatively high inter observer
210 reliability. The Interclass Correlation Coefficient (ICC) has a value of 0.92 (Dalla Costa et al., 2014).

211

212 **Horse Grimace Scale**

213 We were able to identify statistically significant changes of the facial expressions between the resting
214 condition and the stressful condition in horses ($p=0,006$, confidence interval [0.489 3.258]). The mean
215 facial expression score for the resting condition is 4.12 (with a standard deviation of 0.57 and an upper and
216 lower confidence interval of 5.42 and 2.83). The mean facial expression score for the condition stress is 6
217 (with a standard deviation of 0.61 and an upper and lower confidence interval of 7.34 and 4.66).
218 Furthermore we calculated the effect size with an F-test with $n=3$, F value=6.383 and $p=0.002$, which
219 additionally shows that the facial expression is highly dependent on the behavioral condition (the third
220 behavioral condition is stress under sedation, which was not used for EEG analysis).

221

222 **EEG**

223 We were not able to detect statistically significant changes of horses' EEG band power between the rest
224 condition and the stress condition in anticipation of a veterinary treatment. Nevertheless, there is a tendency
225 towards slightly elevated EEG band power during the stress condition in comparison to the rest condition.
226 In contrast, we were able to identify major changes of phase amplitude coupling between the rest, and the
227 stress condition (Fig 3). A progressive decay of phase amplitude coupling between 8Hz low frequency and
228 the gamma and high gamma band takes place from rest towards stress. Besides the mere decay of coupling
229 density, a qualitative change regarding phase relation between the high and low frequency is clearly visible.
230 For the rest condition, the coupling patterns extend from gamma to high gamma (up to 250 Hz) with
231 maximal coupling coefficients during the up stroke and the down stroke of the 8 Hz low frequency
232 (indicated as white sine wave in Fig 3a). For the condition stress (Fig 3b), the phase amplitude coupling

233 pattern is still visible in the gamma range but overall coupling strength is lower in comparison to the resting
234 state. Statistically significant differences of phase related amplitude modulation between the rest and the
235 stress condition can be found during the upstroke (around 90° of the phase frequency) and during the down
236 stroke (around 260°) (Fig 4), confirming the optical impression from the Canolty maps (supplementary
237 table 1). Furthermore, only the down stroke of the 8Hz phase frequency reveals strong coupling coefficients
238 with gamma and high gamma EEG bands. The coefficient of correlation (Rho) between the EEG derived
239 data (Coupling coefficients of the Canolty map) and the horse grimace scale is -0.86 ($p=0.00031$) for the
240 down stroke of the phase frequency (here at 290°) and 0.71 ($p=0.01$) for the up stroke of the phase
241 frequency. The quality of raw data is good, the presence of nested activity (faster frequencies on top of slow
242 frequencies) was confirmed with a wavelet analysis (Fig 5 A,B).

243 Discussion

244 Why assess welfare in horses? The horse is both companion as well as working animal (Hausberger et al.,
245 2019). Facial expressions associated with pain and stress are well described (for example Dalla Costa et al.,
246 2014) and relatively easy to assess for a trained observer. Horses raise several issues of animal welfare
247 status, as, for example, regarding training methods, sports, as working animals and even as companions
248 (boredom) (Hausberger et al., 2019). To judge about the validity and utility of EEG measurements in the
249 context of animal welfare, horses are perfectly suited because they are used to handling procedures (which
250 reduces the impact of the EEG application procedure itself on the subjects' behavior) and their facial
251 expressions are well defined by the HGS, which we used as comparative value.

252 As has been proposed earlier (Klemm, 1992), we were able to extract differences in EEG network
253 activity during stress and rest in horses, mental states that are obviously characterized by significant
254 changes in HGS. In order to validate the behavioral states "stress" and "rest" in horses, we used the horse
255 grimace scale (Dalla Costa et al., 2014, 2018). Phase amplitude coupling seems to be an extremely robust
256 tool to extract activity patterns in the brain, associated with distinct behavioral states to assess animal
257 welfare. One reason for the robustness might be that phase amplitude coupling is extracting information
258 that is inherently linked to intrinsic neural network phenomena. The measurement does not rely on
259 absolute values, which may be influenced by technical or intra-individual issues, but on a relational
260 modulation index. Furthermore, phase related amplitude modulations seem to be an ubiquitous
261 phenomenon for neural networks, as they are also involved in the generation of peristaltic movements of
262 the intestinal tract (Huizinga et al., 2015). In fact, phase amplitude coupling in the intestinal tract is also
263 associated with the regulation of peristaltic movements according to incoming stimuli (for example food
264 intake). Further studies with a higher number of animals and more electrode positions may be beneficial
265 to confirm our results and to gain further insights regarding anatomical correlations of certain behavioral
266 representations in the EEG. Here, we used one electrode in a parietal position. This position is near to the

267 somatosensory cortex, a well characterized cortical region which is responsible for the representation of
268 one's own body. Other electrode positions may give different results, as, for example, frontal electrode
269 locations and should be addressed in subsequent studies.

270 Our results indicate a change of network activity during stress in the region of the somatosensory cortex.
271 The progressive decay of coupling strength between the rest and the stress condition, with a maximum at
272 half way of the down stroke (260°, figure 4), rather than an abrupt change, may be due to the general
273 wave characteristics of envelope-signals, which are recorded from bigger neural networks. We can only
274 speculate that the underlying entrainment of smaller sub-networks may work cascaded to form the
275 progressive decay. A combination with non-invasive imaging techniques, as, for example, MRI or fMRI
276 would be interesting to gain further insights regarding the location and regional dynamics of network
277 entrainment. However, the technique is extremely challenging for behaving horses.

278 It can be excluded that physical pain is the main driver for the change of neural network activity because
279 we took all stress recordings in the anticipation state, before any kind of physical pain or sedation
280 appeared. The representation may look different in other brain regions. The mere touching or handling of
281 the horse or the presence of people can be excluded as influencing factors, because these factors appeared
282 in both conditions. Since the brain is more or less a black box in the case of non-invasive EEG
283 measurements, it is very difficult or maybe impossible to reason about the origin of the coupling pattern
284 on the cellular level with our method. The strong kind of stress reaction, which is probably associated
285 with a medical treatment, may be relatively conserved among individuals. This may be different for minor
286 forms of stress as, for example, during training, handling or social interaction. In these cases, we would
287 expect a high intra-individual difference. To understand the change of phase amplitude coupling in
288 relation to behavior in a better way, much more data are needed with different studies, different animals
289 and different behavioral contexts.

290

291 Facial expression can hardly be used to recognize welfare in species like birds, reptiles etc. with poor
292 facial expression. If it is possible to establish reliable EEG patterns associated with stress for different
293 species in future studies, a translational approach for species with poor facial expression might be
294 possible. It must be kept in mind that the activity of the brain is highly dynamic, also known as neural
295 plasticity. The context can change the activity of the brain. Every measurement of the EEG can also
296 potentially influence the content of the EEG – some kind of uncertainty relation. Telemetric EEG
297 recordings are extremely useful in this context, because they do not restrict the freedom of movement of
298 the animals. In this context, it must also be discussed whether the location (home stall during the rest
299 condition versus treatment location during the stress condition) had an impact on the EEG. This
300 possibility cannot be fully excluded. But, the home stall and the examination stand are located in the same

301 building; furthermore, both locations are familiar to the horses. Of course, the examination stand might
302 generally be associated with veterinary interventions for these horses because they are routinely used to
303 train veterinary students for several diagnostic techniques. Therefore, the change of PAC patterns cannot
304 be triggered by novelty (here: a novel environment) but the stress factor may arise indirectly from the
305 location, which is associated with stress rather than directly due to the veterinary treatment itself.

306

307 Since we did not use “experimental” horses exclusively for our study but demonstration horses of the
308 university that were used for teaching purposes in a hands-on training for veterinary students, we were not
309 able to select the horses in an optimal way for the purpose of the study. The number of training sessions
310 was limited to six veterinary interventions at six different days with three different horses. It would be
311 important to repeat this study with more horses and more observations.

312

313 Another important factor is the miniaturization of EEG amplifiers as well as comfortable electrodes that
314 are as small as possible. For our future studies with a higher number of electrodes, we developed light
315 curing polymer electrodes (de Camp et al., 2018). Furthermore, in a current project, the amplifier with 8
316 Channels will be miniaturized to 9x12mm. This EEG system will be potentially useful to assess EEG
317 measurements in small species like birds or rodents. Another system is considered as a stackable (bus-)
318 system, to include other bio-signals as for example ECG or breathing. Welfare monitoring may gain
319 robustness by integrating multi-modal data.

320

321 **Conclusions**

322 We hypothesized that the HGS as well as the modulation index (phase amplitude coupling, PAC) derived
323 from EEG data are significantly different in the horses in accordance to different behavioral conditions and
324 second, that there is an association between HGS and PAC, which means the EEG could be an objective
325 tool for the assessment of animal welfare.

326 In conclusion, we were able to find an association between the scientifically validated horse grimace scale
327 and an EEG pattern, associated with two distinct behavioral states, namely stress and rest in horses. Phase
328 amplitude coupling might be a robust tool for the objective assessment of animal welfare and well-being of
329 animals. Furthermore, it may be useful to judge about brain states as well as comfort of neonates or disabled
330 persons, who are unable to communicate actively.

331 Our pilot study gives preliminary evidence that EEG measurements can be an objective tool for the
332 assessment of animal welfare and stress.

333

334

335 Acknowledgements

336

337 We would like to thank Prof. Heidrun Gehlen, PD Dr. Dr. Ann Kristin Barton and Sabita Stöckle

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435

436 **Figure legends**

437 **Fig 1. Horse in examination stand.** The telemetry unit is fixed at the shoulder with a piece of tape. As an
438 example, typical facial expressions in this picture are: Ears oriented backwards (score 2), closed eyes
439 (here 0), tension above eyes (score 1), tension in the region around jaw muscles (score 1), tension around
440 muzzle and prominent chin (score 1), tension around nozzles, flattened profile (score 2). The sum of all
441 facial expression scores is 7 for this image.

442 **Fig 2. Electrode positions.** The ground and reference electrode were placed above the nose (2,3), the
443 recording electrode was placed in a parietal position between the right eye and ear (1).

444

445 **Fig 3. Canolty maps for rest EEG and stress EEG.** Phase related amplitude modulation is shown as
446 heat map. The low frequency for both behavioral conditions is 8 Hz (indicated as white sine wave in
447 subplot a). Maximal amplitude modulation is visible during the up- and down stroke of the low frequency
448 in the gamma and high gamma band with a peak at 130 Hz during rest (subplot a). In the stress condition
449 (subplot b) the coupling pattern is quantitatively weaker, additionally the phase relation is changed.
450 Amplitude modulation is maximal during the down stroke, the upstroke is only weakly associated with
451 amplitude modulation in contrast to the resting condition (subplot a). Maximal modulation index values
452 are again visible around 130 ° in the high gamma range.

453 **Fig 4. Number of statistically significant differences of phase related amplitude modulation between**
454 **rest and stress.** Most differences of the EEG derived modulation index between behavioral states can be
455 found for the upstroke of the phase frequency around 60°. A minor fraction of significant differences is
456 visible during the down stroke around 210°.

457 **Fig 5. EEG raw data trace with nested activity of multiple bands.** One second of original EEG
458 recording is shown as raw data trace (upper panel) and wavelet analysis (lower panel). High power is

459 coded as warm color (red). The wavelet analysis reveals nested activity in the alpha, beta and gamma
460 band of the EEG.
461

Figure 1

Figure 1 Horse in examination stand.

The telemetry unit is fixed at the shoulder with a piece of tape. As an example, typical facial expressions in this picture are: Ears oriented backwards (score 2), closed eyes (here 0), tension above eyes (score 1), tension in the region around jaw muscles (score 1), tension around muzzle and prominent chin (score 1), tension around nozzles, flattened profile (score 2). The sum of all facial expression scores is 7 for this image.



Figure 2

Figure 2 Electrode positions.

The ground and reference electrode were placed above the nose (2,3), the recording electrode was placed in a parietal position between the right eye and ear (1).



Figure 3

Figure 3 Canolty maps for rest EEG and stress EEG.

Phase related amplitude modulation is shown as heat map. The low frequency for both behavioral conditions is 8 Hz (indicated as white sine wave in subplot a). Maximal amplitude modulation is visible during the up- and down stroke of the low frequency in the gamma and high gamma band with a peak at 130 Hz during rest (subplot a). In the stress condition (subplot b) the coupling pattern is quantitatively weaker, additionally the phase relation is changed. Amplitude modulation is maximal during the down stroke, the upstroke is only weakly associated with amplitude modulation in contrast to the resting condition (subplot a). Maximal modulation index values are again visible around 130 ° in the high gamma range.

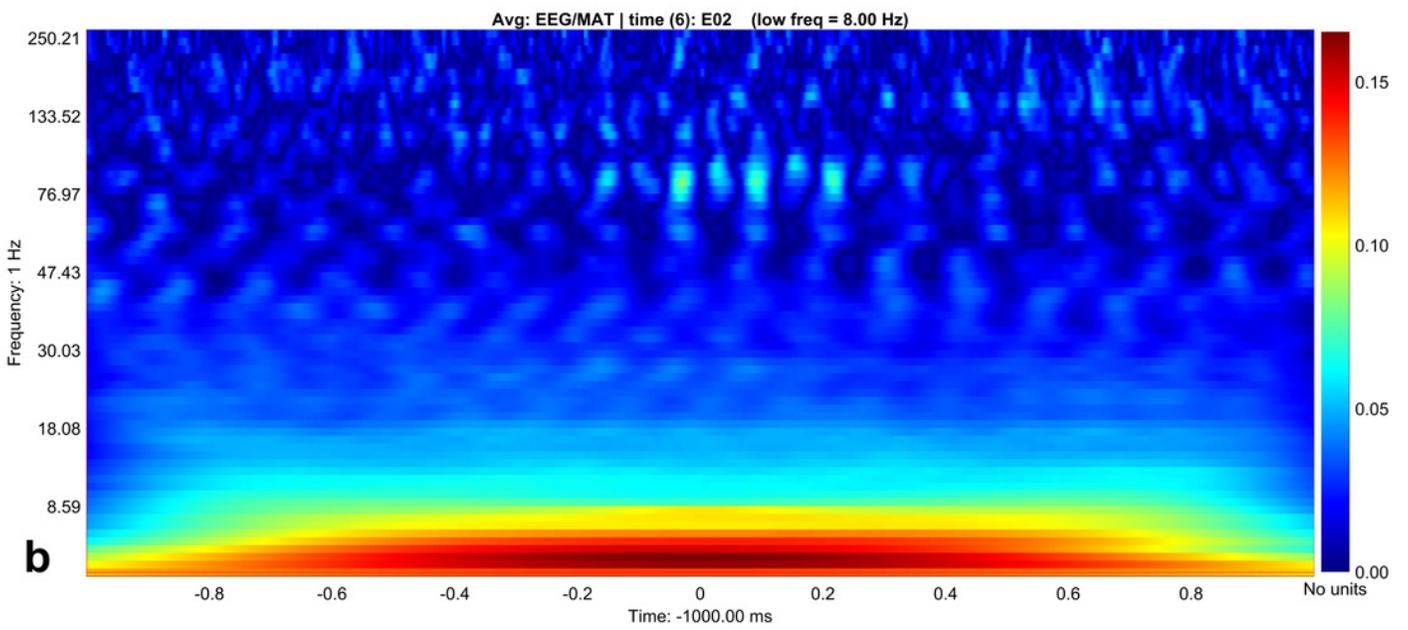
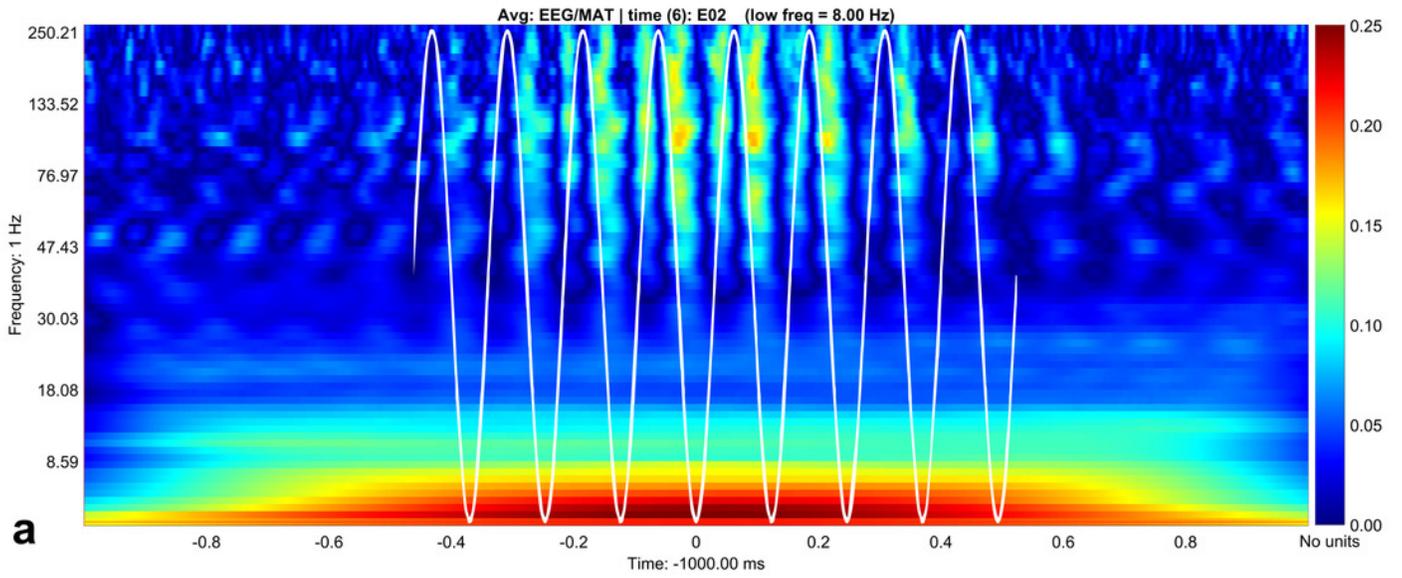


Figure 4

Fig 4. Number of statistically significant differences of phase related amplitude modulation between rest and stress.

Most differences of the EEG derived modulation index between behavioral states can be found for the upstroke of the phase frequency around 60° . A minor fraction of significant differences is visible during the down stroke around 210° .

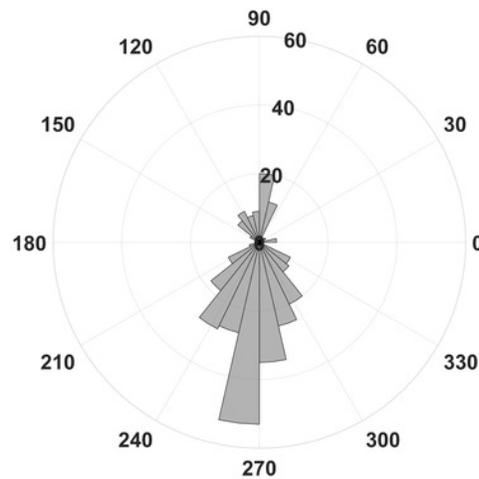


Figure 5

Fig 5. EEG raw data trace with nested activity of multiple bands.

One second of original EEG recording is shown as raw data trace (upper panel) and wavelet analysis (lower panel). High power is coded as warm color (red). The wavelet analysis reveals nested activity in the alpha, beta and gamma band of the EEG.

