

# Preparation and in vitro release kinetics of ivermectin sustained-release bolus optimized by response surface methodology

Xiangchun Ruan<sup>1,2</sup>, Xiuge Gao<sup>1</sup>, Ying Gao<sup>1</sup>, Lin Peng<sup>1</sup>, Hui Ji<sup>1</sup>, Dawei Guo<sup>1</sup> and Shanxiang Jiang<sup>1</sup>

<sup>1</sup> College of Veterinary Medicine, Nanjing Agricultural University, Nanjing, Jiangsu, China

<sup>2</sup> College of Animal Science and Technology, Anhui Agricultural University, Hefei, Anhui, China

## ABSTRACT

Sustained-release formulations of ivermectin (IVM) are useful for controlling parasitic diseases in animals. In this work, an IVM bolus made from microcrystalline cellulose (MCC), starch and low-substituted hydroxypropyl cellulose (LS-HPC) was optimized by response surface methodology. The bolus was dissolved in a cup containing 900 mL of dissolution medium at 39.5 °C, under with stirring at 100 rpm. A quadratic model was formulated using analysis of variance according to the dissolution time. The optimized formulation of the bolus contained 8% MCC, 0.5% starch, and 0.25% LS-HPC. The length, width, and height of the prepared IVM bolus were  $28.12 \pm 0.14$ ,  $16.1 \pm 0.13$ , and  $13.03 \pm 0.05$  mm, respectively. The bolus weighed  $11.4842 \pm 0.1675$  g (with a density of  $1.95 \text{ g/cm}^3$ ) and contained  $458.26 \pm 6.68$  mg of IVM. It exhibited in vitro sustained-release for over 60 days, with a cumulative amount and percentage of released IVM of  $423.72 \pm 5.48$  mg and  $92.52 \pm 1.20\%$ , respectively. The Korsmeyer–Peppas model provided the best fit to the dissolution release kinetics, exhibiting an  $R^2$  value close to 1 and the lowest Akaike Information Criterion among different models. The parameter  $n$  (0.5180) of the Korsmeyer–Peppas model was between 0.45 and 0.89. It was demonstrated that the release mechanism of the IVM bolus followed a diffusive erosion style.

Submitted 26 March 2018

Accepted 21 July 2018

Published 31 July 2018

Corresponding author  
Shanxiang Jiang, navy@sina.com

Academic editor  
Joao Rocha

Additional Information and  
Declarations can be found on  
page 10

DOI 10.7717/peerj.5418

© Copyright  
2018 Ruan et al.

Distributed under  
Creative Commons CC-BY 4.0

OPEN ACCESS

**Subjects** Veterinary Medicine, Pharmacology

**Keywords** Ivermectin, Bolus, Dissolution kinetic model, Korsmeyer–Peppas, Sustained-release

## INTRODUCTION

In vitro drug release from a dosage form is a valuable tool in the development of new pharmaceutical formulations. Ivermectin (IVM), an antiparasitic macrolide, is widely used in cattle, sheep, pigs, and other animals. Long-acting or sustained-release formulations of IVM have been authorized for its use in animals in several countries (*Martinez, Lindquist & Modric, 2010*). IVM can be incorporated into a soluble silicate glass ingredient to form a sustained-release bolus. The release profile of the bolus affects the bioavailability and clinical effects of the active ingredient. Therefore, the evaluation of the bolus release profile is an important step in the development of new IVM formulations.

Soluble glasses are biomaterials with good biocompatibility, widely used in cosmetic (*Shimono et al., 1998*) and biomedical (*Alekseeva et al., 2012; Bitar et al., 2005*) industries. Once implanted in the body, some soluble silicate glasses can bond to bone and muscles, and this behavior is referred to as bioactivity and good biocompatibility (*Hench, 1998; Hench & Polak, 2002*). Soluble silicate glass (one component of the bolus) is a biomaterial with good biocompatibility, and is not toxic to animals. It has a porous structure on the surface, so it can readily attach to the gastrointestinal tract to reduce the irritation by parasites. Thus, soluble silicate glass within a bolus given by oral administration appears to be a useful approach. The first bioactive glass was developed by Larry Hench at the University of Florida in 1969 (*Hench, 2006*). A bolus formulated with soluble glass containing trace elements was used for dietary supplementation in animals by Allen and colleagues (*Allen et al., 1979*). The tissue-regeneration ability of bioactive glasses has also been demonstrated (*Hench, 1998; Hench & Polak, 2002*). Soluble silicate glass within a bolus given by oral administration to animals was released and attached to gastrointestinal tissue. It was adapted to the physiological environment and should provide long-lasting repair. So, it could aid healing of gut damage caused by parasites. Although boluses formulated with metallic or plastic shells (*Anderson et al., 1980; Jones & Bliss, 1983*) can remain in the animal body after long-term use, the IVM bolus formulated with soluble glass can be readily absorbed or excreted, reducing potential risks to animals.

Response surface methodology (RSM) is a set of statistical and mathematical techniques frequently applied in nanotechnology, chemistry, and medicine (*Asfaram et al., 2015; Belwal et al., 2016; Dharma et al., 2016; Maran et al., 2017; Oliveira et al., 2016*) to build a model for the optimization of variable parameters in systems involving complex interactions (*Homayoonfal, Khodaiyan & Mousavi, 2015*). The modeling process involves some runs to optimize the individual parameters using the Box–Behnken design. Generally, analysis of variance (ANOVA) is performed for testing the statistical accuracy of a quadratic polynomial fitted to the experimental data. The quadratic regression model provides the coefficient of determination ( $R^2$ ) for the response values, which can then be attributed to the identified independent variables. A non-significant lack-of-fit for all variables indicates that the polynomial model provides a statistically accurate representation of the responses. In addition, larger  $F$  and smaller  $p$  values also denote a more accurate regression model.

In this study, an IVM sustained-release bolus was prepared and optimized by RSM. The release kinetics of the IVM bolus was studied by in vitro dissolution tests (*Chen et al., 2018; Wang et al., 2018*), whereas the release patterns of the bolus were analyzed by model fitting of the in vitro release data (*Feng, Li & Tan, 2017; Ramteke et al., 2014*).

## MATERIALS AND METHODS

### Materials

Ivermectin was purchased from Shandong Qifa Pharmaceutical Co., Ltd (Jinan, China). Soluble silicate glass ( $\text{SiO}_2:\text{Na}_2\text{O}$ , 3.4:1 m/m) was prepared in the Laboratory of Veterinary Pharmacology and Toxicology, Nanjing Agricultural University (Nanjing, China). Microcrystalline cellulose (MCC), starch, and low-substituted hydroxypropyl cellulose

**Table 1** Disintegration time measured in Box–Behnken design runs.

Std	Run	MCC (%)	Starch (%)	LS-HPC (%)	Disintegration time (d)
14	1	9	0.5	0.38	15
2	2	10	0.3	0.38	3
10	3	9	0.7	0.25	50
1	4	8	0.3	0.38	7
11	5	9	0.3	0.5	5
6	6	10	0.5	0.25	35
4	7	10	0.7	0.38	14
5	8	8	0.5	0.25	65
8	9	10	0.5	0.5	16
3	10	8	0.7	0.38	6
12	11	9	0.7	0.5	7
7	12	8	0.5	0.5	10
13	13	9	0.5	0.38	12
15	14	9	0.5	0.38	13
9	15	9	0.3	0.25	35

(LS-HPC) were kindly provided by Anhui Sunhere Pharmaceutical Excipients Co., Ltd (Hefei, China). We employed a mechanical pill press (AMHL-60) produced by Changzhou Aomuhalei Machinery Co., Ltd (Jintan, China) and a dissolution apparatus (SY-6D) obtained from Huanghai Drug Test Instruments Co., Ltd (Shanghai, China).

## Methods

### *Optimization of bolus formulation*

The MCC, starch, and LS-HPC levels were the factors varied in the RSM analysis. The MCC levels considered were 8% and 10%, together with starch levels of 0.3% and 0.7%, and LS-HPC levels of 0.25% and 0.5%. The effects of these factors were tested by Box–Behnken design using Design Expert 8.0 (Stat-Ease, Inc., Minneapolis, MN, USA), as shown in [Table 1](#). We prepared a mixture containing barium sulfate and soluble silicate glass (2:1, w/w), which were granulated and passed through a 12-mesh sieve after adding an appropriate amount of water to wet. Then, the particles were dried at 60 °C for 30 min, and further passed through a 14-mesh sieve after size stabilization. The bolus was compressed by applying a pressure of 750 kg/cm<sup>2</sup> using the mechanical pill press, and then dissolved in a cup containing 900 mL dissolution medium at 39.5 °C under stirring at 100 rpm. The dissolution medium was prepared as described by Menke ([Menke & Steingass, 1988](#)), except that sheep rumen fluid was not added. The bolus formulation was optimized according to the dissolution time. According the above optimized formulation, an appropriate amount of IVM was added to a 12.6 g blank bolus. Then, the IVM-containing bolus was prepared using the method described above. The length, width, and height of the prepared IVM bolus were 28.12 ± 0.14, 16.1 ± 0.13, and 13.03 ± 0.05 mm, respectively. The bolus weighed 11.4842 ± 0.1675 g, contained 458.26 ± 6.68 mg of IVM, and its density was 1.95 g/cm<sup>3</sup>.

### ***In vitro* release kinetics of IVM bolus**

Six IVM boluses used as parallel samples ( $n = 6$ ) were dissolved using the United States Pharmacopoeia apparatus II at 100 rpm, maintaining the temperature of the dissolution medium at 39.5 °C. The dissolution medium consisted of 900 mL of artificial rumen fluid containing 4.5 g of sodium dodecyl sulfate (Ding et al., 2015). The preparation method of the artificial rumen fluid was according to Menke & Steingass (1988) and was slightly modified. Briefly, A solution: 13.2 g of calcium chloride dihydrate, 10.0 g of manganese chloride tetrahydrate, 1.0 g of cobalt chloride hexahydrate, and 8.0 g of ferrous chloride hexahydrate were dissolved in 100 mL of distilled water. B solution: 35.0 g of sodium bicarbonate and 4.0 g of ammonium bicarbonate were dissolved in 1,000 mL of distilled water. C solution: 5.7 g of sodium dihydrogen phosphate, 6.2 g of potassium dihydrogen phosphate, and 0.6 g of magnesium sulfate heptahydrate were dissolved in 1,000 mL of distilled water. The reducing solution consisted of 95 mL of distilled water, four mL of one M sodium hydroxide, and 625 mg of sodium sulfide 9-hydrate. A total of 400 mL of distilled water, 0.1 mL of A solution, 200 mL of B solution, 200 mL of C solution, and 40 mL of reducing solution were sequentially added to form the artificial rumen fluid. The samples were collected every day until the end of the experiment, whereas the dissolution medium was changed every day. The samples were analyzed using a well-established method (Alvinerie et al., 1999) with slight modifications. Briefly, 0.5 mL of the deliquated dissolution medium was mixed with one mL of ethyl acetate for 3 min. Then, the solvent-sample mixture was centrifuged at  $13,225 \times g$  for 10 min. The supernatant was transferred to a tube and the extraction was repeated once. The combined supernatants were dried under a stream of nitrogen (Anpel Laboratory Technologies, Shanghai, China), and then re-suspended in 100  $\mu$ L of a solution of *N*-methylimidazole (Aladdin, Los Angeles, CA, USA) in acetonitrile (1:1,  $v/v$ ) (De Montigny, Shim & Pivnichny, 1990). Derivatization was initiated by addition of 150  $\mu$ L of trifluoroacetic anhydride solution (Aladdin) in acetonitrile (1:2,  $v/v$ ). After reacting for 30 min, the solution was centrifuged at  $13,225 \times g$  for 10 min at  $-4$  °C. Finally, an aliquot (20  $\mu$ L) of this solution was injected directly into a High performance liquid chromatography (HPLC) system (Waters, Milford, MA, USA). HPLC analyses were carried out using a reverse-phase Eclipse XDB-C18 column ( $\Phi = 5$   $\mu$ m,  $4.6 \times 250$  mm) and a water/methanol (3:97,  $v/v$ ) mobile phase at a flow rate of 1.0 mL/min, at a temperature of 40 °C. IVM release was monitored with a spectrofluorometric detector (Waters 2475; Waters, Milford, MA, USA) at excitation and emission wavelengths of 365 and 475 nm, respectively. The cumulative amount and percentage of released IVM were determined according to the corresponding in vitro release data.

### ***Statistical analysis***

The release pattern of the IVM bolus was analyzed using several standard kinetic models including zero order, first order, Korsmeyer–Peppas, Higuchi, Hixson–Crowell, and Weibull models (Feng, Li & Tan, 2017; Ramteke et al., 2014). The in vitro release data obtained from the dissolution medium were fitted to the above kinetic models using the respective formulas, and the corresponding dissolution kinetic curves were constructed. The best fitting model was identified according to two statistical parameters, the regression

**Table 2** ANOVA for response surface quadratic model of disintegration time data.

Source	Sum of squares	df	Mean square	F value	p-value	prob > F
Model	4,600.82	9	511.2	23.47	0.0014	Significant
A-MCC	50	1	50	2.3	0.1902	
B-Starch	91.12	1	91.12	4.18	0.0962	
C-LS-HPC	2,701.12	1	2,701.12	124	0.0001	
AB	36	1	36	1.65	0.2549	
AC	324	1	324	14.87	0.0119	
BC	42.25	1	42.25	1.94	0.2225	
A2	1.85	1	1.85	0.085	0.7823	
B2	158.01	1	158.01	7.25	0.0431	
C2	1,125.39	1	1,125.39	51.66	0.0008	
Residual	108.92	5	21.78			
Lack of fit	104.25	3	34.75	14.89	0.0636	Not significant
Pure error	4.67	2	2.33			
Cor total	4,709.73	14				

coefficient ( $R^2$ ) and the Akaike Information Criterion (AIC). In particular, after comparing the  $R^2$  and AIC values obtained for the different kinetic models, it was found that the best model of the dissolution kinetics exhibited  $R^2$  values near to 1 and the lowest AIC value. Statistical analyses were performed using Microsoft Office Excel® (Microsoft Corporation, Redmond, WA, USA) and Origin 9.1 (OriginLab, Hampton, MA, USA).

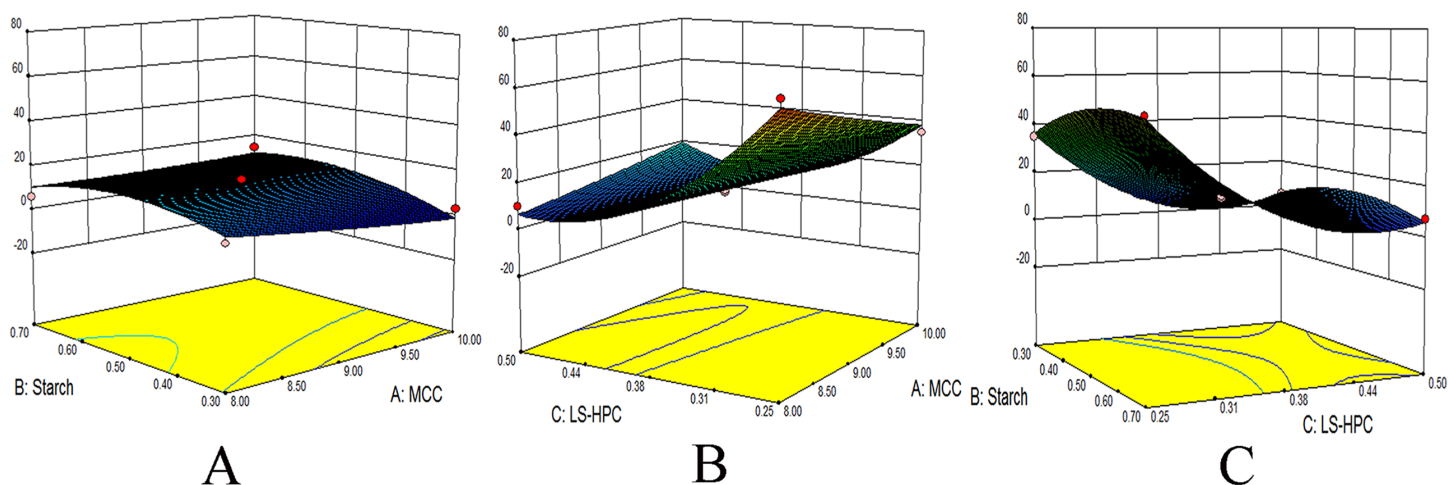
## RESULTS

### Formulation optimization

Different MCC, starch, and LS-HPC contents resulted in different dissolution times of the corresponding boluses (Table 1). The longest and shortest dissolution times were 65 and 3 days, respectively. ANOVA was used to assess the adequacy of a quadratic model selected to represent the experimental data (Table 2). LS-HPC and starch were found to have extremely significant ( $p < 0.01$ ) and significant ( $p < 0.05$ ) effects on the bolus dissolution time, respectively. The interactions between two of the three independent variables (MCC, starch, and LS-HPC levels) were analyzed using 3D contour plots (Fig. 1). The optimized bolus formulation contained 8% MCC, 0.5% starch, and 0.25% LS-HPC.

### In Vitro release kinetics of IVM Bolus

The 15 tests with different compositions were optimized by Box–Behnken design for the formulation of IVM bolus. The optimized bolus formulation contained 8% MCC, 0.5% starch, and 0.25% LS-HPC. IVM boluses optimized with RSM were studied by in vitro release kinetics. Six IVM boluses (six replicates) were dissolved in the dissolution medium. Almost all IVM boluses showed cracks. Only the size of the crack might be a little different. Shown in Fig. 2B was one of the six cracking boluses after 4 h immersion in the



**Figure 1** 3D contour surfaces of bolus disintegration time. Effect of MCC-starch (A), MCC-LS-HPC (B), and starch-LS-HPC (C) interactions on disintegration time. [Full-size](#) DOI: 10.7717/peerj.5418/fig-1

dissolution medium. The appearance of cracks in the dissolution medium of IVM bolus was primarily the result of the action of disintegrating agents. However, the bolus maintained a compact shape, and its content was released through the cracks. The bolus exhibited sustained IVM release for more than 60 days (Fig. 2).

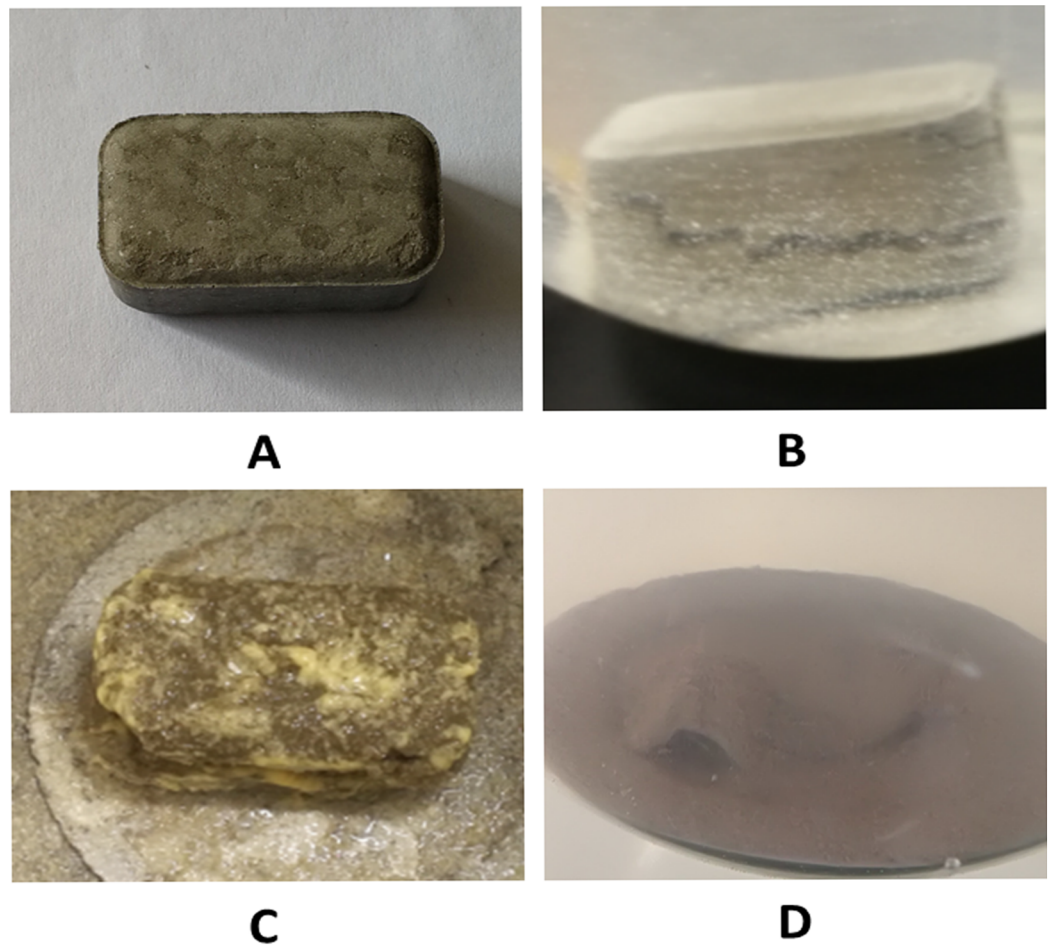
A significant burst effect was observed, with  $48.37 \pm 3.04$  mg IVM released in the first day, followed by a slower release. A sustained-release of two to eight mg IVM/day occurred from day 7 to day 53. The released amount of IVM increased to ten to twelve mg/day from day 54 to day 57, and then declined until the release was completed (Fig. 3A). The total released amount of IVM was  $423.72 \pm 5.48$  mg, corresponding to  $92.52 \pm 1.20\%$  of the initial content (Fig. 3B).

### Statistical analysis

Different dissolution kinetic models were applied to fit the dissolution data (Fig. 4), the calculated  $R^2$  and AIC parameters corresponding to each model are shown in Table 3. We found that the Weibull model failed to fit the data, whereas a satisfactory goodness of fit was obtained for the Korsmeyer–Peppas model. In particular, this model provided the best fit to the dissolution kinetic data, as it produced an  $R^2$  value close to 1 and the lowest AIC among the tested models (Table 3). Moreover, the  $n$  parameter (0.5180) of the Korsmeyer–Peppas model was between 0.45 and 0.89. These results thus demonstrate that the release of IVM occurs through a diffusive erosion mechanism (Korsmeyer et al., 2012).

## DISCUSSION

Silicate soluble glass (one component of the bolus) is a biomaterial with good biocompatibility, is not harmful to animals over the long term (Njanja, Bell & Westcott, 1998). Glass particles within the bolus formulation disintegrate, but some of the particles are resorbed in the body right up to complete degradation, and some of particles are not

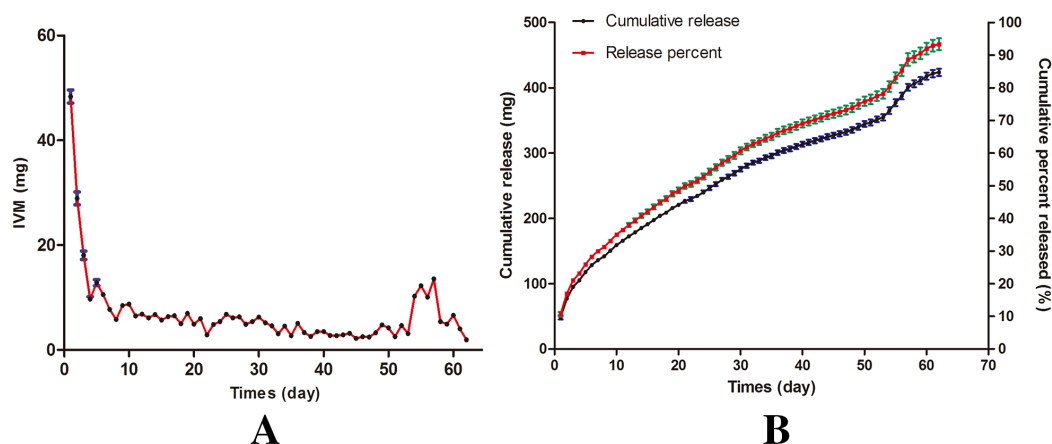


**Figure 2** The appearance changes of IVM bolus during in vitro release tests. (A) IVM bolus formulation. (B) A small crack appeared after IVM bolus release in the dissolution medium at 4 h. (C) IVM bolus was placed in the dissolution medium for 30 days. A minor portion (edges and corners) of the IVM bolus fell off and dissolved, but its shape was basically intact. (D) A small part of the shell of IVM bolus was left in the dissolution medium at 60 days (Photo credit: Xiang Chun Ruan).

Full-size  DOI: [10.7717/peerj.5418/fig-2](https://doi.org/10.7717/peerj.5418/fig-2)

resorbed in time and can be excreted with feces (Hench, 2006). Silicate glass within a bolus given by oral administration appears to be a safe method.

The size, shape, and density of ruminant bolus have been investigated by Telfer and Cardinal (Cardinal, 1985; Telfer, 1984). The size and the shape of the bolus changes according to the ruminant animal. However, the bolus density is the most important factor determining its transit time in rumen. Owing to its high density, barium sulfate is used as barium meal for X-ray detection. It has been reported that the sustained-release bolus can contain up to 70–80% barium sulfate (Wood, Toothill & Dietz, 1994). Therefore, barium sulfate was used in this work to regulate the density of the IVM bolus. The density of deworming tablets was reported to be approximately  $3.0 \text{ g/cm}^3$  (Marsten, 1962), whereas the density of formulations developed for captive ruminants was lower,  $1.8 \text{ g/cm}^3$  (Vandamme & Ellis, 2004). Therefore, the density of the IVM bolus ( $1.95 \text{ g/cm}^3$ ) appears suitable to remain in rumen for an appropriate period of time.



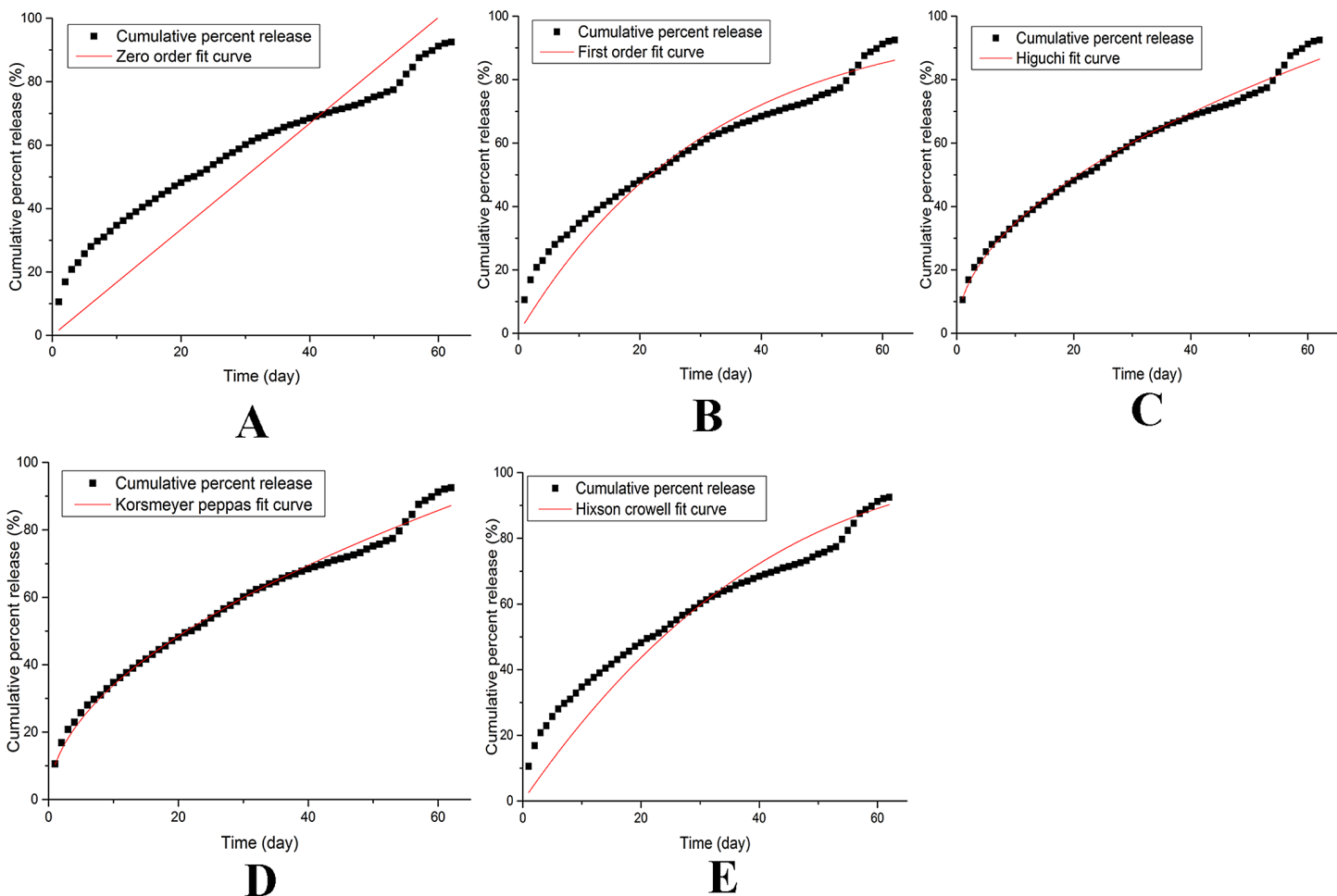
**Figure 3** In vitro release kinetics of IVM bolus. (A) IVM released in vitro. (B) Cumulative and percent release of IVM. [Full-size !\[\]\(5fd6ef84f97f42d7f8b34275f1b65312\_img.jpg\) DOI: 10.7717/peerj.5418/fig-3](https://doi.org/10.7717/peerj.5418/fig-3)

Ivermectin bolus cracked in the dissolution medium and released after 10 days. The dissolved components of the IVM bolus remained relatively constant. It maintained a relatively stable release. The flatter portion of the curve is shown between 10 and 53 days. Although in vivo pharmacokinetic studies have not been conducted, the release levels of IVM bolus from 10 to 60+ days are likely to be biologically active. Therefore, we assume that IVM bolus could maintain to be in bioactive amounts over 60 days. After a relatively stable release of the IVM bolus, the dissolution of IVM is accelerated and the amount of IVM release increases due to the final disintegration of the bolus. The peak in the release curve was at 50–60 days. The small external shell remained at 60 days. IVM release was decreased until it was not being detected after 62 days.

The cracks in the IVM bolus were the result of the action of the disintegrants (starch and LS-HPC). The IVM was released through the crack and mainly released in a diffusion style at an initial stage. Afterwards, it might be dominated in an erosion mode and achieve a relatively stable release. The presence of gaps determines the release kinetics of IVM bolus. Different disintegrants, such as sodium carboxymethyl cellulose and sodium carboxymethyl starch, have different effects on the release kinetics of IVM bolus.

The present bolus exhibited sustained IVM release for more than 60 days in vitro, with a cumulative percentage of released IVM higher than 90%. About 10% of the IVM content ( $48.37 \pm 3.04$  mg) was released in the first day, which is ten times higher the IVM therapeutic dosage for a sheep of 25 kg body weight. Extended parasite exposure of IVM may improve its efficacy against anthelmintic-resistant parasites (Alvarez et al., 2015). Parasitological data tend to demonstrate that the oral route is more effective against intestinal nematodes (Mckellar & Benchaoui, 1996). Significantly higher IVM concentrations in abomasal content have been measured after intraruminal treatment compared with subcutaneous injection in sheep (Lloberas et al., 2012). However, IVM injection via the subcutaneous route has been shown to elicit transient pain in goats (Njanja, Bell & Westcott, 1985), so oral administration of IVM would be more appropriate. In cattle or goat industries, long-acting products are used widely because they: (i) can treat





**Figure 4** Models of release kinetics of IVM bolus in dissolution medium. (A) Zero-order. (B) First-order. (C) Higuchi. (D) Korsmeyer–Peppas. (E) Hixson–Crowell.

Full-size [DOI: 10.7717/peerj.5418/fig-4](https://doi.org/10.7717/peerj.5418/fig-4)

**Table 3** Dissolution kinetic model fitting parameters.

Model	Equation	Parameters	R	AIC
Zero order	$y = k \times x$	1.6709	0.6653	563.54
First order	$y = 100 \times [1 - \exp(-k \times x)]$	0.0319	0.9360	460.94
Higuchi	$y = k \times x^{0.5}$	10.9806	0.9885	356.53
Korsmeyer–Peppas	$y = k \times x^n$	10.2859, 0.5180	0.9891	352.47
Hixson–Crowell	$y = 100[1 - (1 - k \times x)^3]$	0.0087	0.8969	490.52
Weibull	$y = 100 \times \{1 - \exp[-(x)^{b/a}]\}$	Failed	Failed	Failed

existing infections by parasitic nematodes and prevent new infections; (ii) need substantially fewer resources to treat animals due to the reduced frequency of administration, livestock handling, and restraint (labor and equipment) (*Forbes, 2013*). Hence, the novel bolus is possible to become a drug-delivery device for anthelmintic agents in cattle and goat industries.

## CONCLUSIONS

The optimized bolus formulation contained 8% MCC, 0.5% starch, and 0.25% LS-HPC, as determined by RSM. The optimized IVM bolus exhibited sustained-release for more than 60 days. The in vitro cumulative release and released percentage of IVM were  $423.72 \pm 5.48$  mg and  $92.52 \pm 1.20\%$ , respectively. The Korsmeyer–Peppas model provided the best fit to the dissolution kinetic data. The release of IVM followed a diffusive erosion mechanism. Further research is needed to investigate the correlation between the in vitro/in vivo release and the clinical treatment effects of IVM boluses.

## ACKNOWLEDGEMENTS

We would like to thank Anhui Sunhere Pharmaceutical Excipients Co., Ltd for kindly providing microcrystalline cellulose, starch and low-substituted hydroxypropyl cellulose. We also thank Changzhou Aomuhalei Machinery Co., Ltd and Hefei Kejing materials technology Co., Ltd for assistance.

## ADDITIONAL INFORMATION AND DECLARATIONS

### Funding

This work was granted support from the National Key Research and Development Program of China (2016YFD0501306). The funders had no role in study design, data collection and analysis, decision to publish, or preparation of the manuscript.

### Grant Disclosures

The following grant information was disclosed by the authors:

National Key Research and Development Program of China: 2016YFD0501306.

### Competing Interests

The authors declare that they have no competing interests.

### Author Contributions

- Xiangchun Ruan conceived and designed the experiments, analyzed the data, prepared figures and/or tables, authored or reviewed drafts of the paper, approved the final draft.
- Xiuge Gao performed the experiments, contributed reagents/materials/analysis tools, prepared figures and/or tables, approved the final draft.
- Ying Gao analyzed the data, approved the final draft.
- Lin Peng performed the experiments, contributed reagents/materials/analysis tools, approved the final draft.
- Hui Ji performed the experiments, contributed reagents/materials/analysis tools, approved the final draft.
- Dawei Guo performed the experiments, contributed reagents/materials/analysis tools, prepared figures and/or tables, approved the final draft.
- Shanxiang Jiang conceived and designed the experiments, approved the final draft.

## Data Availability

The following information was supplied regarding data availability:

The raw data are provided as [Supplemental Files](#).

## Supplemental Information

Supplemental information for this article can be found online at <http://dx.doi.org/10.7717/peerj.5418#supplemental-information>.

## REFERENCES

- Alekseeva T, Abou Neel EA, Knowles JC, Brown RA. 2012. Development of conical soluble phosphate glass fibers for directional tissue growth. *Journal of Biomaterials Applications* **26**(6):733–744 DOI [10.1177/0885328210394396](https://doi.org/10.1177/0885328210394396).
- Allen WM, Drake CF, Sansom BF, Taylor RJ. 1979. Trace element supplementation with soluble glasses. *Annales de Recherches Veterinaires Annals of Veterinary Research* **10**:356–358.
- Alvarez L, Suarez G, Ceballos L, Moreno L, Canton C, Lifschitz A, Mate L, Ballent M, Virkel G, Lanusse C. 2015. Integrated assessment of ivermectin pharmacokinetics, efficacy against resistant *Haemonchus contortus* and P-glycoprotein expression in lambs treated at three different dosage levels. *Veterinary Parasitology* **210**(1–2):53–63 DOI [10.1016/j.vetpar.2015.03.001](https://doi.org/10.1016/j.vetpar.2015.03.001).
- Alvinerie M, Sutra JF, Galtier P, Lifschitz A, Virkel G, Sallovitz J, Lanusse C. 1999. Persistence of ivermectin in plasma and faeces following administration of a sustained-release bolus to cattle. *Research in Veterinary Science* **66**(1):57–61 DOI [10.1053/rvsc.1998.0240](https://doi.org/10.1053/rvsc.1998.0240).
- Anderson N, Laby RH, Prichard RK, Hennessey D. 1980. Controlled release of anthelmintic drugs: a new concept for prevention of helminthosis in sheep. *Research in Veterinary Science* **29**(3):333–341.
- Asfaram A, Ghaedi M, Hajati S, Rezaeinejad M, Goudarzi A, Purkait MK. 2015. Rapid removal of Auramine-O and Methylene blue by ZnS:Cu nanoparticles loaded on activated carbon: a response surface methodology approach. *Journal of the Taiwan Institute of Chemical Engineers* **53**:80–91 DOI [10.1016/j.jtice.2015.02.026](https://doi.org/10.1016/j.jtice.2015.02.026).
- Belwal T, Dhyani P, Bhatt ID, Rawal RS, Pande V. 2016. Optimization extraction conditions for improving phenolic content and antioxidant activity in *Berberis asiatica* fruits using response surface methodology (RSM). *Food Chemistry* **207**:115–124 DOI [10.1016/j.foodchem.2016.03.081](https://doi.org/10.1016/j.foodchem.2016.03.081).
- Bitar M, Knowles JC, Lewis MP, Salih V. 2005. Soluble phosphate glass fibres for repair of bone-ligament interface. *Journal of Materials Science: Materials in Medicine* **16**(12):1131–1136 DOI [10.1007/s10856-005-4718-3](https://doi.org/10.1007/s10856-005-4718-3).
- Cardinal JR. 1985. Controlled drug delivery: veterinary applications. *Journal of Controlled Release* **2**:393–403 DOI [10.1016/0168-3659\(85\)90061-6](https://doi.org/10.1016/0168-3659(85)90061-6).
- Chen XJ, Yan J, Yu SY, Wang PP. 2018. Formulation and in vitro release kinetics of Mucoadhesive blend gels containing matrine for buccal administration. *AAPS PharmSciTech* **19**(1):470–480 DOI [10.1208/s12249-017-0853-7](https://doi.org/10.1208/s12249-017-0853-7).
- De Montigny P, Shim JSK, Pivnichny JV. 1990. Liquid chromatographic determination of ivermectin in animal plasma with trifluoroacetic anhydride and N-methylimidazole as the derivatization reagent. *Journal of Pharmaceutical and Biomedical Analysis* **8**(6):507–511 DOI [10.1016/0731-7085\(90\)80060-3](https://doi.org/10.1016/0731-7085(90)80060-3).

- Dharma S, Masjuki HH, Ong HC, Sebayang AH, Silitonga AS, Kusumo F, Mahlia TMI. 2016.** Optimization of biodiesel production process for mixed *Jatropha curcas*–*Ceiba pentandra* biodiesel using response surface methodology. *Energy Conversion and Management* **115**:178–190 DOI [10.1016/j.enconman.2016.02.034](https://doi.org/10.1016/j.enconman.2016.02.034).
- Ding D, Sheng XL, Liang KX, Xu Q, Liu W. 2015.** Study on Ivermectin Nanoemulsion for transdermal drug delivery. *China Animal Husbandry & Veterinary Medicine* **42**:401–407.
- Feng LL, Li N, Tan YJ. 2017.** Preparation process and in vitro release model of Baicalin Liposomes optimized by Box-Behnken and design. *Journal of Chinese Medicinal Materials* **40**:2905–2910.
- Forbes AB. 2013.** LongRange™ (eprinomectin 5%) extended-release injection parasiticide and the utility of extended-activity antiparasitics in cattle. *Veterinary Parasitology* **192**(4):308–312 DOI [10.1016/j.vetpar.2012.11.036](https://doi.org/10.1016/j.vetpar.2012.11.036).
- Hench LL. 1998.** Biomaterials: a forecast for the future. *Biomaterials* **19**(16):1419–1423 DOI [10.1016/s0142-9612\(98\)00133-1](https://doi.org/10.1016/s0142-9612(98)00133-1).
- Hench LL. 2006.** The story of Bioglass®. *Journal of Materials Science* **17**(11):967–978 DOI [10.1007/s10856-006-0432-z](https://doi.org/10.1007/s10856-006-0432-z).
- Hench LL, Polak JM. 2002.** Third-generation biomedical materials. *Science* **295**(5557):1014–1017 DOI [10.1126/science.1067404](https://doi.org/10.1126/science.1067404).
- Homayoonfal M, Khodaiyan F, Mousavi M. 2015.** Modelling and optimising of physicochemical features of walnut-oil beverage emulsions by implementation of response surface methodology: effect of preparation conditions on emulsion stability. *Food Chemistry* **174**:649–659 DOI [10.1016/j.foodchem.2014.10.117](https://doi.org/10.1016/j.foodchem.2014.10.117).
- Jones RM, Bliss DH. 1983.** The susceptibility of *Ostertagia* and *Cooperia* to morantel tartrate after extended exposure to the morantel sustained release bolus. *Veterinary Parasitology* **12**(3–4):329–336 DOI [10.1016/0304-4017\(83\)90039-0](https://doi.org/10.1016/0304-4017(83)90039-0).
- Korsmeyer RW, Gurny R, Doelker E, Buri P, Peppas NA. 2012.** Mechanisms of solute release from porous hydrophilic polymers. *International Journal of Pharmaceutics* **15**(1):25–35 DOI [10.1016/0378-5173\(83\)90064-9](https://doi.org/10.1016/0378-5173(83)90064-9).
- Lloberas M, Alvarez L, Entrocasso C, Virkel G, Lanusse C, Lifschitz A. 2012.** Measurement of ivermectin concentrations in target worms and host gastrointestinal tissues: influence of the route of administration on the activity against resistant *Haemonchus contortus* in lambs. *Experimental Parasitology* **131**(3):304–309 DOI [10.1016/j.exppara.2012.04.014](https://doi.org/10.1016/j.exppara.2012.04.014).
- Maran JP, Manikandan S, Nivetha CV, Dinesh R. 2017.** Ultrasound assisted extraction of bioactive compounds from *Nephelium lappaceum* L. fruit peel using central composite face centered response surface design. *Arabian Journal of Chemistry* **10**:S1145–S1157 DOI [10.1016/j.arabjc.2013.02.007](https://doi.org/10.1016/j.arabjc.2013.02.007).
- Marsten HR. 1962.** Therapeutic pellet for ruminants. *US Patent No* 3,056,724.
- Martinez MN, Lindquist D, Modric S. 2010.** Terminology challenges: defining modified release dosage forms in veterinary medicine. *Journal of Pharmaceutical Sciences* **99**(8):3281–3290 DOI [10.1002/jps.22095](https://doi.org/10.1002/jps.22095).
- Mckellar QA, Benchaoui HA. 1996.** Avermectins and milbemycins. *Journal of Veterinary Pharmacology and Therapeutics* **19**(5):331–351 DOI [10.1111/j.1365-2885.1996.tb00062.x](https://doi.org/10.1111/j.1365-2885.1996.tb00062.x).
- Menke HH, Steingass H. 1988.** Estimation of the energetic feed value obtained from chemical analysis and in vitro gas production using rumen fluid. *Animal Research and Development* **28**:7–55.
- Njanja JC, Bell JF, Westcott RB. 1985.** Apparent lack of toxicity in adult East African goats on parenterally administered ivermectin. *Bulltin of Animal Health and Production in Africa* **33**:123–127.

- Njanja JC, Bell JF, Westcott RB. 1998.** Development of soluble phosphate glasses and class-ceramics for biomedical applications. In: *The 6th International Otto Schott Colloquium, Jena, Germany*, 162–167.
- Oliveira TIS, Rosa MF, Cavalcante FL, Pereira PHF, Moates GK, Wellner N, Mazzetto SE, Waldron KW, Azeredo HMC. 2016.** Optimization of pectin extraction from banana peels with citric acid by using response surface methodology. *Food Chemistry* **198**:113–118 DOI [10.1016/j.foodchem.2015.08.080](https://doi.org/10.1016/j.foodchem.2015.08.080).
- Ramteke KH, Dighe PA, Kharat AR, Patil SV. 2014.** Mathematical models of drug dissolution: a review. *Scholars Academic Journal of Pharmacy* **3**:388–396.
- Shimono F, Yamamoto K, Onishi T, Miyoshi R. 1998.** Cosmetic products containing a soluble glass. Ishizuka Garasu Kabushiki Kaisha. Patent 5766611. Available at <http://www.freepatentsonline.com/5290544.html>.
- Telfer SB. 1984.** Controlled release glass (CRG)—its action and application in sheep. *Proceedings of the Sheep Veterinary Society* **8**:82–85.
- Vandamme TF, Ellis KJ. 2004.** Issues and challenges in developing ruminal drug delivery systems. *Advanced Drug Delivery Reviews* **56(10)**:1415–1436.
- Wang T, Wu C, Fan GJ, Li TT, Gong H, Cao FL. 2018.** Ginkgo biloba extracts-loaded starch nano-spheres: preparation, characterization, and in vitro release kinetics. *International Journal of Biological Macromolecules* **106**:148–157 DOI [10.1016/j.ijbiomac.2017.08.012](https://doi.org/10.1016/j.ijbiomac.2017.08.012).
- Wood IB, Toothill RB, Dietz JC. 1994.** Sustained release bolus effective for the prolonged prevention, treatment or control of nematode, acarid and endo- and ectoparasitic infestations of ruminants. US Patent US5322692A. Available at <https://patents.google.com/patent/US5322692>.