

## Anatomical and biomechanical traits of broiler chickens across ontogeny. Part II. Body segment inertial properties and muscle architecture of the pelvic limb

In broiler chickens, genetic success for desired production traits is often shadowed by welfare concerns related to musculoskeletal health. Whilst these concerns are clear, a viable solution is still elusive. Part of the solution lies in knowing how anatomical changes in afflicted body systems that occur across ontogeny influence standing and moving. Here, to demonstrate these changes we quantify the segment inertial properties of the whole body, trunk (legs removed) and the right pelvic limb segments of five broilers at three different age groups across development. We also consider how muscle architecture (mass, fascicle length and other properties related to mechanics) changes for selected muscles of the pelvic limb. All broilers used had no observed lameness, but we document the limb pathologies identified post mortem, since these two factors do not always correlate, as shown here. The most common leg disorders, including bacterial chondronecrosis with osteomyelitis and rotational and angular deformities of the lower limb, were observed in chickens at all developmental stages. Whole limb morphology is not uniform relative to body size, with broilers obtaining large thighs and feet between four and six weeks of age. This implies that the energetic cost of swinging the limbs is markedly increased across this growth period, perhaps contributing to reduced activity levels. Hindlimb bone length does not change during this period, which may be advantageous for increased stability despite the increased energetic costs. Increased pectoral muscle growth appears to move the centre of mass cranio-dorsally in the last two weeks of growth. This has direct consequences for locomotion (potentially greater limb muscle stresses during standing and moving). Our study is the first to measure these changes in the musculoskeletal system across growth in chickens, and reveals how artificially selected changes of the morphology of the pectoral apparatus may cause deficits in locomotion.

1 **TITLE:**

2 Anatomical and biomechanical traits of broiler chickens across ontogeny. Part II. Body segment  
3 inertial properties and muscle architecture of the pelvic limb

4  
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**INTRODUCTION:**

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The poultry industry is a rapidly expanding enterprise (over 870 million broilers slaughtered in the UK; DEFRA 2013 statistics), in which production continues to increase globally by over 130% in some countries (Scanes 2007). In addition to increased production, the broiler chicken has gained an unusual repertoire of anatomical traits, which are repeatedly emphasized in scientific studies and highlight what has developed into a successful breeding programme for obtaining desired production characteristics (e.g. Havenstein et al., 2003; Paxton et al., 2010, 2013). However, a crossroads has been reached where efficient broiler production is haunted by welfare concerns (Julian, 1998; Mench, 2004; Knowles et al., 2008). Broilers may suffer from heart failure and sudden death syndrome (Julian, 1998; Maxwell and Robertson, 1998; Olkowski et al., 2007), reduced adaptive immune function (Cheema et al., 2003), leg weakness (see review; Bradshaw et al., 2002), poor reproductive performance (Siegel and Dunnington, 1987; Hocking, 1993) and appear to be susceptible to suboptimal management of nutrition and their environment (e.g. Vestergaard and Sanotra, 1999; Kestin et al., 2001; Scott, 2002; Brickett et al., 2007; Buijs et al., 2009). Unfortunately, whilst the welfare and economic concerns associated with these issues are clear, there is no optimal evidence-based solution that resolves all concerns surrounding broiler chicken production.

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To move toward such a solution, a deeper understanding of how broiler body shape and musculoskeletal function develops during growth and how these changes may influence locomotion is required. Part 1 of this series (Tickle et al., MS) characterized how broiler organ and pectoral muscle growth varies with increasing body mass, with a focus on respiratory system development and changes in organ size, highlighting important repercussions to breathing/ cardiorespiratory performance. Here, we delve deeper into how these and other anatomical changes have affected the overall size and shape of the broiler and investigate how relevant traits have likely influenced their locomotor abilities.

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To help achieve our aim, we detail the muscle architectural properties of the major pelvic limb muscles (identified previously by Paxton et al., 2010 as the hip, knee and ankle extensors in broilers) and document how these scale with body size. Skeletal muscle is one of the organs that is most adaptable to environmental change (Lieber, 1986), and an integral component of locomotion (supporting and powering the movement). Muscle mechanical performance is mostly dependent on a few key architectural properties; namely mass, fascicle length and pennation angle. These parameters are typically used to calculate physiological cross-sectional area (PCSA)

67 and thereby estimate muscular capacity for force-generation (PCSA) versus length change  
68 (fascicle length) (Powell et al., 1984; Burkholder et al., 1994; Lieber and Friden, 2000). For  
69 broilers, muscle architecture data on the broiler currently exist for animals at six weeks of age  
70 (see Paxton et al., 2010), but how these properties change across growth in the broiler is  
71 unknown. This study therefore focuses on the scaling (i.e., size related, isometric or allometric;  
72 Biewener, 1989; Alexander et al., 1981; Alexander and Ker, 1990) relationships of select pelvic  
73 limb muscles to reveal changes in individual muscle characteristics of individual muscles from  
74 hatching to slaughter age (~six weeks). We also consider how the pelvic limb bones (femur,  
75 tibiotarsus and tarsometatarsus) scale with body size in the broiler chicken, as effective scaling of  
76 the hindlimb bones can reduce the rate at which stress increases with body mass (McMahon,  
77 1973, 1975; Garcia and da Silva, 2004).

78 In addition, differences in limb orientation and motion, and overall gait dynamics, among  
79 avian taxa can be partially attributed to variation in body centre of mass (CoM) position (Gatesy  
80 and Biewener, 1991; Abourachid, 1993; Hutchinson, 2004). Manion (1984) estimated CoM  
81 position for chickens across ontogeny (5-19 days) and noted a cranioventral shift and a  
82 subsequent change in limb orientation during standing and walking (more flexed during standing,  
83 but more extended during walking). The broiler CoM position has been addressed in preliminary  
84 computational analyses by Allen et al., (2009) and was found to shift caudodorsally. Other  
85 previous research suggests that broilers have a more cranially positioned CoM induced by a large  
86 pectoral muscle mass (Abourachid, 1993; Corr et al., 2003a). To better understand the influence  
87 of CoM on locomotor ability in broilers, we therefore quantify the variation in CoM position  
88 (3D) across ontogeny and relate this variation to anatomical changes documented here and in Part  
89 I of this study (Tickle et al., MS).

90 All broilers used here are considered 'normal' –i.e. no observed lameness, but we  
91 document the limb pathologies (identified post mortem) within our study populations. This is  
92 essential, because the pathological changes in affected birds do not often relate to walking ability  
93 (assessed using gait score and force plate measurements) (Sandiland et al., 2011). We quantify  
94 the inertial properties (mass, centre of mass and radius of gyration) of each limb and major body  
95 segment (Fig. 1), because these help reveal basic locomotor habits (e.g. limb tapering –i.e. a  
96 proximal to distal reduction in muscle mass reflects a specialization for power versus force  
97 development; Alexander et al., 1981; Pasi and Carrier, 2003; Hutchinson, 2004, Payne et al.,  
98 2005a, 2005b; Smith et al., 2006). Both centre of mass position and radius of gyration are also  
99 good descriptors of body area distribution and resistance to rotational movements (Kilbourne,

100 2013). Importantly, inertial properties in chickens and more specifically broilers are almost  
101 completely unstudied. Only a few studies have documented the inertial properties of other  
102 ground running birds (e.g., emus, Goetz et al., 2008; guinea fowl, Daley et al., 2007; Rubenson  
103 and Marsh, 2009; quail, Andrada et al., 2013; lapwing, Nyakatura et al., 2012). This study not  
104 only provides a novel insight into characteristics that influence broiler locomotor function, but  
105 also provides the inertial properties necessary to develop models for dynamic analyses of  
106 movement, which have been highly successful in improving our understanding of human  
107 pathological gait (e.g. Steel et al., 2012; Fey et al., 2013; Allen et al., 2013).

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## MATERIALS AND METHODS:

### 110 *Birds*

111 Fresh male cadavers of a commercial broiler strain at different ages (days 1, 13, 29, 32  
112 and 40; Table 1) were used for the hind limb muscle analysis and then a further five broilers of  
113 the same commercial strain at approximately 14, 28 and 42 days of age (2, 4 and 6 weeks old)  
114 were used to calculate the centre of mass (CoM) of the whole body, trunk and the pelvic limb  
115 segments --i.e. the thigh, drumstick, shank and foot (Fig. 1). Hatchlings (day 1) are not included  
116 in these CoM data, since our focus is in later stages of their development when breast muscle  
117 growth is more evident and leg health issues are apparent. These chickens had been previously  
118 killed by cervical dislocation. Pelvic limb bone dimensions (femur, tibiotarsus and  
119 tarsometatarsus) were also recorded at 2, 4 and 6 weeks of age. These data are from the same  
120 chickens used in Part I (Tickle et al., MS), which focuses on anatomy of the musculoskeletal  
121 respiratory apparatus and changes in body and organ size across ontogeny. As our data are cross-  
122 sectional rather than longitudinal, this study approximates an ontogenetic analysis, via inference  
123 from comparisons among individuals. All chickens were raised in a commercial setting under  
124 similar management guidelines and were not outwardly influenced by a laboratory setting. Full  
125 ethical approval for this experiment was granted by the RVC Ethics Committee (approval URN  
126 No. 2008-0001) under a Home Office license.

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### 128 *Pathology*

129 All birds were macroscopically evaluated to establish the incidence of leg pathologies  
130 (marked as present/ absent unless otherwise stated; Table 2). Each chicken was examined for  
131 bacterial chondronecrosis with osteomyelitis (BCO) in the femur and tibiotarsus, tibial  
132 dyschondroplasia (TD), tibial rotation (RT) and valgus/varus deformities (VVD). Tibial rotation

133 above 20° was considered abnormal. Similar to other studies (e.g. Shim et al., 2012) VVD was  
 134 classified as mild, moderate or severe following the methods described by Letierrier and Nys  
 135 (1992).

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### 137 ***Muscle Architecture***

138 The left pelvic limb from each individual (refer to Table 1) was dissected, with fourteen  
 139 specific muscle-tendon units (see Table 3 for muscle names and abbreviations) being identified  
 140 and systematically removed. Muscles identified included the main hip, knee and ankle extensors,  
 141 which are involved in limb support during the stance phase and have been shown to have either  
 142 massive, short-fibred muscles favouring greater force-generating capacity or have long parallel-  
 143 fibred muscles for fast contraction (Paxton et al., 2010), as in many other terrestrial species.  
 144 Architectural measurements taken included muscle mass ( $M_m$ ; tendon removed), which was  
 145 measured on an electronic balance ( $\pm 0.001\text{g}$ ), muscle fascicle length ( $L_f \pm 1\text{mm}$ ), and fibre  
 146 pennation angle ( $\theta$ ), where appropriate ( $\pm 1^\circ$ ). In order to account for variation of fascicle length  
 147 and pennation angle within a muscle,  $L_f$  and  $\theta$  were calculated as the mean of five measurements  
 148 made across each muscle. Physiological cross-sectional area (PCSA) was calculated for each  
 149 muscle (Eq. 1; Sacks and Roy, 1982) from these measurements according to the equation:

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$$151 \quad PCSA = \frac{\rho L_f \dot{V}^{-1}}{M_m \cos \theta} \quad (1)$$

152

153 Muscle tissue density ( $\rho$ ) was assumed to be  $1.06\text{g cm}^{-3}$ , the standard value for  
 154 mammalian and avian muscle (Mendez and Keys, 1960; Paxton et al., 2010).

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### 156 ***Centre of Mass and Inertial Properties***

157 Computed tomography (CT) scans were acquired of five male bird cadavers from each  
 158 group. The cadavers were scanned with a GE Lightspeed 8-detector scanner at 100mA and 120  
 159 kVp X-ray beam intensity using a 1mm CT slice thickness. In order to minimise postural effects  
 160 on CoM estimates, the birds were placed in the same upright position with their left side resting  
 161 on a radiolucent cushion for scanning and limbs posed as similarly as possible (Fig. 1a). Mimics  
 162 14.12 imaging software (Materialise; Leuven, Belgium) was then used to segment the resulting  
 163 DICOM image files, creating a 3D representation of the skeleton, body and the pelvic limb  
 164 segments (trunk, thigh, drumstick, shank and the foot; Fig. 1b). We used predefined thresholds

165 set for bone and flesh, with some manual adjustment from those baseline values as appropriate to  
 166 ensure smooth, plausible rendering. Custom software (Hutchinson et al., 2007; Allen et al.,  
 167 2009)) was then used to estimate the whole body/ segment CoM. This method allows accurate  
 168 specification of the CoM relative to any user defined point on the body or segment. These points  
 169 are easily identified using bony landmarks visible on the CT images and are essential for putting  
 170 CoM position in the context of gross morphology, which is necessary for biomechanical analyses.  
 171 Using the 3D model representations of the skeleton, whole body CoM position was quantified  
 172 relative to the right hip, trunk CoM was taken relative to the pelvis (centre point between the hips  
 173 on the pelvis), and for the remaining segments, CoM position was expressed relative to the  
 174 proximal end of the bone (Fig. 2). Three-dimensional coordinates (x [craniocaudal], y  
 175 [dorsoventral] and z [mediolateral]) for the CoM were then recorded. Whole body CoM position  
 176 was expressed as a percentage of femur length (see Allen et al., 2009).

177 Segment anatomical properties that we measured and present here include segment mass  
 178 (m; as % body mass), segment length (L; see Fig. 2), centre of mass (as % segment length), and  
 179 radius of gyration (r; as % segment length), which are essential information required to calculate  
 180 the moments of inertia ( $\text{kgm}^2$ ; Eq. 3) and subsequently complete the set of inertial properties  
 181 required for biomechanical analyses:

182

$$183 \quad R = (I \text{ m}^{-1})^{0.5} \quad (2)$$

184

185 The radius of gyration (% segment length; Eq. 2) was calculated using the principal  
 186 moment of inertia (I) and mass of the segment, both estimated using the custom software. The  
 187 mean difference between the dissected segment mass recorded and that estimated were small (<  
 188 5%). These data also provide further information on muscle mass distribution within the limb.

189

$$190 \quad I = m(r L)^2 \quad (3)$$

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### 192 ***Bone Scaling Dataset***

193 Data from Part I of this study were also used for this analysis. The individual bone  
 194 lengths of the left pelvic limb were recorded ( $\pm 1\text{mm}$ ) for each of four age groups: day 1 (n=10),  
 195 ~14 days (n=20), ~28 days (n=19), ~42 days (n=19). Total leg length was defined as the sum of  
 196 the individual pelvic limb bone lengths. Limb bone proportions were calculated as a percentage  
 197 of total leg length.

198

199 ***Statistical Analysis***

200 All of our analyses take into account differences in body size across age groups. To  
201 analyse the muscle architecture data, the linear relationship between log-transformed body mass  
202 and muscle mass, fascicle length and PCSA were examined using the reduced major-axis  
203 regression (RMA) function in the statistical program PAST (Hammer et al., 2001). RMA  
204 regression was appropriate for analysis of these morphological characters because error in both x  
205 and y variables is considered (Rayner, 1985; Sokal and Rohlf, 1995). Upper and lower 95%  
206 confidence intervals (CIs) and the  $R^2$  value for each regression line were calculated to quantify  
207 the variation around the mean (Fig. 3, Table 4). Isometric scaling was assumed when the scaling  
208 exponent  $\pm$  95% CIs overlapped the expected value. Reduced major-axis regression was also  
209 used to examine the linear relationship between log-transformed body mass and bone length.  
210 This was done using custom Matlab (The Mathworks, Nattick, MA, USA) software code. The  
211 95% CIs and the  $R^2$  value for each regression line were also calculated (Fig. 4). Similar to the  
212 statistical analysis used for the muscle architecture data, isometric scaling was assumed when the  
213 scaling exponent  $\pm$  95% CIs overlapped the expected value.

214 For CoM values and segment anatomical properties, the statistics used followed those set  
215 out in Part I of this study. In brief, a Shapiro-Wilk normality test, in combination with  
216 considering subsequent PP and QQ plots of the data, and Levene's test for equal variances were  
217 used to test the assumptions of a one-way analysis of variance (ANOVA). An ANOVA test was  
218 then conducted with a subsequent Bonferroni post-hoc test to check for differences among the  
219 three age groups. If equal variances were violated, the Welch statistics are reported in  
220 conjunction with the results of a subsequent Games-Howell post-hoc test (Table 8).

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222

**RESULTS:**223 ***Pathology***

224 There were a number of pathological changes in the study population at all stages of  
225 development (see Table 2). Bacterial chondronecrosis with osteomyelitis (BCO) was present in  
226 all populations both in the femur and proximal tibia. There was an increased incidence of BCO  
227 in the femur as the broilers aged, with 88% of the six week old chickens affected. Tibial  
228 dyschondroplasia was present in all populations with no apparent correlation with age (average  
229 41%). Rotated tibia was more prevalent in the younger birds (~33% of the study population).

230 Valgus angulation of the lower limb was seen only in the six-week old chickens, with  
231 approximately 45% of these chickens affected. No varus deformities were observed.

232

### 233 ***Muscle architecture***

234 Across ontogeny, the masses of the major hip, knee and ankle extensor muscles generally  
235 scale with positive allometry, increasing in relative size as broilers grew (Table 4). The  
236 exceptions were the FMTM (M. femorotibialis medialis), TCF (M. tibialis cranialis caput  
237 femorale), PIF (M. puboischiofemoralis) and IC (M. iliotibialis cranialis), which did not change  
238 significantly with body mass. Interestingly, fascicle length, in general, did not change with body  
239 mass, but scaled isometrically. However, the IL (M. iliotibialis lateralis) muscle showed an  
240 increase in fascicle length, whereas the GM (M. gastrocnemius medialis) showed a decrease in  
241 fascicle length. Despite these changes in fascicle length, PCSA appeared to increase  
242 allometrically across ontogeny in the majority of the pelvic limb muscles. The IC and TCF,  
243 however, scaled more in accordance with isometry.

244

### 245 ***Whole Body Centre of Mass***

246 Whole body CoM moved caudodorsally until 28 days of age. By 42 days of age there  
247 was a significant cranial shift in CoM position, moving ~10% cranially and ~30% more dorsally  
248 in the last two weeks approaching slaughter age (Table 5).

249

### 250 ***Segment Properties***

251 There was a 50-fold range in body mass of our sample of broiler chickens (Table 1),  
252 ranging from ~0.04kg at one day old to ~2.4kg at 40 days of age. Trunk mass contribution to  
253 whole body mass increased across ontogeny and was ~5% larger at 42 days of age relative to the  
254 youngest group. Similarly, a significantly larger relative thigh muscle mass was found in older  
255 birds (by ~3% body mass) compared to the younger broilers. Drumstick mass increased  
256 significantly with age whereas shank mass remained unchanged. Between 28 and 42 days, the  
257 chickens' foot mass also increased significantly by ~30% (see Table 6).

258 Trunk CoM moved caudally between 28 and 42 days, and the thigh, drumstick and shank  
259 CoM moved to more proximal positions (Table 5). In contrast, the foot's CoM moved more  
260 distally at 42 days of age.

261 The radii of gyration about the axes of long-axis rotation (Table 6) experienced an  
262 increase in the foot segments of the six week old broilers and remained unchanged in the thigh,

263 drumstick and shank. However, the radius of gyration of the whole trunk segment showed a  
264 decrease for long-axis rotation – i.e. a lower resistance to yaw. The radii of gyration in the  
265 parasagittal plane, decreased in the drumstick and shank across broiler ontogeny, but  
266 progressively increased in the foot. There was also a relative reduction of  $r\%$  about the axis of  
267 abduction/ adduction rotation. Radii of gyration for the thigh remained unchanged.

268

### 269 ***Bone Scaling***

270 Tibiotarsus and tarsometatarsus length scaled isometrically with body mass, whereas  
271 femur length scaled with slight negative allometry (Fig. 4). As a result, there was a relative  
272 increase in total leg length from 14 days to 28 days. Limb length remained unchanged between  
273 four and six weeks. The femur accounts for ~30% of total leg length and the tibiotarsus accounts  
274 for ~41% of leg length. The tarsometatarsus is relatively shorter than the other pelvic limb bones  
275 accounting for ~29% of total leg length.

276

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## DISCUSSION

278 The genetic success of the modern broiler and the subsequent changes to the morphology  
279 of broiler chickens have been well documented, in order to determine the lines' commercial  
280 performance (e.g. Gous et al., 1999) and compare both growth responses and physiological  
281 adaptations resulting from distinctive selection pressures (e.g. Havenstein et al., 2003a, b;  
282 Reddish and Lilburn, 2004; Schmidt et al., 2009). A marked change in total pectoral muscle mass  
283 of the commercial broiler is a common finding of all these prior studies. Similarly, we found this  
284 mass to represent ~20% of total body mass in slaughter age chickens (see Part I; Tickle et al.,  
285 MS). Part I revealed how enlarged pectoral muscle mass, among other anatomical changes, may  
286 compromise the efficacy of the respiratory apparatus. Here we show how these changes influence  
287 the locomotor ability of the broiler.

288

### 289 ***Pathology***

290 Leg weakness in broilers comprises not only nonspecific gait problems and lower activity  
291 levels, but also a wide range of disorders that are generally classified as infectious, degenerative,  
292 or developmental (for a review see Bradshaw et al., 2002). The most common disorders include  
293 bacterial chondronecrosis with osteomyelitis (BCO), angular and torsional deformities (e.g.  
294 valgus-varus (VVD) and rotated tibia (RT)) and tibial dyschondroplasia (TD). With the  
295 exception of VVD, these conditions were observed in birds at all developmental stages in this

296 study. BCO was common in the broilers (Table 2), far exceeding previous estimates of infection  
297 in commercial flocks (approximately 0.5% ). Incidence of BCO in the femur peaked at 88% of  
298 42-day-old birds. This variation is likely due to differences in how these estimates of infection  
299 were determined. Femoral head separation (FHS; epiphyseolysis) dominated in our study's birds,  
300 which we concur should be attributed to underlying traumatic (osteochondrosis) or infectious  
301 (osteomyelitis) femoral head pathology (following Wideman et al., (2013)). FHS is often shown  
302 separately in studies to show the progression of the disease (e.g. Wideman et al., 2012; Wideman  
303 and Pevzner, 2012; Wideman et al., 2013), but here we are purely interested in the presence or  
304 absence of the condition. Furthermore, the high percentage of birds we found to have BCO may  
305 reflect a predisposition to the condition or differences in husbandry practices . Increasing  
306 occurrence of BCO over development is consistent with previous results that identified peak  
307 incidence at around five weeks of age (McNamee 1999a). Increasing incidence over  
308 development may reflect increased stresses acting on the bone, which are thought to contribute to  
309 BCO (Wideman, 2013). Similarly, BCO in the tibiotarsus was widespread and increased with  
310 age, showing a peak at 42 days (Table 2). BCO causes lesions in the load-bearing growth plates  
311 of the femur and tibiotarsus, so rapid growth and weight gain may be an aggravating factor when  
312 bacterial infection is present. Considering the widespread incidence of BCO in birds that were  
313 otherwise deemed healthy, bone lesions are a significant problem affecting welfare standards in  
314 broiler chickens.

315 TD commonly leads to growth plate abnormalities, infections and tibial deformation  
316 (Lynch et al., 1992) but, similar to BCO, TD does not necessarily induce lameness of sufficient  
317 severity to impair walking ability (Pattison, 1992). TD has been found to occur between 2 and 8  
318 weeks of age and our findings are consistent with this observation (Table 2). However,  
319 considerable variation exists in the reported prevalence of TD, ranging in 42 day old birds from  
320 approximately 2% to 50% of total flock population. Incidence of TD in this study was relatively  
321 high and occurred in all age groups, peaking at 28 days (57%). However, determining why the  
322 incidence of TD is high in this study is difficult because the condition reflects a complicated  
323 interaction of contributing factors, including dietary deficiencies, toxins, genetic predisposition  
324 and rapid growth rate .

325 Valgus-varus deformities (VVD) were observed in 42-day-old birds, but was not present  
326 in younger broilers (Table 2). Comparable reports indicate that VVD occurs with varying  
327 incidence, affecting as few as 0.5% to 30-40% of birds in a flock . The prevalence of VVD in  
328 this study fell near the high end of the reported range, with 45% of birds at 42 days of age

329 observed to have mild or moderate VVD. Our observation that symptoms of VVD occur only in  
330 older broilers is consistent with the progressive nature of this deformity . However, no deformity  
331 was seen in 28-day-old birds, which is perhaps surprising because this is approximately the age  
332 that VVD often becomes prominent , although the timing of onset is known to vary .

333 Rotated Tibia (RT) occurred in birds at all developmental stages at a higher than expected  
334 rate (i.e., value) compared to previous work (0.2%, Bradshaw et al., 2002)). However, Bradshaw  
335 et al., reported a reduced proportion of RT in older broilers, which perhaps indicates that affected  
336 birds were culled because the condition becomes clearly obvious around 21 days of age . The  
337 exact aetiology of RT is unknown; however TD and VVD may exacerbate the incidence of RT ,  
338 thereby contributing to the relatively high proportion of birds with an outward torsion of the tibial  
339 shaft.

340 Overall, there is a clear need to monitor the leg health of flocks, not only to aid breeders  
341 to make adjustments to management practices or genetics when necessary, but also to quickly  
342 identify lame birds for euthanasia on welfare grounds. The high incidence of leg pathologies  
343 highlights the problem of maintaining high growth rates and breast muscle mass ( $M_b$ ) at the  
344 expense of broiler anatomy and physiology. In addition, lameness represents a significant  
345 economic cost to the industry as birds with leg weakness are prematurely culled or have an  
346 increased incidence of mortality (Mench, 2004). Efforts to improve the health of growing  
347 broilers will have the twin benefit of improving both welfare standards and productivity.

348

### 349 ***Muscle Architecture***

350 Architectural properties used to calculate the effective physiological cross-sectional area  
351 (PCSA) (Gans and Bock, 1965) of muscle take into account the effect of pennate fascicles on  
352 maximizing force per unit area. PCSA is thus greater in pennate muscles and is directly  
353 proportional to its force generation capacity (Burkholder et al., 1994; Lieber and Friden, 2000).  
354 In broilers, the PCSA of the major hip, knee and ankle extensors (essential for supporting body  
355 mass and maintaining an upright standing posture; Gatesy 1999; Reilly, 2000; Hutchinson, 2004),  
356 scale with positive allometry – i.e., these muscles have a greater force-generating capacity  
357 (reflected in their relatively larger PCSAs) as the broiler develops (Table 4, Fig. 3). As a result,  
358 muscular force production capacity in broiler chickens should increase with age, likely as a direct  
359 consequence of weight vs. force scaling constraints imposed by resisting gravity and inertia (e.g.,  
360 Corr et al., 2003). However, these muscles still have smaller force-generating capabilities and  
361 shorter, presumably slower-contracting muscles than their wild counterpart, the Giant Junglefowl

362 (Paxton et al., 2010). Broiler chickens appear to generally increase the PCSA of their pelvic limb  
363 muscles by increasing muscle mass, rather than by increasing fascicle length, which scaled  
364 isometrically (Table 4, Fig. 3). This increase in mass is likely due to increased hypertrophy  
365 (increase in muscle fibre size), which is well known to occur in broiler skeletal muscle and is the  
366 assumed dominant model for postnatal growth (Aberle and Stewart, 1983; Soike and Bergman,  
367 1998; Remignon et al., 1994; Goldspink and Yang, 1999). In addition, muscular force production  
368 is invariant to muscle fascicle length, but longer fascicles exact a metabolic cost because a larger  
369 volume of muscle is activated for each Newton of force (Kram and Taylor, 1990; Roberts et al.,  
370 1998). Thus, the isometric scaling of fascicle length we observed in this study avoids such added  
371 costs.

372 Interestingly, the PCSAs of the *M. iliotibialis cranialis* (IC) and *M. tibialis cranialis caput*  
373 *femorale* (TCF) scale more in accordance with isometry. The relative force-generating capacity  
374 of these muscles therefore remains unchanged throughout the growth of the broiler. The TCF is a  
375 knee extensor and ankle flexor and is assisted by other muscles that also serve as knee extensors  
376 and ankle flexors (e.g., *M. femorotibialis* and *M. extensor digitorum longus*). Similarly, the IC is  
377 also a knee extensor, but additionally acts as a hip flexor, supported by the *M. iliotrochantericus*  
378 *caudalis* (ITC; known to be significantly larger in the broiler [Paxton et al., 2010]) to flex and  
379 medially rotate the femur. The additional support of these muscles may help to explain why the  
380 IC and TCF scale in unusually isometric ways. The IC and TCF may be redundant, especially  
381 when limb motion in these broilers is likely to be 1) knee-driven (e.g. Gatesy, 1999; Reilly, 2000;  
382 Hutchinson and Allen, 2009), requiring action of the major knee flexors (*M. iliofibularis*,  
383 *M. flexor cruris lateralis*), and 2) three-dimensional, demanding large supportive forces at the hip  
384 for the considerable mediolateral forces they experience when they walk (Paxton et al., 2013).  
385 However, biomechanical analyses of *in vivo* function are needed to test how much their function  
386 alters with growth in broilers.

387

### 388 ***Centre of Mass and Inertial Properties***

389 At the youngest age (14 days old) studied here, chickens' trunk mass accounted for ~75%  
390 of total body mass. At slaughter weight (around 42 days of age), total trunk mass had increased  
391 to ~80% total body mass. The ~5% increase in trunk mass is largely attributable to pectoral  
392 muscle growth, which occurred at a relatively faster rate than body mass (see Part I Tickle et al.,  
393 2014).

394 Interestingly, relative hind limb segment mass (summed segment masses; muscle and  
395 bone mass combined) did not decrease during growth, accounting for ~15% of total body mass at  
396 slaughter age and thus representing a total 5% body mass increase across ontogeny. The  
397 proportion of bone mass contributing to total segment mass is likely small because the muscle to  
398 bone ratio is known to be high in commercial broilers (Ganabadi et al., 2009). The increase in leg  
399 mass was instead incurred by increases in drumstick and thigh muscle mass. Drumstick segment  
400 mass increased across ontogeny, becoming relatively larger at each age category, whereas thigh  
401 segment mass only had substantial changes during the last two weeks of growth (from 28 – 42  
402 days old). Thigh muscle mass increased by ~3% of total body mass during this period. Changes  
403 in thigh and drumstick segment mass are expected, as these segments yield the most meat and are  
404 the most consumed portions (alongside breast meat) on the market (Broadbent et al., 1981).  
405 However, the increase in hind limb segment mass is striking and comparable to a progenitor  
406 population (total limb muscle mass ~16%) at the same approximate physiological mass and  
407 indeed larger than its wild counterpart at the same age by ~4% body mass (see Paxton et al.,  
408 2010). Previous studies typically show an ontogenetic reduction in the investment of metabolic  
409 resources towards pelvic limb muscle growth (e.g. Berri et al., 2007; Schmidt et al., 2009) and  
410 the main drivers of selection in broiler chickens are still a greater yield of breast muscle mass and  
411 a faster post-hatch growth rate (Arthur and Albers, 2003). Thus, changes in leg muscle mass may  
412 not reflect a direct difference in selection pressures. However, a relative increase in hind limb  
413 muscle mass may reflect a functional demand for larger hip and knee extensors to support their  
414 increasing body mass. Corr et al., (2003a) studied two strains of birds (relaxed and selected)  
415 raised on two different feeding regimes and suggested that the large pectoral muscle mass of the  
416 broiler has displaced their CoM cranially. Similarly, Abourachid (1993) suggested that increased  
417 stresses on the pelvic limbs of heavier broad-breasted turkeys were induced by a more cranially  
418 positioned CoM. We found that broilers show a change in whole body CoM position consistent  
419 with these previous findings, shifting from a caudodorsal to a craniodorsal location between 28  
420 and 42 days of age, which would increase demand for muscular force production to balance it.  
421 Interestingly, the centre of mass of the Giant Junglefowl (a representative progenitor population)  
422 has been shown to move caudodorsally, not craniodorsally, across ontogeny. This cranial shift in  
423 broilers may therefore be the direct result of increased pectoral muscle mass growth between four  
424 and six weeks of age.

425 In all cases, the craniocaudal CoM location in broilers was far more cranial than previous  
426 estimates. Allen et al., (2009) estimated CoM cranial position to be ~38% of femur length,

427 compared to the 70-90% femur length estimated in this study. On the other hand, dorsoventral  
428 estimates broadly corresponded to literature values (Allen et al., 2009). The difference in  
429 craniocaudal CoM position likely relates directly to pectoral muscle growth. The pectoral muscle  
430 mass of the broilers used in this study yielded an additional ~4% of total body mass in  
431 comparison to the broilers used by Allen et al., (2009). One limitation of our study is that whole  
432 body CoM was normalized by femur length, which did scale with slight negative allometry (see  
433 discussion below). Using femur length may introduce a slight bias to our results, but  
434 normalization by other factors including total limb length have been shown to yield the same  
435 result (Allen et al., 2009).

436         There are also substantial changes in the distal segment of the pelvic limb between 28  
437 and 42 days. Foot mass increases by ~30% and foot CoM moves distally. Large feet may serve  
438 to improve the apparent stability reported in the broiler (e.g. Corr et al., 2003b) during the stance  
439 phase of gait. However, larger feet will influence the broiler's ability to accelerate and decelerate  
440 the limb during swing, which in turn can affect the metabolic cost of locomotion (Kilbourne,  
441 2013; Kilbourne and Hoffman, 2013). Both an increase in mass and a more distal shift in the  
442 limb's mass distribution will effectively increase a limb's moment of inertia, (i.e., resistance to  
443 angular acceleration, Steudel, 1990; Wickler et al., 2004; Kilbourne and Hoffman, 2003). Broiler  
444 pelvic limbs would therefore require more metabolic energy to accelerate and decelerate them as  
445 the birds grow. However, the influence of mass is much smaller than the influence of the  
446 distribution of the mass (radii of gyration reported here) on the moment of inertia. Doubling  
447 mass would essentially double the moment of inertia, whereas doubling the radii of gyration  
448 would increase the moment of inertia four-fold (Eq. 3). The radii of gyration in the parasagittal  
449 plane and about the axes of long-axis rotation increased in the foot segments of the ~42 day old  
450 broiler. Thus, increased radii of gyration in the foot segment of the broiler contribute  
451 significantly to the limb's moment of inertia.

452         We found that broilers' whole pelvic limb morphology changed across ontogeny, with the  
453 main changes in the thigh and foot segments. These segments had increased muscle mass and a  
454 more distal mass distribution (rather than having relatively longer limbs; see bone scaling  
455 discussion), resulting in relatively larger moments of inertia. The changes in limb morphology  
456 are likely to assist in supporting the increased supportive forces required by a more cranially  
457 positioned CoM and to help improve stability during locomotion. However, these changes also  
458 likely exact a relatively higher metabolic cost to locomotion.

459

## 460 ***Bone Scaling***

461 We have shown that femur length scaled with slight negative allometry, whereas the  
462 lengths of the tibiotarsus and tarsometatarsus scale with isometry across broiler ontogeny (Fig. 4).  
463 Regardless, total relative limb length remained unchanged from four to six weeks in growing  
464 broilers may be an adaptation related to their apparent instability (Paxton et al., 2013).  
465 Maintaining shorter limbs may act to moderate the lateral motion of the CoM and aid balance  
466 (Bauby and Kuo, 2000). However, short limbs also likely lead to an increased energetic cost  
467 (Steudel-Numbers and Tilken, 2004).

468 Here we have considered how pelvic limb morphology changes during broiler ontogeny,  
469 in coordination with other changes such as pectoral muscle mass. Together, these changes have  
470 influenced broiler morphology across ontogeny, which may have influenced locomotor ability as  
471 well. The relative force-generating capacity of the hind limb muscles is greater in older broilers,  
472 and is primarily achieved through increasing muscle mass but maintaining a constant fascicle  
473 length. Increases in thigh segment mass and a relative increase in the moment of inertia of the  
474 distal limb (due mainly to increased foot size) may reflect adaptations to cope with the apparent  
475 instability and a more cranially positioned CoM as broilers grow. Although the architectural  
476 changes we have observed have obvious advantages for maintaining an upright posture and  
477 forward progression of broiler chickens, these morphological changes likely have a negative  
478 impact on locomotion, exacting relatively higher metabolic costs during growth, which may have  
479 knock-on consequences for activity levels and even overall health.

480

481

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484

485

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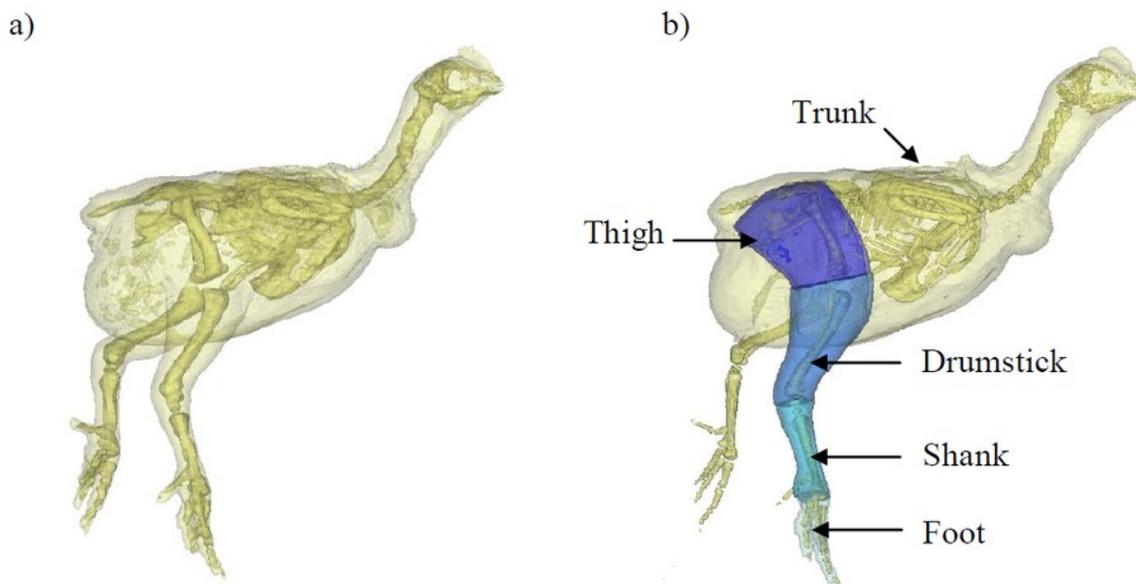
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# Figure 1

**Figure 1 - A 3D model representation of the broiler showing the body and pelvic limb segments.**

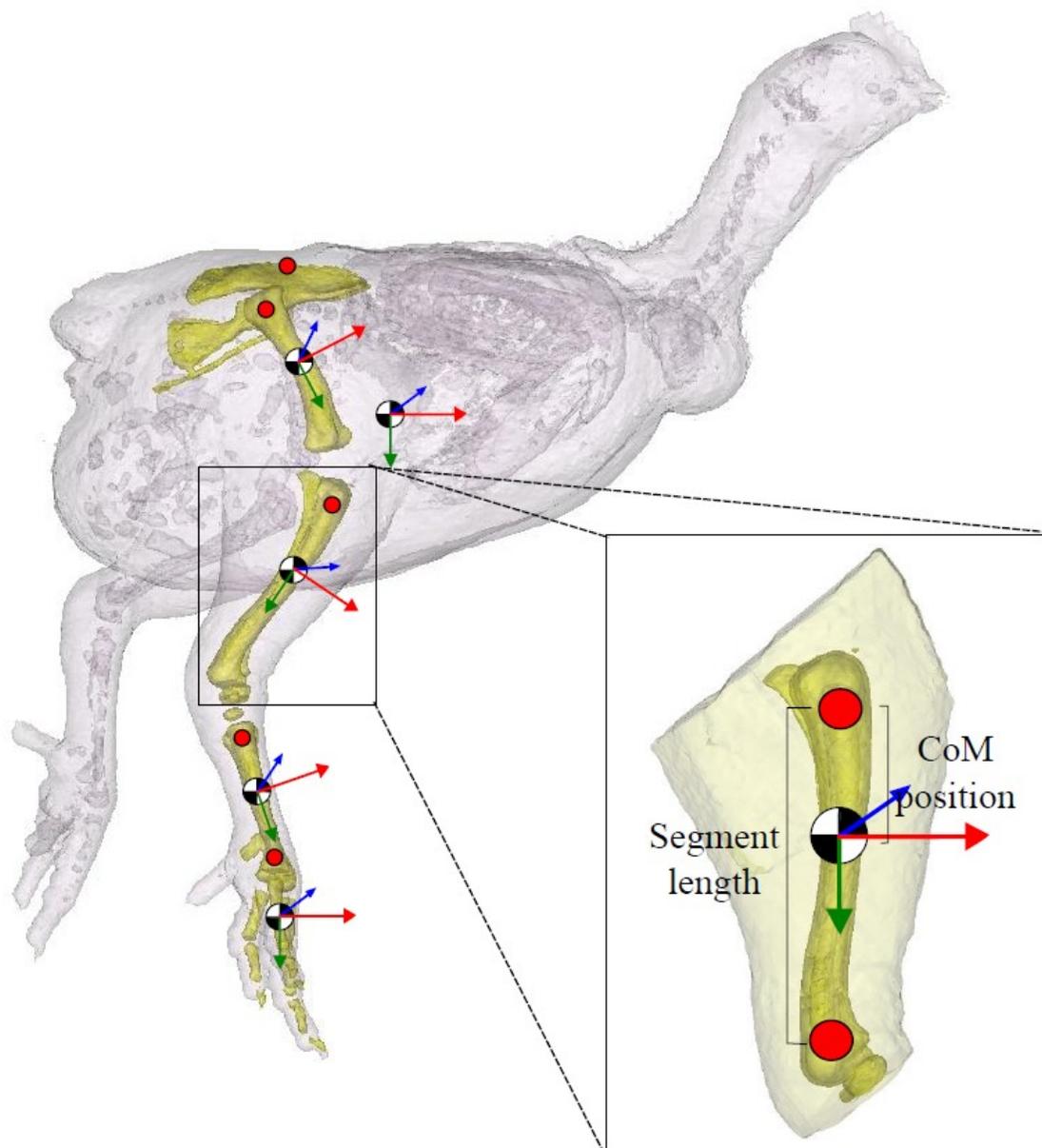
Fig. 1 shows the 3D model representation of the broiler's body and its corresponding segments created within MIMICS software. Each chicken was placed in the same upright position with their left side resting on a radiolucent cushion during scanning. Fig. 1a shows the whole body and skeleton produced within this software and Fig. 1b shows the trunk (leg flesh removed) and pelvic limb segments. The translucent outline represents the 'virtual flesh' of the models used to estimate the inertial properties (mass, centre of mass and radius of gyration) of each segment.



# Figure 2

## Figure 2 – Segment inertial properties

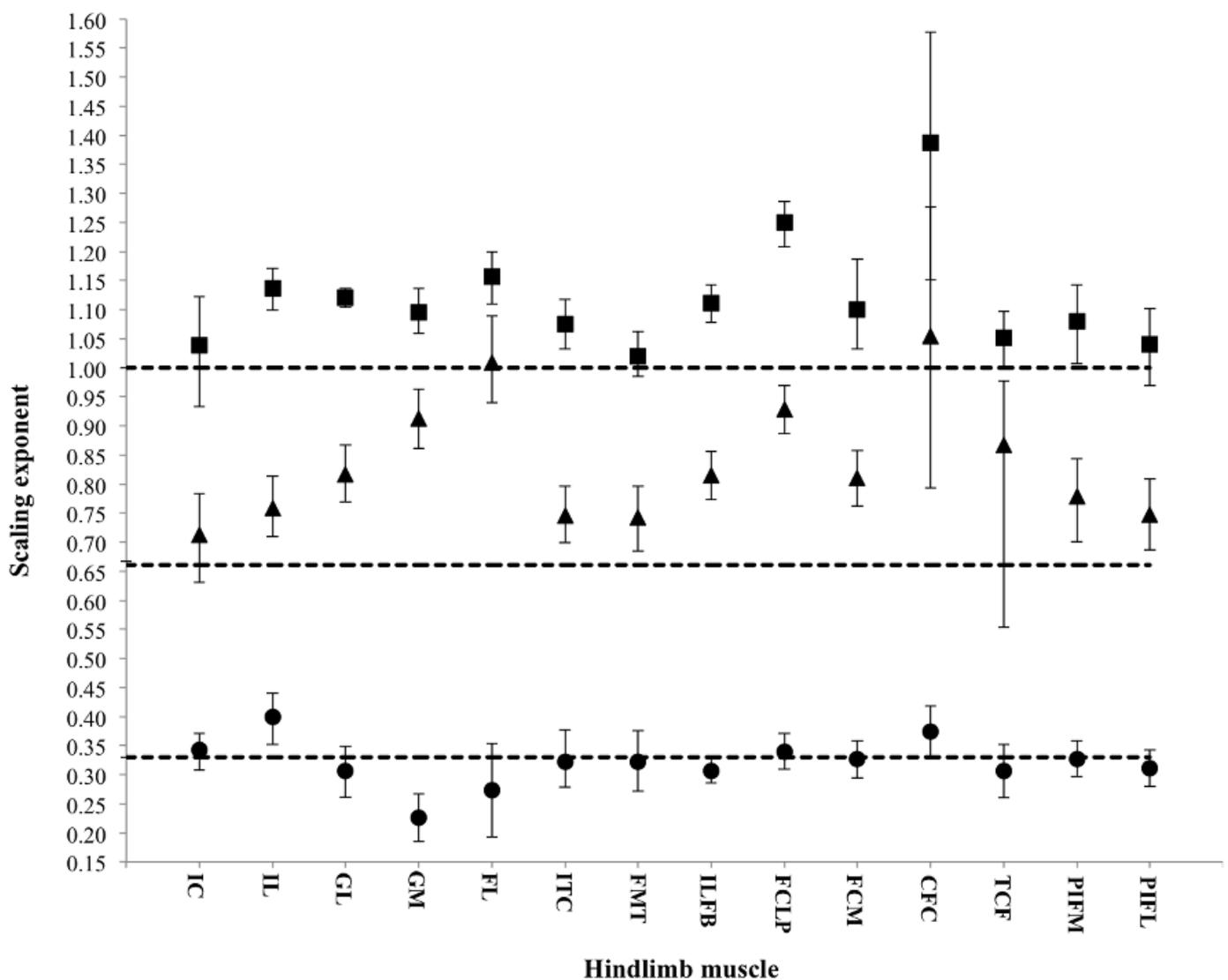
The pelvis, femur, tibia, tarsometatarsus and the bones of the foot are highlighted in this 3D model. Centre of mass (CoM) position is shown (black/ white circle; approximate position given). Trunk CoM was taken relative to the pelvis (centre point between the hips on the pelvis), and for the remaining segments, CoM position was expressed relative to the proximal end of the bone (red markers shown). The local anatomical coordinate system for each segment is given (x (red), y (green) and z (blue)). Segment length (excluding the pelvis) is defined as the distance between the proximal and distal marker on the segment, as shown.



## Figure 3

**Figure 3 - Scaling exponents of pelvic limb muscle properties as a function of increasing body mass**

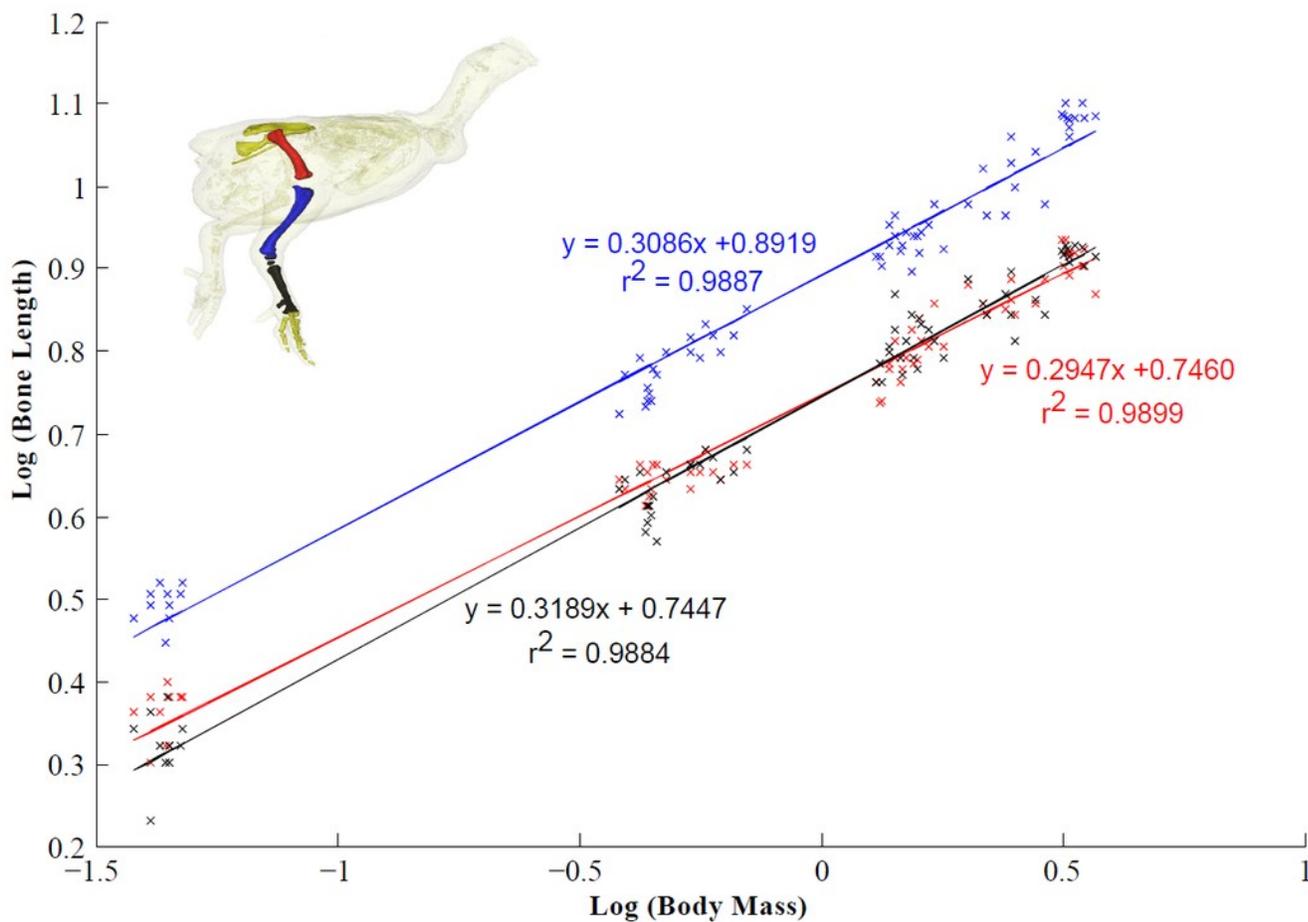
Symbols indicate the regression slope for muscle mass (squares), physiological cross-sectional area (PCSA; triangles) and muscle fascicle length (circles). Error bars represent upper and lower 95% confidence intervals. Dashed lines represent, expected values for isometric (directly proportional) scaling of muscle properties with body mass ( $y = 1.0$ : muscle mass,  $y = 0.67$ : PCSA,  $y = 0.33$ : muscle fascicle length).



# Figure 4

**Figure 4 – Scaling relationship of the pelvic limb bones (femur, tibiotalus and tarsometatarsus)**

95% confidence intervals (CIs) for the femur, tibiotalus and tarsometatarsus are  $0.2947 \pm 0.0104$ ,  $0.3086 \pm 0.0114$  and  $0.3189 \pm 0.0120$  respectively (scaling exponent  $\pm$  CI). Isometric scaling of the tibiotalus and tarsometatarsus is concluded because the 95% CIs overlapped the expected value (0.33). The femur scaled with slight negative allometry.



**Table 1** (on next page)**Table 1 – Subject data**

Data represented here are for the broiler chickens used only for muscle architecture and are means  $\pm$  standard deviation. These data form part of the mean data presented in Table 2, Part I of this study.

**Table 1 – Subject data**

Age (days)	Sample size (n)	Body mass (kg)
1	10	0.044 ± 0.01
13	10	0.431 ± 0.08
29	5	1.542 ± 0.05
32	5	1.738 ± 0.08
40	7	2.452 ± 0.09

Data represented here are for the broiler chickens used only for muscle architecture and are means ± standard deviation. These data form part of the mean data presented in Table 2, Part I of this study.

## **Table 2**(on next page)

### **Table2 – Incidence of pathology across growth in broiler chickens**

Data are presented as percentage of total study population. Bacterial chondronecrosis (BCO) and tibial dyschondroplasia (TD) were marked as present or absent. The severity of these abnormalities was not considered. Where present, valgus/ varus deformities (VVD) were classified as mild (10-25°), moderate (25-45°) or severe (>45°) following the methods described by Leterrier and Nys (1992). Tibial rotation (RT) above 20° was considered abnormal. Pathologies may have been recorded in one pelvic limb or both pelvic limbs of the individual birds; this is not distinguished here.

**Table 2 – Incidence of pathology across growth in broiler chickens**

Age (days)	BCO (femur)	BCO (tibiotarsus)	TD (present)	VVD				RT (abnormal)	Total
				normal	mild	moderate	severe		
14	63	53	43	100	0	0	0	33	
28	75	93	57	100	0	0	0	15	
42	88	97	24	55	42	3	0	16	

Data are presented as percentage of total study population. Bacterial chondronecrosis (BCO) and tibial dyschondroplasia (TD) were marked as present or absent. The severity of these abnormalities was not considered. Where present, valgus/ varus deformities (VVD) were classified as mild (10-25°), moderate (25-45°) or severe (>45°) following the methods described by Leterrier and Nys (1992). Tibial rotation (RT) above 20° was considered abnormal. Pathologies may have been recorded in one pelvic limb or both pelvic limbs of the individual birds; this is not distinguished here.

## **Table 3**(on next page)

**Table3 – The major muscles of the chicken pelvic limb**

**Table 3 – The major muscles of the chicken pelvic limb**

<b>Muscle</b>	<b>Abbreviation</b>
M. iliotibialis cranialis	IC
M. iliotibialis lateralis	IL
M. gastrocnemius pars lateralis	GL
M. gastrocnemius pars medialis	GM
M. fibularis longus	FL
M. iliotrochantericus caudalis	ITC
M. femorotibialis medialis	FMT
M. iliofibularis	ILFB
M. flexor cruris lateralis pars pelvica	FCLP
M. flexor cruris medialis	FCM
M. caudofemoralis pars caudalis	CFC
M. tibialis cranialis caput femorale	TCF
M. puboischiofemoralis pars medialis	PIFM
M. puboischiofemoralis pars lateralis	PIFL

**Table 4**(on next page)**Table 4 – RMA regression analyses**

Data here are the RMA regression analyses that were used to determine the linear relationships between pelvic limb muscle architecture and body mass. Expected regression slopes for isometric growth are given for each parameter. Symbols next to each calculated regression slope indicate isometric growth (=), positive allometry (+; emphasized in bold) or negative allometry (-; emphasized in italics). All regressions were significant ( $p < 0.05$ ).

**Table 4 – RMA regression analyses**

Muscle	$M_m$ expected slope: 1.00	PCSA expected slope: 0.67	$L_t$ expected slope: 0.33									
	Slope	Lower 95% CI	Upper 95% CI	R <sup>2</sup>	Slope	Lower 95% CI	Upper 95% CI	R <sup>2</sup>	Slope	Lower 95% CI	Upper 95% CI	R <sup>2</sup>
IC	1.038 (=)	0.933	1.123	0.961	0.712 (=)	0.630	0.783	0.938	0.342 (=)	0.308	0.372	0.923
IL	<b>1.136 (+)</b>	1.099	1.171	0.994	<b>0.759 (+)</b>	0.709	0.814	0.968	<b>0.399 (+)</b>	0.352	0.440	0.938
GL	<b>1.121 (+)</b>	1.104	1.136	0.998	<b>0.817 (+)</b>	0.769	0.868	0.977	0.306 (=)	0.261	0.349	0.859
GM	<b>1.095 (+)</b>	1.059	1.136	0.992	<b>0.912 (+)</b>	0.861	0.963	0.977	<i>0.226 (-)</i>	0.185	0.268	0.801
FL	<b>1.156 (+)</b>	1.109	1.199	0.988	<b>1.009 (+)</b>	0.940	1.089	0.945	0.274 (=)	0.193	0.354	0.420
ITC	<b>1.075 (+)</b>	1.032	1.118	0.989	<b>0.746 (+)</b>	0.699	0.796	0.969	0.322 (=)	0.279	0.377	0.844
FMTM	1.021 (=)	0.985	1.062	0.984	<b>0.743 (+)</b>	0.685	0.796	0.948	0.322 (=)	0.271	0.375	0.758
ILFB	<b>1.112 (+)</b>	1.078	1.143	0.994	<b>0.815 (+)</b>	0.773	0.856	0.981	0.307 (=)	0.286	0.330	0.961
FCLP	<b>1.250 (+)</b>	1.208	1.286	0.992	<b>0.929 (+)</b>	0.887	0.969	0.979	0.339 (=)	0.309	0.371	0.924
FCM	<b>1.101 (+)</b>	1.032	1.187	0.958	<b>0.811 (+)</b>	0.762	0.857	0.974	0.326 (=)	0.294	0.358	0.938
CFC	<b>1.387 (+)</b>	1.151	1.578	0.926	<b>1.054 (+)</b>	0.793	1.277	0.869	0.374 (=)	0.329	0.419	0.881
TCF	1.052 (=)	1.000	1.097	0.979	0.867 (=)	0.553	0.977	0.887	0.306 (=)	0.260	0.352	0.720
PIFM	1.079 (=)	1.007	1.143	0.969	<b>0.779 (+)</b>	0.701	0.843	0.933	0.327 (=)	0.297	0.358	0.893
PIFL	1.040 (=)	0.969	1.102	0.975	<b>0.748 (+)</b>	0.687	0.808	0.952	0.311 (=)	0.280	0.343	0.918

Data here are the RMA regression analyses that were used to determine the linear relationships between pelvic limb muscle architecture and body mass.

Expected

regression slopes for isometric growth are given for each parameter. Symbols next to each calculated regression slope indicate isometric growth (=), positive allometry (+; emphasized in bold) or negative allometry (-; emphasized in italics). All regressions were significant ( $p < 0.05$ ).

## **Table 5**(on next page)

### **Table5 – Whole body centre of mass position**

Data represented are means  $\pm$  standard deviation. Centre of mass (CoM) position is calculated as a percentage of femur length and is expressed relative to the right hip joint of the chicken. Craniocaudal and dorsoventral positions are shown. Data with no common superscript differ significantly at the 0.05 level.

**Table 5 – Whole body centre of mass position**

Age Group	CoM Position (% femur length)	
	Craniocaudal	Dorsoventral
14 days	90.6 ± 10.7 <sup>1</sup>	<b>89.8 ± 13<sup>1</sup></b>
28 days	68.3 ± 5.0 <sup>1,2</sup>	55.4 ± 17.7 <sup>2</sup>
42 days	<b>76.6 ± 12.2<sup>2</sup></b>	28.2 ± 19.5 <sup>2</sup>

Data represented are means ± standard deviation. Centre of mass (CoM) position is calculated as a percentage of femur length and is expressed relative to the right hip joint of the chicken. Craniocaudal and dorsoventral positions are shown. Data with no common superscript differ significantly at the 0.05 level.

**Table 6**(on next page)**Table 6 – Pelvic limb segment inertial properties**

Data represented are means  $\pm$  standard deviation. Centre of mass position (CoM) is located relative to the proximal end of the segment (trunk CoM is relative to the centre line between the hips), and is shown along the craniocaudal (for trunk) or proximodistal (for limbs) axis(Fig. 2). Data in a column with no common superscript differ significantly at the 0.05 level.

**Table 6 – Pelvic limb segment inertial properties**

Segment	Age Group	Segment Mass (% body mass)	CoM Position (% segment length)	Radius of Gyration (% segment length)		
				x	y	z
Trunk	14 days	74.6 ± 1.7 <sup>a</sup>	19.5 ± 2.5	23.2 ± 1.0	41.1 ± 0.3 <sup>b</sup>	35.0 ± 1.9 <sup>a</sup>
	28days	78.0 ± 1.8 <sup>a,b</sup>	20.1 ± 4.3	24.0 ± 1.2	40.0 ± 1.7 <sup>b</sup>	37.1 ± 1.8 <sup>a,b</sup>
	42 days	81.7 ± 3.2 <sup>b</sup>	15.3 ± 2.7	33.3 ± 12.0	<b>37.1 ± 1.8<sup>a</sup></b>	37.8 ± 0.8 <sup>b</sup>
Thigh	14 days	5.19 ± 1.4 <sup>a</sup>	<b>43.7 ± 4.3<sup>a</sup></b>	47.2 ± 8.5	44.1 ± 7.4	49.6 ± 14.5
	28days	5.22 ± 0.4 <sup>a</sup>	<b>38.1 ± 2.0<sup>b</sup></b>	48.3 ± 6.2	40.6 ± 4.2	52.1 ± 8.8
	42 days	<b>8.21 ± 1.0<sup>b</sup></b>	<b>28.7 ± 2.4<sup>c</sup></b>	46.2 ± 7.0	42.5 ± 4.3	52.3 ± 7.1
Drumstick	14 days	<b>3.9 ± 0.3<sup>a</sup></b>	30.1 ± 14.2	49.1 ± 6.3	24.9 ± 2.9	<b>51.0 ± 6.1<sup>a</sup></b>
	28days	<b>4.6 ± 0.5<sup>b</sup></b>	32.7 ± 2.3	40.0 ± 5.3	25.6 ± 4.0	40.2 ± 7.1 <sup>a,b</sup>
	42 days	<b>5.66 ± 0.2<sup>c</sup></b>	24.2 ± 4.2	34.0 ± 12.4	21.2 ± 11.7	<b>34.3 ± 12.2<sup>b</sup></b>
Shank	14 days	0.98 ± 0.1 <sup>a</sup>	<b>36.1 ± 10.3<sup>a</sup></b>	50.5 ± 1.2 <sup>a</sup>	18.1 ± 0.2	50.8 ± 1.1 <sup>a</sup>
	28days	1.02 ± 0.1 <sup>a,b</sup>	17.3 ± 5.5 <sup>b</sup>	49.8 ± 2.3 <sup>a</sup>	17.2 ± 1.2	50.2 ± 2.5 <sup>a</sup>
	42 days	1.23 ± 0.2 <sup>b</sup>	22.6 ± 6.3 <sup>b</sup>	<b>38.0 ± 4.1<sup>b</sup></b>	23.3 ± 20.7	<b>37.1 ± 2.7<sup>b</sup></b>
Foot	14 days	0.63 ± 0.03 <sup>a</sup>	38.6 ± 4.3 <sup>a</sup>	34.3 ± 0.9	35.2 ± 1.8 <sup>b</sup>	23.3 ± 1.4
	28days	0.61 ± 0.07 <sup>a</sup>	28.4 ± 7.3 <sup>a</sup>	31.0 ± 2.3	<b>21.2 ± 6.3<sup>a</sup></b>	28.0 ± 4.5
	42 days	<b>0.91 ± 0.12<sup>b</sup></b>	<b>51.9 ± 9.1<sup>b</sup></b>	38.7 ± 16.4	29.9 ± 3.9 <sup>b</sup>	29.7 ± 21.4

Data represented are means ± standard deviation. Centre of mass position (CoM) is located relative to the proximal end of the segment (trunk CoM is relative to the centre line between the hips), and is shown along the craniocaudal (for trunk) or proximodistal (for limbs) axis (Fig. 2). Data in a column with no common superscript differ significantly at the 0.05 level.

## Table 7 (on next page)

### Table 7 – Pelvic limb bone segment dimensions

Data presented here are for the left pelvic limb only, and are means  $\pm$  standard deviation.

Total leg length is the sum of the individual pelvic limb bones. Absolute values for leg length are presented here, but normalized values (divided by body mass  $^{1/3}$ ) were used for the statistical analysis to compare how leg length changed across ontogeny (see Fig. 4 for scaling relationship). Data in a column with no common superscript differ significantly at the 0.05 level.

**Table 7 – Pelvic limb bone segment dimensions**

Age Group	Sample size	Leg Length(cm)	Individual bones (% leg length)		
			Femur	Tibiotarsus	Tarsometatarsus
1 day	10	<b>7.5 ± 0.44<sup>a</sup></b>	30.4 ± 0.68	41.5 ± 1.8	28.0 ± 1.4
14 days	19	14.9 ± 0.93 <sup>b</sup>	29.9 ± 0.6	40.9 ± 1.1	29.2 ± 1.0
28 days	19	21.4 ± 1.3 <sup>b</sup>	29.3 ± 1.1	40.4 ± 1.5	30.2 ± 1.1
42 days	20	26.9 ± 2.2 <sup>b</sup>	29.0 ± 1.1	42.0 ± 1.4	29.0 ± 0.7

Data presented here are for the left pelvic limb only, and are means ± standard deviation.

Total leg length is the sum of the individual pelvic limb bones. Absolute values for leg length are presented here, but normalized values (divided by body mass<sup>1/3</sup>) were used for the statistical analysis to compare how leg length changed across ontogeny (see Fig. 4 for scaling relationship). Data in a column with no common superscript differ significantly at the 0.05 level.

## **Table 8**(on next page)

### **Table8 - Levene's test and ANOVA results**

Degrees of freedom = ( $df_{\text{between}}$  ,  $df_{\text{within}}$  ). Where the assumption of equal variances cannot be met (significant Levene's test result), the Welch statistics are reported.

	Levene's test	Degrees of freedom	F	P	<b>Table 8 - Levene's test and ANOVA results</b>
<b>Bone lengths:</b>					
Total Leg Length	< 0.001	3,34.7	968.5	< 0.001	
<b>Segment properties:</b>					
Whole Body CoM (cranial-caudal)	0.435	2,12	6.629	0.011	
Whole Body CoM (Dorsal-ventral)	0.475	2,11	16.729	< 0.001	
<b>Trunk:</b>					Degrees of freedom =
Mass	0.295	2,12	11.638	0.002	(df <sub>between</sub> ,
CoM position	0.193	2,12	3.227	0.076	df <sub>within</sub> ).
Radius of gyration (x)	<0.001	2,7.1	2.088	0.194	Where the
Radius of gyration (y)	0.004	2,4.881	9.732	0.020	assumption
Radius of gyration (z)	0.171	2,12	4.551	0.034	of equal
<b>Thigh:</b>					variances
Mass	0.180	2,12	13.65	0.001	cannot be
CoM position	0.547	2,12	30.675	< 0.001	met
Radius of gyration (x)	0.555	2,11	0.108	0.899	(significant
Radius of gyration (y)	0.508	2,12	0.514	0.611	Levene's test
Radius of gyration (z)	0.103	2,12	0.099	0.907	result), the
<b>Drumstick:</b>					Welch
Mass	0.002	2,6.885	69.702	< 0.001	statistics are
CoM position	0.054	2,12	1.261	0.318	reported.
Radius of gyration (x)	0.358	2,12	3.902	0.050	
Radius of gyration (y)	0.270	2,12	1.024	0.388	
Radius of gyration (z)	0.441	2,12	4.533	0.034	
<b>Shank:</b>					
Mass	0.583	2,12	4.820	0.029	
CoM position	0.503	2,12	7.985	0.006	
Radius of gyration (x)	0.129	2,12	31.746	< 0.001	
Radius of gyration (y)	0.012	2,5.542	1.297	0.695	
Radius of gyration (z)	0.301	2,12	59.342	<0.001	
<b>Foot:</b>					
Mass	0.295	2,12	18.969	<0.001	
CoM position	0.502	2,12	13.332	0.001	
Radius of gyration (x)	0.027	2,6.047	4.376	0.465	
Radius of gyration (y)	0.189	2,12	1.920	0.001	
Radius of gyration (z)	0.027	2,5.831	2.367	0.717	