

# Gait changes in a line of mice artificially selected for longer limbs

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In legged terrestrial locomotion, the duration of stance phase, i.e., when limbs are in contact with the substrate, is positively correlated with limb length, and negatively correlated with the metabolic cost of transport. These relationships are well documented at the interspecific level, across a broad range of body sizes and travel speeds. However, such relationships are harder to evaluate within species (i.e., where natural selection operates), largely for practical reasons, including low population variance in limb length, and the presence of confounding factors such as body mass, or training. Here, we compared spatiotemporal kinematics of gait in Longshanks, a long-legged mouse line created through artificial selection, and in random-bred, mass-matched Control mice raised under identical conditions. We used a gait treadmill to test the hypothesis that Longshanks have longer stance phases and stride lengths, and decreased stride frequencies in both fore- and hind limbs, compared with Controls. Our results indicate that gait differs significantly between the two groups. Specifically, and as hypothesized, stance duration and stride length are 8-10% greater in Longshanks, while stride frequency is 8% lower than in Controls. However, there was no difference in the touch-down timing and sequence of the paws between the two lines. Taken together, these data suggest that, for a given speed, Longshanks mice take significantly fewer, longer steps to cover the same distance or running time compared to Controls, with important implications for other measures of individual variation in whole-organism performance, such as the metabolic cost of transport.

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16 **ABSTRACT**

17           In legged terrestrial locomotion, the duration of stance phase, i.e., when limbs are in contact  
18 with the substrate, is positively correlated with limb length, and negatively correlated with the  
19 metabolic cost of transport. These relationships are well documented at the interspecific level, across a  
20 broad range of body sizes and travel speeds. However, such relationships are harder to evaluate within  
21 species (i.e., where natural selection operates), largely for practical reasons, including low population  
22 variance in limb length, and the presence of confounding factors such as body mass, or training. Here,  
23 we compared spatiotemporal kinematics of gait in Longshanks, a long-legged mouse line created  
24 through artificial selection, and in random-bred, mass-matched Control mice raised under identical  
25 conditions. We used a gait treadmill to test the hypothesis that Longshanks have longer stance phases  
26 and stride lengths, and decreased stride frequencies in both fore- and hind limbs, compared with  
27 Controls. Our results indicate that gait differs significantly between the two groups. Specifically, and as  
28 hypothesized, stance duration and stride length are 8-10% greater in Longshanks, while stride frequency  
29 is 8% lower than in Controls. However, there was no difference in the touch-down timing and sequence  
30 of the paws between the two lines. Taken together, these data suggest that, for a given speed,  
31 Longshanks mice take significantly fewer, longer steps to cover the same distance or running time  
32 compared to Controls, with important implications for other measures of individual variation in whole-  
33 organism performance, such as the metabolic cost of transport.

34


35 **INTRODUCTION**


36           In terrestrial legged locomotion, a stride is divided into two phases: stance, when the foot/paw  
37 is in contact with the ground, and swing, when the foot leaves the substrate as the limb transitions to  
38 the next stance phase. Stance duration is influenced by a number of anatomical and biomechanical  
39 factors, including limb length. Limb length is positively correlated with step length, the distance traveled  
40 while a foot is in contact with the ground. As stance duration is simply step length divided by travel  
41 speed, for a given travel speed, organisms with relatively longer limbs typically have longer stance  
42 durations [1]. [Stance duration is itself an important determinant of whole-organism performance,](#)  
43 [especially in relation to the metabolic cost of moving the body.](#) During level walking and running, muscle  
44 forces produced by the limbs, integrated over the stance phase, must equal bodyweight integrated over  
45 the whole stride. Longer stance phases reduce muscle force production rates per unit of body mass, in  
46 turn reducing the overall metabolic cost of supporting the body during locomotion [2-5]. Hence, it  
47 follows that organisms with longer limbs and stance durations also tend to have a relatively lower mass-  
48 specific metabolic cost per unit of distance traveled, often called the cost of transport or COT ( $\text{J kg}^{-1} \text{m}^{-1}$ )  
49 [2, 4].

50           The relationships between limb length, stance duration (also known as “contact time”) and COT  
51 are well documented at the interspecific level, e.g., among terrestrial quadrupedal mammals in which  
52 limb length and COT data were sampled from the same individuals [1-4, 6-8]. In contrast, these  
53 relationships have been more equivocal at the population level, where differences among individuals in  
54 whole organism performance due to variation in these factors have the potential to lead to differential  
55 reproductive success (i.e., where natural selection operates [9]). [Several studies in human populations,](#)  
56 [have shown a correlation between limb length and gait variables such as stance duration \[10-12\] , as](#)  
57 [well as between limb length and COT in walking and running, after controlling for other factors that](#)

58 influence COT, such as body mass (e.g., Refs [13-18], but see also Ref. [19]). Fewer intraspecific studies  
59 have examined the relationships between hind limb length, kinematics, and COT within quadrupedal  
60 species, and these are limited to comparisons among breeds of dogs or horses. Longer limbs are  
61 associated with greater stance duration in dogs [20, 21] and horses [22, 23], but while hind limb length  
62 can be predictive of COT in dogs [13], taller horses do not necessarily have lower COT [24].

63 One of the practical challenges in relating limb length to locomotor mechanics among  
64 individuals *within* populations, is that only a limited range of limb lengths can realistically be sampled,  
65 meaning that either variation in skeletal anatomy is too small to detect subtle effects of leg length on  
66 gait (i.e., a low signal-to-noise ratio), or impractically large samples are necessary to do so.

67 Another important limitation of the comparative approach to studying the relationship between  
68 limb anatomy and locomotor mechanics - both within and between species - is the complexity of teasing  
69 apart the relative impact on gait of body mass, skeletal anatomy, posture and other biological factors  
70 (e.g., proportions of muscle fiber types [25]). Within species, many of these factors are genetically and  
71 phenotypically correlated, and interact with each other, and with other factors such as age, body  
72 composition (e.g., lean mass), and training, which makes it harder to quantify the relative contributions  
73 of limb length alone to gait variation among individuals. For example, among artificially bred dog and  
74 horse species, differences in size and limb length are typically correlated with other changes in body  
75 proportions and conformation can affect kinematics and may influence metabolic cost [21, 22]. 

76 Similarly, among species, fundamental differences in posture (e.g., quadrupedalism vs bipedalism, limb  
77 joint extension angles, limb design (e.g., plantigrady vs unguligrady) and orders of magnitude of   
78 differences in body mass may also obscure the effects of limb skeletal anatomy on locomotor mechanics  
79 [26].

80 Here, we use an experimental evolution model to explore the relationship between limb length  
81 and locomotor kinematics. Longshanks mice have been selectively bred for increases in tibia length  
82 independently of body mass [27, 28]. After 14 generations, Longshanks tibiae were on average 14%  
83 longer than a random-bred wild-type cohort of the same genetic background (hereafter Controls), but  
84 average body masses were the same in both groups. By pooling Longshanks and Control mice, we have  
85 created a new population of mice in which the range of variation in limb length is artificially increased,  
86 thereby circumventing sample size and resolution issues. More importantly, in this sample the  
87 potentially confounding effects of body mass, diet, training, somatic growth, age and even genetic  
88 background, are more rigorously controlled. We used the unique Longshanks mouse to investigate the  
89 proximate relationships between limb morphology and locomotor mechanics within species. We test  
90 the hypothesis that, at a given speed, increased limb length produces predictable changes in gait  
91 parameters. Specifically, we predict an increase in stance duration and stride length, and a parallel  
92 decrease in stride frequency.

## 93 METHODS

### 94 1. Samples

95 All animal procedures were approved by the Health Sciences Animal Care Committee at the  
96 University of Calgary (protocol AC13-0077), and were conducted in accordance with best practices  
97 outlined by the Canadian Council on Animal Care. We used a sex-balanced sample of adult mice ( $156 \pm$   
98 17 days, mean  $\pm$  SD) selected at random from 12 Longshanks families (hereafter LS,  $n=11$  females, 11  
99 males) and 12 Control families (hereafter C,  $n=12$  females, 11 males) lines at generation F14. Details of  
100 the selective breeding protocol are given elsewhere [27]. Mice were housed individually and kept under  
101 similar environmental conditions, in a separate room from the main colonies of the selective breeding  
102 experiment, maintained at 22-25C, humidity 50-70% on a 12-hour light/dark cycle. Mice were given food



103 and water ad libitum. ~~The food provided was a low-fat food (low-fat Pico-Vac lab rodent chow (20%~~  
104 ~~protein, 4.5% fat).~~

## 105 2. Gait data collection and analysis

### 106 a) Gait treadmill procedure

107 *Training phase:* Beginning at 10 weeks old, each mouse completed a total of eight training trials  
108 on a closed chamber treadmill (Columbus Instruments, Columbus, OH) over the course of five months.  
109 In the first two trials, the treadmill was inactive, as these trials allowed the mice to acclimate to the  
110 novel treadmill environment. For the remaining six trials, mice completed an initial 5-10-minute  
111 habituation period, followed by a running schedule as follows: four minutes at 5 m/min, three minutes  
112 at 10m/min, three minutes at 15m/min, three minutes at 20m/min, and a 90 second cool-down period.

113 Within three days of completing the final training trial, gait data for each mouse were collected  
114 using a TreadScan gait treadmill (Cleversys, Reston, VA). Mice were weighed to the nearest 0.01g prior  
115 to being placed in the treadmill. The TreadScan apparatus comprises a transparent, variable-speed  
116 treadmill belt (190mm L, 38mm W) enclosed within a Plexiglas chamber. While mice run on the  
117 treadmill, their paw placements are recorded on the ventral surface through the use of a mirror placed  
118 at 45 degrees to a high-speed camera recording at 100 frames per second. To improve digital tracking of  
119 footprints, the contrast between paws and fur was enhanced by applying red food coloring to the  
120 plantar surfaces of the paws. The mice were run for approximately three minutes during which three 20-  
121 second digital video recordings were taken at each of three test speeds: 10, 15, and 20 m/min. After the  
122 first video was captured, each foot was manually traced for approximately 20 frames (equivalent to a  
123 full locomotor cycle) to create a foot model for all subsequent analyses.

124

125 *b) Gait variables and analysis*

126 The TreadScan software automatically tracks stance and swing phases of each paw and  
127 subsequently generates multiple gait variables from the video footage. A Matlab script (v.2012b, Reston,  
128 MA) was first used to extract gait variables from the TreadScan output spreadsheet from all individual  
129 strides recorded for each mouse at each speed. For consistency, and because lighting and visibility of  
130 kinematics was better for the animal's right side, only gait variables for the right forelimb and hind limb  
131 paws were used for analysis, with the exception of the touch-down sequence of the four paws (see  
132 below).

133 The following variables were obtained for the right fore- and hind limb paws from the TreadScan  
134 output spreadsheets: (1) Stance Time: Time (ms) during which that foot was in contact with the belt; (2)  
135 swing time (ms): time during which that foot is not in contact with the treadmill; (3) Stride Length (mm):  
136 distance travelled between two stance phases of the same foot. Note that, as the mice are stationary  
137 relative to the treadmill, stride length is estimated as the product of stride time (i.e., stance time plus  
138 swing time) and treadmill belt speed; (4) stride Frequency (Hz): 1/mean stride duration. To determine  
139 whether the increased limb length of Longshanks resulted in a change in its gait sequence relative to  
140 Controls, we also obtained timing data for each paw during a full stride cycle. Specifically, using the  
141 initiation of stance in the right forepaw as a reference, we obtained the relative timing of touch-down  
142 for the other paws, expressed as a percentage of a full stride cycle.

143 A second Matlab (v.2012b, Reston, MA) script was used to obtain means for each gait parameter  
144 in each individual's right fore- and hind limb paws, based on one or more sets of at least three  
145 consecutive steps. Outliers, defined as data points that were greater than two standard deviations away  
146 from their respective means, were removed and the mean was recalculated. Individuals' gait variable  
147 means were based on a minimum of 3 steps in each limb type and speed condition (mean: 17 steps,



148 range 3 – 63). Videos of the slowest speed, 10m/min, were excluded from our analyses due to the  
149 difficulty in selecting a section of video with enough consecutive strides to obtain reliable gait patterns  
150 ~~at this relatively slow speed.~~

151 Statistical analyses of the gait and gait sequence variables were performed using four separate  
152 sets of generalized linear models (GLM). In the first two sets, GLMs were used to test for mean  
153 differences between lines (LS1 vs C) and speeds (20 and 25 m/min) in each gait variable *within* a limb  
154 type. In the third set of GLMs, we compared mean fore- and hind limb gait variables between the mouse  
155 lines at the fastest speed. Finally, we used a GLM to test for mean differences between lines and speeds  
156 in gait sequence variables. In all GLMs, we first used a full factorial model, in which line, speed or limb  
157 type were treated as categorical predictors, and body mass was included as a continuous predictor  
158 (covariate). The models included interaction terms for the respective categorical factors (i.e., Line x  
159 Speed, or Line x Limb Type), as well as covariate-by-factor interaction terms (i.e., homogeneity of slopes  
160 tests). In all but one variable (see below), none of the covariate-by-factor interaction terms were  
161 significant, i.e., the effect of the categorical factors (e.g., speed) on the responses (gait variables) was  
162 not dependent on the magnitude of body mass. As argued by Engqvist [29], in the absence of significant  
163 covariate-by-factor interaction terms, GLM analyses should be re-run without these terms, as failing to  
164 exclude them implies that the main effects of the factors cannot be generalized over the range of the  
165 covariate. Conversely, however, a significant covariate-by-factor interaction term indicates that any  
166 significant mean differences among the factors are only true at the intercept, i.e., where the covariate –  
167 body mass in this case - is equal to 0.

168 In the fourth set of GLM analyses, we found a significant interaction between mouse line and  
169 body mass in the timing of touch-down of the left hind paw relative to the right forepaw ( $F(7,82) = 4.04$ ,  
170  $p=0.047$ ). However, the inclusion of this interaction term had only a small effect on the least squares

171 (LS) means among groups. For example, at the covariate mean (42.93g), the difference in LS means  
172 when the interaction term was excluded vs. included was less than 1% across all groups (range: 0.4-  
173 0.9%), while at the 10<sup>th</sup> and 90<sup>th</sup> percentile of body mass this difference was less than 10% (range: 4.5-  
174 9.5%). Hence, given its modest impact on the actual gait variable response over the covariate range, and  
175 to be consistent with the remaining analyses, we excluded all covariate x factor interactions from this  
176 GLM. In all GLM analyses, relevant post-hoc pairwise comparisons on all gait variables were made using  
177 Tukey's HSD tests. All analyses were carried out in Statistica software (v.10.0, Statsoft, Tulsa, OK).

### 178 *3. Morphometric Data Collection and Analysis*

179           After completing the gait trials, mice were euthanized by CO<sub>2</sub> inhalation, weighed and  
180 immediately frozen at -20C. As part of an ongoing digital tomography archive of the Longshanks  
181 experiment, full body micro-CT scans were made using a Skyscan 1173  $\mu$ CT scanner at a resolution of 45  
182  $\mu$ m (65-70 kV, 75-105  $\mu$ A). One of the Longshanks bodies was not recovered following euthanasia. 3D  
183 isosurfaces of the scans were produced using Amira v.5.4.2 (Visage Imaging, Berlin, Germany). Bone  
184 lengths were determined by calculating the linear distance between 3D digital landmarks placed on  
185 specific anatomical features of the limb long bones. Micro-CT measurements are superior to linear  
186 measurements from dissected limbs, as soft tissues are not visible on the  $\mu$ CT scans, and the placement  
187 of digital landmarks on homologous anatomical features across individuals is highly repeatable[28].

188           The following anatomical features were used for landmark placements: (1) humerus length –  
189 from the center of the proximal articular surface to the distal-most point on the medial epicondyle, (2)  
190 ulna length – from the tip of the olecranon process to the tip of the styloid process, (3) carpo-  
191 metacarpus – from the proximal articular facet of the central carpal to the tip of the distal articular  
192 facet, (4) scapula length – from the caudal end of the spine of the scapula to the tip of the center of the  
193 glenoid (5) third manual proximal phalanx - from the center of the proximal to the center of the distal

194 articular facets, (6) femur length - from the center of the medial condyle to the tip of the greater  
195 trochanter, (7) tibia length – from the anterior-most lip on the proximal epiphysis to the most distal  
196 point on the medial malleolus, (8) tarso-metatarsus – from the proximal dorsal border of the centrale  
197 tarsal bone to the dorsal border of the distal articular facet of the third metatarsal, (9) third pedal  
198 proximal phalanx - from the center of the proximal to the center of the distal articular facets. Limb bone  
199 lengths were also summed within limb to obtain forelimb and hind limb anatomical lengths. Two-tailed  
200 t-tests were used to compare mean body mass and limb bone lengths between the groups.

## 201 RESULTS

### 202 *Morphometric differences*

203 Mean body mass was not significantly different between Control and Longshanks mice in either  
204 the test trials or the *ex vivo* CT scanning (**Table 1**). In the forelimb, all bones were significantly longer in  
205 Longshanks when compared to Control mice. Longshanks scapulae were on average 6.6% longer, humeri  
206 were ~12.5% longer, ulnae ~10.7%, and the hand bones (carpo-metacarpus and third proximal phalanx)  
207 were ~4% longer. When summed across the elements, the anatomical length of the forelimb in  
208 Longshanks, including the scapula [30, 31] was on average 9.1%, or approximately 4.2 mm, longer than  
209 Control forelimbs. Hind limb bones were all significantly longer in Longshanks mice compared to the  
210 Control mice: Longshanks mice had a 7.4% longer femur, 14.3% longer tibia (**Figure 1**), 9.5 % longer  
211 tarso-metatarsus, and 9.3% longer pedal proximal phalanx (Table 1). When summed across elements  
212 (femur + tibia + foot elements), the Longshanks hind limb was on average 10.7%, or 5.2 mm, longer than  
213 Control hind limbs. Selection for relative tibia length in Longshanks thus caused disproportionate  
214 changes in the other limb bones, such that overall the Longshanks forelimb increased in length slightly  
215 less than the hind limb, although the mean difference in length between the limbs is not significantly

216 different between Longshanks (mean  $\pm$  SD = 2.84 $\pm$ 2.85mm) and Control (1.89 $\pm$ 2.08mm) (**Table 1**, t-test,  
217  $t(42) = 1.27$ ,  $p = 0.21$ ).

### 218 *Gait differences*

219 *Line and speed effects on gait within limbs:* The first two sets of GLMs indicate that body mass  
220 was not significantly correlated with any gait variable in the forelimb, but in the hind limb was  
221 significantly negatively correlated with swing duration, and positively correlated with stance duration  
222 (**Table 2**). Both speed and line type had significant effects on forelimb and hind limb stance duration,  
223 stride length and stride frequency (Table 2, all standardized slopes significantly different from zero,  
224  $p < 0.001$ ). In the forelimb, speed had a significant effect on swing duration, while in the hind limb there was  
225 no change in swing duration due to speed (Table 2). There was no significant interaction between line  
226 type and speed in either limb, indicating that running faster did not affect gait variables in Longshanks  
227 and Control mice differently ( $0.19 < p < 0.92$ ).

228 Pairwise comparisons between lines indicate that at the lower speed, mean stance duration was  
229 significantly longer, by 10.7% in the forelimb and 9.1% in the hind limb, ~~respectively~~, in Longshanks  
230 compared to Controls (**Table 3, Figure 2**). At the faster speed, the difference between lines in mean  
231 forelimb stance duration (7.5%) trended towards significance (Tukey's HSD,  $p = 0.087$ ), while in  
232 Longshanks, hind limb stance duration was over 12.7% longer (Tukey's HSD,  $p < 0.001$ ). Swing durations  
233 did not differ between the lines in either limb, however forelimb swing times were significantly shorter  
234 at the faster speed (Table 3, Figure 2). Mean forelimb and hind limb stride lengths are greater by 7-8% in  
235 Longshanks at both speeds, while ~~similarly~~ mean stride frequency in both limbs at both speeds is  
236 decreased by 7-8% in Longshanks.

237 *Line and limb effects on gait within speed:* The GLM analysis with limb type and line as factors  
238 (fast speed only) revealed a significant effect of limb type on swing and stance durations in the

239 Longshanks mouse, with the forelimb having a relatively longer swing phase and shorter stance phase  
240 compared to the hind limb (Table 4, Tukey's HSD,  $p < 0.05$ ). As expected, however, stride duration, stride  
241 length and stride frequencies are the same between the fore- and hind limb within line. In other words,  
242 in Longshanks, stance duration as a percentage of stride duration (i.e., duty factor) is different in the  
243 forelimb and hind limb, but fore- and hind-limb cycles are of equal duration.

244 *Line and speed effects on gait sequence:* The mean relative timing of paw touch-downs is shown  
245 in Table 5, and gait sequences are shown in Figure 3. The GLM analysis showed no effect of line on gait  
246 sequence data, but speed had a significant effect on the gait sequence of the forepaws (standardized  
247  $\beta = -0.23$ ,  $F_{4,85} = 4.21$ ,  $p = 0.03$ ), with contact of the contralateral forepaw occurring 4-5% earlier at the  
248 faster speed in both lines (Tukey's post-hoc HSD,  $p = \text{n.s.}$ ). Combining the touch-down sequence and  
249 stance duration data at 20 m/min, both lines have very similar gait sequence profiles, although  
250 Longshanks mice have relatively longer hind limb stance phases (greater duty factors, Figure 3).

## 251 DISCUSSION AND CONCLUSION

252 Gait is influenced by a number of anatomical (e.g., mass, skeletal size) and biomechanical  
253 factors (e.g., speed, bipedal vs. quadrupedal locomotion). Limb length is positively correlated with step  
254 length, and hence with stance duration, in terrestrial species across a broad range of body sizes and limb  
255 lengths [1-3]. Whether this relationship also holds true within populations is less clear, however, largely  
256 due to the challenge of sampling adequate variation among individuals in limb bone length to detect  
257 subtle differences in gait, and sampling limb bone lengths that are not also correlated with other  
258 variables that influence gait.

259 We used the long-limbed Longshanks mouse line to test the hypothesis that these mice would  
260 have longer strides, longer stance durations and thus lower stride frequencies when compared to mice  
261 from a random-bred control group. Crucially, these two groups have been raised under the same

262 conditions and were trained on the treadmill using identical protocols. In addition, they have the same  
263 average body mass, and come from the same genetic background. Hence, we were able to isolate the  
264 effects of limb bone length on gait parameters from other potentially confounding factors such as  
265 training, speed and body mass.

266 Our results provide strong support for our hypothesis, in both limbs: at the lower speed  
267 Longshanks had 9-10% longer stance durations, 7-8% longer strides and stride durations, and thus 7-8%  
268 lower stride frequencies. At the faster speed, swing durations in the forelimb were reduced in both  
269 lines, while Longshanks' stance duration for the hind limb was longer by 12.7%. Overall, however, the  
270 differences in stride length and duration, and stride frequency between the lines in both limbs remained  
271 7-8% at 20 m/min. Interestingly, there was no difference between Longshanks and Control in swing  
272 times of either limb, at either speed. Equivalent swing times suggest that, despite its increase in bone  
273 lengths, the natural swing period of the limbs in Longshanks have not changed substantially relative to  
274 Controls, although this could also be due to greater muscle work to move the limb during the swing  
275 phase in Longshanks. Similar natural periods could result from a similar distribution of muscle mass in  
276 both lines, despite the increased limb length in Longshanks. Future work will more carefully assess ~~in~~  
277 ~~these populations to determine why their mean swing phase durations do not differ.~~

278 The gait sequence data show that the increase in limb length in Longshanks did not impact the  
279 relative timing and sequence of stance initiation in the four limbs at 20 m/min (Table 5, Figure 3).  
280 Moreover, the forelimb duty factors are very similar in both lines at this speed (~0.59, Table 4).  
281 However, the relatively longer stance duration of the Longshanks hind limbs at 20 m/min increases its  
282 duty factor slightly relative to Controls (0.647 vs 0.612, Table 4). The reasons for the longer stance  
283 duration in the Longshanks hind limb are unclear, but may relate to the fact that overall the Longshanks

284 hind limb increased in length slightly more than the forelimb as a result of selection on tibia length  
285 (Table 1).

286 One limitation of this study is the absence of kinematic data from lateral views of the limbs in  
287 these mice, which precludes us from determining precisely if and how limb protraction, retraction, and  
288 joint angles have changed in Longshanks as a consequence of changes in the relative lengths of its limb  
289 bones (Table 1). As a first approximation, we used our morphometric and gait data to estimate  
290 differences in joint angles in the hind limbs of Longshanks vs Controls, based on preliminary limb angular  
291 excursion data. Step length is the horizontal distance the hip travels while the paw is in contact with the  
292 substrate. On a treadmill, the proximal joints are effectively stationary, and step length represents  
293 instead the distance traveled by the paw while in contact with the treadmill belt. Stance on a treadmill  
294 can thus be modeled as a “support triangle”, described by the hip joint (vertex) and the points of paw-  
295 belt contact at touch-down and toe-off (Figure 4). The base of the triangle represents step length, the  
296 height is the vertical distance between the hip and substrate. The triangle’s sides represent the hind  
297 limb at touch-down and toe-off, and their lengths at these time points are determined by the limb’s  
298 joint angles and bone lengths.

299 When the limb angular excursion (i.e., the vertex angle) is known, the lengths of the triangle’s  
300 sides can be estimated. We obtained hind limb protraction and retraction angles from a small sample of  
301 Longshanks and Control mice from generation F22 (n = 5 each), running at 20 m/min (**Figure S1**). The  
302 hind limb protraction, retraction, and excursion angles did not differ significantly between the lines  
303 (**Table S1**), and the overall mean excursion angle was  $74.7^\circ \pm 2.8$  (mean  $\pm$ SEM). Thus, even though step  
304 length in Longshanks hind limbs was 12.7% longer, the angles in the support triangle in both lines were  
305 the same, implying that the hind limb support triangle’s sides in Longshanks are all also  $\sim$ 12.7% longer.  
306 Using the sine rule, we estimated the mean triangle side length at touch-down (i.e., protraction) to be

307 38.91mm in Controls, and 43.85mm in Longshanks, while at toe-off (retraction) mean lengths were  
308 28.09mm and 31.72mm, respectively (Figure S1).

309 Combining these support lengths with the mean lengths of the femur, tibia and tarso-  
310 metatarsus in each line (Table 1), and assuming that the hind paw at touch-down is horizontal and at  
311 toe-off the tarso-metatarsus is perpendicular to the treadmill (Figure S1), we solved graphically for  
312 mean knee and ankle joints in Longshanks and Control (Figure 4). Mean angles in Longshanks hind limbs  
313 are all very similar to Controls. The greatest difference is in the knee at touch-down, which is  $\sim 5^\circ$ , or 4%,  
314 more extended in Longshanks than in Control mice. This small difference may be due to the fact that the  
315 tibia and femur in Longshanks did not increase in length proportionately (+14.3% vs +7%). Overall, the  
316 10.7% increase in hind limb length in Longshanks likely accounts for much of the 12.7% increase in its  
317 hind limb step length, and necessitates only minor joint extensions at the knee and ankle in Longshanks  
318 (Figure 4). Limb angular changes in the forelimb are likely equally small, however given that the mean  
319 increase in forelimb step length (+7.5%) is less than the overall increase in forelimb length (+9%), the  
320 joint angular changes in that limb in Longshanks more likely entailed flexion rather than extension,  
321 absent any changes in forelimb excursion angles between the lines. More precise limb kinematics will  
322 clearly be required to confirm these data and determine the combination of changes adopted by  
323 Longshanks to increase step and stride lengths in both limbs.

324 Our findings have implications with respect to the cost of transport in Longshanks. The derived  
325 morphology of the Longshanks mouse altered its gait in a predictable fashion, resulting in increased  
326 stance durations and stride lengths relative to Controls. Both of these characteristics contribute to the  
327 cost of transport in terrestrial organisms. Increased stance time distributes the muscle forces necessary  
328 to support body weight over a longer interval, lowering the *rate* of muscle force production, i.e., the  
329 volume of muscle recruited per distance traveled [2-5]. Complementary to this, increasing stride length



330 reduces the number of steps required to cover a given distance, reducing activation costs [4]. Thus, our  
331 gait data predict that, all else being equal, including limb and joint angles as estimated above, the mass-  
332 specific cost of transport in Longshanks should be lower when compared with Control mice. We are  
333 currently testing this hypothesis with the use of a metabolic treadmill in Longshanks and Control.

334           Variation in whole organism performance directly impacts evolutionary fitness, and is an  
335 important driver of adaptive evolution [9, 32-34]. In the process of selecting for a target morphological  
336 trait (longer tibiae relative to body mass), we have “forward engineered” a morphology in Longshanks  
337 with a quantifiable impact on whole organism *biomechanical* performance. We do not yet know the  
338 impact of the observed change in gait on *physiological* performance (e.g., metabolism, especially cost of  
339 transport), and it is challenging to relate any differences in these measures of whole organism  
340 performance to differences in survival and reproductive success of Longshanks and Control mice in the  
341 wild, as these are laboratory-reared animals raised in highly controlled and homogeneous  
342 environments. Nevertheless, this study demonstrates the relationship of selectable phenotypic variation  
343 in skeletal anatomy to variation among individuals in whole organism performance, in the form of  
344 locomotor mechanics. Hence, it provides an important link between population-level, microevolutionary  
345 processes and the adaptive origins of macroevolutionary diversity in limb musculoskeletal anatomy  
346 among terrestrial mammals.

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350  $\mu$ CT scanner, and to Kevin Chapman in the Behavioral Core Facility in the Cumming School of Medicine  
351 (University of Calgary) for assistance with the TreadScan system. John Bertram and Douglas Syme  
352 provided useful feedback at several stages of the study, and their help is gratefully acknowledged. We  
353 also wish to thank three reviewers and the associate editor, for providing feedback and suggestions on a  
354 previous version of the manuscript.

355 **FIGURE CAPTIONS**

356 **Figure 1:**  $\mu$ CT scans of two individuals from the study sample closest to mean raw tibia length in Control  
357 (C, 18.85mm) and Longshanks (LS, 21.45mm).

358 **Figure 2:** Comparison of gait variables in Longshanks and Control mice at 15 and 20 m/min. Boxplots of  
359 swing duration (A, in milliseconds), stance duration (B, in milliseconds), stride length (C, in mm), and  
360 stride frequency (D, in seconds<sup>-1</sup>) in Longshanks (shaded box) and Control mice (open box). Horizontal  
361 lines within boxes represent medians, boxes indicate interquartile ranges, whiskers indicate non-outlier  
362 ranges, and outliers are indicated with black dots. Solid brackets below boxplots denote statistically  
363 significant mean differences between the lines within a speed, dotted brackets above boxplots indicate  
364 statistically significant differences between speeds within lines (at the  $p < 0.05$  level). For clarity,  
365 differences between limbs within speed are not shown (see Table 4).

366 **Figure 3:** Mean gait sequence in Control (grey boxes) and Longshanks (thin black boxes). The solid boxes  
367 represent the stance phases of each paw, the white boxes the swing phases. Total length, from 0 to 1,  
368 represents a full stride cycle of the right fore paw, where 0 touch-down and 1 = touch-down of the  
369 following cycle. The stance phase durations of the left paws are duplicated from the right side, as only

370 the latter were analyzed (see methods). Dashed boxes highlight the slightly longer stance time relative  
371 to stride time in the hind limbs of Longshanks. Abbreviations: LH = left hind paw, LF = left forepaw, RF =  
372 right forepaw, RH, right hind paw.

373 **Figure 4:** Diagram of the support triangle in Control (black) and Longshanks (red), obtained using mean  
374 step length and the mean protraction, retraction and excursion angles from an unrelated sample of mice  
375 from both groups (n = 5 each). Step length (base of the support triangle) and these angles were used to  
376 obtain the lengths of sides of the support triangle in each group. Using the mean long bone lengths in  
377 each group (Table 1), we then solved graphically for angles at the ankle and knee, on the assumption that  
378 the tarso-metatarsus was approximately flat at touch-down, and perpendicular to the treadmill at toe-off  
379 (Figure S1).

380 **Figure S1:** Sample video footage of a mouse running on a treadmill, showing the frame at the initiation  
381 of stance for the right hind paw (A, touch-down), and the last frame before the initiation of the swing  
382 phase for the same limb (B, toe-off). A stick model of the right hind limb is superimposed on each frame,  
383 showing the approximate location of the hip, knee, ankle and metatarsophalangeal joints (white circles),  
384 as well as the femur, tibia, tarso-metatarsus and forefoot (phalanges) (black lines). This model was used  
385 to estimate the protraction angle at touch down (P), and the retraction angle at toe-off (R). The sum of  
386 the protraction and retraction angles is the excursion angle.

#### 387 **TABLE CAPTIONS**

388 **Table 1:** Morphometric Data: Body masses at the gait (TreadScan) and  $\mu$ CT scanning stages, and fore-  
389 and hind limb bone lengths between Control and Longshanks mice, expressed as means (SEM).

390 Significance of the difference in means for all variables was determined using two-tailed t-tests. One  
391 Longshanks body was not recovered from euthanasia prior to scanning (n=21).

392 **Table 2:** Standardized coefficients (betas, with standard errors) for each predictor variable in the linear  
393 model for the gait variables in each limb. For Line, factor levels are Control = 0, Longshanks = 1, for  
394 Speed, factor levels are 15 m/min = 0, 20 m/min = 1. Covariate-by-factor interaction terms were  
395 excluded from the analyses (see Methods). The gait sequence data are shown as a fraction of the full  
396 stride cycle for the right forepaw (from 0 to 1).

397 **Table 3:** Limb gait parameters at 15 and 20 m/min in Longshanks (LS, N=22) vs Control (C, N=23) mice.  
398 Data reported as least squares means  $\pm$  SEM, based on a full factorial linear model, with Line and Speed  
399 as categorical factors, and body mass as a continuous predictor (see Table 2). Significance of differences  
400 in pairwise comparisons of means were determined using post-hoc Tukey's HSD tests. Statistical  
401 significance ( $p < 0.05$ ) of mean differences between lines within speed is indicated in bold, and between  
402 speeds within line with an asterisk. ( $p < 0.05$ ).

403 **Table 4:** Comparison of fore- and hind limb gait parameters at 20 m/min in Longshanks (LS, N=22) vs  
404 Control (C, N=23) mice. Data reported as least squares means  $\pm$  SEM, based on a full factorial linear  
405 model, with Line and Limb Type as categorical factors, and body mass as a continuous predictor.  
406 Significance of differences in pairwise comparisons of means were determined using post-hoc Tukey's  
407 HSD tests. Statistical significance ( $p < 0.05$ ) of mean differences between lines within limb type is  
408 indicated in bold, and between limb types within line with an asterisk. ( $p < 0.05$ ).

409 **Table 5:** Comparison of gait sequences in Longshanks and Control. Data reported as means  $\pm$  SEM, based  
410 on a full factorial linear model, with Line and Speed as categorical factors, and body mass as a  
411 continuous predictor. Means represent the proportion of a full stride cycle of the right forepaw (from 0  
412 = stance initiation to 1 = stance initiation of the next cycle) at which the other paws initiate their stance  
413 phases. No significant differences were found between lines within speed, or between speeds within  
414 line (Tukey's HSD tests).

415 **Table S1:** Comparison of limb excursion angles during stance in Control and Longshanks mice. Data  
416 reported as means  $\pm$  SEM (in degrees), in a sample of 10 mice unrelated to the mice used in this study.  
417 The angle values for each individual were based on 4-5 steps. No significant differences were found  
418 between the lines in any of the angles (two-tailed t-tests,  $0.13 < p < 0.83$ ).

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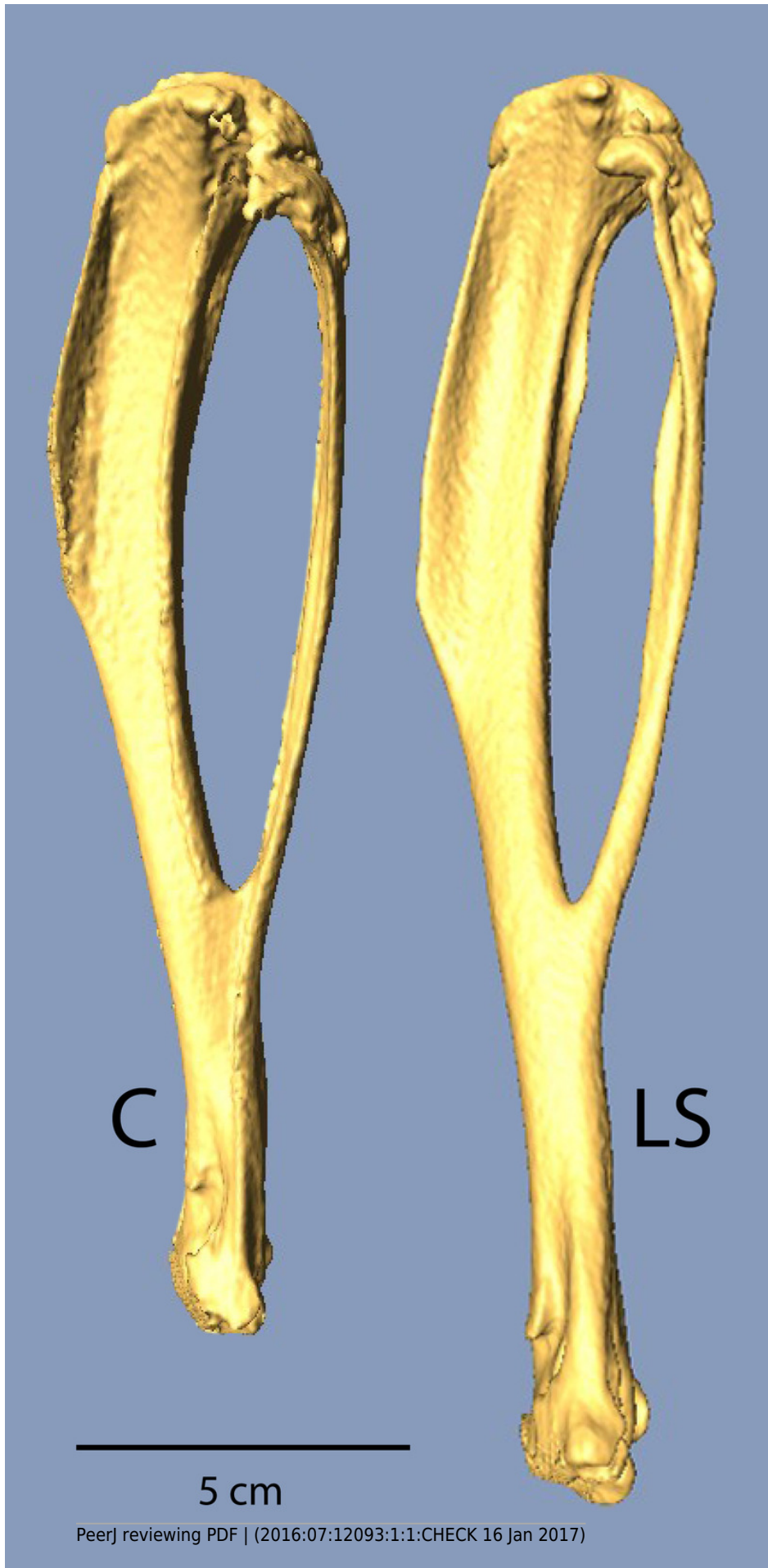
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501

# Figure 1

Figure 1 -  $\mu$ CT scans of Longshanks and Control tibiae

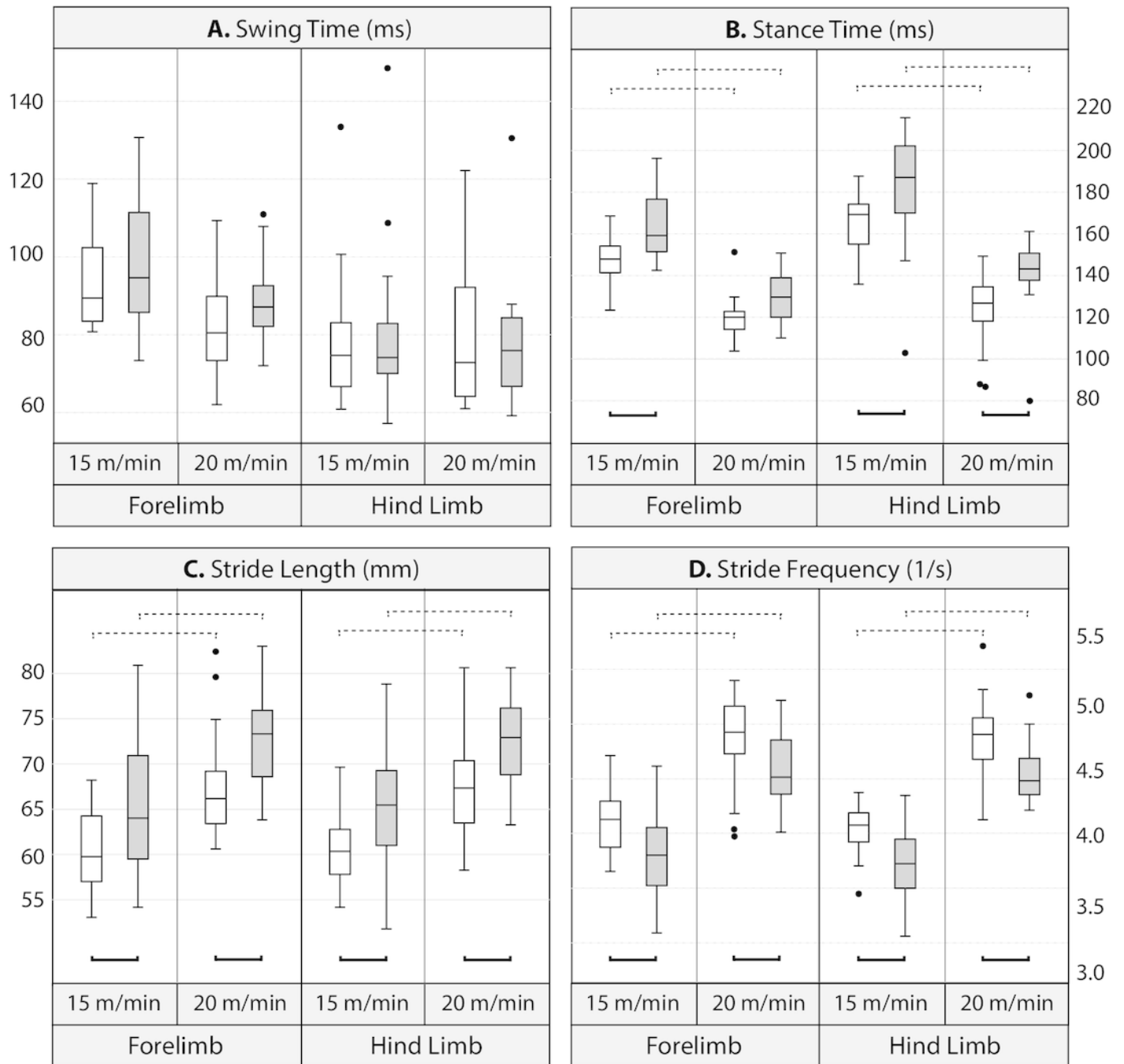
$\mu$ CT scans of two individuals from the study sample closest to mean raw tibia length in Control (C, 18.85mm) and Longshanks (LS, 21.45mm).



## Figure 2

### Figure 2 - Boxplots

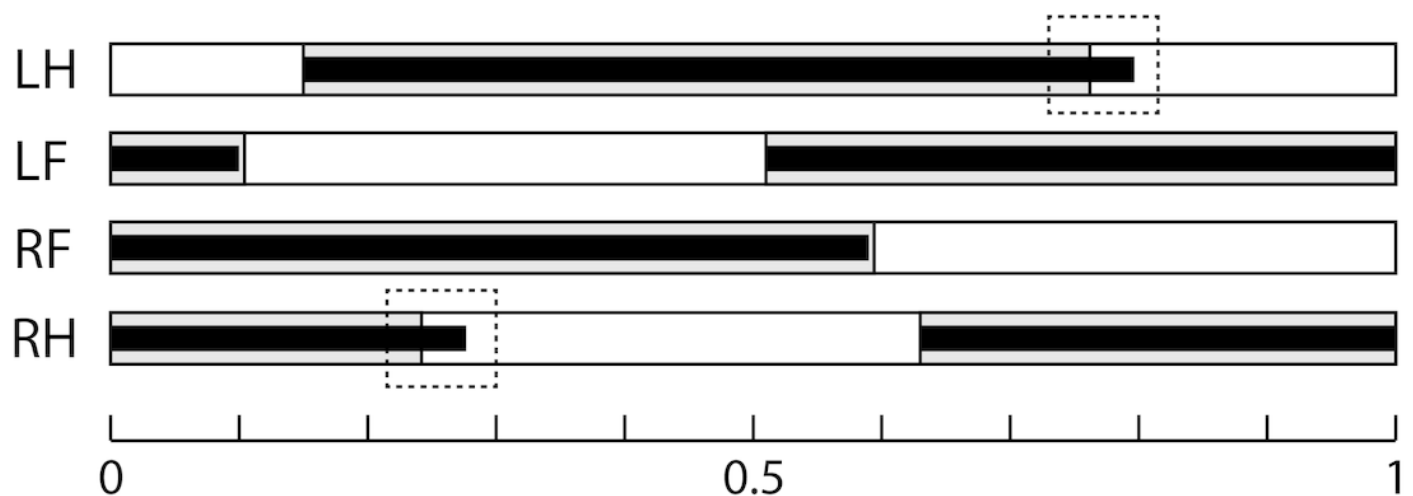
Comparison of gait variables in Longshanks and Control mice at 15 and 20 m/min. Boxplots of swing duration (A, in milliseconds), stance duration (B, in milliseconds), stride length (C, in mm), and stride frequency (D, in seconds<sup>-1</sup>) in Longshanks (shaded box) and Control mice (open box). Horizontal lines within boxes represent medians, boxes indicate interquartile ranges, whiskers indicate non-outlier ranges, and outliers are indicated with black dots. Solid brackets below boxplots denote statistically significant mean differences between the lines within a speed, dotted brackets above boxplots indicate statistically significant differences between speeds within lines (at the  $p < 0.05$  level). For clarity, differences between limbs within speed are not illustrated (see Table 4).



## Figure 3

Figure 3 - Gait Sequence

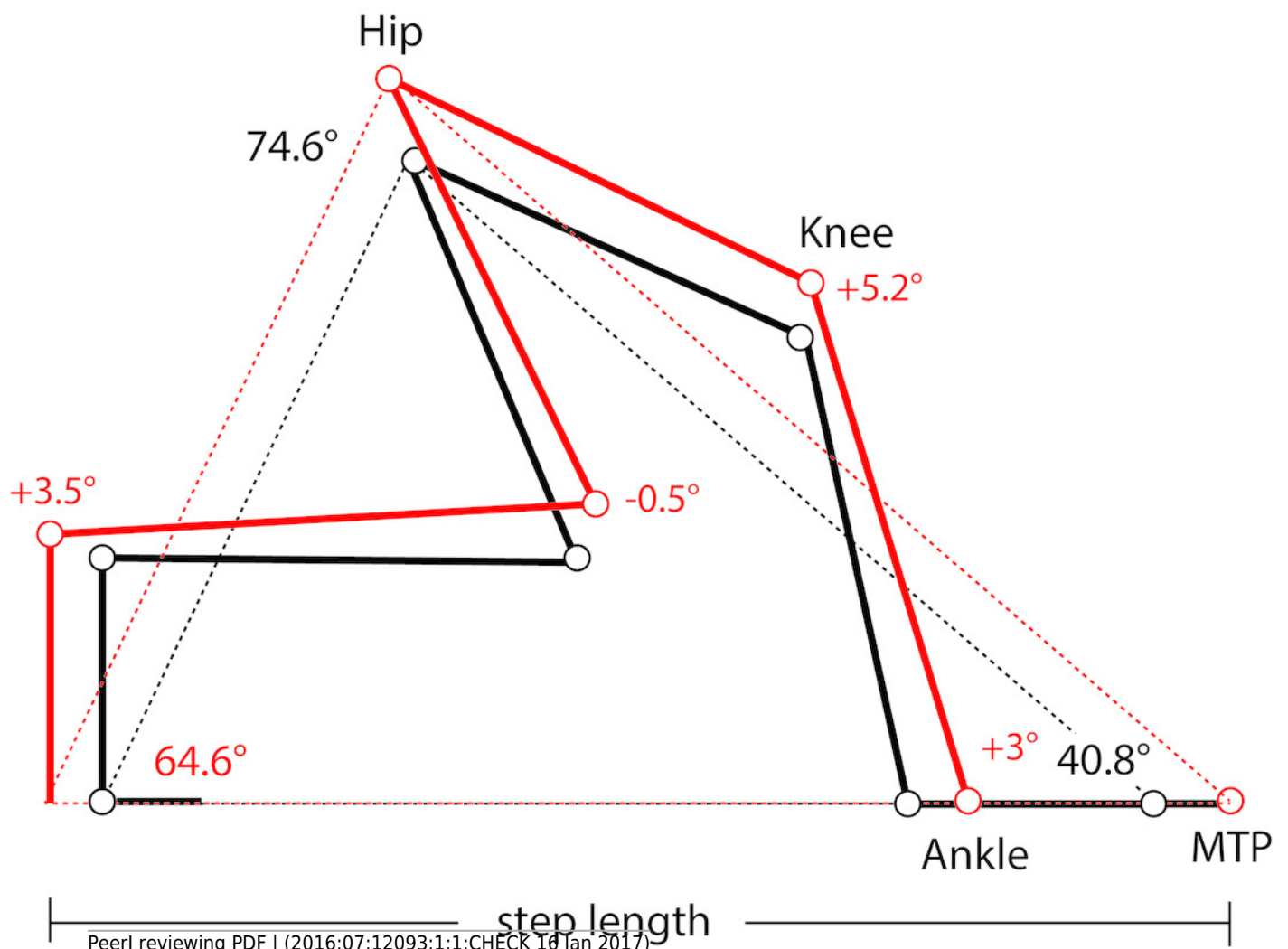
Mean gait sequence in Control (grey boxes) and Longshanks (thin black boxes). The solid boxes represent the stance phases of each paw, the white boxes the swing phases. Total length, from 0 to 1, represents a full stride cycle of the right fore paw, where 0 touch-down and 1 = touch-down of the following cycle. The stance phase durations of the left paws are duplicated from the right side, as only the latter were analyzed (see methods). Dashed boxes highlight the slightly longer stance time relative to stride time in the hind limbs of Longshanks. Abbreviations: LH = left hind paw, LF = left forepaw, RF = right forepaw, RH, right hind paw



## Figure 4

Figure 4 - Support Triangle

Diagram of the support triangle in Control (black) and Longshanks (red), obtained using mean step length and the mean protraction, retraction and excursion angles from an unrelated sample of mice from both groups ( $n = 5$  each). Step length (base of the support triangle) and these angles were used to obtain the lengths of sides of the support triangle in each group. Using the mean long bone lengths in each group (Table 1), we then solved graphically for angles at the ankle and knee, on the assumption that the tarso-metatarsus was approximately flat at touch-down, and perpendicular to the treadmill at toe-off (Figure S1).



**Table 1** (on next page)

## Table 1

Morphometric Data: Body masses at the gait (TreadScan) and  $\mu$ CT scanning stages, and fore- and hind limb bone lengths between Control and Longshanks mice, expressed as means (SEM). Significance of the difference in means for all variables was determined using two-tailed t-tests. One Longshanks body was not recovered from euthanasia prior to scanning (n=21).



- 1 **Table 1:** Morphometric Data: Body masses at the gait (Treadscan) and  $\mu$ CT scanning stages, and fore-
- 2 and hind limb bone lengths between Control and Longshanks mice, expressed as means (SEM).
- 3 Significance of the difference in means for all variables was determined using two-tailed t-tests.. One
- 4 Longshanks body was not recovered from euthanasia prior to scanning (n=21).

	Longshanks (n=21)	Control (n=23)	Statistic
Body mass (gait trials) (g)	43.73 (1.31) (n=22)	42.18 (1.27)	t = 0.84, df = 43, p = 0.40
Body mass ( $\mu$ CT scan) (g)	45.81 (1.43)	44.55 (1.60)	t = 0.58, df = 42, p = 0.56
Scapula	13.83 (0.15)	12.97 (0.08)	t = 5.07, df = 42, p < 0.001
Humerus	13.65 (0.11)	12.17 (0.07)	t = 12.02, df = 42, p < 0.001
Ulna	17.02 (0.13)	15.36 (0.08)	t = 11.34, df = 42, p < 0.001
Carpo-metacarpus	4.43 (0.04)	4.26 (0.03)	t = 3.69, df = 42, p < 0.001
Manual proximal phalanx 3	2.14 (0.02)	2.06 (0.02)	t = 2.89, df = 42, p < 0.01
Femur	18.5 (0.25)	17.2 (0.17)	t = 4.39, df = 42, p < 0.001
Tibia	21.44 (0.33)	18.75 (0.18)	t = 7.37, df = 42, p < 0.001
Tarso-metatarsus	10.62 (0.17)	9.7 (0.10)	t = 4.79, df = 42, p < 0.001
Pedal proximal phalanx 3	3.35 (0.06)	3.06 (0.03)	t = 4.47, df = 42, p < 0.001
Forelimb	51.07 (0.38)	46.82 (0.20)	t = 10.11, df = 42, p < 0.001
Hind limb	53.91 (0.76)	48.71 (0.43)	t = 6.11, df = 42, p < 0.001

5

**Table 2** (on next page)

## Table 2

Standardized coefficients (betas, with standard errors) for each predictor variable in the linear model for the gait variables in each limb. For Line, factor levels are Control = 0, Longshanks = 1, for Speed, factor levels are 15 m/min = 0, 20 m/min = 1. Covariate-by-factor interaction terms were excluded from the analyses (see Methods). The gait sequence data are shown as a fraction of the full stride cycle for the right forepaw (from 0 to 1).

- 1 **Table 2:** Standardized coefficients (betas, with standard errors) for each predictor variable in the linear  
 2 model for each gait variable in each limb. For Line, factor levels are Control = 0, Longshanks = 1, for  
 3 Speed, factor levels are 15 m/min = 0, 20 m/min = 1. Covariate-by-factor interaction terms were  
 4 excluded from the analyses (see methods). The gait sequence data are shown as a fraction of the full  
 5 stride cycle for the right forepaw.

	Effect	Swing (ms)	Stance (ms)	Stride Length (mm)	Stride Freq. (1/s)
<b>FORELIMB</b>	Mass	0.102 (0.098)	0.006 (0.064)	0.068 (0.085)	-0.057 (0.068)
	Line	0.183 (0.098)	0.296 (0.064)**	0.362 (0.085)**	-0.293 (0.068)**
	Speed	-0.373 (0.098)**	-0.752 (0.063)**	0.503 (0.084)**	0.720 (0.067)**
	Line*Speed	0.051 (0.098)	-0.082 (0.063)	0.010 (0.084)	-0.034 (0.067)
<b>HIND LIMB</b>	Mass	-0.308 (0.104)*	0.2 (0.065)*	0.023 (0.084)	-0.030 (0.064)
	Line	0.033 (0.104)	0.27 (0.065)**	0.358 (0.084)**	-0.312 (0.064)**
	Speed	-0.021 (0.103)	-0.72 (0.065)**	0.522 (0.083)**	0.745 (0.064)**
	Line*Speed	-0.06 (0.103)	0.006 (0.065)	0.015 (0.083)	-0.002 (0.064)

6 \* p < 0.05, \*\* p < 0.001

**Table 3** (on next page)

## Table 3

Limb gait parameters at 15 and 20 m/min in Longshanks (LS, N=22) vs Control (C, N=23) mice. Data reported as least squares means  $\pm$  SEM, based on a full factorial linear model, with Line and Speed as categorical factors, and body mass as a continuous predictor (see Table 2). Significance of differences in pairwise comparisons of means were determined using post-hoc Tukey's HSD tests. Statistical significance ( $p < 0.05$ ) of mean differences between lines within speed is indicated in bold, and between speeds within line with an asterisk. ( $p < 0.05$ ).

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 4 pairwise comparisons of means were determined using post-hoc Tukey's HSD tests. Statistical  
 5 significance ( $p < 0.05$ ) of mean differences between lines within speed are indicated in bold, and between  
 6 speeds within line with an asterisk. ( $p < 0.05$ ).

	Speed	Line	Swing (ms)	Stance (ms)	Stride Length (mm)	Stride Freq. (1/s)
FORELIMB	15m/mi n	C	94.07 (2.66)*	<b>147.91 (2.64)*</b>	<b>60.50 (1.15)*</b>	<b>4.15 (0.07)*</b>
		LS	97.67 (2.72)*	<b>163.8 (2.7)*</b>	<b>65.35 (1.18)*</b>	<b>3.87 (0.07)*</b>
	20m/mi n	C	82.39 (2.66)*	119.77 (2.64)*	<b>67.31 (1.15)*</b>	<b>4.98 (0.07)*</b>
		LS	88.83 (2.72)*	128.75 (2.7)*	<b>72.45 (1.18)*</b>	<b>4.61 (0.07)*</b>
HIND LIMB	15m/mi n	C	77.07 (3.48)	<b>166.42 (3.67)*</b>	<b>60.87 (1.11)*</b>	<b>4.12 (0.06)*</b>
		LS	80.25 (3.56)	<b>181.57 (3.76)*</b>	<b>65.44 (1.13)*</b>	<b>3.78 (0.07)*</b>
	20m/mi n	C	78.4 (3.48)	<b>124.73 (3.67)*</b>	<b>67.63 (1.11)*</b>	<b>4.95 (0.06)*</b>
		LS	77.5 (3.56)	<b>140.55 (3.76)*</b>	<b>72.61 (1.13)*</b>	<b>4.60 (0.07)*</b>

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**Table 4**(on next page)

## Table 4

Comparison of fore- and hind limb gait parameters at 20 m/min in Longshanks (LS, N=22) vs Control (C, N=23) mice. Data reported as least squares means  $\pm$  SEM, based on a full factorial linear model, with Line and Limb Type as categorical factors, and body mass as a continuous predictor. Significance of differences in pairwise comparisons of means were determined using post-hoc Tukey's HSD tests. Statistical significance ( $p < 0.05$ ) of mean differences between lines within limb type is indicated in bold, and between limb types within line with an asterisk. ( $p < 0.05$ ).

- 1 **Table 4:** Comparison of fore- and hind limb gait parameters at 20 m/min in Longshanks (LS, N=22) vs  
 2 Control (C, N=23) mice. Data reported as least squares means  $\pm$  SEM, based on a full factorial linear  
 3 model, with Line and Limb Type as categorical factors, and body mass as a continuous predictor.  
 4 Significant differences in pairwise comparisons of means were determined using post-hoc Tukey's HSD  
 5 tests. Statistical significance ( $p < 0.05$ ) of mean differences between lines within limb type are indicated  
 6 in bold, and between limb types within line with an asterisk. ( $p < 0.05$ ).

Limb Type	Line	Swing (ms)	Stance (ms)	Stride (ms)	Stride Length (mm)	Stride Freq. (1/s)
FORE	C	82.04 (3)	120.12 (2.76)	<b>202.16 (3.32)</b>	<b>67.31 (1.11)</b>	<b>4.97 (0.07)</b>
	LS	89.2 (3.07)*	128.39 (2.82)*	<b>217.59 (3.39)</b>	<b>72.45 (1.13)</b>	<b>4.61 (0.07)</b>
HIND	C	78.88 (3)	<b>124.37 (2.76)</b>	<b>203.25 (3.32)</b>	<b>67.68 (1.11)</b>	<b>4.95 (0.07)</b>
	LS	77 (3.07)*	<b>140.93 (2.82)*</b>	<b>217.92 (3.39)</b>	<b>72.56 (1.13)</b>	<b>4.61 (0.07)</b>

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**Table 5** (on next page)

## Table 5

Comparison of gait sequences in Longshanks and Control. Data reported as means  $\pm$  SEM, based on a full factorial linear model, with Line and Speed as categorical factors, and body mass as a continuous predictor. Means represent the proportion of a full stride cycle of the right forepaw (from 0 = stance initiation to 1 = stance initiation of the next cycle) at which the other paws initiate their stance phases. No significant differences were found between lines within speed, or between speeds within line (Tukey's HSD tests).



1 **Table 5: Comparison of gait sequences in Longshanks and Control.** Data reported as means  $\pm$  SEM,  
 2 based on a full factorial linear model, with Line and Speed as categorical factors, and body mass as a  
 3 continuous predictor. Means represent the proportion of a full stride cycle of the right forepaw (from 0  
 4 = stance initiation to 1 = stance initiation of the next cycle) at which the other paws initiate their stance  
 5 phases. No significant differences were found between lines within speed, nor between speeds within

Speed	Line	Ipsilateral (right) hind paw	Contralateral (left) forepaw	Contralateral (right) hind paw
15m/min	C	0.63 (0.01)	0.53 (0.01)	0.16 (0.01)
	LS	0.63 (0.01)	0.54 (0.01)	0.16 (0.01)
20m/min	C	0.63 (0.01)	0.51 (0.01)	0.15 (0.01)
	LS	0.63 (0.01)	0.51 (0.01)	0.14 (0.01)

6 line (Tukey's HSD tests).

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