

# Biomechanical, physiological and anthropometrical predictors of performance in recreational runners

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**Background.** The maximal running speed ( $V_{MAX}$ ) determined on a graded treadmill test is well-recognized as a running performance predictor. However, few studies have assessed the variables that predict  $V_{MAX}$  in recreationally active runners. **Methods.** We used a mathematical procedure combining Fick's law and metabolic cost analysis to verify the relation between 1)  $V_{MAX}$  versus anthropometric and physiological determinants of running performance and, 2) theoretical metabolic cost versus running biomechanical parameters. Linear multiple regression and bivariate correlation were applied. We aimed to verify the biomechanical, physiological, and anthropometrical determinants of  $V_{MAX}$  in recreationally active runners. Fifteen recreationally active runners participated in this observational study. A Conconi and a steady-state running test were applied using a heart rate monitor and a simple video camera to register the physiological and mechanical variables, respectively. **Results.** Statistical analysis revealed that the speed at the second ventilatory threshold, theoretical metabolic cost, and fat-mass percentage confidently estimated the individual running performance as follows:  $V_{MAX} = 58.632 + (-0.183 * \text{fat percentage}) + (-0.507 * \text{heart rate percentage at second ventilatory threshold}) + (7.959 * \text{theoretical metabolic cost})$  ( $R^2=0.62$ ,  $p=0.011$ ,  $RMSE=1.50 \text{ km}\cdot\text{h}^{-1}$ ). Likewise, the theoretical metabolic cost was significantly explained ( $R^2=0.91$ ,  $p=0.004$ ,  $RMSE=0.013 \text{ a.u.}$ ) by the running spatiotemporal and elastic-related parameters (contact and aerial times, stride length and frequency, and vertical oscillation) as follows:  $\text{theoretical metabolic cost} = 10.421 + (4.282 * \text{contact time}) + (-3.795 * \text{aerial time}) + (-2.422 * \text{vertical oscillation})$

stride length) + (-1.711 \* stride frequency) + (0.107 \* vertical oscillation). **Conclusion.** Critical determinants of elastic mechanism, such as maximal vertical force and vertical and leg stiffness were unrelated to the metabolic economy.  $V_{MAX}$ , a valuable marker of running performance, and its physiological and biomechanical determinants can be effectively evaluated using a heart rate monitor, treadmill, and a digital camera, which can be used in the design of training programs to recreationally active runners.

1 **Biomechanical, physiological, and anthropometrical**  
2 **predictors of maximal velocity in recreationally active**  
3 **runners**

4  
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## 34 **Abstract**

35 **Background.** The maximal running speed ( $V_{MAX}$ ) determined on a graded treadmill test is well-  
36 recognized as a running performance predictor. However, few studies have assessed the variables  
37 that predict  $V_{MAX}$  in recreationally active runners. **Methods.** We used a mathematical procedure  
38 combining Fick's law and metabolic cost analysis to verify the relation between 1)  $V_{MAX}$  versus  
39 anthropometric and physiological determinants of running performance and, 2) theoretical  
40 metabolic cost versus running biomechanical parameters. Linear multiple regression and  
41 bivariate correlation were applied. We aimed to verify the biomechanical, physiological, and  
42 anthropometrical determinants of  $V_{MAX}$  in recreationally active runners. Fifteen recreationally  
43 active runners participated in this observational study. A Conconi and a steady-state running test  
44 were applied using a heart rate monitor and a simple video camera to register the physiological  
45 and mechanical variables, respectively. **Results.** Statistical analysis revealed that the speed at the  
46 second ventilatory threshold, theoretical metabolic cost, and fat-mass percentage confidently  
47 estimated the individual running performance as follows:  $V_{MAX} = 58.632 + (-0.183 * \text{fat}$   
48  $\text{percentage}) + (-0.507 * \text{heart rate percentage at second ventilatory threshold}) + (7.959 * \text{theoretical}$   
49  $\text{metabolic cost})$  ( $R^2=0.62$ ,  $p=0.011$ ,  $RMSE=1.50 \text{ km.h}^{-1}$ ). Likewise, the theoretical  
50 metabolic cost was significantly explained ( $R^2=0.91$ ,  $p=0.004$ ,  $RMSE=0.013 \text{ a.u.}$ ) by the running  
51 spatiotemporal and elastic-related parameters (contact and aerial times, stride length and  
52 frequency, and vertical oscillation) as follows:  $\text{theoretical metabolic cost} = 10.421 + (4.282 * \text{contact}$   
53  $\text{time}) + (-3.795 * \text{aerial time}) + (-2.422 * \text{stride length}) + (-1.711 * \text{stride frequency}) +$   
54  $(0.107 * \text{vertical oscillation})$ . **Conclusion.** Critical determinants of elastic mechanism, such as  
55 maximal vertical force and vertical and leg stiffness were unrelated to the metabolic economy.  
56  $V_{MAX}$ , a valuable marker of running performance, and its physiological and biomechanical  
57 determinants can be effectively evaluated using a heart rate monitor, treadmill, and a digital  
58 camera, which can be used in the design of training programs to recreationally active runners.

59

60 **Key words:** locomotion, maximal running speed, maximal incremental test, fat percentage,

61 anaerobic threshold, metabolic cost, kinematics, heart rate.

## 62 Introduction

63           Recreational runners engage in the activity with various objectives, ranging from  
64 participation in long-distance running events to the improvement of physical conditioning  
65 (Scheerder, Breedveld and Borgers, 2015). These objectives can be achieved through changes in  
66 biomechanical, physiological, and anthropometrical factors (Foster and Lucia, 2007; Novacheck,  
67 1998; Saunders, Pyne, Telford and Hawley, 2004), which may lead to improved running  
68 performance (Saunders, Pyne, Telford and Hawleypu, 2004; Foster et al., 2007; Tartaruga,  
69 Brisswalter, Peyré-Tartaruga, Avila, Alberton, Coertjens, Cadore, Tiggemann, Silva, & Krueel,  
70 2012). However, beyond these primary factors, secondary factors such as anatomical factors  
71 (e.g., lower limb size) can also play crucial role in determining running economy, which is  
72 clearly important for overall running performance (Foster et al., 2007).

73           Conceptual models present these variables directly or indirectly (Basset and Howley,  
74 2000; Saunders et al., 2004). Biomechanical factors, for example, are associated to movement  
75 patterns that possibly play a significant role in running performance, such as maximal vertical  
76 force, vertical stiffness ( $K_{\text{VERT}}$ ), leg stiffness ( $K_{\text{LEG}}$ ), stride frequency, stride length, contact time,  
77 aerial time, and vertical oscillation of the center of mass (Boullosa, Esteve-Lanao, Casado,  
78 Peyré-Tartaruga, da Rosa and Del Coso, 2020; Gómez-Molina, Ogueta-Alday, Camara,  
79 Rodríguez-Marroyo and García López, 2017; Saunders et al., 2004). Physiological and  
80 anthropometrical factors, such as heart rate corresponding to the onset of blood lactate  
81 accumulation, maximal running speed ( $V_{\text{MAX}}$ ), speed associated with the second ventilatory  
82 threshold ( $V_{2\text{VT}}$ ), body mass, and fat percentage, can also be determinants of performance (Abe,  
83 Sakaguchi, Tsuchimochi, Endo, Miyake, Miyahiro, Kanamaru and Niihata, 1999; Boullosa et al.,  
84 2020; Daniels, 2013; Gómez-Molina et al., 2017).

85           The variable with a strong predictive power for running performance is  $V_{MAX}$  (Gómez-  
86 Molina et al., 2017; Houmard, Craib, O'Brien, Smith, Israel, and Wheeler, 1991; Noakes,  
87 Myburgh and Schall, 1990; Scott and Houmard, 1994; Stratton et al., 2009). Stratton et al. (2009)  
88 demonstrated that the  $V_{MAX}$  is strongly correlated with long-distance running performance in  
89 both trained and untrained individuals. Similarly, Scott et al. (1994) observed this association  
90 between  $V_{MAX}$  and running performance among trained men and women. Furthermore, the  $V_{MAX}$   
91 has been utilized as a critical performance marker for trained runners (Lanferdini, Silva,  
92 Machado, Fischer and Peyré-Tartaruga, 2020). Current literature has shown that somatic and  
93 exertion variables, including age, body mass index, maximum oxygen uptake, blood lactate  
94 concentration at anaerobic threshold, and pulmonary ventilation, accurately estimate  $V_{MAX}$  in  
95 more than 4000 endurance runners (Wiecha, Kasiak, Cieśliński, Maciejczyk, Mamcarz and Śliż,  
96 2022). However, many studies have been limited to either trained or elite athletes, thus limiting  
97 the generalizability of findings regarding the specific variables determining  $V_{MAX}$  in  
98 recreationally active runners through low-cost tests with simple instrumentation (Abe et al.,  
99 1999; Gómez-Molina et al., 2017; Lanferdini et al., 2020; McLaughlin, Howley, Bassett,  
100 Thompson and Fitzhugh, 2010). Further, very simple measures as body mass, fat mass, previous  
101 performance data of training and races may give important clues on performance prediction in  
102 distance runners (Melo, Bernardo, Silva, Rosa, Coimbra and Peyré-Tartaruga, 2018; Melo,  
103 Tartaruga, de Borba, Boullosa, da Silva, Bernardo, Coimbra, Oliveira, da Rosa and Peyré-  
104 Tartaruga, 2022). Allometric models have also been applied to understand the relationship  
105 between biomechanics versus running economy and performance (Detoni, Oliveira, Ferreira,  
106 Queiroga, Peyré-Tartaruga and Tartaruga, 2015; Tartaruga, Brisswalter, Mota, Alberton,  
107 Gomeñuka and Peyré-Tartaruga, 2013).

108 Measurements of biomechanical, physiological, and anthropometrical variables can be  
109 easily determined through low-cost field tests, such as the maximal incremental test and the  
110 rectangular running test on a treadmill, based on known protocols for monitoring the individuals'  
111 heart rate and recording gait patterns (Marfell-Jones, Stewart and De Ridder, 2012; Sentija,  
112 Vucetic and Markovic, 2007; Morin, Dalleau, Kyröläinen, Jeannin and Belli, 2005). These tests  
113 enable the estimation of athletes' maximal aerobic capacity and the observation of their  
114 mechanical running patterns during the test, as shown by many studies that performed those  
115 respective tests (Tartaruga et al., 2012; Tartaruga et al., 2013; Lanferdini et al., 2020). As a  
116 result, professional coaches and researchers can use this information to estimate running  
117 performance by determining  $V_{MAX}$  (Stratton et al., 2009). In addition, there are approaches that  
118 utilize maximal incremental tests to evaluate running economy (di Prampero, Salvadego, Fusi  
119 and Grassi, 2009). Surprisingly, little information exists on relationship between elastic  
120 mechanism variables and metabolic cost in recreational runners (Peyré-Tartaruga, Dewolf, di  
121 Prampero, Fábica, Malatesta, Minetti, Monte, Pavei, Silva-Pereyra, Willems and Zamparo,  
122 2021). Further, previous study has shown that the elastic mechanism plays a crucial role in the  
123 relationship between metabolic cost and speed of running in trained runners (Carrard, Fontana  
124 and Malatesta, 2018).

125 Therefore, we aimed to investigate the biomechanical, physiological, and  
126 anthropometrical determinants of  $V_{MAX}$  in recreationally active runners. We hypothesized that  
127 anthropometrical factors, such as body mass and fat percentage, along with the physiological  
128 variable  $V_{2VT}$  would emerge as the primary predictors of  $V_{MAX}$ , given the high heterogeneity  
129 observed among recreationally active runners. Further, our second objective was to relate  
130 biomechanical variables of running versus metabolic cost. Thus, we also hypothesized that

131 mechanical variables related to the elastic mechanism would be associated with the metabolic  
132 cost. This hypothesis is based on the findings of da Rosa and coworkers, who clearly  
133 demonstrated landing-takeoff asymmetries of running optimized in runners with good  
134 performance in comparison to runners with lower performance (da Rosa, Oliveira, Gomeñuka,  
135 Masiero, da Silva, Zanardi, de Carvalho, Schons and Peyré-Tartaruga, 2019).

136

## 137 **Materials & Methods**

### 138 **Participants**

139 The study was approved by the Research Ethics Committee of Universidade Federal do  
140 Rio Grande do Sul (Protocol number 2.437.616), according to the Declaration of Helsinki.  
141 Fifteen recreationally active runners (age  $30.7 \pm 7.3$ ; height  $167.2 \pm 8$ ; body mass  $67.4 \pm 11.3$ )  
142 participated in the present study (see Table 1), six males and nine females. Participants were  
143 classified as recreationally active based on their engagement in at least 150 to 300 min of  
144 moderate-intensity running training or 75 to 150 of vigorous-intensity running training per week,  
145 along with muscle-strengthening exercises for 2 or more days a week as complementary training  
146 (McKay, Stellingwerff, Smith, Martin, Mujika, Goosey-Tolfrey, Sheppard and Burke, 2022).  
147 The inclusion criteria for participation in this study included being free of chronic joint pain,  
148 musculoskeletal or bone injuries over the 6-month period preceding the experiments. All  
149 participants were part of the running extension project of the Research Group LOCOMOTION -  
150 Mechanics and Energetics of Terrestrial Locomotion. They were informed about the risks and  
151 benefits of the study, and voluntarily signed an informed consent form agreeing to participate in  
152 this study.

153

## 154 **Experimental Design**

155           This is a cross-sectional study following the recommendations of the STROBE checklist  
156 (von Elm, Altman, Egger, Pocock, Gøtzsche, Vandenbroucke and STROBE, 2014). All data  
157 were collected in a single day for each subject. At the first moment of the visit, body mass,  
158 height, and the data needed to calculate the fat percentage were collected. Subsequently, all  
159 subjects performed a 5-minute warm-up at 10 km.h<sup>-1</sup> before conducting the maximal incremental  
160 test protocol on a treadmill (Super ATL Inbrasport-Inbramed, Porto Alegre, Brazil). Thirty  
161 seconds of running in the sagittal plane were recorded in the 4<sup>th</sup> minute of warm-up on the  
162 treadmill using a digital camera (Casio EX-ZR1000, 120 Hz, Tokyo, Japan) for biomechanical  
163 data analysis. The main part of the maximal incremental test started at 6 km.h<sup>-1</sup>, with an increase  
164 of 1 km.h<sup>-1</sup> per minute until the participants reached exhaustion. Heart rate was recorded every  
165 10 seconds during the maximal incremental test (Polar FT1, Kempele, Finland) to estimate heart  
166 rate associated to second ventilatory threshold (HR<sub>2VT</sub>) and maximal heart rate (HR<sub>MAX</sub>). Rating  
167 of perceived effort (RPE) (1 to 10 items) was collected at the end of each test stage (Borg, 1982).

168           To minimize the impact of confounding factors, the participants utilized their regular  
169 running shoes throughout the analysis. Furthermore, all subjects involved in the study typically  
170 underwent treadmill evaluations as part of their routine every three months.

171

## 172 **Anthropometry**

173           Body mass (kg) was measured using a portable electronic scale (model UP-150, Urano,  
174 São Paulo, Brazil) with a resolution of 100 g. Height, body perimeters and the sum of skinfolds  
175 were assessed using a tape measure and a caliper, both with resolutions of 1 mm (CESCORF,  
176 Porto Alegre, Brazil), to determine the fat percentage according to the International Society for

177 Advancement of Kinanthropometry (Marfell-Jones et al., 2012). All data collections were  
178 performed by an experienced technician, independent of the research.

179

### 180 **Maximal Incremental Test**

181 The protocol began with a 5-minute warm-up at 10 km.h<sup>-1</sup> on a treadmill set at a fixed 1%  
182 inclination. Participants had a 4-minute rest between the warm-up and the main test. The initial  
183 speed of the test was 6 km.h<sup>-1</sup>, with an additional 1 km.h<sup>-1</sup> added each minute until participants  
184 reached exhaustion. The RPE was assessed at the end of each stage (Sentija et al., 2007). The  
185 heart rate was recorded every 10 seconds during the incremental test. The  $V_{MAX}$  and  $HR_{MAX}$   
186 were determined by the highest speed and heart rate achieved during a complete running stage  
187 (60 s), respectively. If the last stage was not completed, the  $V_{MAX}$  and  $HR_{MAX}$  would be  
188 determined by the speed and HR of the previous complete stage. Subsequently, the runners were  
189 instructed to walk for two minutes at 4 km.h<sup>-1</sup> for recovery (see Figure 1).

190

### **Insert Figure 1 here**

191 Using the HR data recorded every 10 seconds by a sensor (Polar FT1, Kempele, Finland)  
192 during the maximal incremental test, the heart rate deflection point for each individual was  
193 identified in order to estimate the  $V_{2VT}$  and the  $HR_{2VT}$  (Sentija et al., 2007). The  $HR_{MAX}$ ,  $HR_{2VT}$ ,  
194  $V_{MAX}$  and  $V_{2VT}$  data obtained during the maximal incremental test were then used to calculate  
195 the theoretical metabolic cost.

196

### 197 **Biomechanical Variables**

198 The biomechanical variables were assessed using a digital camera (Casio EX-ZR1000,  
199 120 Hz, Tokyo, Japan). The foot landing and take-off events on the ground were identified

200 during ten steps in the Kinovea software version 0.8.15 at a constant speed of 10 km.h<sup>-1</sup>.  
201 Regarding to the validity of the Kinovea software, differences of 0.83, 2.02 and -1.19 degrees  
202 were observed for hip, knee, and ankle angles, respectively, when compared to 3D motion  
203 analysis software. In addition, it was observed a good correlation in terms of intra-rater reliability  
204 over two sessions (ICC > 0.85) for hip, knee, and ankle angles (Fernández-González, Koutsou,  
205 Cuesta-Gómez, Carratalá-Tejada, Miangolarra-Page and Molina-Rueda, 2020).

206 After the event identification, the contact time (s), aerial time (s), stride length (m) and  
207 stride frequency (Hz) were determined (Tartaruga et al., 2012). The maximal vertical force  
208 ( $F_{MAX}$ ) was calculated using Equation 1. From this variable, the vertical oscillation of the center  
209 of mass ( $\Delta y$ ) was estimated using the equations proposed by Morin et al. (2005):

210

211 *Equation 1*

212

213

214 *Equation 2*

215 Where  $m$  is the body mass of the runners (kg),  $g$  the gravitational acceleration (m.s<sup>2</sup>), AT and CT  
216 are aerial time (s) and contact time (s), respectively.

217 Moreover, the vertical stiffness ( $K_{VERT}$ ) and the leg stiffness ( $K_{LEG}$ ) were also calculated  
218 using the equations proposed by Morin et al. (2005):

219

220 *Equation 3*

221

222

223 *Equation 4*

224 Where  $\Delta L$  is the leg deformation (m), represented by the following equation:

225

226

*Equation 5*

227 Where  $v$  is the treadmill speed ( $\text{m}\cdot\text{s}^{-1}$ ) and  $L$  is the leg length of the runners (m) measured in  
228 standing (Morin et al., 2005).

229

### 230 **Theoretical metabolic cost**

231 In sport settings, heart rate has been used for evaluating the effort conditions in several  
232 modalities, such as running (Swain, Leutholtz, King, Haas, and Branch, 1998; Castagna,  
233 Krustrup and Povoas, 2022), cycling (Guimarães, Farinatti, Midgley, Vasconcellos, Vigário and  
234 Cunha, 2019), swimming (Hauber et al., 1997), and Nordic walking (Monteiro, Franzoni,  
235 Cubillos, de Oliveira Fagundes, Carvalho, Oliveira, Pantoja, Schuch, Rieder, Martinez and  
236 Peyré-Tartaruga, 2018). However, a drawback of heart rate-based methods is the variability  
237 influenced by age, sex, BMI, and fitness level (Hiilloskorpi, Fogelholm, Laukkanen, Pasanen,  
238 Oja, Mänttari and Natri, 1999). For a better control of these confounding factors, the literature  
239 has used the percentage of heart rate reserve (% HRR), which is based on the resting and  
240 maximum heart rate, demonstrating a strong association with oxygen uptake (Cunha, Farinatti  
241 and Midgley, 2011). So, the % HRR has been proposed as a predictor of energy expenditure.  
242 Also, % HRR was accordingly validated as a proxy for oxygen uptake in laboratory settings for  
243 endurance exercises (Guimarães et al., 2019).

244 Thus, in our study, the % HRR was associated with  $\text{HR}_{2\text{VT}}$  and considered a proxy of  
245 oxygen consumption. Additionally, this value was divided by the  $V_{2\text{VT}}$ , converting the  
246 representative value of metabolic power to metabolic cost with units relative to energy expended

247 per unit distance traveled (Peyré-Tartaruga and Coertjens, 2018), here referred as theoretical  
248 metabolic cost (arbitrary units, a.u.):

249

250

*Equation 6*

251 The dataset is available in <https://doi.org/10.6084/m9.figshare.23912724>.

252

### 253 **Statistical Analysis**

254 The data were presented as means, standard deviations and confidence intervals. The  
255 Shapiro-Wilk test was used to assess the data normality. Initially, backward multiple linear  
256 regression was performed to determine the relationship between the independent variables [body  
257 mass (kg), fat percentage (%),  $HR_{2VT}$  (bpm),  $HR_{MAX}$  (bpm), theoretical metabolic cost (a.u.), and  
258  $V_{2VT}$  ( $km \cdot h^{-1}$ )] and the dependent variable,  $V_{MAX}$  ( $km \cdot h^{-1}$ ). Subsequently, another backward  
259 multiple linear regression was applied to verify the relationship between the independent  
260 variables [contact time (s), aerial time (s), stride length (m), stride frequency (Hz), vertical  
261 oscillation of the center of the mass (cm), maximal vertical force ( $N \cdot kg^{-1}$ ),  $K_{LEG}$  ( $N \cdot m^{-1}$ ), and  
262  $K_{VERT}$  ( $N \cdot m^{-1}$ )] and the dependent variable, theoretical metabolic cost (a.u.). Expecting moderate  
263 or high collinearity between certain pairs of regressors due to deterministic relation between  
264 some variables, collinearity tests were performed and redundant factors were removed (body  
265 mass and  $V_{2VT}$  were removed in the  $V_{MAX}$  model; and maximal vertical force was removed in the  
266 theoretical metabolic cost model). In the collinearity statistics, tolerance and variance inflation  
267 factor test the assumption of multicollinearity. As a rule of thumb if variance inflation factor  $>10$   
268 and tolerance  $<0.1$  the assumptions have been greatly violated. If the average variance inflation  
269 factor  $>1$  and tolerance  $<0.2$  the model may be biased. Variance inflation factor  $<1$  and tolerance  
270  $>0.2$  confirms the model assumptions. Also, violation of assumptions was checked using Durbin-

271 Watson test. All analyzes were performed using the statistical software Jasp (Version 0.16.2,  
272 Netherlands) for Mac. The significance level adopted was  $\alpha = 0.05$ .

273

## 274 Results

275 Table 1 shows the biomechanical, physiological and anthropometrical recreationally  
276 active runners variables in mean, standard deviation and 95% confidence interval.

277 **Insert Table 1 here**

278 The backward regression model for  $V_{MAX}$  resulted in a highly significant model ( $F(2,12)$   
279  $= 8.995$ ,  $R^2 = 0.62$ ,  $p = 0.011$ ) and a regression equation of

280

281  $V_{MAX} = 58.632 + (-0.183 * \text{fat percentage}) + (-0.507 * \text{HR2VT\_perc}) + (7.959 * \text{Cost\_theor})$

282

*Equation 7*

283 where HR2VT\_perc is the heart rate as a percentage of  $HR_{MAX}$ , and Cost\_theor is the theoretical  
284 metabolic cost. Specifically, three significant regression coefficients were found: fat percentage  
285 ( $b_1 = -0.183$ ,  $t = -2.981$ ,  $p = 0.013$ ), heart rate as a percentage of  $HR_{MAX}$  ( $b_2 = -0.507$ ,  $t = 2.464$ ,  $p$   
286  $= 0.031$ ), and theoretical metabolic cost ( $b_3 = 7.959$ ,  $t = 0.841$ ,  $p = 0.042$ ).

287 Similarly, the backward regression model for theoretical metabolic cost also resulted in a  
288 highly significant model ( $F(5,9) = 15.936$ ,  $R^2 = 0.91$ ,  $p = 0.004$ ) and a regression equation as  
289 follows

290

291  $\text{Cost\_theor} = 10.421 + (4.282 * \text{contact time}) + (-3.795 * \text{aerial time}) + (-2.422 * \text{stride length}) +$   
292  $(-1.711 * \text{stride frequency}) + (0.107 * \text{vertical oscillation})$

293

*Equation 8*

294 where  $Cost_{theor}$  is the theoretical metabolic cost. Specifically, five significant regression  
295 coefficients were found, contact time ( $b_1 = 4.282$ ,  $t = 1.780$ ,  $p = 0.006$ ), aerial time ( $b_2 = -3.795$ ,  
296  $t = 6.221$ ,  $p = 0.002$ ), stride length ( $b_3 = -2.422$ ,  $t = 4.142$ ,  $p = 0.009$ ), stride frequency ( $b_4 =$   
297  $1.711$ ,  $t = 4.551$ ,  $p = 0.006$ ), and vertical oscillation ( $b_5 = 0.107$ ,  $t = 2.963$ ,  $p = 0.031$ ).

298

299 Figures 2a e 2b show the relationship between  $V_{MAX}$  versus  $V_{2VT}$  ( $R^2 = 0.86$ ,  $p < 0.001$ )  
300 and fat percentage ( $R^2 = 0.34$ ,  $p = 0.021$ ), respectively.

301 **Insert Figure 2 here**

302 Marginal effects of biomechanical variables on theoretical metabolic cost are presented in  
303 Figure 3.

304 **Insert Figure 3 here**

305

## 306 Discussion

307 The purposes of this study were twofold. First, we sought to verify which physiological  
308 ( $HR_{2VT}$ ,  $HR_{MAX}$ , theoretical metabolic cost, and  $V_{2VT}$ ) and anthropometrical variables (body  
309 mass, fat percentage) are determinant of  $V_{MAX}$  in recreationally active runners. Also, we sought  
310 to relate biomechanical ( $K_{VERT}$ ,  $K_{LEG}$ , maximal vertical force, contact time, aerial time, stride  
311 length, stride frequency and vertical oscillation of the center of mass) variables are determinant  
312 of metabolic cost in recreationally active runners. Therefore, this is the first study to our  
313 knowledge to demonstrate specific physiological ( $V_{2VT}$ ) and anthropometrical (fat percentage)  
314 variables determining  $V_{MAX}$  in recreationally active runners (Figure 4). We found that velocity  
315 associated with second ventilatory threshold, metabolic cost and fat percentage were predictors  
316 of  $V_{MAX}$ . Furthermore, our study provided new insights about the mechanical determinants of

317 metabolic cost of running. We found that simple spatiotemporal variables and vertical oscillation  
318 were identified as determinants of the metabolic cost. Interestingly, the elastic mechanisms were  
319 not related to metabolic cost. These results reinforce the understanding that estimates of the  
320 elastic mechanism based on temporal parameters of running do not appear to be sensitive, as  
321 already observed in master athletes (Pantoja, Morin, Peyré-Tartaruga and Brisswalter, 2016;  
322 Cavagna, Legramandi and Peyré-Tartaruga, 2008). On the other hand, the role of vertical  
323 oscillation in the metabolic cost of running is in line with previous findings in highly trained  
324 endurance runners (Tartaruga et al., 2012).

325 **Insert Figure 4 here**

326 According to our results,  $V_{2VT}$ , theoretical metabolic cost, and fat-mass percentage  
327 collectively accounted for 62% of the total variance in  $V_{MAX}$ . These findings agree with several  
328 studies performed with recreational, trained and elite runners (Noakes et al., 1990;  
329 Zacharogiannis and Farrally, 1993; Abe et al., 1999; Basset et al., 2000; Stratton et al., 2009;  
330 Melo et al., 2022; Zillmann, Knechtle, Rüst, Knechtle, Rosemann and Lepers, 2013; Gómez-  
331 Molina et al., 2017). Noakes et al. (1990), considering  $V_{MAX}$  as a performance predictor in  
332 trained runners, also associated this role to the  $V_{2VT}$ . Furthermore, Gómez-Molina et al. (2017)  
333 and Stratton et al. (2009) substantiate this association by incorporating  $V_{2VT}$  to  $V_{MAX}$  in the  
334 multiple linear regression equation, resulting in a significant enhancement in the prediction of the  
335 performance output in trained runners. The association between  $V_{2VT}$  and  $V_{MAX}$  can be justified  
336 as both variables represent the aerobic and anaerobic maximal capacities of the athletes,  
337 respectively (Gómez-Molina et al., 2017). Higher mitochondrial density and enzymatic activity  
338 lead to lower metabolic acidosis, allowing runners to cover greater distances or increase running

339 speed without compromising the oxidative metabolism (Bassett et al., 2000; Gómez-Molina et  
340 al., 2017).

341 In addition, increases in running speed during long-distance events are common, mainly  
342 at the beginning and in the final sprint of the race (Maroński, 1996). However, a higher fat  
343 percentage in recreational runners is not favorable to increase the  $V_{MAX}$  values. Notably, very  
344 low-fat mass has been observed in African elite runners, who exhibit both low muscle volume  
345 and a low-fat percentage, contributing to a lower total body mass. This characteristic allows them  
346 to reach higher speeds throughout long-distance running events (Zillman et al., 2013). This  
347 perspective aligns with previous research by Hoogkamer, Kipp, Spiering and Kram (2016),  
348 where they demonstrated that a 100 g increase in body mass results in approximately a 1%  
349 decrease in the 3000 m running performance. Concerning long-distance events, Zillmann et al.  
350 (2013) supported the findings of the present study, demonstrating a negative association between  
351 fat percentage and  $V_{MAX}$ . Therefore, the fat percentage seems to be determining factor for  
352 optimal running performance in this population, as  $V_{MAX}$  is directly affected.

353 The multiple linear regression test did not show an association between variables related  
354 to the elastic mechanism and metabolic cost in the present study. Initial variations in stride length  
355 appear to be fundamental for achieving higher speeds, while stride frequency becomes crucial at  
356 high speeds (Novacheck, 1998; Peyré-Tartaruga et al., 2021). However, the negative association  
357 between stride length and contact time may be confounded by variations in speed (Gómez-  
358 Molina et al., 2017), as changes in these variables are known to occur to increase running speed.  
359 Therefore, our results may not have shown associations due to the relatively slow speed used in  
360 the present study ( $10 \text{ km}\cdot\text{h}^{-1}$ ).

361 The spring-mass model during running can be characterized by two major variables  
362 associated with the leg and the vertical stiffness of the center of mass ( $K_{\text{LEG}}$  and  $K_{\text{VERT}}$ ,  
363 respectively) (Morin et al., 2005), and these variables appear to be influenced by speed and  
364 performance level (Carrard et al., 2018). Rogers, Whatman, Pearson and Kilding (2017)  
365 evaluated  $V_{\text{MAX}}$  and  $K_{\text{LEG}}$  during the 50 m sprint, along with tendon stiffness,  $K_{\text{VERT}}$  (during  
366 unilateral and bilateral drop jump), running economy on a treadmill (12, 14, 16 and 18 km.h<sup>-1</sup>),  
367  $K_{\text{LEG}}$  at 14 km.h<sup>-1</sup> and velocity associated with the maximal oxygen consumption in 11 highly  
368 trained male runners. They found large and moderate correlations between the values of  $K_{\text{LEG}}$   
369 (during the 50 m sprint) and  $K_{\text{VERT}}$  (in unilateral jump) with the running economy at 14 km.h<sup>-1</sup>  
370 (Rogers et al., 2017), supporting the concept that tendon stiffness in the lower limb could  
371 influence the global stiffness models (running and jump), thereby running performance.

372 Regarding performance level, Burn, Gonzalez, Zandler and Zernicke (2021) found that  
373 speed influences the biomechanical behavior and spring-mass characteristics in middle-distance  
374 elite (international/Olympic) vs trained (regional) with an average speed of 6.90 m.s<sup>-1</sup> and 6.06  
375 m.s<sup>-1</sup> for 1500 m, respectively. The authors noted spatiotemporal and spring-mass parameter  
376 differences across running speeds between 10 to 18 km.h<sup>-1</sup>. Elite runners demonstrated greater  
377 stability in contact time, longer aerial time, and a lower duty factor than well-trained runners  
378 (Burn et al., 2021). The spring-mass characteristics in both groups showed that  $F_{\text{MAX}}$  and  $K_{\text{VERT}}$   
379 increased with speed, while  $K_{\text{LEG}}$  showed minimal changes, with elite runners exhibiting high  
380 values (Burn et al., 2021).

381 Contrary to these findings, our study did not reveal associations between variables related  
382 to the elastic mechanism and metabolic cost in recreationally active runners. It suggests that  
383 individuals engaging in leisurely exercise may adapt their step frequency and length to minimize

384 vertical oscillation of the center of mass (Tartaruga et al., 2012) and leg deformation (Morin,  
385 Samozino, Zameziati, & Belli, 2007), optimizing the task. Therefore, it could potentially  
386 counterbalance any impairment in  $F_{MAX}$  during each step due to a lower level of training (da  
387 Rosa et al., 2019), without significant effects on  $K_{VERT}$  and  $K_{LEG}$  at 10 km.h<sup>-1</sup>.

388 On the other hand, a critical association was found between  $HR_{2VT}$  and  $V_{MAX}$  in the  
389 present study. Indeed, this finding is in line with previous results where Abe et al. (1999)  
390 observed a strong correlation between heart rate during the onset of blood lactate accumulation  
391 and  $V_{MAX}$  in elite long-distance runners with similar performance levels. The heart rate found by  
392 Abe et al. (1999) may correspond to  $HR_{2VT}$  in the present study, given that the exercise intensity  
393 was close to 4 mM, corresponding to the blood lactate values at the second ventilatory threshold  
394 approximately. Additionally, the values for  $HR_{2VT}$  and  $HR_{MAX}$  are consistent with previous  
395 findings (Bunc, Hofmann, Leitner, & Gaisl, 1995; Hofmann, Bunc, Leitner, Pokan, & Gaisl,  
396 1994; Hofmann et al., 1997; Vucetić, Sentija, Sporis, Trajković, & Milanović, 2014;  
397 Zacharogiannis et al., 1993). Moreover, our study found no association between  $HR_{MAX}$  and  
398  $V_{MAX}$ , also in line with the results reported by Gómez-Molina et al. (2017) and Noakes et al.  
399 (1990). A similar previous study has sought to relate the determinants of running velocity  
400 (Weicha et al., 2022). However, the runners used in Weicha's study were at a higher level than  
401 ours, and using the approach recommended by McKay et al. (2022), their athletes are considered  
402 trained athletes (tier 2) and ours recreationally active (tier 1).

403 The primary limitation of this study was the analysis of the biomechanical variables at a  
404 fixed speed of 10 km.h<sup>-1</sup>. Conceptual models suggest variations in biomechanical responses with  
405 increasing running speed, including step length, step frequency, contact time, and aerial time  
406 (Novacheck, 1998; Peyré-Tartaruga et al., 2021). Another limitation was the absence of blood

407 lactate concentration evaluation during the maximal incremental test. This evaluation would have  
408 brought  $HR_{2VT}$  and  $V_{2VT}$  closer to the actual second ventilatory threshold, offering better  
409 associations with results in the literature.

410         Conversely, our study provides a practical and valuable approach for analyzing the  
411 determinants of running performance and evaluating training development in recreationally  
412 active runners. The results can offer insights for coaches working with amateur and professional  
413 running groups, particularly those guiding inexperienced runners aiming to improve their health  
414 indicators or seeking information through science to enhance their running practice. Coaches  
415 should prioritize attention to the fat percentage, especially when using speed to control intensity  
416 (Daniels, 2013), preventing injuries from weight overload. Additionally, coaches can focus on  
417 improving  $V_{2VT}$  to enhance the aerobic capacity of recreationally active runners, often through  
418 high-intensity models (Silva et al., 2017). This procedure, in turn, can contribute to improved  
419 running performance and the development of new biomechanical features (Daniels, 2013).  
420 Therefore, this study provides valuable information for achieving optimal running performance  
421 ( $V_{MAX}$ ).

422         Further, refining the heart rate ratio model (Castagna et al., 2022) gives a simple equation  
423 for estimating the metabolic cost during running. The only input variables were the maximal, rest  
424 and exercise heart rate. Using combustion enthalpy parameters (Peyré-Tartaruga and Coertjens,  
425 2018), we are able to obtain a single equation for determining the metabolic cost of running.  
426 While these findings are encouraging, a couple of assumptions of the model have to be kept into  
427 account. Conditions where the cardiac output is not a key constraint of performance, as at  
428 supramaximal intensities (higher than  $V_{MAX}$ ), the model presented is limited (Lepretre,

429 Koralsztein and Billat, 2004). Indeed, at supramaximal intensities, glycolytic metabolism  
430 precludes the estimation of metabolic cost using only aerobic pathways.

431         Considering the established interactions between physiological, anthropometrical, and  
432 biomechanical variables, we suggest exploring non-linear approaches in future studies. Although  
433 not the most suitable for the present research questions, future studies could employ these  
434 methods to address the complexity of running performance. Network models, for instance, could  
435 offer valuable insights, even taking into account critical aspects as sex effects on the  
436 relationships studied here (e.g., Manchado-Gobatto, Torres, Marostegan, Rasteiro, Hartz,  
437 Moreno, Pinto and Gobatto, 2022; Pereira, Gobatto, Lewis, Ribeiro, Beck, Dos Reis, Sousa and  
438 Manchado-Gobatto, 2018). Furthermore, future studies may include additional variables  
439 contributing to determining  $V_{MAX}$ . Specifically, investigating biomechanical variables during the  
440 maximal incremental test, such as external and internal mechanical work, mechanical efficiency  
441 (Peyré-Tartaruga et al., 2021; Peyré-Tartaruga et al., 2018), and muscle and tendon mechanical  
442 properties, could offer further insights into the complex interplay affecting  $V_{MAX}$ .

443

## 444 **Conclusions**

445         In conclusion, our study demonstrates that  $V_{2VT}$ , metabolic cost, and fat-mass  
446 percentage can explain 62% of the variability in  $V_{MAX}$ . Also, 90% of the variability in  
447 metabolic cost is accounted for by simple spatiotemporal variables (contact and aerial time,  
448 stride frequency and length, and vertical oscillation). Therefore, we concluded that recreationally  
449 active runners with higher  $V_{2VT}$ , lower metabolic cost, and a lower fat percentage will likely  
450 present better  $V_{MAX}$  performance.

451

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653 **FIGURE CAPTIONS**

654

655 **Figure 1. Experimental design.** Maximal incremental test (Sentija et al., 2007). Maximal running  
656 speed ( $V_{MAX}$ ), speed associated with the second ventilatory threshold ( $V_{2VT}$ ), heart rate associated  
657 with the second ventilatory threshold ( $HR_{2VT}$ ), maximal heart rate ( $HR_{MAX}$ ), contact time (CT),  
658 aerial time (AT), stride length (SL) e stride frequency (SF).

659

660 **Figure 2. Bivariate correlations.** Relationship between maximal running speed ( $V_{MAX}$ ) during  
661 the maximal incremental test, versus speed associated with the second ventilatory threshold ( $V_{2VT}$ ,  
662 a) and fat percentage (b).

663

664 **Figure 3. Marginal effects of biomechanical variables on theoretical metabolic cost of**  
665 **running.** Marginal effects of contact and aerial times, stride length and frequency, and vertical  
666 oscillation on theoretical metabolic cost of running based on intervals of prediction (dashed lines)  
667 and intervals of confidence (gray areas) at 95%.

668

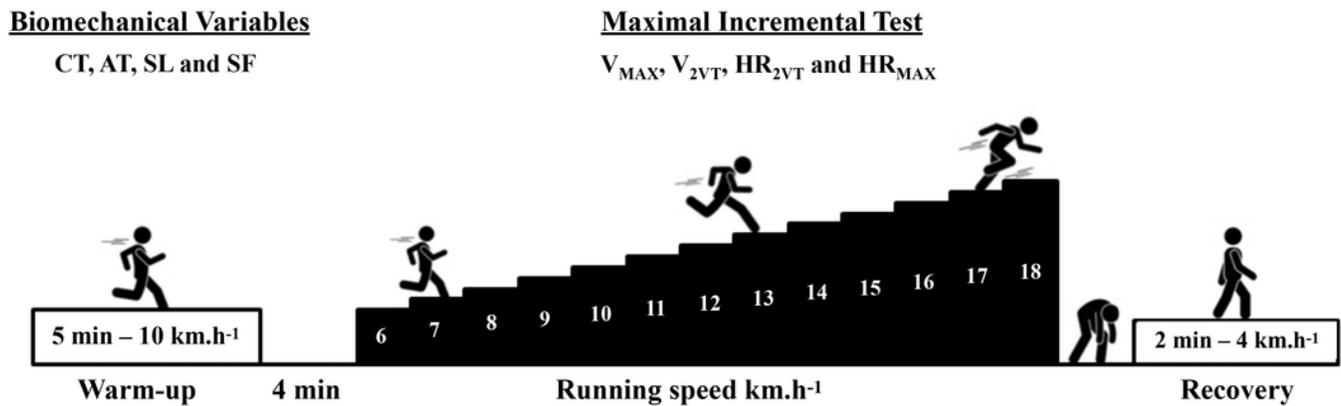
669 **Figure 4. Conceptual model for predicted  $V_{MAX}$  in recreationally active runners.**  
670 Physiological determinants of running performance and the respective biomechanical  
671 determinants of metabolic cost of running.

672

# Figure 1

Experimental design.

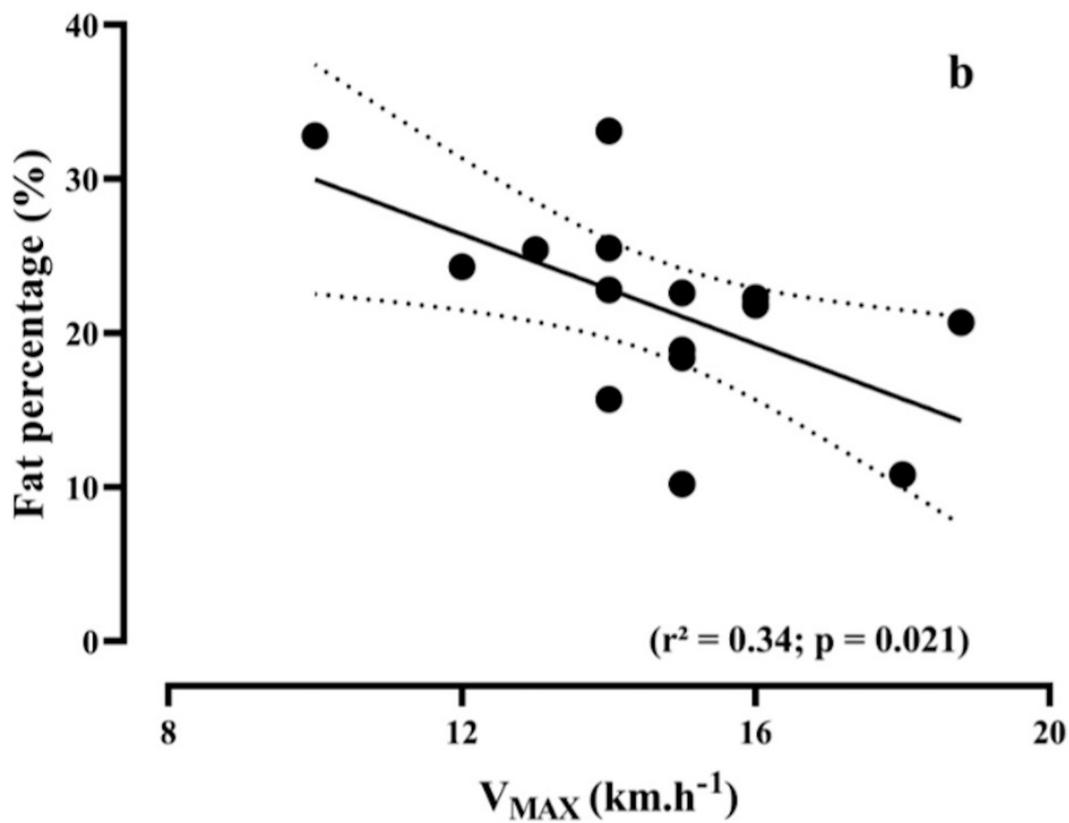
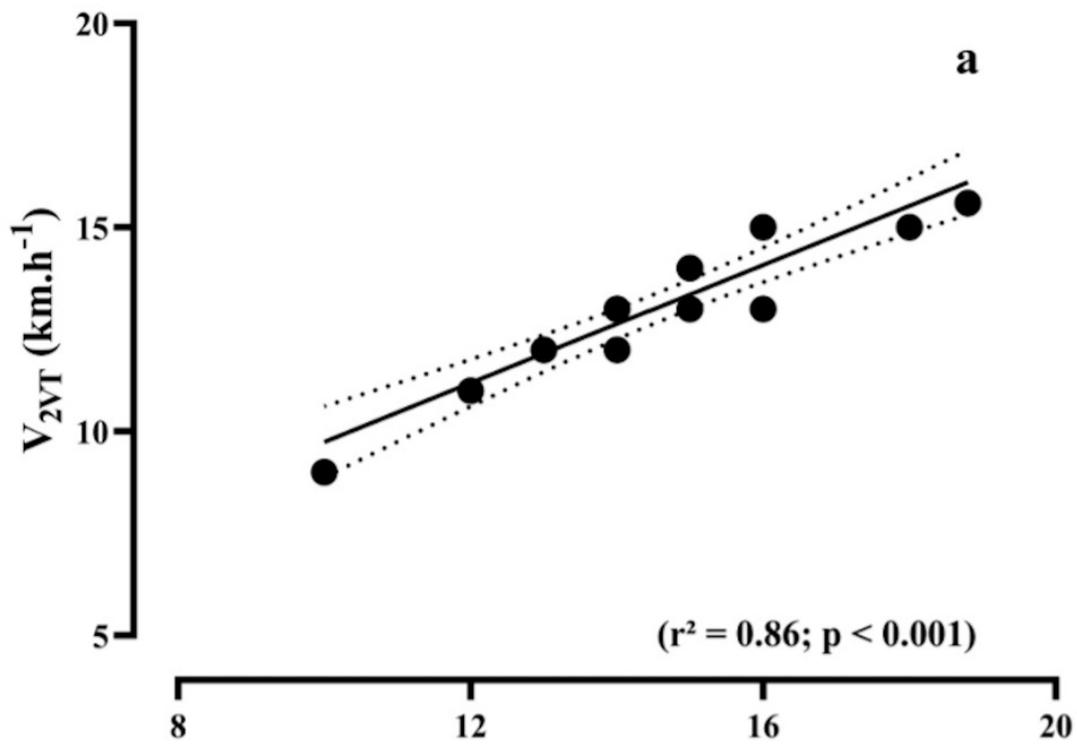
Maximal incremental test (Sentija et al., 2007). Maximal running speed ( $V_{MAX}$ ), speed associated with the second ventilatory threshold ( $V_{2VT}$ ), heart rate associated with the second ventilatory threshold ( $HR_{2VT}$ ), maximal heart rate ( $HR_{MAX}$ ), contact time (CT), aerial time (AT), stride length (SL) e stride frequency (SF).



## Figure 2

Bivariate correlations.

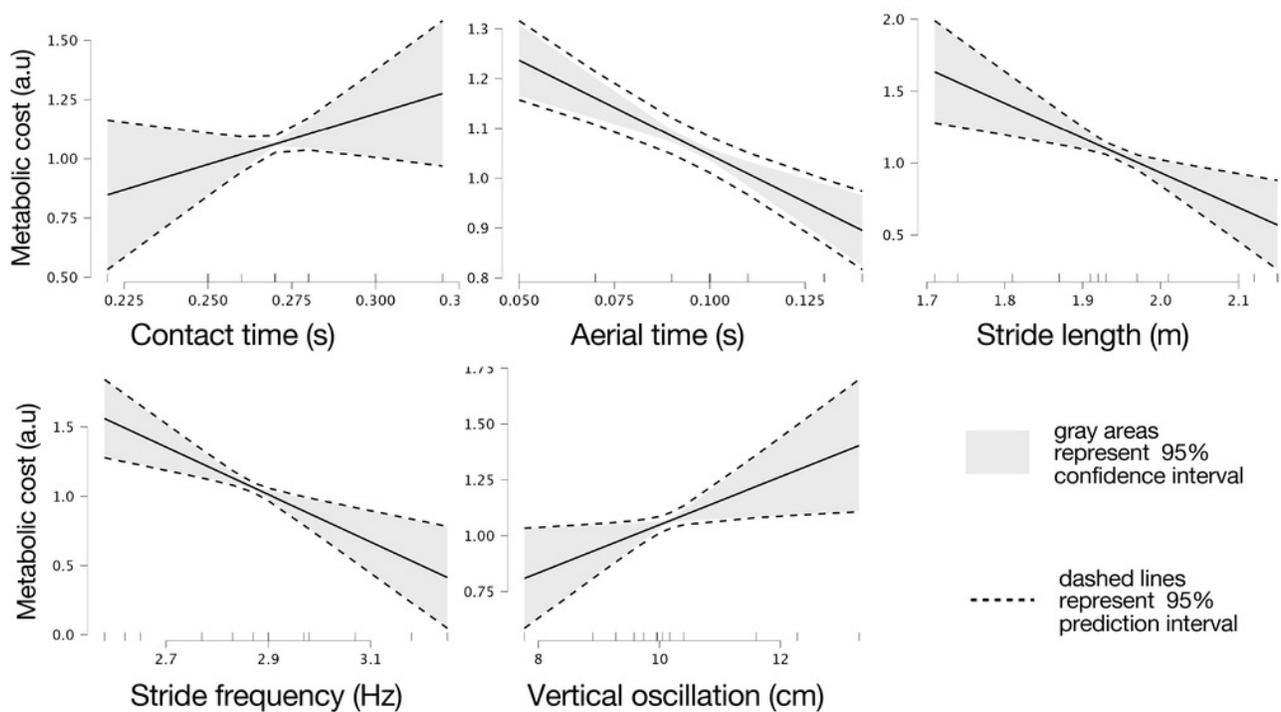
Relationship between maximal running speed ( $V_{MAX}$ ) during the maximal incremental test, versus speed associated with the second ventilatory threshold ( $V_{2VT}$ , a) and fat percentage (b).



## Figure 3

Marginal effects of biomechanic variables on theoretical metabolic cost of running.

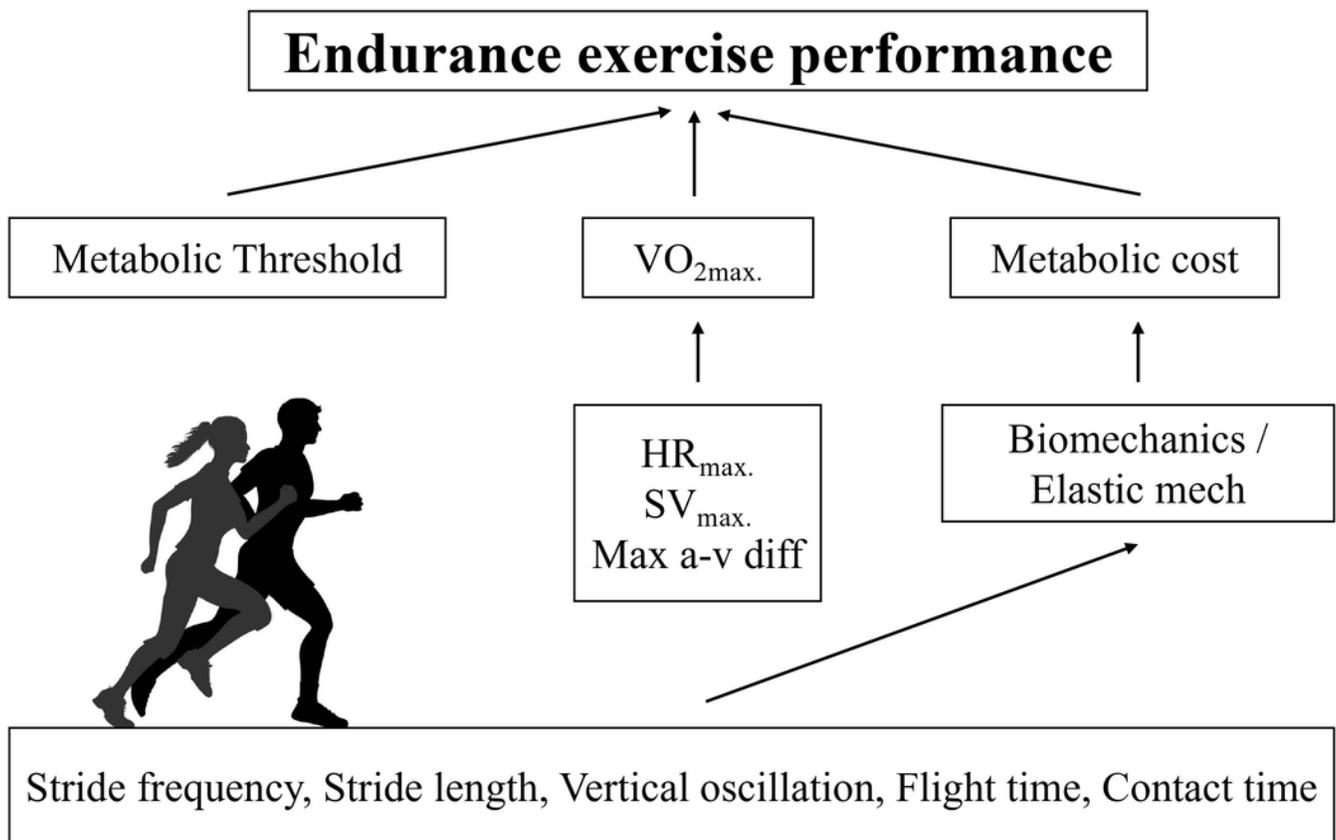
Marginal effects of contact and flight times, stride length and frequency, and vertical oscillation on theoretical metabolic cost of running based on intervals of prediction (dashed lines) and intervals of confidence (gray areas) at 95%.



## Figure 4

Conceptual model for predicted  $V_{MAX}$  in recreational runners.

Physiological determinants of running performance and the respective biomechanical determinants of metabolic cost of running.



**Table 1** (on next page)

Table 1. Values of mean, standard deviation (SD) and confidence interval (CI) of anthropometrical, physiological and biomechanical variables in recreationally active runners.

Note. Leg length ( $L$ ), leg deformation ( $\Delta L$ ), heart rate associated to second ventilatory threshold ( $HR_{2VT}$ ), maximal heart rate ( $HR_{MAX}$ ), speed associated with the second ventilatory threshold ( $V_{2VT}$ ), maximal running speed ( $V_{MAX}$ ), theoretical metabolic cost ( $Cost_{theor}$ ), contact time (CT), aerial time (AT), stride length (SL), stride frequency (SF), vertical oscillation of the center of mass ( $\Delta y$ ), maximal vertical force ( $F_{MAX}$ ), leg stiffness ( $K_{LEG}$ ), vertical stiffness ( $K_{VERT}$ ).

1 **TABLES**

2 **Table 1.** Values of mean, standard deviation (SD) and confidence interval (CI) of  
 3 anthropometrical, physiological and biomechanical variables in **recreationally active** runners

	<i>Female (n=9)</i>	<i>Male (n=6)</i>	<i>Total (n=15)</i>	
Variable	Mean / SD	Mean / SD	Mean / SD	CI (95%)
Age (years)	30.2 ± 6.9	31.3 ± 8.5	30.7 ± 7.3	27 to 34.3
Height (cm)	162.6 ± 6.5	174.2 ± 4.2	167.2 ± 8	163.2 to 171.3
L (m)	0.88 ± 0.05	0.92 ± 0.02	0.90 ± 0.04	0.87 to 0.92
ΔL (m)	0.09 ± 0.02	0.10 ± 0.02	0.09 ± 0.02	0.08 to 0.10
Body mass (kg)	63.7 ± 9.0	73.0 ± 12.9	67.4 ± 11.3	61.7 to 73.1
Fat percentage (%)	25.2 ± 4.8	16.4 ± 5.2	21.7 ± 6.5	18.4 to 25
HR <sub>2VT</sub> (bpm)	185.1 ± 6.9	174.5 ± 11.5	180.9 ± 10.2	175.7 to 186
HR <sub>MAX</sub> (bpm)	192.1 ± 6.7	185.5 ± 11.8	189.5 ± 9.3	184.7 to 194.2
V <sub>2VT</sub> (km.h <sup>-1</sup> )	12.6 ± 1.7	13.9 ± 1.3	13.1 ± 1.7	12.26 to 13.96
V <sub>MAX</sub> (km.h <sup>-1</sup> )	13.9 ± 2.0	15.8 ± 2.1	14.7 ± 2.2	13.56 to 15.75
Cost_theor	1.07 ± 0.05	1.06 ± 0.04	1.07 ± 0.04	1.044 to 1.086
CT (s)	0.26 ± 0.02	0.28 ± 0.03	0.27 ± 0.03	0.26 to 0.28
AT (s)	0.09 ± 0.03	0.09 ± 0.02	0.09 ± 0.03	0.08 to 0.11
SL (m)	1.93 ± 0.13	1.97 ± 0.16	1.95 ± 0.14	1.87 to 2.02
SF (Hz)	2.89 ± 0.19	2.84 ± 0.24	2.87 ± 0.21	2.77 to 2.97
Δy (cm)	9.8 ± 1.2	10.6 ± 1.5	10.8 ± 2.9	9.46 to 10.84
F <sub>MAX</sub> (N.kg <sup>-1</sup> )	1.4 ± 0.2	1.5 ± 0.2	1.4 ± 0.2	1.31 to 1.53
K <sub>LEG</sub> (N.m <sup>-1</sup> )	16.1 ± 4.2	16.1 ± 3.1	16.1 ± 3.7	14.23 to 17.96

$K_{\text{VERT}}$  (N.m<sup>-1</sup>)                       $16.3 \pm 4.3$                        $16.2 \pm 3.1$                        $16.2 \pm 3.7$                       14.36 to 18.13

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4     Note. Leg length (L), leg deformation ( $\Delta L$ ), heart rate associated to second ventilatory threshold ( $HR_{2\text{VT}}$ ),  
5     maximal heart rate ( $HR_{\text{MAX}}$ ), speed associated with the second ventilatory threshold ( $V_{2\text{VT}}$ ), maximal running  
6     speed ( $V_{\text{MAX}}$ ), theoretical metabolic cost (Cost\_theor), contact time (CT), aerial time (AT), stride length (SL),  
7     stride frequency (SF), vertical oscillation of the center of mass ( $\Delta y$ ), maximal vertical force ( $F_{\text{MAX}}$ ), leg stiffness  
8     ( $K_{\text{LEG}}$ ), vertical stiffness ( $K_{\text{VERT}}$ ).  
9