

Multiple propane gas burns rate procedure to determine accuracy and linearity of indirect calorimetry systems : An experimental assessment of a method

Mohammad Ismail ^{Equal first author, 1}, **Sanaa Alsubheen** ², **Angela Loucks-Atkinson** ³, **Matthew Atkinson** ⁴, **Thamir Alkanani** ³, **Liam P Kelly** ^{Corresp., 5}, **Fabien Basset** ^{Corresp. Equal first author, 3}

¹ School of Human Kinetics and Recreation, Memorial University of Newfoundland, St John's, Newfoundland, Canada

² School of Physical Therapy Faculty of Health and Rehabilitation Sciences, Western University, London, Ontario, Canada

³ School of Human Kinetics and Recreation, Memorial University of Newfoundland, St. John's, Newfoundland, Canada

⁴ Department of mathematics and Statistics, Memorial University of Newfoundland, St. John's, Newfoundland, Canada

⁵ Faculty of Medicine, Memorial University of Newfoundland, St. John's, Newfoundland, Canada

Corresponding Authors: Liam P Kelly, Fabien Basset

Email address: lpkelly@mun.ca, fbasset@mun.ca

Objective: Indirect calorimetry (IC) systems measure the fractions of expired carbon dioxide (F_eCO_2), and oxygen (F_eO_2) recorded at the mouth to estimate whole-body energy production. The fundamental principle of IC relates to the catabolism of high-energy substrates such as carbohydrates and lipids to meet the body's energy needs through the oxidative process, which are reflected in the measured oxygen uptake rates ($\dot{V}O_2$) and carbon dioxide production rates ($\dot{V}CO_2$). Accordingly, it is important to know the accuracy and validity of $\dot{V}O_2$ and $\dot{V}CO_2$ measurements when estimating energy production and substrate partitioning for research and clinical purposes. Although several techniques are readily available to assess the accuracy of IC systems at a single point for $\dot{V}CO_2$ and $\dot{V}O_2$, the validity of such procedures is limited when used in testing protocols that incorporate a wide range of energy production (e.g., basal metabolic rate and maximal exercise testing). Accordingly, we built an apparatus that allowed us to manipulate propane burn rate in such a way as to assess the linearity of IC systems. This technical report aimed to assess the accuracy and linearity of three IC systems using our in-house built validation procedure. **Approach:** A series of trials at different propane burn rates (PBR) (i.e., 200, 300, 400, 500, and 600 mL min⁻¹) were run on three IC systems: Sable, Moxus, and Oxycon Pro. The experimental values for $\dot{V}O_2$ and $\dot{V}CO_2$ measured on the three IC systems were compared to theoretical stoichiometry values. **Results:** A linear relationship was observed between increasing PBR and measured values for $\dot{V}O_2$ and $\dot{V}CO_2$ (99.6%, 99.2%, 94.8% for the Sable, Moxus, and Jaeger IC systems, respectively). In terms of system error, the

Jaeger system had significantly ($p < 0.001$) greater $\dot{V}O_2$ (mean difference (M) = -0.057, standard error (SE) = 0.004), and $\dot{V}CO_2$ (M = -0.048, SE = 0.002) error compared to either the Sable ($\dot{V}O_2$, M = 0.044, SE = 0.004; $\dot{V}CO_2$, M = 0.024, SE = 0.002) or the Moxus ($\dot{V}O_2$, M = 0.046, SE = 0.004; $\dot{V}CO_2$, M = 0.025, SE = 0.002) IC systems. There were no significant differences between the Sable or Moxus IC systems. Conclusion: The multiple PBR approach permitted the assessment of linearity of IC systems in addition to determining the accuracy of fractions of expired gases.

Multiple propane gas burns rate method to determine accuracy and linearity of indirect calorimetry systems: An experimental assessment of a method

¹Mohammad Ismail (mi4114@mun.ca)*

²Sanaa Alsubheen (salsubhe@uwo.ca)

¹Angela Loucks-Atkinson (aloucksa@mun.ca)

³Matthew Atkinson (matkinso@gmail.com)

¹Tim Alkanani (talkanani@mun.ca)

⁴Liam P Kelly (lpkelly@mun.ca) ✉

¹Fabien A. Basset (fbasset@mun.ca)* ✉

¹School of Human Kinetics and Recreation, Memorial University, St John's, NL, Canada.

² School of Physical Therapy, Western University, London, ON, Canada.

³Department of mathematics and Statistics, Memorial University, St. John's, NL, Canada.

⁴Faculty of Medicine, Memorial University, St John's, NL, Canada.

* Equal first author

Corresponding Authors:

✉ Fabien A. Basset

School of Human Kinetics and Recreation, Memorial University of Newfoundland

230 Elizabeth Avenue, St. John's, NL, Canada, A1C 5S7

Phone: (709) 864-6132; Fax: (709) 864-3979

✉ Liam P. Kelly

Janeway Pediatric Research Unit, Faculty of Medicine, Memorial University

Janeway Hostel, 300 Prince Philip Drive, St. John's, NL, Canada A1B 3V6

Phone: (709) 777-4972

Running head: Validation of indirect calorimetric systems

Abstract

Objective: Indirect calorimetry (IC) systems measure the fractions of expired carbon dioxide (F_{eCO_2}), and oxygen (F_{eO_2}) recorded at the mouth to estimate whole-body energy production. The fundamental principle of IC relates to the catabolism of high-energy substrates such as carbohydrates and lipids to meet the body's energy needs through the oxidative process, which are reflected in the measured oxygen uptake rates ($\dot{V}O_2$) and carbon dioxide production rates ($\dot{V}CO_2$). Accordingly, it is important to know the accuracy and validity of $\dot{V}O_2$ and $\dot{V}CO_2$ measurements when estimating energy production and substrate partitioning for research and clinical purposes. Although several techniques are readily available to assess the accuracy of IC systems at a single point for $\dot{V}CO_2$ and $\dot{V}O_2$, the validity of such procedures is limited when used in testing protocols that incorporate a wide range of energy production (e.g., basal metabolic rate and maximal exercise testing). Accordingly, we built an apparatus that allowed us to manipulate propane burn rate in such a way as to assess the linearity of IC systems. This technical report aimed to assess the accuracy and linearity of three IC systems using our in-house built validation procedure. **Approach:** A series of trials at different propane burn rates (PBR) (i.e., 200, 300, 400, 500, and 600 mL min⁻¹) were run on three IC systems: Sable, Moxus, and Oxycon Pro. The experimental values for $\dot{V}O_2$ and $\dot{V}CO_2$ measured on the three IC systems were compared to theoretical stoichiometry values. **Results:** A linear relationship was observed between increasing PBR and measured values for $\dot{V}O_2$ and $\dot{V}CO_2$ (99.6%, 99.2%, 94.8% for the Sable, Moxus, and Jaeger IC systems, respectively). In terms of system error, the Jaeger system had significantly ($p < 0.001$) greater $\dot{V}O_2$ (mean difference (M) = -0.057, standard error (SE) = 0.004), and $\dot{V}CO_2$ (M = -0.048, SE = 0.002) error compared to either the Sable ($\dot{V}O_2$, M = 0.044, SE = 0.004; $\dot{V}CO_2$, M = 0.024, SE = 0.002) or the Moxus ($\dot{V}O_2$, M = 0.046, SE = 0.004; $\dot{V}CO_2$, M = 0.025, SE = 0.002) IC systems. There were no significant differences between the Sable or Moxus IC systems. **Conclusion:** The multiple PBR approach permitted the assessment of linearity of IC systems in addition to determining the accuracy of fractions of expired gases.

Keywords: Accuracy, energy production, indirect calorimetry, linearity, propane gas.

Introduction

Of primary interest to use indirect calorimetry (IC) in the study of human thermoregulation is the measurement of fractions of expired oxygen (F_{eO_2}) and carbon dioxide (F_{eCO_2}) for estimation of energy production or substrate turnover under various environmental conditions (e.g., at rest, during exercise, and in cold or hot environments) (Jequier and Felber 1987). Chemical, electronic, and spectroscopic technologies have been implemented to perform these measurements. Indirect calorimetry systems integrate discrete electronic analyzers to record F_{eO_2} and F_{eCO_2} in line with measures of flow rate (e.g., flowthrough respirometry) or ventilation rate (e.g., breath-by-breath measurements) in addition to the temperature, pressure, and humidity of ambient and expired air using computer-controlled analog-to-digital signal processing (Leonard 2012). Several instrument configurations range from simple or semi-automated mixing chamber systems to highly sophisticated, fully automated breath-by-breath measurement devices (Matarese 1997). Each instrument incorporated in the IC system contributes errors in measuring whole-body oxygen uptake ($\dot{V}O_2$) and carbon dioxide production ($\dot{V}CO_2$), affecting estimates of energy production and substrate turnover. The expected accuracy of IC systems can differ between manufacturers, and the user is often left to rely on the devices' technical notes to estimate the accuracy of their measured outcomes. However, technical notes generally report specifications for the individual analyzers and not the IC system as a whole. Accordingly, additional procedures are needed to assess the accuracy of IC measures under conditions that reflect the testing environment, especially when investigating small metabolic differences between the experimental and control conditions (Lighton 2008).

Researchers and clinicians in the biological/medical sciences routinely implement IC technology to study the effects of behavioral and environmental manipulations on whole-body energy metabolism in humans under resting and exercise conditions (Brooks, Fahey, and Baldwin 2005). Several techniques have been developed to assess the accuracy of outcomes recorded through IC; however, few are designed to simulate the energy production rates recorded among humans at rest and during light physical activity. Burning of methanol (Cooper and Storer 2001) or propane (Lighton 2008) and nitrogen dilution (Fedak, Rome, and Seeherman 1981) are the most commonly applied techniques to validate IC measurements (i.e., $\dot{V}O_2$ and $\dot{V}CO_2$). Yet, the determination of signal linearity through the generation of multiple propane burn rates or levels

of nitrogen dilution remains rarely performed. Lack of appropriate validation may cause inaccurate interpretations of VO_2 and VCO_2 measurements and, consequently, lead to large errors in calculating substrate partitioning and energy production (Ferrannini 1988). Advancements in sensor technologies will continue to increase the accuracy and reliability of IC measurements in both laboratory and field settings and render energy production assessment promptly available (Haugen, Chan, and Li 2007). However, the accuracy and linearity of the measurements under various experimental and clinical conditions warrant special considerations for the enhancement of existing methodologies used to validate IC outcomes (Levine, Eberhardt, and Jensen 1999). Therefore, the present manuscript reports a new propane gas validation procedure designed to assess the accuracy and linearity of VO_2 and VCO_2 measurements taken at different propane burn rates (PBR).

Materials and methods

The accuracy and linearity of three IC systems available in our exercise physiology laboratory (i.e., Jaeger Oxycon Pro, Jaeger- now CareFusion, Hochberg, Germany; Moxus Modular Metabolic System, AEI technologies, IL, USA; and Sable Classic Line, Sable Systems International, Las Vegas, NV, USA) were assessed with an in-house built device for manipulating PBR and recovering the products of complete propane combustion (i.e., CO_2 and H_2O) into the mixing chambers of the IC systems. All IC systems were set for flow-through respirometry measurements (i.e., excurrent flow measurement or negative pressure system). During Jaeger and Moxus measurements, subsampled air was dried by passing through a twin-tube Nafion sample line or tube filled with magnesium perchlorate, respectively. Water vapor pressure was recorded during Sable measurements, and flow rate (FR), F_{eO_2} , and F_{eCO_2} were corrected (see equations below).

Technical characteristics of the indirect calorimetric systems

The ViaSys Jaeger Oxycon Pro is a quasi-modular IC system consisting of a twin tube (Nafion sample line), a turbine volume transducer (flow range = $0\text{--}300 \text{ L}\cdot\text{min}^{-1}$; accuracy = 2%), a subsample pump (flow rate ranging from 200 to 220 $\text{ml}\cdot\text{min}^{-1}$), a 6 L mixing chamber, a fuel-cell oxygen sensor (accuracy = 0.05%; resolution = 0.01%; full range = $0\text{--}25\%$; time response = 0.08

sec), a dual infrared carbon dioxide sensor (accuracy = 0.05%; resolution = 0.01%; full range = 0-15%; time response = 0.08 sec).

The Moxus Modular Metabolic System, consists of a turbine for determination of ventilation volume [VMM-400 (flow range = 0-800 L•min⁻¹; accuracy = 1%)], a 4.2 L mixing chamber, a subsample pump (flow rate ranging from 10-500 mL•min⁻¹), a zirconia oxygen sensor [3A/I Oxygen analyzers (accuracy = 0.01%; resolution = 0.01%; full range = 0-100%; time response = 0.1 sec)] and a dual infrared carbon dioxide sensor [CD-3A Carbon Dioxide (accuracy = 0.02 %; resolution = 0.01%; full range = 0-15%; time response = 0.025 sec)]. To investigate differences in oxygen sensor technologies (i.e., zirconia vs. paramagnetic), Moxus IC system validity measures were recorded with its gas analyzers (3A/I and CD-3A) integrated with Sable technologies for generating FR and subsample rate (described below).

The Sable Classic Line is a modular IC system consisting of a subsample pump (sub-sampler, SS4 – linearized mass flow meter ranging from 0-2000 ml•min⁻¹), a water vapor analyzer (RH-300 – resolution = 0.001% and full range = 0-100% RH non-condensing), a dual infrared carbon dioxide sensor [CA-10 Carbon Dioxide (accuracy = 1%; resolution = 0.00001%; full range = 0-10%; time response = 0.5 sec), a paramagnetic oxygen sensor [PA-10 Oxygen analyzers (accuracy = 0.1%; resolution = 0.0001%; full range = 0-100%; time response = 0.2 sec)] and an air mass flow generator and controller (FK-500 – accuracy = 0.05 L•min⁻¹; full range = 50-500 L•min⁻¹).

Calibration of IC Systems

Before data collection, oxygen and carbon dioxide analyzers were calibrated with medically certified calibration gases (1% CO₂ and 100% N₂ for Sable and 4% CO₂ and 16% O₂ for Moxus and Jaeger). In terms of FR, the Oxycon Pro's turbine volume transducer was calibrated using the manufacturer's built-in automated calibration procedures. Outcomes of the Sable's air mass flow generator and controller were validated using the nitrogen dilution technique described by Fedak et al. (1981). A series of N₂ gas flows (1000, 500, 250, 150 ml•min⁻¹) were randomly selected at two different ventilation rates (55 and 75 L min⁻¹) and injected into the incurrent air through a canopy. The actual experimental values of N₂ gas were compared to their theoretical value (Fedak, Rome, and Seeherman 1981).

Multiple Propane Burn Rate Device

The overarching aim of the current methodological study was to develop a procedure to assess the validity of VO_2 and VCO_2 measurements recorded at rest and during light exercise in human subjects. Given that propane gas combustion provides one of the best methods for simulating whole-body energy metabolism (Rising et al. 2017), a device was built to enable the complete combustion of propane at different mass flow rates (described as propane burn rate (PBR) to avoid confusion with the flow rate used during flow-through respirometry) and the recovery of VO_2 and VCO_2 . The in-house built propane gas validation system consists of the following sequential connections. First, a tank of chemically pure (99%) propane gas (SPG-PROCHP6 – Air-Liquids Canada) with a two-stage Western Medical gas regulator (model M1-940-PG, Westlake, Ohio) and its gas hose is connected to a one-way Matheson mass-flow transducer (model 8141) that is subsequently connected to a Matheson mass-flow controller, model 8240 (East Rutherford, NJ) and to a Bunsen burner – vertical metal tube of 60 mm high and 4 mm inside diameter (ID). The burner is located in a 2.4 L glass canopy that flows into a 0.4 L glass tubing. The entire system is connected to IC systems by a 1.4-inch diameter hose (Figure 1). The pressure in the gas line flowing out of the cylinder is maintained at ten psi. The regulator is fitted with a ¼ inch MNPT brass needle valve and a high-pressure gas hose (4mm ID, 7mm outside diameter, OD) to prevent potential propane leaks. The flow rates were expressed in STP-corrected volumes from the analog output that varied from 0 to 5 volts on a 0% to 100% full scale (Lighton 2008). The data collection is detailed in the next section, and its results are shown in the results section.

Insert Figure 1 about here

Data collection and reduction

A series of PBRs (200, 300, 400, 500, and 600 mL min⁻¹) were selected and tested at two different FRs to assess each IC system's accuracy and linearity. According to the Jaeger recommendations for resting metabolic rate, the flow rate was set at 20 and 40 L•min⁻¹ using the digital volume transducer described above. For the Sable IC system and Moxus gas analyzers, flow rates were set at 55 and 75 L min⁻¹. Three 30-min trials per PBR and FR were randomly performed on each IC system. Also, 15-min of baseline (i.e., room air) was recorded before and after each PBR trial equating to 60-min measurement periods. All trials were conducted at one

location and at the same time of the day. In addition, the F_eO_2 , F_eCO_2 , FR, barometric pressure (BP), water vapor pressure (WVP), chamber temperature ($T^{\circ}C$ -Ch), and room temperature ($T^{\circ}C$ -Rm) were recorded.

Propane gas stoichiometry equations

Pure propane (C_3H_8) is an odorless, colorless, flammable gas. Complete combustion of one mole of 100% C_3H_8 produces three moles of CO_2 and 4 moles of H_2O for every five moles of O_2 consumed according to the stoichiometry reaction depicted in Equation 1.



Therefore, under standard pressure and temperature (STPD), 22.44 L of C_3H_8 would react with 112.2 L of O_2 for the reaction to be completed to produce 67.2 L of CO_2 . At standard conditions, the molecular mass of 100% C_3H_8 is 44 g, and 1 g of propane would then require 2.55 L of O_2 (i.e., 112.2 L of O_2 to burn 44 g of propane) to produce 1.53 L CO_2 , that is, 67.2 L of CO_2 results from the burning of 44 g of propane. It can then be deduced that optimal C_3H_8 combustion results in RER equal to 0.60 (Lighton 2008).

The present technical report used a mass flow meter for an accurate PBR. The PBR was calculated using the following formula:

Mass flow rate ($g\ min^{-1}$) = volume flow rate x propane density	Eq.2
---	------

Flow-through respirometry equations

The measured fraction of expired gases (F_eO_2 and F_eCO_2) and FR recorded by the Sable IC system were first corrected for the effect of WVP using Dalton's law of partial pressures.

$F'_eO_2 = F_eO_2 \times BP / (BP - WVP)$	(Eq.3)
---	--------

Where F'_eO_2 and F_eO_2 represent a fraction of expired air dry and moist oxygen.

$F'_eCO_2 = F_eCO_2 \times BP / (BP - WVP)$	(Eq.4)
---	--------

Where F'_eCO_2 and F_eCO_2 represent a fraction of expired air dry and moist carbon dioxide.

$$FR' = FR \times (BP - WVP) / BP \quad (Eq.5)$$

Where FR' and FR represent dry and moist air FR, respectively.

To correct for any drift in the fraction of oxygen, the following equation developed by Lieberman et al. (2015) was computed:

$$F_iO_{2ss} = F_iO_{2f} + [(F_iO_{2f} - F_iO_{2i}) \times (T_{ss} - T_i) / (T_f - T_i)] \quad (Eq.6)$$

Where F_iO_{2i} is the initial fractional amount of oxygen in the inspired air stream measured at equilibrium before each PBR (baseline pre-); F_iO_{2f} is the final fractional amount of oxygen in the inspired air stream measured at equilibrium after each PBR (baseline post-); T_{ss} is the time into each PBR at steady state; T_f is the time when final inspired oxygen fraction is measured; T_i is the time when initial inspired oxygen fraction is measured.

The calculation of VO_2 , VCO_2 , and RER was performed using the following equations:

$$VO_2 = FR_e [(F_iO_2 - F_e'O_2) - F_iO_2 (F_e'CO_2 - F_iCO_2)] / (1 - F_iO_2) \quad (Eq.7)$$

Where FR_e is expired flow rate; F_iO_2 stands for the fraction of inspired unscrubbed oxygen; $F_e'O_2$ stands for expired dry oxygen; $F_e'CO_2$ for expired dry carbon dioxide; and F_iCO_2 stands for the fraction of inspired unscrubbed carbon dioxide.

$$VCO_2 = FR_e [(F_e'CO_2 - F_iCO_2) + F_iCO_2 (F_iO_2 - F_e'O_2)] / (1 + F_iCO_2) \quad (Eq.8)$$

where acronyms stand as in Eq.7

$$RER = VCO_2 / VO_2 \quad (Eq.9)$$

Where RER is the quotient of VCO_2 over VO_2 .

The metabolic data (VO_2 , VCO_2 , and RER) were then truncated by 10 min (5 min at the beginning and end of each data collection period). An average value was reported for the

remaining 20 min. To determine the accuracy and linearity of the three different IC systems, respirometry data were compared to the stoichiometry theoretical VO_2 and VCO_2 values under standard conditions for the five PBRs studied. Given that the same propane burn rates were used to validate the three IC systems, data are expressed as the mean difference between stoichiometry theoretical value and mean experimental values (i.e., $M\Delta = \text{STV} - \text{MEV}$).

Statistical analysis

Statistical analyses were performed using SPSS, version 23 (SPSS Inc., Chicago, IL, USA). Unless otherwise specified, all values are reported as mean \pm standard deviation, and an alpha level of 0.05 was used to indicate statistical significance. Tests for statistical assumptions were performed; homogeneity of variance was tested using Levene's test, and normality was tested using the Kolmogorov-Smirnov test. First, descriptive statistics were conducted. Second, a series of one-way ANOVA was used to assess the effect of ventilation rates (55 L min⁻¹, 75 L min⁻¹ for Sable and Moxus, 20 L min⁻¹, 40 L min⁻¹ for Jaeger) on the fraction of gases. Third, a linear regression analysis was performed to examine the linearity between the volumes of VO_2 and VCO_2 , with PBR for the three systems. Regression analysis was also performed to test the linearity between N_2 flow rates with VO_2 during validation of the Sable mass flow generator and controller. Fourth, Bland-Altman plots followed by linear regressions were created to evaluate the mean difference (error) between systems outputs and the stoichiometry theoretical VO_2 , VCO_2 , and RER values for all systems at all PBRs. Lastly, two-factor ANOVAs were conducted to evaluate the effects of the three IC systems and the five PBRs for VO_2 , VCO_2 , and RER error. A mixed models design was used with systems being a fixed effect and PBR a random effect. A corrected F-test was calculated (Neter et al. 1996) for the random factor as mixed models in SPSS incorrectly uses *MS from the interaction* as the error term (denominator). The correction is to use *MS error* as the denominator. SPSS correctly uses *MS error* in the F-test for the interaction, which is also considered random. SPSS correctly uses the *MS from the interaction* as the error term (denominator) for the fixed factor's F-test. Effect sizes were calculated for F-test: Omega-squared (Ω^2) was used for the fixed effect of the system, and rho (ρ) was used for the random effect of flow rate as was the interaction effect. In case of significant interactions, Tukey and Bonferroni post-hoc tests were applied.

Results

Exploratory and Descriptive Statistics

Descriptive statistics were performed on VO_2 , VCO_2 , and RER (Table 1). Levene's test for testing homogeneity of variance (VO_2 , VCO_2) for PBRs was significant. Homogeneity of variance between levels of PBR was violated for all outcome variables for all systems. However, F-statistics are robust when there are no equal variances (Field 2015), especially in a balanced design. A test of normality (Kolmogorov-Smirnov) was performed within PBRs. The assumption of normality was not met for all data. Within overall PBRs (regardless of system), normality was only met for the 200 ml min^{-1} condition for both VO_2 and VCO_2 . When normality was examined by system, assumptions of normality were met for both VO_2 and VCO_2 for every PBR.

Validation of Sable mass flow generator

Simple linear regression analyses were conducted to assess the linear relationship between N_2 flow rates and actual experimental VO_2 (mL min^{-1}) for the Sable system. Results showed a strong linear relationship between the actual experimental VO_2 and the N_2 flow rates ($R_{\text{adj}}^2 = 0.996$; $\beta = 0.998$; 95% CI (0.174-0.183); $p < 0.001$).

Effect of flow rate on respirometry outcomes

A series of 15 one-way ANOVAs [2 FR (55 L min^{-1} , 75 L min^{-1} for Sable and Moxus, 20 L min^{-1} , 40 L min^{-1} , for Jaeger) X 5 PBRs (200, 300, 400, 500, 600 mL min^{-1})] revealed no significant effect of FR on VO_2 and VCO_2 outcomes for the Sable, Moxus, and Jaeger IC systems. Accordingly, data was pooled for each PBR (i.e., FR as a variable was ignored). The average of the six experimental trials per PBR is shown in Table 1.

Insert table 1 about here

Linear relationship of VO_2 and VCO_2 by PBR per system

A linear regression analysis was run to assess the linearity between the VO_2 , VCO_2 , and the PBR through the determination of linear regression equations ($y = b_0 + b_x + \epsilon$) for each system. Table 2 shows that for the Sable system, PBR explains 99.6 % of the variability in VO_2 and VCO_2 ($R^2=0.996$), while it explains 99.2% and 99.4% of the variability in VO_2 and VCO_2 , respectively, for the Moxus. However, the Jaeger system had the worst linear scores compared to the other

two systems (94.8%, and 94.2 %, for VO_2 and VCO_2 , respectively). Furthermore, the mean values of VO_2 and VCO_2 were lowest for the 200 ml min^{-1} condition and increased as PBR increased for the three systems (Figure 2).

Insert table 2 and Figure 2 about here

Assessing error of VO_2 , VCO_2 , and RER for each system

To assess the relationship between the error in the system (VO_2 , VCO_2 , and RER) and the PBR, Bland-Altman plots were created and were followed by linear regression analysis for each system. As shown in Table 3, there were weak, moderate, and strong linear relationships between the VO_2 , VCO_2 errors, and the PBR for the Sable, Moxus, and Jaeger systems, respectively. Also, VO_2 and VCO_2 errors of the Sable system had a non-significant p -value, which indicates that the Sable system had the lowest error in both volumes compared to the other two systems. However, although p -values were significant for both Moxus and Jaeger systems, the VO_2 and VCO_2 errors of the Moxus system had a weaker relationship with PBR and, therefore, lower error than the Jaeger system. The Jaeger system had the highest error among the three systems.

Insert Table 3 about here

A two-factor [3 (IC) \times 5 (PBR's)] ANOVA was conducted to evaluate the effects of the three systems and the five PBR's on VO_2 , VCO_2 , and RER error. For VO_2 the results indicate a significant interaction between system and propane burn rate ($F_{(8,75)} = 3.328$, $p = 0.0026$). Approximately 26.6% ($\rho = 0.266$) of the variance in VO_2 error is accounted for by the interaction factor. The results show a non-significant main effect of propane burn rate on VO_2 error ($F_{(4,75)} = 1.0714$, $p = 0.3767$), and it accounts for only 0.2% ($\rho = 0.00286$) of the variability in VO_2 error. The main fixed effect of system was found to be significant ($F_{(2,8)} = 67.028$, $p < 0.001$). All else held constant, the fixed main effect of system accounts for approximately 83% ($\Omega^2 = 0.8293$) of the variability in VO_2 . The Jaeger system had significantly ($p < 0.001$) greater VO_2 error ($M = -0.057$, $SE = 0.004$) compared to either the Sable ($M = 0.044$, $SE = 0.004$) or Moxus ($M = 0.046$, $SE = 0.004$) systems. There were no significant differences between Sable or Moxus systems on the above-mentioned variables (Figure 3).

Insert Figure 3 about here

The results for $\dot{V}\text{CO}_2$ indicate a significant interaction between systems and PBR ($F_{(8,75)} = 10.722, p < 0.001$). Approximately 54% ($\rho = 0.539$) of the variance in $\dot{V}\text{CO}_2$ is accounted for by the interaction factor. The results show a significant main effect of PBR on $\dot{V}\text{CO}_2$ ($F_{(4,75)} = 9.375, p < 0.001$) and it accounts for 14.8% ($\rho = 0.148$) of the variability in $\dot{V}\text{CO}_2$. The main fixed effect of system is also significant ($F_{(2,8)} = 34.966, p < 0.001$). All else held constant, the fixed main effect of system accounts for approximately 89% ($\Omega^2 = 0.8947$) of the variability in $\dot{V}\text{CO}_2$. The Jaeger system had significantly ($p < 0.001$) greater $\dot{V}\text{CO}_2$ error ($M = -0.048, SE = 0.002$) compared to either the Sable ($M = 0.024, SE = 0.002$) or Moxus ($M = 0.025, SE = 0.002$) systems. There were no significant differences between Sable and Moxus systems on the above-mentioned variable (Figure 3).

The results for RER indicate a significant interaction between system and PBR ($F_{(8,75)} = 3.332, p = 0.003$). Approximately 20% ($\rho = 0.2044$) of the variance in RER is accounted for by the interaction factor. The results show a significant main effect of PBR on RER ($F_{(4,75)} = 7.8125, p < 0.001$) and it accounts for 21.8% ($\rho = 0.2184$) of the variability in RER. The main fixed effect of system is also significant ($F_{(2,8)} = 4.993, p = 0.039$). All else held constant, the fixed main effect of system accounts for approximately 23.8% ($\Omega^2 = 0.2381$) of the variability in RER. The Jaeger system had significantly ($p < 0.001$) greater RER error ($M = -0.028, SE = 0.003$) compared to either the Sable ($M = -0.005, SE = 0.003$) or Moxus ($M = -0.005, SE = 0.003$) systems. There were no significant differences between Sable and Moxus systems on the above-mentioned variable (Figure 3).

Discussion

Laboratories using IC routinely implement propane gas validation techniques (Melanson et al. 2010, White et al. 1996). However, procedures are rarely performed to assess both the accuracy and the linearity of individual systems. We, therefore, built a device that enabled the manipulation of PBR during flow-through respirometry measurements. The custom-built device was used to evaluate the accuracy and linearity of IC systems readily available in our exercise physiology laboratory. Also, the multiple PBR procedure was implemented at two flow rates with each IC system (55 L min⁻¹, 75 L min⁻¹ for Sable and Moxus, 20 L min⁻¹, 40 L min⁻¹, for Jaeger) to investigate the effect of flow rate on $\dot{V}\text{O}_2$ and $\dot{V}\text{CO}_2$ measurements. The primary

outcome of the current study revealed that the multiple PBR procedure agreed with the stoichiometric theoretical values (Table 2), and strong linear responses were observed, suggesting that the technique could be used to evaluate the accuracy and linearity of IC systems. Further, burning propane gas at rates within the range of whole-body energy metabolism in human subjects at rest and during light physical activity revealed differences in accuracy and linearity between IC systems.

Accuracy and linearity of the indirect calorimetry systems

The accuracy of the IC system typically refers to the closeness between the measured value and the “true” value (theoretical stoichiometry value). In contrast, linearity refers to systematic and random errors (Cooper and Storer 2001). Regression analyses and ANOVA were performed to determine the accuracy and linearity of the three IC systems on VO_2 , VCO_2 , and RER. The ventilation rates were pooled because statistical outcomes showed that the two ventilation rates at the studied PBRs did not alter the VO_2 and VCO_2 . As shown in Table 1, the mean difference between experimental and theoretical values of the Sable and Moxus systems overestimated VO_2 , and the mean differences were stable across the 5 PBRs. On the contrary, the Jaeger system underestimated VO_2 , and the mean differences increased with progressing PBR. The multiple PBR procedure demonstrated a high consistency for RER values for both Sable and Moxus systems. Our technical report showed that both Sable and Moxus systems responded similarly to propane gas combustion. However, it is important to note that the Moxus O_2 and CO_2 analyzers were incorporated into the Sable Classic Line technologies. Accordingly, further studies are needed using the complete Moxus Modular Metabolic System before making comparisons between the two IC systems. Special consideration should be given to the technologies used to measure FR during flow-through respirometry. The Sable system incorporates a mass flow meter, which is not affected by fluctuations in temperature and pressure (Lighton 2008). However, systems that integrate volumetric flow meters need to correct for changes in temperature and pressure (Lighton 2008). The increased discrepancy between experimental and theoretical values observed with the Jaeger system at increasing PBR may reflect a lack of appropriate correction for temperature changes.

The regression analysis of PBR vs. experimental values revealed a robust linear relationship for the three systems, meaning that both $\dot{V}O_2$ and $\dot{V}CO_2$ increased with propane gas combustion (Table 2). However, when linear regression was performed on the $\dot{V}O_2$ and $\dot{V}CO_2$ errors (difference), the Sable system provided the most accurate measurements evidenced by the least error values (i.e., R_{adj}^2 was the least with a non-significant p values ($p = 0.37$, $p = 0.13$) for $\dot{V}O_2$ and $\dot{V}CO_2$, respectively).

The Sable and Moxus systems showed no change in mean difference for $\dot{V}O_2$, $\dot{V}CO_2$, and RER throughout progressive PBRs (Figure 3), indicating more stable and reliable metabolic outcomes than the Jaeger system. The observed mean differences between analyzers could stem from the type of O_2 analyzer (sensor) implemented in these systems. As time elapses, the fuel-cell oxygen sensor becomes noisy, unstable, and unreliable, an issue not always addressed by the manufacturer's conventional medical gas calibration procedures. This is particularly true for fuel cells with faster response times but shorter lifespans. Conversely, paramagnetic (Sable System) and zirconia (Moxus) oxygen analyzers do not degrade over time if well maintained. Therefore, one cannot discard the temperature effect to account for the difference in O_2 response. The paramagnetic oxygen analyzer has a temperature compensation circuitry that efficiently reduces the impact of temperature fluctuations. In contrast, the zirconia-cell oxygen analyzer does not fluctuate with temperature change owing to its high temperature operating capability. However, a sudden shift in temperature or a high operating temperature may induce significant drift in the fuel-cell O_2 analyzer (Lighton 2008), which the thermal compensation array may not correct. On the other hand, the CO_2 analyzers offer far more stable readings with little to no drift. Accordingly, the observed discrepancy between experimental and theoretical values for both $\dot{V}O_2$ and $\dot{V}CO_2$ with increasing PBR (Figure 3-B) suggests that the effects of temperature on flow rate may explain the poor performance of the Jaeger system compared to the other two IC systems.

Reliability of the indirect calorimetry systems

Reliability refers to the reproducibility or repeatability of the readings of the gas analyzer under identical conditions (Cooper and Storer 2001). The reliability of each IC system was determined by calculating the coefficient of variation (CV) of $\dot{V}O_2$ and $\dot{V}CO_2$. Our results showed that CV

values of VO_2 and VCO_2 ranged from 1% to 5% and from 1% to 4% for the Sable and Moxus systems, respectively. On the other hand, the Jaeger system had CV ranging from 7% to 10% for VO_2 and VCO_2 , respectively. Our data indicate that the Sable and Moxus systems provided more reliable measures of VO_2 and VCO_2 compared to the Jaeger system.

Propane gas technique compared to other techniques

The present study was conducted to validate the outcomes of IC systems using commercially available gas mass flow devices, and as such, it represents a novel approach in comparison to techniques/procedures routinely performed in other human physiology laboratories. For example, Melanson et al. (2010) conducted propane gas combustion tests to validate the outcomes of their whole room IC system, which integrated similar Sable System technologies (the O_2 analyzer incorporated a fuel cell rather than paramagnetic). The Sable system provided more than 98% of the expected recovery of VO_2 and VCO_2 during the propane combustion trials. In addition to validation through propane combustion tests, the authors also investigated the system's ability to detect known changes in energy metabolism in humans transitioning from rest to light exercise, and then to more moderate intensity exercise. Again, the whole room IC system performed as anticipated. However, in the latter experiment, the expected accuracy of the measurements taken at different metabolic rates is dependent on the systems linearity. Accordingly, performing the propane combustion test at multiple PBRs, as outlined in the current study, would strengthen the interpretation of these outcomes.

In a recent study, Rising et al. (2015) used propane gas combustion to determine the accuracy of another whole room Sable metabolic system. The IC system was subjected to multiple ($n=10$) propane (99.5% purity) combustion tests to simulate 24-hour metabolic measurements. The burn rate (0.15 ± 0.025 g/min) was determined by obtaining the weight before and after completion of each combustion test using a calibrated analytical balance. Although within acceptable and non-statistically different limits, the Sable system was observed to under report mean VO_2 values when comparing the outcomes of combustion to that of propane stoichiometry (Rising et al. 2015). In the current study, mean experimental values for VO_2 were higher than the stoichiometry theoretical value at the five PBRs tested. Slight discrepancies between studies could be explained by differences in oxygen sensor technology (i.e., fuel cell vs. paramagnetic),

indirect calorimetry method (i.e., ventilated hood vs. whole room) and validation procedure. The current multiple burn rate procedure adds to previously implemented propane combustion validation techniques by enabling the assessment of system accuracy and linearity within a single session. Furthermore, assessment of the accuracy and linearity of metabolic outcomes could allow for the correction of systematic error, which will be the focus of future work.

Other commonly used techniques to calibrate IC systems include alcohol combustion and butane gas burning. The two methods bear on stoichiometry calculations similar to that for the combustion of propane gas (i.e., O_2 is consumed, and CO_2 and water are produced) (Toien 2013). For instance, Marks et al. (1987) calculated VO_2 and VCO_2 after burning known masses of ethanol and methanol gases (pure alcohol) in an open-circuit IC system. The authors reported that gas volumes differed by less than 5% from their theoretical values, confirming alcohol combustion as a valid technique for calibrating IC systems in neonates. Furthermore, Miodownik et al. (1998) described a methanol-burning lung model, which reported less than 0.005% reading error attributed to carbon monoxide gas production. Finally, Nunn, Makita, and Royston (1989) showed that a known amount of butane gas burned in a closed-circuit IC system yielded, for one mole of butane, 6.5 moles of O_2 , and an RER of 0.61, providing a simple and robust technique to test IC system performance. However, although all these procedures produced good outcomes, they are not routinely implemented in a manner to evaluate the linearity of IC systems. quickly and efficiently. Therefore, the use of gas mass flow meter technology to monitor PBR represents a more comprehensive procedure that will enhance the validation IC outcomes under a variety experimental condition. In fact, Perez-Suarez et al. (2018) published a quality control study in which they implemented the proposed PBR method based on our approach (Ismail 2017).

Conclusion

This work aimed to refine the propane gas validation technique. We had no intent to compare indirect calorimetry systems to promote one over the others. Each system was built for specific applications and, as such, differed from each other. The current technical report describes a complimentary propane gas validation procedure to assess the accuracy and linearity of indirect calorimetry. The IC systems output must yield an accurate fraction of gases for the computation of VO_2 and VCO_2 and energy production in medicine, nutrition, and exercise sciences.

Generally, companies manufacturing indirect calorimetry systems provide customers with calibration procedures to address accuracy issues. However, to ascertain the quality of data acquisition, IC's accuracy and linear response should be validated regularly. We recommend using the described multiple propane burn rate validation procedure to assess the accuracy and linearity of IC systems.

Acknowledgments

The work was supported by an internal grant from the School of Human Kinetics and Recreation, Memorial University, St. John's, NL, Canada.

10. Declaration of interest

The authors report no declarations of interest.

References

- Brooks, George A., Thomas D. Fahey, and Kenneth M. Baldwin. 2005. *Exercise physiology : human bioenergetics and its applications*. 4th ed. Boston: McGraw-Hill.
- Cooper, Christopher B., and Thomas W. Storer. 2001. *Exercise testing and interpretation : a practical approach*. Cambridge, U.K. ; New York, NY, USA: Cambridge University Press.
- Fedak, M. A., L. Rome, and H. J. Seeherman. 1981. "One-step N2-dilution technique for calibrating open-circuit VO2 measuring systems." *J Appl Physiol Respir Environ Exerc Physiol* 51 (3):772-6. doi: 10.1152/jappl.1981.51.3.772.
- Ferrannini, E. 1988. "The theoretical bases of indirect calorimetry: a review." *Metabolism* 37 (3):287-301. doi: 10.1016/0026-0495(88)90110-2.
- Field, A.P. 2015. *Discovering Statistics Using IBM SPSS Statistics: And Sex and Drugs and Rock 'n' Roll*: SAGE Publications, Limited.
- Haugen, H. A., L. N. Chan, and F. Li. 2007. "Indirect calorimetry: a practical guide for clinicians." *Nutr Clin Pract* 22 (4):377-88. doi: 10.1177/0115426507022004377.
- Ismail, M.A. 2017. "Validation of a propane gas calibration device for indirect calorimetric systems." Master of Science School of Human Kinetics and Recreation, Memorial University of Newfoundland (12848).
- Jequier, E., and J. P. Felber. 1987. "Indirect calorimetry." *Baillieres Clin Endocrinol Metab* 1 (4):911-35. doi: 10.1016/s0950-351x(87)80011-3.
- Leonard, W. R. 2012. "Laboratory and field methods for measuring human energy expenditure." *Am J Hum Biol* 24 (3):372-84. doi: 10.1002/ajhb.22260.
- Levine, J. A., N. L. Eberhardt, and M. D. Jensen. 1999. "Role of nonexercise activity thermogenesis in resistance to fat gain in humans." *Science* 283 (5399):212-4. doi: 10.1126/science.283.5399.212.
- Lighton, John R. B. 2008. *Measuring metabolic rates : a manual for scientists*. Oxford ; New York: Oxford University Press.
- Marks, K. H., P. Coen, J. R. Kerrigan, N. A. Francalancia, E. E. Nardis, and M. T. Snider. 1987. "The Accuracy and Precision of an Open-Circuit System to Measure Oxygen-Consumption and Carbon-Dioxide Production in Neonates." *Pediatric Research* 21 (1):58-65. doi: Doi 10.1203/00006450-198701000-00014.
- Matarese, L. E. 1997. "Indirect calorimetry: Technical aspects (Reprinted from Support Line, vol 14, pg 6-12, 1997)." *Journal of the American Dietetic Association* 97 (10):S154-S160. doi: Doi 10.1016/S0002-8223(97)00754-2.
- Melanson, E. L., J. P. Ingebrigtsen, A. Bergouignan, K. Ohkawara, W. M. Kohrt, and J. R. B. Lighton. 2010. "A new approach for flow-through respirometry measurements in humans." *American Journal of Physiology-Regulatory Integrative and Comparative Physiology* 298 (6):R1571-R1579. doi: 10.1152/ajpregu.00055.2010.
- Miodownik, S., J. Melendez, V. A. Carlon, and B. Burda. 1998. "Quantitative methanol-burning lung model for validating gas-exchange measurements over wide ranges of FIO2." *Journal of Applied Physiology* 84 (6):2177-2182. doi: DOI 10.1152/jappl.1998.84.6.2177.
- Neter, John, Michael H Kutner, Christopher J Nachtsheim, and William Wasserman. 1996. "Applied linear statistical models."

Nunn, J. F., K. Makita, and B. Royston. 1989. "Validation of Oxygen-Consumption Measurements during Artificial-Ventilation." *Journal of Applied Physiology* 67 (5):2129-2134. doi: DOI 10.1152/jappl.1989.67.5.2129.

Perez-Suarez, I., M. Martin-Rincon, J. J. Gonzalez-Henriquez, C. Fezzardi, S. Perez-Regalado, V. Galvan-Alvarez, J. W. Juan-Habib, D. Morales-Alamo, and J. A. L. Calbet. 2018. "Accuracy and Precision of the COSMED K5 Portable Analyser." *Frontiers in Physiology* 9. doi: ARTN 1764 10.3389/fphys.2018.01764.

Rising, R., K. Whyte, J. Albu, and X. Pi-Sunyer. 2015. "Evaluation of a new whole room indirect calorimeter specific for measurement of resting metabolic rate." *Nutrition & Metabolism* 12. doi: ARTN 46 10.1186/s12986-015-0043-0.

Toien, O. 2013. "Automated open flow respirometry in continuous and long-term measurements: design and principles." *Journal of Applied Physiology* 114 (8):1094-1107. doi: 10.1152/japplphysiol.01494.2012.

White, M. D., G. Bouchard, B. Buemann, N. Almeras, J. P. Despres, C. Bouchard, and A. Tremblay. 1996. "Reproducibility of 24-h energy expenditure and macronutrient oxidation rates in an indirect calorimeter." *Journal of Applied Physiology* 80 (1):133-139. doi: DOI 10.1152/jappl.1996.80.1.133.

Figure 1

Table 1

Descriptive statistics of the Sable, Moxus, and Jaeger metabolic carts including the SD, SE, CV of mean $\dot{V}O_2$ (ml min⁻¹), $\dot{V}CO_2$ (ml min⁻¹), and RER.

System	PBR	$\dot{V}O_2$ (ml•min ⁻¹)					$\dot{V}CO_2$ (ml•min ⁻¹)					RER				
		Mean	SD	SE	CV	Mean difference	Mean	SD	SE	CV	Mean difference	Mean	SD	SE	CV	Mean difference
Sable	200	263	14.0	5.7	0.05	-48	158	7.9	3.2	0.05	-29	0.60	0.01	0.00	0.02	0.00
	300	363	6.9	2.8	0.02	-40	215	4.5	1.8	0.02	-21	0.59	0.01	0.00	0.02	0.01
	400	478	5.8	2.4	0.01	-48	284	5.0	2.0	0.02	-26	0.59	0.01	0.00	0.02	0.01
	500	585	12.6	5.1	0.02	-47	346	6.4	2.6	0.02	-23	0.59	0.01	0.00	0.02	0.01
	600	685	9.0	3.7	0.01	-39	409	4.9	2.0	0.01	-22	0.59	0.01	0.00	0.02	0.01
Moxus	200	245	5.8	2.4	0.02	-30	148	3.7	1.5	0.03	-19	0.60	0.02	0.01	0.03	0.00
	300	368	4.2	1.7	0.01	-45	217	3.8	1.6	0.02	-23	0.59	0.01	0.00	0.02	0.01
	400	486	14.6	6.0	0.03	-56	288	8.8	3.6	0.03	-30	0.59	0.01	0.01	0.02	0.01
	500	583	21.8	8.9	0.04	-45	346	11.5	4.7	0.03	-23	0.59	0.02	0.01	0.03	0.01
	600	700	12.6	5.1	0.02	-54	418	6.0	2.5	0.01	-31	0.59	0.01	0.00	0.02	0.00
Jaeger	200	187	19.4	8.0	0.1	28	114	8.2	3.3	0.07	15	0.61	0.05	0.02	0.08	-0.01
	300	281	26.5	10.8	0.1	43	163	11.9	4.9	0.07	31	0.58	0.03	0.01	0.05	0.02
	400	368	40.6	16.6	0.1	62	208	20.1	8.2	0.1	50	0.56	0.01	0.01	0.02	0.03
	500	474	31.9	13.0	0.07	64	262	17.7	7.2	0.07	61	0.55	0.01	0.00	0.02	0.04
	600	560	42.2	17.2	0.08	86	307	26.8	11.0	0.09	80	0.57	0.01	0.01	0.02	0.05

PBR: propane gas burn rate, $\dot{V}O_2$: volume of oxygen, $\dot{V}CO_2$: volume of carbon dioxide, SD: standard deviation, SE: standard error. CV: coefficient of variance, RER: respiratory exchange ratio

Figure 2

Table 2

Linearity analysis of the Sable, Moxus, and Jaeger metabolic carts including Beta, R^2 , Confidence Interval (CI), and p-value of $\dot{V}O_2$ (ml min⁻¹) and $\dot{V}CO_2$ (ml min⁻¹) errors.

System	$\dot{V}O_2$ (ml•min ⁻¹) Error				$\dot{V}CO_2$ (ml•min ⁻¹) Error			
	β	R^2	95 % CI	p-value	β	R^2	95 % CI	p-value
Sable	0.998	0.996	(0.001, 0.001)	0.001	0.998	0.996	(0.001,0.001)	0.001
Moxus	0.996	0.992	(0.001, 0.001)	0.001	0.997	0.994	(0.001,0.001)	0.001
Jaeger	0.974	0.948	(0.001, 0.001)	0.001	0.944	0.942	(0.00, 0.001)	0.001

$\dot{V}O_2$: volume of oxygen per minute, $\dot{V}CO_2$: volume of carbon dioxide per minute

Figure 3

Table 3

Regression analysis of $\dot{V}O_2$ (ml min⁻¹), $\dot{V}CO_2$ (ml min⁻¹), and RER errors by propane flow levels which followed the Bland-Altman plots for each metabolic cart (Sable, Moxus, Jaeger).

System	$\dot{V}O_2$ (ml•min ⁻¹) Error				$\dot{V}CO_2$ (ml•min ⁻¹) Error				RER Error			
	β	SE	R_{adj}^2	t-value (p-value)	β	SE	R_{adj}^2	t-value (p-value)	β	SE	R_{adj}^2	t-value (p-value)
Sable	-0.168	0.000	-0.006	-0.903 (0.37)	-0.281	0.000	0.046	-1.552 (0.13)	-0.379	0.000	0.134	-3.848 (0.001)
Moxus	0.438	0.000	0.163	2.575 (0.02)	0.425	0.000	0.151	2.484 (0.02)	-0.162	0.000	-0.009	0.869 (0.4)
Jaeger	-0.536	0.000	0.262	-3.363 (0.002)	-0.807	0.000	0.639	-7.227 (0.001)	-0.679	0.000	0.441	-4.891 (0.001)

$\dot{V}O_2$: volume of oxygen per minute, $\dot{V}CO_2$: volume of carbon dioxide per minute, SE: standard error, RER: respiratory exchange ratio

Figure 4

Figure 1

Schematic representation of the in-house built propane gas device utilized to assess the accuracy and linearity of indirect calorimetry systems. The propane gas device encompasses a tank of chemically pure propane gas with a two-stage Western Medical gas regulator and its gas hose connected to a one-way gas mass-flow transducer subsequently connected to a gas mass-flow controller, and to a Bunsen burner. The burner is located into a 2.4 L glass canopy that flows into a 0.4 L glass tubing. From there, the entire system is connected to IC by a 1.4-inch diameter hose.

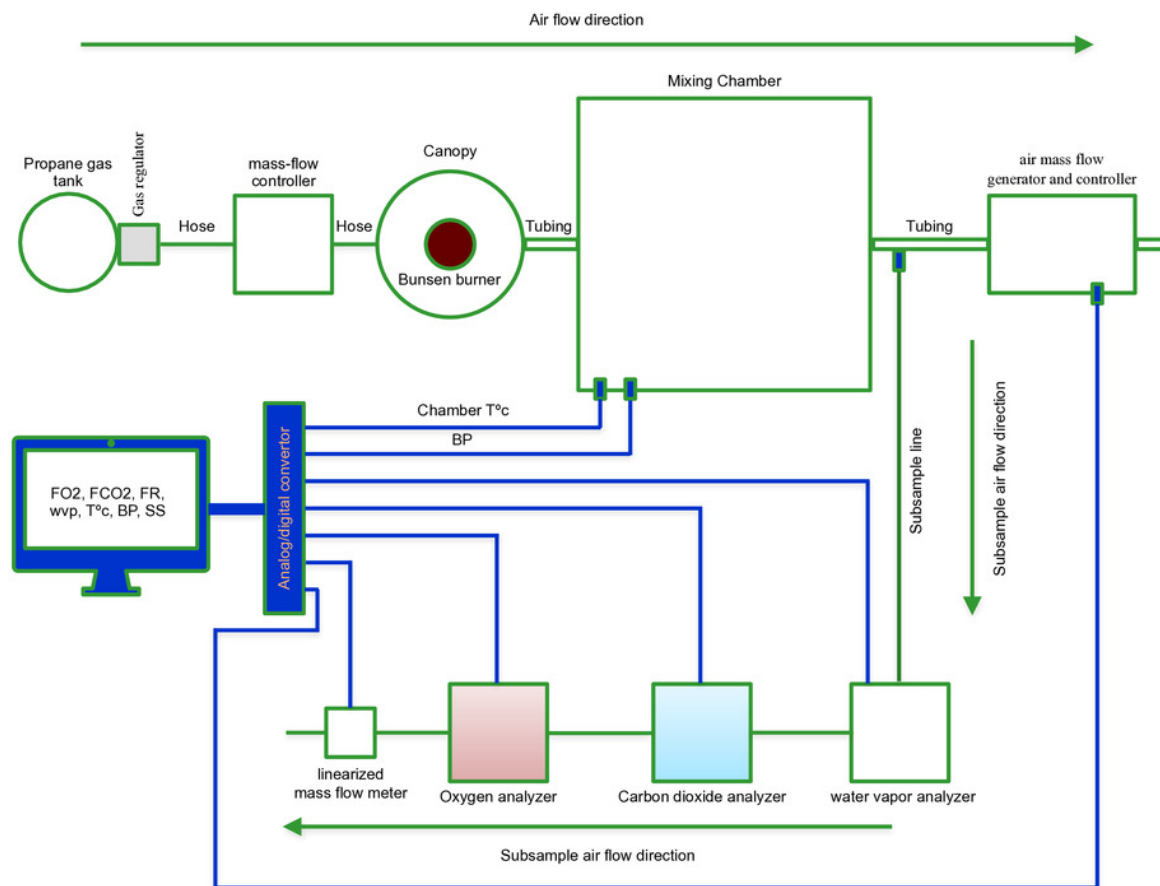


Figure 5

Figure 2

Mean rates of oxygen uptake ($\dot{V}O_2$, L min⁻¹; A), carbon dioxide production ($\dot{V}CO_2$, L min⁻¹; B), and respiratory exchange ratio (RER; C) measured during propane gas combustion tests with three metabolic carts: Sable system (dashed line), Moxus system (solid line), and Jaeger system (dotted line). Values are means SD.

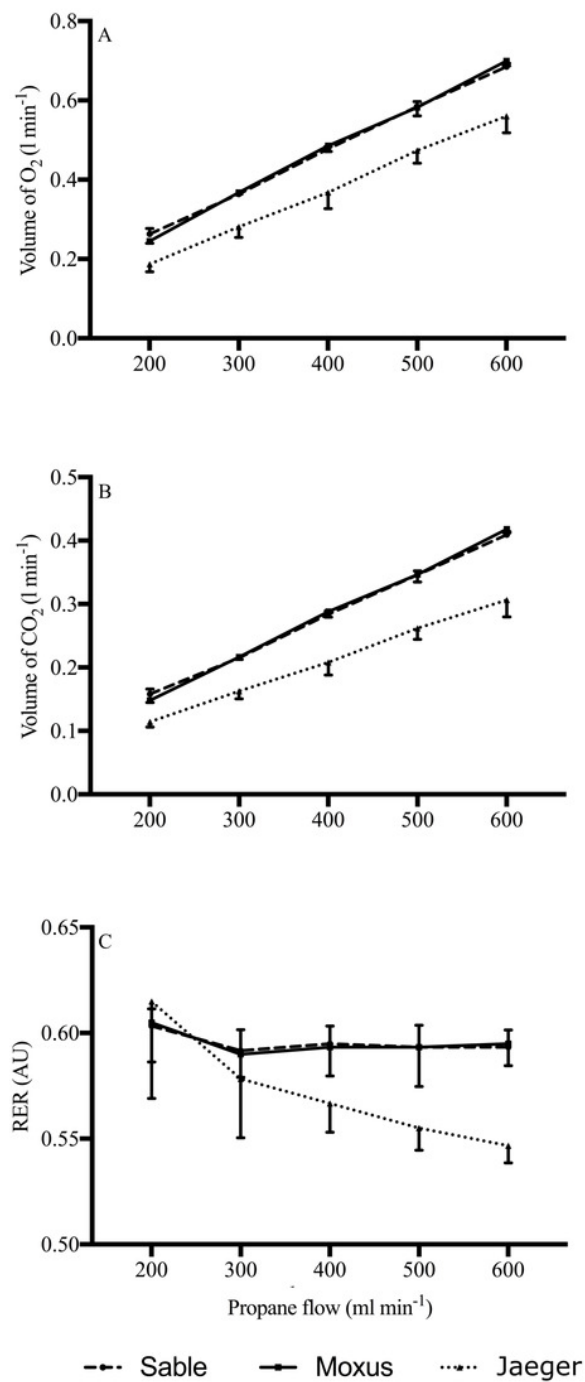


Figure 6

Figure 3

Mean difference (delta) between the stoichiometric theoretical values and the actual experimental values of oxygen uptake ($\dot{V}O_2$, L min⁻¹; A), carbon dioxide production ($\dot{V}CO_2$, L min⁻¹; B) and respiratory exchange ratio (RER; C) measured during propane gas combustion tests with three indirect calorimetric systems: Sable system (dashed line), Moxus system (solid line), and Jaeger system (dotted line). Values are means

